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## **Title**

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# **Journal**

Scientific Reports, 9(1)

# **Authors**

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# **Publication Date**

2019-04-04

## **DOI**

10.1038/s41598-019-42093-1

Peer reviewed

# SCIENTIFIC REPERTS

Received: 4 September 2018 Accepted: 21 March 2019 Published online: 04 April 2019

# **Controlling the transverse proton OPENrelaxivity of magnetic graphene oxide**

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**The engineering of materials with controlled magnetic properties by means other than a magnetic feld is of great interest in nanotechnology. In this study, we report engineered magnetic graphene oxide (MGO) in the nanocomposite form of iron oxide nanoparticles (IO)-graphene oxide (GO) with**  tunable core magnetism and magnetic resonance transverse relaxivity (r<sub>2</sub>). These tunable properties are obtained by varying the IO content on GO. The MGO series exhibits r<sub>2</sub> values analogous to those **observed in conventional single core and cluster forms of IO in diferent size regimes—motional averaging regime (MAR), static dephasing regime (SDR), and echo-limiting regime (ELR) or slow motion regime (SMR). The maximum r2 of 162±5.703mM<sup>−</sup><sup>1</sup>s<sup>−</sup>1 is attained for MGO with 28 weight percent (wt%) content of IO on GO and hydrodynamic diameter of 414 nm, which is associated with the SDR.These fndings demonstrate the clear potential of magnetic graphene oxide for magnetic resonance imaging (MRI) applications.**

Magnetic materials such as superparamagnetic iron oxide nanoparticles (IO) have attracted mounting interest for a wide range of applications in nanomedicine $^{1-4}$  $^{1-4}$  $^{1-4}$ , magneto-mechanical actuation $^5$  $^5$ , energy storage $^{6-8}$  $^{6-8}$  $^{6-8}$ , optoelec-tronics<sup>9[,10](#page-9-6)</sup>, and environmental remediation<sup>[11](#page-9-7)–15</sup> due to their biocompatibility, hydrophilicity, distinct morphology, and unique magnetic and electric properties. In medical diagnostics, the MRI applications of such materials are of paramount interest, and they are widely used as MRI negative contrast agents  $(CAs)^{16,17}$  due to their hallmark characteristics of spin-spin or transverse relaxation enhancement.

In pursuit of high-performance MRI CAs, the surface modifcation of IO is mostly executed in the form of core-shell<sup>[18,](#page-9-11)19</sup> and Janus structure<sup>20</sup> using polymer stabilizers along with their controlled shape and size. In addition, with the advances in the research of graphene-based materials, GO has been utilized for surface modi-fication of IO owing to its oxygenated functionalities, i.e., epoxide, hydroxyl, carbonyl, and carboxyl moieties<sup>21,[22](#page-10-3)</sup> and biocompatibility<sup>23,24</sup>. These functionalities can serve as the conjugation sites for IO to form GO-based nanocomposites, and in particular, magnetic graphene oxide (MGO). Recently, IO/GO-based nanocomposites have been proposed as  $T_1^{25}$  $T_1^{25}$  $T_1^{25}$  and  $T_2$  CAs<sup>4,[26](#page-10-7),27</sup> for MRI. However, no systematic studies on the tunable magnetic behavior and magnetic resonance (MR) relaxivity of such materials have been reported, and its corresponding size regime correlation remains unsettled.

Some groups have recently explored the tunability of magnetic resonance transverse relaxivity  $(r_2)$  in single core or cluster forms of IO in the PEGylated core-shell nanostructures. The distinct  $r_2$  values of IO with size range ~5–14 nm were reported via optimization of the coating thickness using PEG with molecular weights of 550, 750, 1000, 2000 and 5000 Da<sup>28</sup>. Similarly, the PEGylated raspberry-like nanoclusters of superparamagnetic IO nanocrystals with a diameter range of 30 to 200 nm were reported with distinct  $r_2$  values associated with three size

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<span id="page-2-0"></span>**Figure 1.** (a) Thermogravimetric analysis (TGA) profile. (b) A plot of calculated iron ('Fe') concentrations from TGA and observed from inductively coupled plasma optical emission spectrometry (ICP-OES). (**c**) Te calibration linear ft of the standard solutions from ICP-OES. (**d**) Intensity and concentration plot obtained from ICP-OES.

regimes–motional averaging regime (MAR), static dephasing regime (SDR), and echo-limiting regime (ELR) or slow motion regime (SMR)<sup>[29](#page-10-10)</sup>, as defined by outer sphere relaxation theory<sup>[30,](#page-10-11)31</sup>.

