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PET/CT Imaging of Chemokine Receptor CCR5 in Vascular Injury Model Using Targeted Nanoparticle

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Abstract

Inflammation plays important roles at all stages of atherosclerosis. Chemokine systems have major effects on the initiation and progression of atherosclerosis by controlling the trafficking of inflammatory cells in vivo through interaction with their receptors. Chemokine receptor 5 (CCR5) has been reported to be an active participant in the late stage of atherosclerosis and has the potential as a prognostic biomarker for plaque stability. However, its diagnostic potential has not yet been explored. The purpose of this study was to develop a targeted nanoparticle for sensitive and specific PET/CT imaging of the CCR5 receptor in an apolipoprotein E knock-out (ApoE^{-/-}) mouse vascular injury model.

Methods—The D-Ala1-peptide T-amide (DAPTA) peptide was selected as a targeting ligand for the CCR5 receptor. Through controlled conjugation and polymerization, a biocompatible poly(methyl methacrylate)-core/polyethylene glycol-shell amphiphilic comblike nanoparticle was prepared and labeled with ⁶⁴Cu for CCR5 imaging in the ApoE^{-/-} wire-injury model. Immunohistochemistry, histology, and real-time reverse transcription polymerase chain reaction (RT-PCR) were performed to assess the disease progression and upregulation of CCR5 receptor.

Results—The ⁶⁴Cu-DOTA-DAPTA tracer showed specific PET imaging of CCR5 in the ApoE^{-/-} mice. The targeted ⁶⁴Cu-DOTA-DAPTA-comb nanoparticles showed extended blood signal and optimized biodistribution. The tracer uptake analysis showed significantly higher accumulations at the injury lesions than those acquired from the sham-operated sites. The competitive PET receptor blocking studies confirmed the CCR5 receptor-specific uptake. The assessment of ⁶⁴Cu-DOTA-DAPTA-comb in C57BL/6 mice and ⁶⁴Cu-DOTA-comb in ApoE^{-/-}

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DISCLOSURE

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Conclusion—This work provides a nanoplatform for sensitive and specific detection of CCR5's physiologic functions in an animal atherosclerosis model.

Keywords

PET/CT; nanoparticles; chemokine receptor; atherosclerosis; CCR5

Atherosclerosis, the leading cause of morbidity and mortality in Westernized societies, is a progressive disease characterized by the development of lipid-rich plaque lesions within vessel walls and extending into the vascular lumen. It is the underlying basis of cardiovascular diseases including myocardial infarction, stroke, and peripheral arterial disease (1). There are several phenotypes associated with the plaque such as inflammation and thin fibrous cap formation during the longitudinal progression of atherosclerosis. Currently, substantial evidence has demonstrated that atherosclerosis is essentially an inflammatory disease, for which inflammation has crucial roles in the initialization, progression, and eventual completion of vascular occlusion, which is the acute clinical event (2,3). Therefore, inflammation specifically associated with the formation and progression of atherosclerosis, risk stratification of patients, and identification of novel therapeutic strategies (4–6).

Molecular imaging has become an important experimental tool for atherosclerosis research in the last decade. It can provide a direct entrance to the processes involved in the development of plaque and its complications at the molecular level to reveal disease diversity, guide specific therapy, and monitor treatment response (7,8). Of various imaging modalities, the combined approach of PET/CT has been widely used because of its high sensitivity, quantitative diagnosis, and the potential for translation into patients (9).

During arterial inflammation, there is induction of expression of a variety of biomarkers such as vascular cell adhesion molecule-1, intercellular adhesion molecule-1, and E-selectin (10). Some molecular probes have been developed to image these biomarkers in preclinical atherosclerosis models with promising results. However, their translational potentials remain to be determined (11,12). Although the clinical tracer ¹⁸F-FDG has been widely used to evaluate the elevated metabolic activity in atherosclerosis, it is essentially a nonspecific tracer and has technical challenges to detect the lesions in coronary arteries because of the size of the vessel and myocardial uptake (4,8,13).

