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7 **Frontal monitoring and parietal evidence:**
8 **mechanisms of error correction**
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Abstract

When we respond to a stimulus, our decisions are based not only on external stimuli but also on our ongoing performance. If the response deviates from our goals, monitoring and decision-making brain areas interact so that future behavior may change. By taking advantage of natural variation in error salience, as measured by the reaction time taken to correct an error (RT_{EC}), here we argue that an evidence accumulation framework provides a potential underlying mechanism for this variable process of error identification and correction, as evidenced by covariation of frontal monitoring and parietal decision-making processes. We study two early EEG signals linked to monitoring within medial prefrontal cortex – the error-related negativity (ERN) and fronto-central theta activity – and a third EEG signal, the error positivity (Pe), that is thought to share the same parietal substrates as a signal (the P3b) proposed to reflect evidence accumulation. As predicted, our data show that on slow RT_{EC} trials, frontal monitoring resources are less strongly employed, and the latency of the Pe is longer. Critically, the speed of the RT_{EC} also covaries with the magnitude of subsequent neural (inter-trial alpha power) and behavioral (post-error slowing) adjustments following the correction. These results are synthesized to describe a timing diagram for adaptive decision-making after errors, and support a potential evidence accumulation mechanism in which error signaling is followed by rapid behavioral adjustments.

Introduction

Activity in parietal and frontal brain regions is critical for adaptive decision-making. Studies in non-human primates suggest a mechanism for decision-making in which information accumulates in parietal (and other) areas until neural activity reaches the threshold level required to make a behavioral response (Mazurek et al. 2003; Gold and Shadlen 2007). Importantly, frontal areas including the medial prefrontal cortex (mPFC) play an important role in this process, monitoring decisions and signaling the need for behavioral adjustments such as the allocation of greater attentional resources (Ito et al. 2003; see Ridderinkhof et al. 2004 and Heekeren et al. 2008 for a review).

Recently the idea has arisen that an evidence accumulation framework may also explain error processing (Murphy et al. 2012; Steinhauser and Yeung 2010; Ullsperger et al. 2010; Wessel et al. 2011; Steinhauser and Yeung 2012). By analogy to the case in which sensory evidence is evaluated, evidence for an erroneous response integrates until a threshold is reached, at which point behavioral corrections can be undertaken. Notably, studies of evidence accumulation in other contexts, such as perceptual decision making, typically take advantage of parametric variation in stimulus salience – e.g. the motion coherence of a moving dot stimulus (Gold & Shadlen, 2007) – to manipulate the amount of sensory evidence. However, the salience of an error cannot be modulated as directly as stimulus salience in perceptual decision making studies. To account for this issue, here we take advantage of natural variation in the reaction time taken to correct the error (RT_{EC}) by dividing instances of error correction into short and long RT_{EC} trials. We

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3 hypothesize that the salience of an error correlates inversely with RT_{EC} , an intuition that
4 recent data suggest can be useful: the Pe peak latency, for example, is correlated with the
5 latency at which error awareness is indicated (Murphy et al. 2012).
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12 With this approach, implications of the evidence accumulation hypothesis can also be
13 addressed for other processes necessary for behavioral corrections after errors, including
14 predictions that vary in their degree of certainty. On the one hand, more rapid
15 accumulation of evidence for an error and faster corrections should likely be preceded by
16 stronger correlates of error commission, as indexed by greater response conflict at the
17 time of the initial response (Rodriguez-Fornells et al. 2002). On the other hand, the effect
18 of the speed of evidence accumulation on subsequent processes is potentially unclear.
19 Under one scenario, more rapid accumulation, indicating greater evidence for an error,
20 might be associated with more demand on the cognitive processes responsible for
21 deciding whether to initiate post-error behavioral adjustments. However, the opposite
22 might also be true: because it indicates more confidence about the existence of an error in
23 the context of a time-limited decision (Kiani et al, 2014), more rapid accumulation might
24 place less demand on the decision to initiate such compensations. Specifically, when
25 greater certainty exists that an error was committed (or that the response was correct, for
26 that matter), the decision about whether to engage post-error behavioral adjustments
27 would be easier, compared to the intermediate case in which lesser, more uncertain
28 evidence for an error accumulates more slowly to threshold. Finally, the rapidity of
29 evidence accumulation might have no effect: if such processes are not triggered until
30 evidence for an error reaches a threshold, identical thresholds should trigger the same
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3 behavioral adjustments, irrespective of speed.
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8 Of course, a great deal of work has previously investigated the neural correlates of error
9 processing, including electroencephalography (EEG) studies that have identified
10 candidate electrophysiological correlates for many of these processes. When an error
11 occurs, monitoring signals originating in the mPFC are represented in initial signals (both
12 ERN and theta power; e.g. Endrass et al. 2007, 2012; Luu et al. 2004) that may act as one
13 of the sources of information indicating a potential error (Ullsperger et al. 2010). A later
14 EEG signal, the error positivity (Pe), is evoked by errors in comparison with correct
15 responses in parietal areas (Falkenstein et al. 2000; Shalgi et al. 2009; Navarro-Cebrian et
16 al. 2013). This Pe signal has been suggested to share the same neural substrates as the
17 P3b (Ridderinkhof et al. 2009; Ullsperger et al. 2010). Since the P3b has recently been
18 shown to reflect evidence accumulation in decision-making (O'Connell et al. 2012; Kelly
19 et al. 2013), the Pe may also represent the accumulation of evidence for error occurrence
20 (Steinhauser and Yeung 2010, 2012). Finally, cognitive (i.e. inter-trial alpha power) and
21 behavioral (post-error slowing) adjustments are commonly observed after errors. In
22 particular, inter-trial alpha suppression after errors in comparison with correct responses
23 has been considered a measure of post-error modulations in cortical arousal (Carp and
24 Compton 2009; Compton et al. 2011; Navarro-Cebrian et al. 2013); and post-error
25 slowing (Rabbitt 1966), defined as a longer RT in the trial following an error (RT_{n+1}), is
26 often used to measure behavioral adjustments after errors.
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55 Thus, in the current study we take advantage of natural variation in the RT_{EC} as a proxy
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3 for parametric variation in the salience of an error, permitting us to evaluate whether the
4 evidence accumulation framework might account for various aspects of error correction.
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6 Specifically, as linked by RT_{EC} values, we analyze whether early error-monitoring
7 mechanisms are associated with subsequent variation of Pe latency, and whether later
8 post-error adjustments covary with error-monitoring and evidence accumulation
9 processes. We predicted the following: (1) faster (slower) RT_{EC} will be associated with
10 an increased (decreased) amplitude of early ERN monitoring processes; (1) faster
11 (slower) RT_{EC} will be associated with shorter (longer) Pe latencies; and (3) faster
12 (slower) RT_{EC} will be associated with both increased (reduced) inter-trial alpha power,
13 and reduced (increased) behavioral slowing on the next trial. In testing these predictions
14 via the RT_{EC} , we seek to determine whether previous error-related findings within the
15 literature can be linked to an accumulator model of error correction.
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34 **Methods**