In this study, we synthesize a series of MGO with diferent concentration of IO and demonstrate that these MGOs possess such size regimes with distinct  $r_2$  values. We assume that the MGO behaves as a spherical system with a size characterized by its hydrodynamic diameter which can be tuned by changing the concentration of the IO, i.e., the higher the concentration of IO, the larger is the size of MGO, and that the MGO can translationally difuse water molecules on its outer sphere region, makes them experience diverse magnetic feld gradients induced by it, and in turn lead to enhanced r<sub>2</sub>. Based upon this assumption, we present a detailed study on the control of  $r_2$  of MGOs as a function of concentration of IO. Further, we aim at maximizing the transverse relaxivity through diferent MGO size regimes and determining its correlation to that observed in conventional single core and cluster forms of IO. More importantly, we developed an intriguing strategy for the synthesis of magnetic graphene oxide capable of governing the tunable transverse relaxivity, which used to be elusive on such nanocomposite materials.

### **Results and Discussion**

We have synthesized MGO samples (MGOs), namely MGO 1, MGO 2, MGO 3 and MGO 4, with 8, 18, 28 and 32% (w/w) of IO on GO respectively in nanocomposite form (see the Methods section for details). Firstly, we employed thermogravimetric analysis (TGA) for the quantifcation of IO percentages on GO using 7mg of each sample. Fig. [1a](#page-2-0) illustrates the TGA profle for GO, MGO 1, MGO 2, MGO 3 and MGO 4. For all MGO samples,  $\sim$ 7% weight loss was seen in the initial stage below 120 °C which was due to the evaporation of the water molecules adsorbed by GO, whose surface is hydrophilic<sup>32</sup>. However, GO showed the prompt weight loss of 13% at this temperature due to the absence of IO. In the next stage, the weight loss was more rapid below 226 °C which is attributed to the pyrolysis and thermal decomposition of oxygen functionalities including −OH, −COOH and  $-$ COOR, to produce H<sub>2</sub>O, CO, and CO<sub>2</sub><sup>[33](#page-10-14)</sup>. In this stage, the presence of diverse percentages of IO on GO in different samples can be perceived with the distinct split of TGA curves. The respective mass losses for the MGOs are noted to be 35%, 26%, 22%, and 20%. The weight loss between 450 °C to 600 °C was due to combustion of the carbon skeleton. 25% of the carbon content was left after heating to 800 °C, and the magnetite (Fe<sub>3</sub>O<sub>4</sub>) was com-pletely oxidized to hematite (Fe<sub>2</sub>O<sub>3</sub>) at this temperature<sup>[34](#page-10-15)</sup>. Based on these observations, the respective IO content in the MGOs was determined to be 10%, 20%, 27% and 32% (w/w) respectively. Using the TGA technique, the iron oxide content in the iron oxide-graphene composite<sup>[35](#page-10-16)</sup> and iron oxide-nitrogen doped reduced graphene oxide was determined previously and was consistent with those calculated from the synthesis.

The ICP-OES technique was used to determine the 'Fe' concentrations in MGOs for the confirmation of IO content in the MGOs. The data of calculated 'Fe' concentrations based upon the wt% of IO observed from TGA,



<span id="page-3-0"></span>**Figure 2.** FE-SEM image of (**a**) as-synthesized GO. TEM images of (**b**) as-synthesized GO; (**c**) MGO 1 (8% IO@ GO), inset top right: selected area electron difraction (SAED) pattern of IO, inset bottom right: HR-TEM image showing lattice fringes of (220) plane of magnetite (Fe<sub>3</sub>O<sub>4</sub>) phase; (**d**) MGO 2 (18% IO@GO); (**e**) MGO 3 (28% IO@GO); and (**f**) MGO 4 (32% IO@GO). Inset of Fig. [2d,e](#page-3-0) corresponds to the size distribution profle of IO particles alone.

and the experimentally observed 'Fe' concentrations from ICP-OES are tabulated in Table S1 in the supporting information (SI). As shown in Fig. [1b,d](#page-2-0), both the calculated and observed 'Fe' concentrations are in reasonable agreement; however, the calculated 'Fe' concentrations in MGO 1 and MGO 2 are marginally higher than that observed from ICP-OES, while it is lower for MGO 3. Based upon these results, we further averaged the values of IO wt% to 8% IO@GO in MGO 1, 18% IO@GO in MGO 2, 28% IO@GO in MGO 3 and 32% IO@GO in MGO 4. The 'Fe' wt% was also quantified by energy-dispersive X-ray (EDX) spectroscopy of MGOs, and the analysis was done on three diferent spots of each MGO (Fig. S1 in SI). It was observed that the MGOs show increasing wt% of IO from MGO 1 to MGO 4 which is consistent with the TGA and ICP-OES measurements.