Chemokines belong to a large family of structurally related and secretable, largely basic, chemotactic cytokines. They are expressed in an array of vascular cells such as endothelial cells and inflammatory cells within the atherosclerotic lesions and regulate leukocyte activation and recruitment to sites of inflammation via interaction with a family of G-protein–coupled receptors (14,15). Recent studies have reported upregulation of chemokine receptors (CRs) on the inflammatory cells identified in human plaque samples. In murine transgenic and knock-out atherosclerosis models, the important roles of several CCRs, including CCR5, CCR2, and CX3CR1, by affecting leukocyte subset recruitment have

already been well defined (16,17). During the progression of atherosclerotic lesions, CCR5 was selectively upregulated in certain subsets of monocytes and played critical roles in mediating their entry into plaques (18), especially in the late stage of the disease (19–21), making it an important biomarker to study the plaque development, progression, and stability by tracking these inflammatory cells. Previously, we have imaged the expression of 8 CRs, including the CCR5, in an apolipoprotein E knock-out (ApoE^{-/-}) mouse vascular injury model with PET/CT (22). In this study, we prepared a CCR5 receptor–specific probe through the conjugation of targeting peptide D-Ala₁-peptide T-amide (DAPTA) (23,24) on a comblike nanoparticle (25,26) for in vivo PET/CT imaging of CCR5 receptor upregulation in the same model. The CCR5 receptor–targeting specificity and imaging efficiency were compared with the control nanoparticles and the DAPTA peptide tracer alone. This work may provide a nanoplatform for sensitive and specific detection of the CCR5's physiologic functions in animal atherosclerosis models.

MATERIALS AND METHODS

Materials were purchased from Sigma-Aldrich and used without further purification unless otherwise stated. The ⁶⁴Cu (half-life = 12.7 h, β^+ = 17%, β^- = 40%) was produced at the Washington University cyclotron facility (27). Functionalized poly(ethyleneglycol) (PEG) derivatives were obtained from Intezyne Technologies. Tris-t-butylester-DOTA, 1,4,7,10tetraazacyclododecane, and DOTA-N-hydroxy-succinimide ester were purchased from Macrocyclics. D-Ala1-peptide T-amide (DAPTA, D-A1STTTNYT-NH2) was customized by CPC Scientific. Centricon tubes were purchased from Millipore. Zeba desalting spin columns were from Pierce. Reversed-phase high-performance liquid chromatography was performed on a system equipped with a UV/VIS detector (Dionex) and a radioisotope detector (B-FC-3200; BioScan Inc.) on a C-18 analytic column (5 mm, 4.6 × 220 mm; Perkin Elmer). Polymeric materials were characterized by ¹H and ¹³C nuclear MR (NMR) spectroscopy using a Bruker 500-MHz spectrometer with the residual solvent signal as an internal reference. Gel permeation chromatography was performed in dimethylformamide on a Waters system equipped with four 5- μ m Waters columns (300 \times 7.7 mm) connected in series with increasing pore size $(10^2, 10^3, 10^4, \text{ and } 10^6 \text{ Å})$ and Waters 410 differential refractometer index and 996 photodiode array detectors. The molecular weights of the polymers were calculated relative to linear polymethyl methacrylate (PMMA) or PEG standards. Infrared spectra were recorded on a Perkin Elmer Spectrum 100 with a Universal ATR sampling accessory. The synthesis and characterization of DOTA-DAPTA, DOTAcomb, and DOTA-DAPTA-comb (Supplemental Figs. 1 and 2) are described in the supplemental materials (available at http://jnm.snmjournals.org).

Mouse Vascular Injury Model

All animal studies were performed in compliance with guidelines set forth by the National Institutes of Health Office of Laboratory Animal Welfare and approved by the Washington University Animal Studies Committee. The mouse vascular injury model was induced in ApoE^{-/-} mice (n = 25, Taconic Inc.) through wire injury on the right femoral artery as described previously (22,28,29). The left femoral artery was also surgically prepared by undergoing incision and closure without guide wire endothelial injury to serve as the sham

site. Wild-type C57BL/6 mice (n = 5) fed with normal chow underwent the same wire-injury procedure and were used as control animals.