The morphology and nanostructure of the synthesized GO and MGOs were observed using field emission scanning electron microscopy (FE-SEM) and field emission transmission electron microscopy (FE-TEM). The aggregated but well-exfoliated GO flakes are clearly seen in Fig. [2a,b](#page-3-0) obtained from FE-SEM and FE-TEM respec-tively. The agglomerated quasi-spherical IO, which is the hallmark of the co-precipitation synthesis<sup>[36](#page-10-17)</sup>, decorated on GO are seen in MGO 1, MGO 2, MGO 3 and MGO 4, as depicted in Fig. 2c-f respectively. The inset in Fig. [2c](#page-3-0) shows the high resolution TEM (HR-TEM) image of the IO and shows the polycrystalline nature with an interplanar lattice spacing of 0.299nm corresponding to the characteristic spacing of (220) planes of magnetite  $(Fe_3O_4)^{36,37}$  $(Fe_3O_4)^{36,37}$  $(Fe_3O_4)^{36,37}$  $(Fe_3O_4)^{36,37}$  $(Fe_3O_4)^{36,37}$ . The IO particle size distribution profile (inset in Fig. [2d,e](#page-3-0)) shows their size ranging from 8 to 25 nm, but mostly 14 to 18 nm in size, suggesting the formation of polydisperse nanoparticles. The size was determined using ImageJ sofware [\(https://imagej.nih.gov/ij/\)](https://imagej.nih.gov/ij/).

The crystallinity and phase formation were analyzed using X-ray diffraction (XRD) as shown in Fig. [3a](#page-4-0). The diffraction patterns show the major characteristic peaks corresponding to the magnetite (Fe<sub>3</sub>O<sub>4</sub>) phase and the well-defined peaks indicate the highly crystalline nature of  $IO^{36,37}$  $IO^{36,37}$  $IO^{36,37}$ . The intensity of the diffraction peaks corresponding to GO gradually decreases as the content of IO increases in MGOs suggesting an increased degree of exfoliation of GO (Fig. [3b\)](#page-4-0). The shift of the GO diffraction peak towards lower 2θ values, which is accompanied by decreasing intensity, is consistent with the anticipated increase of the GO interlayer stacking distance in MGOs<sup>[4](#page-9-1)</sup>. The diffraction peak positions observed at 10.14°, 10.34°, 10.11°, 10.02° and 9.93°, correspond to the interlayer stacking distance (d) of 0.970nm, 0.95nm, 0.980nm, 0.981nm and 0.994nm, for GO, MGO 1, MGO 2, MGO 3 and MGO 4, respectively (Fig. [3e\)](#page-4-0).

The characteristic transmittance peaks associated with the major functional groups described in TGA analysis were identifed in ATR-FTIR spectra. According to the ATR-FTIR spectra (Fig. [3c\)](#page-4-0), the corresponding vibrations at the characteristics peaks positions are: 570 cm<sup>-1</sup> (Fe–O vibration), 803 cm<sup>-1</sup> (C–O epoxy stretching



<span id="page-4-0"></span>

vibration), 1069 cm<sup>−1</sup> (C−O alkoxy stretching vibration), 1261 cm<sup>−1</sup> (C−O epoxy stretching vibration), 1381 cm<sup>−1</sup> (O–H bending vibration), 2851 cm<sup>-1</sup> (CH<sub>2</sub> asymmetric vibration), 2923 cm<sup>-1</sup> (CH<sub>2</sub> symmetric vibration), and 3200 cm<sup>-1</sup> − 3700 cm<sup>-1</sup> (O-H stretching vibration and H<sub>2</sub>O molecules). The Fe-O vibrational mode in MGOs experiences a slight blueshift than in IO, which may be ascribed to its partial confinement between GO layers.

The composition and structural change of IO, GO, and MGOs were examined using Raman spectroscopy. The Raman spectrum of bare IO (see Fig. [3d\)](#page-4-0) shows the characteristic peaks of magnetite (Fe<sub>3</sub>O<sub>4</sub>), in agreement with XRD data. However, the spectrum also shows peaks characteristic of maghemite (Fe<sub>2</sub>O<sub>3</sub>) due to the phase change induced by the focused laser irradiation<sup>38</sup> in the Raman microprobe employed for the experiment. The two  $A_{1g}$ vibrational modes observed at 212 cm $^{-1}$  and 494 cm $^{-1}$  and two  $\rm E_g$  vibrational modes observed at 270 cm $^{-1}$  and 590 cm<sup>-1</sup> are associated with the maghemite (Fe<sub>2</sub>O<sub>3</sub>) phase. An E<sub>g</sub> vibrational mode seen at 378 cm<sup>-1</sup> represents the characteristic magnetite (Fe<sub>3</sub>O<sub>4</sub>) phase, which is predominant. A noticeable broad band centered at 1280 cm<sup>-1</sup> (marked by an arrow) is ascribed to the scattering of two magnons resulting from their interaction created on neighboring antiparallel spin sites<sup>[39](#page-10-20)</sup>. The Raman spectra of GO and MGOs show the prevailing peaks corresponding to G and D bands of GO. The G band peak, centered at 1588 cm<sup>-1</sup>, originates from the first order scattering of the  $E_{2g}$  mode at  $\Gamma$ -point or the in plane stretching motion between sp<sup>2</sup> carbon systems. The presence of the D band peak at 1355 cm<sup>-1</sup> is due to the second-order double resonant process between non-equivalent K points in the Brillouin zone of graphene<sup>40,41</sup>. The D-mode arises by disorder due to the edge, structural defects, asymmetric  $sp^2$ -hybridized carbon systems, and hence the D band is known as a disorder band<sup>42</sup>. The presence of IO induces a structural defect to the basal plane of GO resulting in an intensifed D band, and the disorder level in GO can be estimated by the relative intensity of the D and G bands ( $I_D/I_G$ ). The estimated  $I_D/I_G$  value (0.962, 0.998, 1.004, 1.021 and 1.016 for GO, MGO 1, MGO 2, MGO 3 and MGO 4, respectively) increases with the IO content in MGOs, which is consistent with the TGA analysis. Te prevailing peaks of GO over IO in MGOs are evident of higher GO content in the composite systems.

X-ray photoelectron spectroscopy (XPS) was employed to study the interactions between IO and GO in MGOs and determine their chemical composition and phases. As observed in Fig. [4a,](#page-5-0) the survey spectra depict prominent peaks at ~284 and 531eV associated with C 1s and O 1s in GO, which also co-exist in the spectra of IO and MGOs together with Fe 2p peaks between 709 and 724 eV. The Fe 2p high resolution spectrum of IO (Fig. [4b\)](#page-5-0) shows the binding energy peaks corresponding to the Fe  $2p_{3/2}$  and Fe  $2p_{1/2}$  spin-orbit peaks of Fe<sub>3</sub>O<sub>4</sub> at 709.5 and 723.1 eV, respectively. This suggests the formation of a mixed oxide of Fe  $(II)$  and Fe  $(III)^{43}$  $(III)^{43}$  $(III)^{43}$ . These peaks are also clearly seen in Fe 2p high resolution spectra of MGOs indicating the successful formation of IO and GO nano-composites. The O 1s spectrum of GO (Fig. [4c\)](#page-5-0) depicts three peaks at 529.3, 530.8 and 531.7 eV associated with the oxygen in hydroxyl (O–H; C–H), carboxylate and/or carbonyl (C–O–O; C=O) and epoxy and/or hydroxyl  $(C-O-C; C-OH)$ , respectively. The peaks of O 1 s in the spectra of MGOs broaden and shift to the lower binding energy towards the characteristics O 1 s of lattice oxygen in Fe<sub>3</sub>O<sub>4</sub> (528.1 eV; Fe–O)<sup>44</sup>. The formation of a new peak at 529.8 eV in MGOs suggests the binding of IO on GO with the oxygen functionalities via Fe–O–C bond.



<span id="page-5-0"></span>**Figure 4.** (**a**) XPS survey spectra of GO, IO, and MGOs. High resolution (**b**) Fe 2p spectra, (**c**) O 1s and (**d**) C 1s spectra of GO, IO, and MGOs with the experimental and deconvolution fttings.

Moreover, the decrease in the XPS intensities of C–O–C and C–OH in MGOs versus GO indicates the bidentate complex formation between carboxylate group and Fe element<sup>45</sup>.

The high-resolution C 1s spectra of GO in Fig. [4d](#page-5-0) show the high-intensity peak of C–O–C; C–OH (285.3 eV) compared to that of C=C (sp<sup>2</sup>) (282.6 eV), C–C (sp<sup>3</sup>) (283.5 eV), C=O (287.1 eV) and O–C=O (287.5 eV) indicating that the GO is oxidized by the hydroxyl and epoxy groups. It is evidently seen that the  $C=C(sp^2)$  and  $C-C$  $(sp<sup>3</sup>)$  peaks in the MGOs shift to lower binding energy from GO. These binding energy values of C=C  $(sp<sup>2</sup>)/C-C$ (sp3 ) expressed as 282.4/283.2 eV, 282.3/283 eV, 282.1/282.7 eV and 282/282.3 eV in MGO 1, MGO 2, MGO 3, and MGO 4, respectively, were shifed indicating the contribution of diferent loading percentages of IO on GO. However, no signifcant decrease in the intensities of the peaks from the oxygen functionalities was observed in MGOs.