Biodistribution Studies

⁶⁴Cu-DOTA-DAPTA-comb and ⁶⁴Cu-DOTA-comb were reconstituted in 0.9% sodium chloride (APP Pharmaceuticals) for intravenous injection. Male C57BL/6 mice weighing 20–25 g (n = 4/group) were anesthetized with inhaled isoflurane, and approximately 370 kBq of labeled nanoparticles (7.2–9.0 µg/kg of body weight) or the DOTA-DAPTA peptide (0.35–0.44 µg/kg of body weight) in 100 µL of saline were injected via the tail vein. The mice were reanesthetized before they were euthanized by cervical dislocation at each time point (1, 24, and 48 h) after injection. Organs of interest were collected, weighed, and counted in a well γ counter (Beckman 8000). Standards were prepared and measured along with the samples to calculate the percentage injected dose per gram of tissue (% ID/g) (27).

Small-Animal PET/CT Imaging

Two weeks after the wire injury, small-animal PET/CT imaging was performed on Apo $E^{-/-}$ mice to determine the uptake and progression at atheroscleroticlike lesions. The injured control C57BL/6 mice (n = 5) were scanned following the same protocol. For PET/CT imaging, mice were injected with ⁶⁴Cu-DOTA-DAPTA (1.85-3.7 MBq in 100 µL of saline), and 0- to 60-min dynamic scans were acquired on the small-animal PET Focus-220 or Inveon PET/CT system (Siemens). For ⁶⁴Cu-DOTA-DAPTA-comb and ⁶⁴Cu-DOTA-comb, 3.7 MBg in 100 µL of saline were injected via tail vein. The imaging sessions were collected on the PET scanners at 1, 4, 24, and 48 h after injection. Both PET scanners were crosscalibrated periodically. Data analysis of the PET images was performed using the manufacturer's software (ASI Pro or IRW; Siemens). The accumulation of the PET tracers at the injury site and on the contralateral sham-operated femoral artery was calculated as %ID/g from the maximum-intensity-projection images. After the last PET/CT scan, the animals were euthanized by cervical dislocation, and the femoral vessels were either perfusion-fixed in situ with freshly prepared 4% paraformaldehyde in 1× phosphate-buffered saline for histopathology and immunohistochemistry or fast-frozen for real-time reverse transcription polymerase chain reaction (RT-PCR) analysis. Competitive receptor blocking studies were performed on Apo $E^{-/-}$ mice with wire injuries for ⁶⁴Cu-DOTA-DAPTA-comb by coinjection of unlabeled DOTA-DAPTA-comb in 100-fold excess (n = 6) at 2 wk after the wire injury, followed by PET scans at 1, 24, and 48 h after injection.

Immunohistochemistry, Histologic Characterization, and RT-PCR Assay

Serial sections (5-µm thick) were cut from paraformaldehyde-fixed (24 h), paraffinembedded specimens. The sections were deparaffinized and rehydrated through a series of xylenes and graded alcohols before undergoing antigen retrieval pretreatment (10 mM Tris, 1 mM ethylenediaminetetraacetic acid, 0.05% polysorbate, pH 9.0, for 10 min). They were treated with 0.3% H₂O₂ for 30 min, followed by blocking serum for 1 h to prevent nonspecific binding (Vectastain; Vector Laboratories). The sections were then incubated overnight at 4°C with primary antibody (anti-CCR5, 1:200 in blocking serum; Abcam). Secondary antibody was applied (Vector Laboratories), and color development was achieved

through horseradish peroxidase-DAB (3,3'-diaminobenzidine tetrahydrochloride) (brown)– based immunostaining kits (Vector Laboratories). Sections were counterstained with tartrazine (yellow). Digital images of the stained sections were obtained using a scanning light microscope (NanoZoomer; Hamamatsu). Additionally, hematoxylin and eosin (H&E) staining was also performed on the consecutively cut specimens.