Magnetic feld and temperature dependent magnetization measurements of IO and MGOs were performed in a physical property measurement system (PPMS) using vibrating sample magnetometry (VSM). The field dependent magnetization (*M–H*) was performed at 5 K and 300 K in the range  $\pm 2T$  of applied field (Fig. [5a](#page-6-0)) while the temperature dependent magnetization (*M–T*), feld cooled (FC) and zero feld cooled (ZFC) magnetic measurements as a function of temperature, were recorded under an external dc feld of 5 mT in the temperature range of 5–400 K (Fig. [5b\)](#page-6-0). The IO exhibited a large saturation magnetization  $(M<sub>s</sub>)$  of 84 emu/g of 'Fe' which increases to 95 emu/g when the temperature is decreased to 5K, suggesting that the magnetic spins are more oriented along the applied field at low thermal energy (Fig. [5a,b](#page-6-0)). The  $M_S$  values of MGOs are observed to be 65, 25, 15 and 10 emu/g for MGO 4, MGO 3, MGO 2, and MGO 1, respectively, at 300K which increased to 76, 30, 18 and 13 emu/g at 5 K. These values are consistent with the weight percentages of IO in respective MGOs. The increased amount of IO in GO creates higher defects that lead to interaction between the local moments<sup>46</sup> resulting in higher saturation magnetization in the MGOs. It is reported that GO shows paramagnetic and antiferromagnetic behaviors at low and room temperature, respectively<sup>[46](#page-10-27)</sup>. The lower M<sub>S</sub> values of MGOs when compared to IO at both 5K and 300K are ascribed to the paramagnetic and antiferromagnetic contribution from GO. The magnetic hysteresis (*M–H*) curves of IO and MGOs measured at 300, and 5K exhibit typical superparamagnetic behavior with negligible coercivity  $(H_C)$  (Fig. [5c,](#page-6-0) top, and bottom)

The  $M_{ZFC}$  (T) curves of all MGOs and IO clearly show irreversibility over a wide temperature range as shown in Fig. [5d.](#page-6-0) This behavior indicates that the thermal energy of the magnetic spins remains insufficient to overcome the anisotropy energy barrier of the IO clusters up to 400 K and therefore, remain blocked. From the  $M_{ZFC}$ (T) curves, it is observed that a 50 mT static magnetic field is not sufficient for rapid alignment of the magnetic moments. A gradual increase in the magnetic moment without forming well-defined blocking temperature  $(T_B)$ is observed as the temperature is raised. The observed behaviors are analogous to those reported in iron-carbon



<span id="page-6-0"></span>**Figure 5.** Magnetic hysteresis (*M–H*) curves of IO and MGOs measured at (**a**) 300K and (**b**) 5K (**c**) *M-H* curves in low magnetic feld region showing negligible coercivity (d) FC and ZFC curves of IO and MGOs.

nanocomposites<sup>47</sup>. The broad  $M_{ZFC}(T)$  curves suggest the presence of a distribution of blocking temperatures due to the distribution of energy barriers governed by the size variation of IO. A plateau-shape in the  $M_{FC}$  (T) curve of MGO 4 below 55K is associated with the freezing of the magnetic moments of iron oxide nanoparticles, resulting in spin-glasslike behavior.

The aqueous dispersibility of such materials is one of the main properties in the design for the MRI applications. Te dynamic light scattering (DLS) and Zeta potential measurements were carried out for the investigation of hydrodynamic size  $(D_H)$  and the aqueous stability of MGOs. The  $D_H$  for MGO 1, MGO 2, MGO 3, and MGO 4 are recorded to be 376 nm, 409 nm, 414 nm, and 434 nm, respectively, which is much larger than that of the IO particles alone (8–25 nm as shown in Fig. [2\)](#page-3-0), as expected. The observed  $D_H$  (Fig. [6a\)](#page-7-0) for MGOs are consistent with the IO content in GO. The MGOs demonstrate excellent aqueous dispersibility with a Zeta potential in the range of −47 to −48mV, essentially constant, which suggests the presence of abundant oxygenated functionalities in  $GO<sup>48</sup>$  $GO<sup>48</sup>$  $GO<sup>48</sup>$ . The schematic representation and optical images of the aqueous dispersed MGOs and their magnetic capture are shown in Fig. S2 in SI.

The measurements of transverse relaxivity  $(r_2)$  of MGOs were performed at 1.41 T. The relaxivity values were calculated from the slope of the relaxation rate  $(R_2=1/T_2)$  versus concentration of iron ([Fe]) graph shown in Fig. [6b,](#page-7-0) where  $T_2$  is the protons' transverse relaxation time at a given concentration of iron. The MGO 1 exhibits the lowest  $r_2$  of 27  $\pm$  0.53 mM<sup>-1</sup>s<sup>-1</sup> (R<sup>2</sup> = 0.998) while  $r_2$  increases to 106  $\pm$  3.75 mM<sup>-1</sup>s<sup>-1</sup> (R<sup>2</sup> = 0.994) in MGO 2. Similarly, the MGO 3 exhibits the highest  $r_2$  value at  $162 \pm 5.70$  mM<sup>-1</sup>s<sup>-1</sup> (R<sup>2</sup> = 0.994) with 28% of IO and  $r_2$ decreases to  $103 \pm 8.00$  mM<sup>-1</sup>s<sup>-1</sup> (R<sup>2</sup> = 0.971) in MGO 4 as the IO content increases to 32%. The exponential decay curves (Fig. S3 in SI) show the steady decrease in transverse intensity with the increase in [Fe]. The size dis-tribution profile of MGOs is shown in Fig. [6d](#page-7-0) to correlate with the dependency of  $r_2$  on the  $D_H$  of MGOs (Fig. [6e\)](#page-7-0) and point to a close analogy to the  $r_2$  values associated with the theoretical size regimes, MAR, SDR, and SMR, which are specifed in classical outer sphere relaxation theory.



<span id="page-7-0"></span>

The dependence of  $r<sub>2</sub>$  on the size of IO is directly related to how far the water molecules (protons) diffuse with respect to the size of IO, *i.e*., the difusion length of water protons relative to the size of IO, as given by the relation $30$ ,

$$
\tau_{\text{diff}} = D^2 / 4 C_{\text{diff}} \tag{1}
$$

where  $\tau_{\text{diff}}$  is the diffusion time of water protons, D is the diameter of IO and  $C_{\text{diff}}$  is the translation diffusivity of water protons. The  $r_2$  values for MGO 1 and MGO 2, with  $D_H$  of 376 nm and 409 nm, respectively, indicate that the MAR condition was achieved signifying that the randomly difusing water protons experience diverse susceptibility gradients with increasing  $D_H$ , which are time-averaged and  $r_2$  is given by the relation<sup>[31](#page-10-12)</sup>,

$$
\mathbf{r}_2 = (16/45) \gamma \tau_D (\Delta \omega)^2 \tag{2}
$$

for  $\tau_{\text{diff}}(\Delta \omega) < 1$ , where  $\gamma$  is the volume fraction of IO,  $\Delta \omega = \gamma(B_{\text{eqtr}}) = \gamma_0(\mu_0 M_s/3)$  is the change in Larmor frequency of protons at the equator of MGO that generates the magnetic field of  $B_{\text{extr}}$ , M<sub>S</sub> is the saturation magnetization of MGO,  $\gamma_0 = 2.67 \times 10^8$  rad·s<sup>-1</sup>·T<sup>-1</sup> is the gyromagnetic ratio of protons, and  $\mu_0 = 4\pi \cdot 10^{-7}$  T·m·A<sup>-1</sup> is the magnetic permeability in vacuum.

Similarly, MGO 3 attains the maximum  $r_2$  value with  $D_H=414$  nm corresponding to the SDR condition, i.e., the distance traveled by diffusion is less than the characteristic separation of IO due to the higher  $D_H$  value, and the water protons do not experience a significant susceptibility gradient, thus yielding maximum r<sub>2</sub>. The SDR is achieved when  $\tau_{\text{diff}}(\Delta \omega) > 1$  and  $r_2$  is given as<sup>[31](#page-10-12)</sup>

$$
r_2 = (2\pi/9) \{ \gamma \gamma_0(\mu_0 M_S) \} \tag{3}
$$

Further increasing the  $D_H$  of IO beyond the SDR condition, the increase in  $r_2$  ceases by echo-limiting or  $T_2^*$ -limiting and  $r_2$  decreases consequently, and this size regime corresponds to the ELR or SMR condition. This depends on the magnitude of diffusion time ( $\tau_D$ ) and the echo time ( $\tau_{TE}$ ), i.e., the time between 90° RF pulse and the peak of echo signal induced. The refocusing 180° RF pulse being antiparallel to the initial 90° RF pulse inverts



<span id="page-8-0"></span>

the dephasing and refocuses the protons to in phase. This slows down the decay of transverse intensity to be slower than in the SDR condition and r<sub>2</sub> decreases, which was observed in MGO 4 with  $D_H$  of 434 nm.

Also, we carried out MR *in vitro*  $T_2$ -weighted MR phantom imaging on MGOs to assess their  $T_2$  contrast enhancement efficacy. The imaging was performed in DI water at 4.7T using multiple spin-echo sequences with a repetition time (TR) = 12000 ms, echo time (TE) = 24 ms, field of view (FOV) = 60, phase = 40 and thick-ness = 1.50 mm. The phantom images, in Fig. [6c,](#page-7-0) show a clear  $T_2$  (negative) contrast enhancement as the 'Fe' concentration increases. It is seen that the MGO 3 produced an enhanced  $T<sub>2</sub>$  contrast due to its higher relaxivity. Figure [6d](#page-7-0) shows a variation of  $r_2$  values of MGOs with  $D_{H}$ .