Tissue RNA was isolated using TRIzol (Invitrogen) per the manufacturer's instruction. RNA isolated from injured and sham femoral arteries was used for real-time RT-PCR. Reverse transcription reactions used 1 μ g of total RNA, random hexamer priming, and Superscript II reverse transcriptase (Invitrogen). The expressions of CCR5 and glyceraldehyde 3-phosphate dehydrogenase (GAPDH) were determined using Taqman assays (Invitrogen) and an EcoTM Real-Time PCR System (Illumina) in duplicate in 48-well plates. PCR cycling conditions were as follows: 50°C for 2 min, 95°C for 21 s, and 60°C for 20 s. GAPDH expression was used as a comparator with C_t calculations.

Statistical Analysis

Group variation is described as mean \pm SD. Groups were compared using 1-way ANOVA with a Bonferroni adjustment. Individual group differences were determined using a 2-tailed Mann–Whitney test. The significance level in all tests was a *P* value of 0.05 or less.

RESULTS

Biodistribution of ⁶⁴Cu-DOTA-DAPTA-Comb

Biodistribution of ⁶⁴Cu-DOTA-comb was previously reported, with most activity accumulated in the mononuclear phagocyte system (liver and spleen) (27). Interestingly, the targeted ⁶⁴Cu-DOTA-DAPTA-comb showed a much improved organ distribution profile. At 1 h after injection, the blood signal of ⁶⁴Cu-DOTA-DAPTA-comb (33.6 ± 7.05 % ID/g, n =6) was slightly higher than that of ⁶⁴Cu-DOTA-comb (25.4 ± 3.04 % ID/g, n = 6) previously reported (Fig. 1) (27). However, its liver and spleen accumulations were both 7 times less (liver, 5.24 ± 1.13 % ID/g vs. 41.9 ± 7.54 % ID/g; spleen, 3.10 ± 0.55 % ID/g vs. 25.4 ± 2.48 % ID/g). At 24 h after injection, in contrast to the fast clearance of ⁶⁴Cu-DOTA-comb from systemic circulation, only one third of ⁶⁴Cu-DOTA-DAPTA-comb was removed from the blood, which led to twice as much (P < 0.001, n = 4) retained in the blood-pool organs. A further study showed that even at 48 h after injection, there was still about half of the initial retention in the blood (15.1 ± 1.70 % ID/g). During the 48-h period, the renal and gastrointestinal tract clearance remained constant, albeit the hepatic and splenic accumulations increased over time, yet both were about 10 % ID/g at the end of this study.

PET/CT Imaging

PET/CT imaging with ⁶⁴Cu-DOTA-DAPTA in the ApoE^{-/-} model (n = 6) at 2 wk after wire injury showed a typical peptide tracer profile with fast renal clearance (Fig. 2A). The summed 0-to 60-min dynamic PET/CT image showed tracer accumulation at the injury lesion, with little uptake observed around the sham site. The quantitative analysis demonstrated almost 2-fold-higher uptake at the injury sites (1.97 ± 0.22 %ID/g, P < 0.001, n = 6) than that obtained from the contralateral thigh (0.69 ± 0.02 %ID/g, n = 6) (Fig. 2B).

The targeted ⁶⁴Cu-DOTA-DAPTA-comb showed rapid accumulation around the injury site and weak uptake at sham site at 1 h after injection (Fig. 3A). Quantitative analysis showed gradually increased tracer uptake at the injured femoral artery from $3.41 \pm 0.40 \text{ \% ID/g}$ (n =6) at 1 h after injection to $5.55 \pm 1.13 \text{ \% ID/g}$ at 24 h after injection, which then plateaued until 48 h (Fig. 3B). In contrast, the tracer uptake at the sham site hardly changed during the 48-h period (1.14 ± 0.32 to $1.50 \pm 0.21 \text{ \% ID/g}$, n = 6), leading to an increased injury-tosham uptake ratio from 3.00 ± 0.92 at 1 h to 4.36 ± 1.11 at the end of the study. Compared with the data obtained with ⁶⁴Cu-DOTA-DAPTA, the ⁶⁴Cu-DOTA-DAPTA-comb illustrated a significantly (P < 0.0005, n = 6) higher uptake at the injury lesion and contrast ratio.

Further, the nonspecific accumulation of ⁶⁴Cu-DOTA-DAPTA-comb was also assessed in wire-injured C57BL/6 control mice. As shown in Figure 4A, the representative PET/CT image at 24 h showed minimum uptake around the injury site. The uptake analysis showed similar tracer accumulation at both injury and sham sites, with no significant difference during the study (Fig. 4B). Further, the control nanoparticle of ⁶⁴Cu-DOTA-comb was also evaluated in the ApoE^{-/-} mice for nonspecific accumulation, with little uptake observed at both injury and sham sites (Fig. 4A). The uptake analysis demonstrated significantly (P < 0.001, n = 6) lower accumulation at the injury lesion than those obtained with targeted ⁶⁴Cu-DOTA-comb (Fig. 4B).

The competitive receptor blocking with the coinjection of unlabeled DOTA-DAPTA-comb at 2 wk after injury resulted in a substantial decrease of tracer uptake at the injury site to a level similar to those obtained at the control site on the representative PET/CT images (Fig. 4A). The quantitative analysis showed that the uptake at the injury lesion had decreased to 1.81 ± 0.10 , 1.92 ± 0.22 , and 1.78 ± 0.27 % ID/g at 1, 24, and 48 h, respectively, all significantly (P < 0.001, n = 6) lower than those obtained in the nonblocking studies (Figs. 3A and 4B). The injury-to-sham uptake ratios were also significantly reduced (1.18 ± 0.19 to 1.35 ± 0.47 , P < 0.005, n = 6) to a level similar to the results obtained with control ⁶⁴Cu-DOTA-comb at the injury lesion.

Histology, Immunohistochemistry, and RT-PCR

The H&E staining of right femoral arteries harvested from the ApoE^{-/-} mice at 2 wk after injury showed significantly progressive atherosclerotic plaque in contrast to the intact vasculature of the sham-operated left femoral artery (Fig. 5). The DAB staining of CCR5 expression on the injury artery was found throughout the injured vessel wall, especially in the medial layer to the thickened neointima that resulted from the wire injury (Fig. 5). On the sham tissue, the vessel wall was much thinner than the injured counterpart and showed significantly less presence of the CCR5 receptor. The quantitative RT-PCR data from the tissue collected at 2 wk after injury demonstrated increased expression of CCR5 RNA on the injured lesion relative to the sham site. The injury-to-sham ratio of RNA expression was 3.91 ± 1.36 (n = 5).

DISCUSSION

We report here the results for PET/CT imaging of CCR5 receptor upregulation associated with wire-injury–induced atherosclerosis in ApoE^{-/-} mice. The presence of the CCR5 receptor was identified with ⁶⁴Cu-DOTA-DAPTA-comb nanoparticles using PET/CT, and immunohistochemistry and RT-PCR in the progressive ApoE^{-/-} model. The imaging capability and superiority of the targeted ⁶⁴Cu-DOTA-DAPTA-comb nanoparticle over the ⁶⁴Cu-DOTA-DAPTA peptide tracer for CCR5 receptor molecular imaging were demonstrated.

It is becoming increasingly clear that many chemokines and their receptors play a role in the development of atherosclerosis, especially for CCR2, CX3CR1, and CCR5 (30). Although there may be some overlap among the functions of these chemokine systems during the development of atherosclerosis, CCR5 has been believed to play a greater role in the progression of unstable plaque (19–21,29). In our previous study, we have reported the upregulation of 8 CRs, including CCR5-which was one of the most expressed receptors in the wire-injury-induced atherosclerosis model-with a promiscuous tracer ⁶⁴Cu-DOTAvMIP-II via PET/CT and immunohistochemistry (22). However, the detection specificity and sensitivity for CCR5 needs to be improved to further explore its pathologic role during the progression of atherosclerosis from early to later stages of the disease. Of the ligands, antagonists, and agonists for CCR5, the DAPTA peptide was selected because of its high binding affinity to the receptor and suitability as a targeting ligand for nanoparticle construction (24,31). As shown in Figure 2, the specific accumulation of ⁶⁴Cu-DOTA-DAPTA at the injured artery was clearly observed. However, its fast pharmacokinetics limited the sensitivity and contrast for CCR5 imaging in vivo, thus making a DAPTAmodified nanoparticle with extended blood circulation a viable candidate for overcoming these difficulties. In related studies, biocompatible poly(methyl methacrylate)-core/ polyethylene glycol-shell amphophilic nanoparticles have shown the ability in controlled functionalization and polymerization to tailor the biodistribution and targeting efficiency for improved PET/CT imaging in an animal disease model (27). Thus, this nanoplatform was conjugated with DAPTA peptide to afford a DAPTA-comb nanostructure in which 10% of the PEG chain ends were functionalized with DAPTA (~14 per particle) for initial in vivo evaluation.