Besides the evaluation of MR efficacy of MGOs, the study of toxic responses of such materials is crucial in MRI applications. We studied the cell viability of human breast adenocarcinoma epithelial cells (MDA-MB-231) when interacted with MGOs via 3-(4,5-dimethylthiazol-2-yl)-5-(3-carboxymethoxyphenyl)-2-(4-sulfophenyl)- 2H-tetrazolium (MTS) assay. The results, in Fig. [7](#page-8-0), show that the MGOs have high biocompatibility, in general, which is consonant with previous reports<sup>[23,](#page-10-4)24</sup>. The fact that MGO 3 has the highest relaxivity and remains nontoxic at least up to 2mM of [Fe] is very promising for contrast agent applications, notwithstanding the fact they have lower relaxivities than SPIOs<sup>28,29</sup> and would require higher concentrations. As explained by Garg *et al.*<sup>49</sup>, nanosized GOs show very low toxicity and can be further improved by surface engineered biocompatible polymers, which may enable them to be efectively employed as contrast agents.

### **Conclusion**

Magnetic graphene oxide with diferent weight percentages of iron oxide nanoparticles decorated on graphene oxide were synthesized in nanocomposite form. The MGOs exhibit tunable magnetic behavior and hydrodynamic sizes consistent with the weight percentages of the constituents. They show distinct MR transverse relaxivity  $(r_2)$ values of  $27 \pm 0.527$ ,  $106 \pm 3.752$ ,  $162 \pm 5.703$  and  $103 \pm 8$  mM<sup>-1</sup>s<sup>-1</sup> corresponding to the hydrodynamic sizes of 376, 409, 414 and 434nm respectively.

These diverse r<sub>2</sub> values associated with the hydrodynamic sizes are analogous to those observed in the theoretical size regimes defned as motional averaging regime (MAR), static dephasing regime (SDR) and echo-limiting regime/slow motion regime (ELR/SMR) in classical outer sphere relaxation theory. Such behavior was previously observed only in the single core or cluster forms of IO. Further, the MGOs demonstrate excellent colloidal stability in aqueous solution and *in vitro* cytocompatibility in cancer cells. These show how to achieve the optimization of transverse relaxivity of magnetic graphene oxide and paves the way for the MRI applications of graphene-based nanocomposite magnetic materials.

### **Methods**

**Materials.** Ferric chloride hexahydrate (FeCl<sub>3</sub>.6H<sub>2</sub>O,  $\geq$ 99%), Ferrous chloride tetrahydrate (FeCl<sub>2</sub>.4H<sub>2</sub>O, 99.99%), Ammonium hydroxide (NH4OH, 28.0–30.0%), Sodium chloride ≥99.5%, Hydrochloric acid 37%, Sodium nitrate (NaNO<sub>3</sub>, ≥99.0%), Potassium permanganate (KMnO<sub>4</sub>, ≥99.0%) were purchased from Sigma-Aldrich.

**Synthesis of magnetic graphene oxide (MGO).** The MGO was synthesized in the form of IO-GO nanocomposite following the protocol reported previously[43](#page-10-24) with minor modifcation. Firstly, the spherical IO were synthesized via the co-precipitation method<sup>36</sup>. In general, 4.14 gm of FeCl<sub>3</sub>.6H<sub>2</sub>O and 1.62 gm of FeCl<sub>2</sub>.4H<sub>2</sub>O was dissolved in 75 mL of deionized water by mechanical stirring. The pH of the solution was adjusted to 10.57 by adding NH<sub>4</sub>OH solution under N<sub>2</sub> atmosphere and vigorous stirring followed by 1 h aging at 70 °C. After cooling the solution, the product was washed via magnetic decantation for 5 times, and the powder form of IO was obtained afer the lyophilization. Secondly, the GO was synthesized via the modifed Hummer and Ofeman's method<sup>50</sup>. Following the washing process, the GO solution was probe sonicated for 24h at 20% amplitude with 30 s 'ON' and 60s 'OFF' to generate the GO fakes. For the synthesis of IO-GO nanocomposite, 240mg of GO was gently sonicated to dissolve in 50ml of deionized (DI) water (~5mg/ml) followed by the addition of 20mg of IO. The mixture was aged for 12h (overnight) at room temperature with constant mechanical stirring to obtain the nanocomposite as MGO 1. Finally, the product was washed using magnetic decantation three times with DI water and was dried by lyophilization. The IO:GO at the ratio of 2:12, 3:12 and 4:12 (w/w) were used for the synthesis of MGO 2, MGO 3 and MGO 4, respectively.