Previously, we have reported the biodistribution of nontargeting ⁶⁴Cu-DOTA-comb nanoparticles with enhanced blood signal but high mononuclear phagocyte system uptake (27). With the conjugation of DAPTA peptide, the blood signal of ⁶⁴Cu-DOTA-DAPTAcomb was further extended, with more than 15 %ID/g remaining even after 48 h of circulation in vivo. Although the hepatic and splenic accumulations of ⁶⁴Cu-DOTA-DAPTA-comb slowly increased during the 48-h study, they were still significantly (P < 0.001, n = 4) lower than those obtained with ⁶⁴Cu-DOTA-comb, reasonably due to the effect of the neutral surface charge (ζ potential, DOTA-DAPTA-comb = 6.2 ± 2 mV vs. DOTAcomb = -35 ± 2 mV), which was consistent with a previous report (27). More importantly, the extended blood signal, in combination with strong binding affinity and high specific activity, required only 1.9 pmol of ⁶⁴Cu-DOTA-DAPTA-comb for in vivo PET imaging. This results in sensitive, specific detection and high contrast for CCR5 in the wire-injured

 $ApoE^{-/-}$ mouse model whereas the control ⁶⁴Cu-DOTA-comb showed minimal nonspecific accumulations at injury lesion at a level similar to that accrued at the sham-operated site.

The quantitative uptake analysis showed that ⁶⁴Cu-DOTA-DAPTA-comb accumulations at the injury lesion were significantly higher than those obtained from the sham site at each time point, with an injury-to-sham uptake ratio as high as 4.4 at the 48-h time point. Further, it was observed that the ⁶⁴Cu-DOTA-DAPTA-comb uptake at the injury lesion increased over time during the study, which is reasonably due to the accumulative binding of circulating ⁶⁴Cu-DOTA-DAPTA-comb to CCR5 receptor recycled back to the cell surface after internalization (32). In contrast to ⁶⁴Cu-DOTA-DAPTA, the uptake of ⁶⁴Cu-DOTA-DAPTA-comb at 1 h was almost twice as much, most likely due to the enhanced targeting efficiency of ⁶⁴Cu-DOTA-DAPTA-comb with the multi copies of DAPTA per nanoparticle. All of these demonstrated the advantage of a long-circulating nanoparticle for cardiovascular disease imaging. Additionally, the minor but not statistically different increase of ⁶⁴Cu-DOTA-DAPTA-comb uptake at the injury lesion between 24 and 48 h indicated that the tracer accumulation was mainly mediated through CCR5 receptor binding not the nonspecific accumulation because the remaining ⁶⁴Cu-DOTA-DAPTA-comb in the blood did not incur any significant nonspecific binding. More importantly, the significant decrease of tracer uptake at the injury lesion via the competitive PET blocking clearly confirmed the targeting specificity of ⁶⁴Cu-DOTA-DAPTA-comb for the CCR5 receptor. Furthermore, the low ⁶⁴Cu-DOTA-DAPTA-comb uptake in the wire-injured C57BL/6 mice shown in Figure 4A eliminates the concern of nonspecific tracer accumulation due to the surgical procedure and corroborated the targeting specificity. However, one potential limitation of this ⁶⁴Cu-DOTA-DAPTA-comb for cardiovascular imaging was the high blood signal, which might increase the background signal and lead to a low contrast ratio. One approach is to increase the amount of targeting peptide conjugated on the nanoparticles. It was demonstrated that not only could the blood signal be significantly reduced but also the targeting efficiency of the nanoparticles could be improved (27,33). Further, the optimized imaging probe needs to demonstrate its improved targeting efficiency not only in the wire-injury model, which may be limited by the potential artificial effect during the injury procedure, but also in a model with spontaneously developed lesion.