**Characterization and cell viability assay.** The thermogravimetry (TG) was performed using a PerkinElmer STA 6000 Simultaneous Thermal Analyzer by heating 7 mg of each MGO powder in the temperature range of 30 to 800 °C at the rate of 5 °C per minute in the presence of a constant N<sub>2</sub> flow of 20 ml/min. The inductively coupled plasma optical emission spectrometry (ICP-OES) was carried out using Optima 8000 Perkin Elmer ICP–OES (PerkinElmer, Inc.). Samples were prepared according to the procedure previously reported<sup>51,52</sup> with a minor modification (see Table S1 in SI). The energy dispersive X-ray (EDX) spectra were obtained in a scanning electron microscope (SEM) JEOL JSM-5800LV with operating voltage of 20 kV. The SEM and TEM images were obtained using a JOEL JSM 7500 F Field emission scanning electron microscope (FE-SEM) and a JEOL JEM 2100 F Field emission transmission electron microscope (FE-TEM) with operating voltage of 200 kV. The X-ray diffraction (XRD) patterns were obtained by a Rigaku SmartLab X-Ray diffractometer using CuK<sub> $\alpha$ </sub> ( $\lambda$  = 1.5406Å) operating at 40 KV and 44 mA. The attenuated total reflectance Fourier transform infrared (ATR-FTIR) spectra were obtained by a Bruker Tensor 27 spectrometer. The Raman spectra were obtained using a Thermo Scientific DXR Confocal Raman Microscope. The X-ray photoelectron spectroscopy (XPS) was performed on a Kratos Axis Ultra X-ray photoelectron spectrometer (Kratos Analytical, Inc., Manchester, UK) using monochromatic Al K $\alpha$  radiation (hv = 1486.6 eV). High resolution spectra were collected using a 0.7 mm  $\times$  0.3 area. The powder samples were loaded for analysis onto double-sided copper tape. The dynamic light scattering (DLS) and Zeta potential were performed using a Malvern Zetasizer Nanoseries Nano-ZS (Malvern Instruments, Malvern, UK) operating a helium-neon laser wavelength of 633 nm and power of 4 mW. The magnetic measurements were performed in a physical property measurement system (PPMS) DynaCool (Quantum Design, Inc.). The magnetic resonance (MR) transverse relaxivity  $(r_2)$  measurements were conducted on the NMReady-60PRO benchtop relaxometer (Nanalysis Corp. Canada) at 1.41T at 30 °C. The  $T_2$ -weighted magnetic resonance (MR) phantom images were obtained by Agilent 4.7T preclinical MRI scanner at 4.7T. The cell viability studies on human breast adenocarcinoma epithelial cells, MDA-MB-231 were analyzed via MTS assay as described in detail previously by our group<sup>36[,53](#page-10-34)</sup>.

**Ethics Approval.** All cell experiments were performed in accordance with the protocols approved by the Biosafety Committee at the Molecular Sciences Research Center, University of Puerto Rico, San Juan, PR 00926, USA.

### **Data Availability**

All data obtained and analyzed in this research work are included in this published article and its Supplementary Information fle.

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### **Acknowledgements**

Tis project was supported in part by the Institute for Functional Nanomaterials (NSF Cooperative Agreement 1002410), the U54 UPR-MD Anderson Cancer Center Partnership Program (NIH National Cancer Institute Grant no. U54 CA096297/CA096300), NIH Research Initiative for Scientifc Enhancement (RISE) Fellowship (Grant no. 5R25GM061151-17), PR Space Grant (NASA Training Grant Number NNX15AI11H) and PR NASA EPSCoR (NASA Cooperative Agreement NNX15AK43A). J.B.-H. received funding from the NSF Cooperative Agreement no. DMR-1157490, DMR-1644779, and the State of Florida, and was supported in part by a grant from the National Cancer Institute of the National Institutes of Health under award number T32CA196589. The authors thank the valuable assistance of Dr. Huadong Zeng for MR phantom images acquisition in AMRIS and Professor Ram S. Katiyar for his research facility.

### **Author Contributions**

B.T., D.D.D. and J.B.-H. conceived and designed the project; B.T., D.D.D., D.B.D., K.D., R.K.S., S.K., M.B.H. performed the experiments; B.T. wrote the manuscript; B.T., D.D.D., J.B.-H., B.R.W. and G.M. analyzed the data, reviewed and commented on the manuscript at all stages. All authors read and approved the manuscript.

### **Additional Information**

**Supplementary information** accompanies this paper at [https://doi.org/10.1038/s41598-019-42093-1.](https://doi.org/10.1038/s41598-019-42093-1)

**Competing Interests:** The authors declare no competing interests.

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