In addition, H&E staining visibly showed the significant progress of vascular lesions at 2 wk after injury in the ApoE^{-/-} mice, with typical characteristics found in atherosclerosis, such as foam cell infiltration, lipid deposition throughout the neointima, smooth muscle cell proliferation, and neointima thickening. Immunohistochemistry via DAB staining depicted the upregulation of CCR5 after wire injury, whereas only minimal expression of the receptor was observed in the sham-operated tissue. More importantly, the quantitative RT-PCR showed significantly higher upregulation of CCR5 in the injured arteries than that expressed in the sham-operated vessel, consistent with the PET/CT imaging data. Further, it is known that CCR5 is mostly expressed in multiple subsets of leukocytes including monocytes and neutrophils (19), which affects the progression and rupture of plaques. It will be important to identify the expression profile of CCR5 in these inflammatory cells during the progression of plaque and combine it with the PET imaging results for a comprehensive evaluation of the role of CCR5 in atherosclerosis in the future studies.

CONCLUSION

In this study, we imaged the expression of the CCR5 receptor with PET/CT in a wireinjury–induced ApoE^{-/-} atherosclerosis model using a DAPTA targeting peptide– conjugated nanoparticle of ⁶⁴Cu-DOTA-DAPTA-comb prepared through modular construction with tailored physical and biologic properties. The improved blood signal, high radiolabeling specific activity, and elevated targeting efficiency of amphophilic ⁶⁴Cu-DOTA-DAPTA-comb afforded in vivo imaging capabilities superior to the ⁶⁴Cu-DOTA-DAPTA peptide alone. The biologic confirmation of the PET image results grants this nanoparticle significant potential as a noninvasive approach for further assessment of the pathologic functions of the CCR5 receptor in animal atherosclerosis models.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

Acknowledgments

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FIGURE 1. Biodistribution of 64 Cu-DOTA-DAPTA-comb in C57BL/6 mice (n = 4/group).



FIGURE 2.

PET/CT image of ⁶⁴Cu-DOTA-DAPTA in wire-injury–induced ApoE^{-/-} mouse atherosclerosis model at 2 wk after injury. (A) Maximum-intensity-projection image showing accumulation of ⁶⁴Cu-DOTA-DAPTA at injured lesion. (B) Uptake analysis of ⁶⁴Cu-DOTA-DAPTA at injured and sham-operated sites. (C) Time–activity curves of ⁶⁴Cu-DOTA-DAPTA at heart and lesion. **P* < 0.05, *n* = 6.



FIGURE 3.

PET/CT images of ⁶⁴Cu-DOTA-DAPTA-comb in wire-injury–induced ApoE^{-/-} mouse atherosclerosis model at 2 wk after injury. (A) Maximum-intensity-projection images showing accumulation of ⁶⁴Cu-DOTA-DAPTA-comb at injured lesion at various time points. (B) Uptake analysis of ⁶⁴Cu-DOTA-DAPTA-comb at injured and sham-operated sites. **P* < 0.05, *n* = 6.



FIGURE 4.

(A) Representative 24-h maximum-intensity-projection images of 64 Cu-DOTA-DAPTAcomb in ApoE^{-/-} mouse, C57BL/6 mouse, 64 Cu-DOTA-comb in ApoE^{-/-} mouse, and 64 Cu-DOTA-DAPTA-comb blocking (DOTA-DAPTA-comb to 64 Cu-DOTA-DAPTA-comb, 100:1) in ApoE^{-/-} mouse at 2 wk after injury. (B) Uptake analysis of corresponding PET images. Quantitative bar graph is below each region of interest. **P* < 0.001, compared with uptake of 64 Cu-DOTA-DAPTA-comb at the injury lesion in ApoE^{-/-} mouse (*n* = 6).



FIGURE 5.

Representative H&E images (left) and DAB images (right) of sham-operated (top) and injured (bottom) femoral arteries from $ApoE^{-/-}$ mouse at 2 wk after injury. Green arrow = foam cells; green arrowhead = smooth muscle cells; CCR5 = brown; counterstain = yellow.