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36 *Participants.* Fifteen UC Berkeley students participated in the experiment in exchange
37 for monetary compensation. One participant was excluded for failing to follow task
38 instructions. Two more subjects were rejected from the EEG analysis due to excessive
39 motion and muscle artifacts. Twelve students were included in the final analysis (nine
40 female) ages 18-25 (mean 20.3 ± 2.0). All subjects gave written informed consent in
41 accordance with the Committee for the Protection of Human Subjects at the University of
42 California, San Francisco and University of California, Berkeley. Subjects were right-
43 handed and had normal or corrected-to-normal vision.
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Procedure. A total of 100 pictures of male and female faces unknown to our subjects were used in the experiments (Navarro-Cebrian et al. 2013). They were converted to black and white and resized to 113 x 151 pixels using Adobe Photoshop CS4 (Adobe Systems, San Jose, CA). Targets subtended 2.55 degrees of visual angle. Pictures were obtained from one of the authors (ANC) and from the Face Database of the Max-Planck Institute for Biological Cybernetics in Tübingen, Germany (<http://faces.kyb.tuebingen.mpg.de>; Troje and Bulthoff 1996). The task was presented using Presentation software (Neurobehavioral Systems, Inc.).

Participants were presented with a previously validated version of the Flanker task (Navarro-Cebrian et al. 2013) designed to produce intermittent errors (Figure 1). All trials contained five high contrast (black and white) human faces, and participants were asked to respond via button press with their right hand (index and middle fingers) whether the target (middle) face was upright or upside down. The trial started with a fixation cross for 200 ms. After the cross disappeared, four flanker faces were shown alone for 80 ms and then together with the target (middle face) for an additional 30 ms. In order to make the task more difficult, the flanker faces could be congruent or incongruent with the target regarding the orientation of the face. After the flanker and target faces disappeared, a group of 5 asterisks was presented in the middle of the screen for 500 ms to indicate when to respond. Importantly, subjects were required to correct themselves as quickly as possible whenever they realized they had made an error by pressing the correct button (giving rise to a second RT denoted as the reaction time taken to correct the error, or RT_{EC} ; see below). An additional inter-trial interval of 550 ms preceded the next trial.

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6 *Behavioral analysis.* Only those trials in which subjects made an error and corrected
7 themselves were used for analysis. Trials were sorted by the reaction time for the second
8 motor response in each error trial – i.e. the RT_{EC} , as determined by the latency of the
9 correction minus the latency of the initial (erroneous) response. We created 2 groups of
10 trials for which the RT_{EC} values were well-differentiated. Based on the RT_{EC} distribution
11 for each subject, in one group trials with a RT_{EC} equal to or shorter than the 25th
12 percentile within subjects were included; in the other group, trials with an RT_{EC} equal to
13 or greater than the 75th percentile within subjects were included. These quartiles were
14 chosen for analysis in order to maximize potential differences in error salience while
15 retaining an adequate number of trials for comparisons. Additionally, we evaluated
16 possible differences in reaction times in the trials following errors (post-error trials;
17 RT_{n+1}), in order to study the relationship to post-error slowing. We predicted that the
18 uncertainty generated in some trials by reduced evidence for the error should lead to
19 slower reaction times in the trials after the errors (i.e. greater post-error slowing).
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41 *EEG procedure.* As noted above, two subjects were rejected from the EEG analysis due
42 to excessive motion and muscle artifacts. EEG data were collected from 64 channels at a
43 sampling rate of 512 Hz (Biosemi; <http://www.biosemi.com>). The Biosemi ActiveTwo
44 system allows low-noise recordings free of interference consisting of a feedback loop
45 between an electrode (CMS) and a passive electrode (DRL- see
46 www.biosemi.com/faq/cms&drl.htm for more details). Vertical and horizontal eye
47 movements were recorded using four electrooculography electrodes placed at the outer
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3 canthi of the right and left eyes, and above and below the right eye, aligned with the
4 pupil. EEG data analysis was performed using MATLAB scripts based on functions from
5 the EEGLAB toolbox (Delorme and Makeig 2004). The data were re-referenced offline
6 to an average reference and filtered to remove frequencies > 50 Hz and < 0.3 Hz.
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8 Portions of continuous data with excessive artifacts were rejected after visual inspection.
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10 In addition, independent components were estimated for individual subjects using the
11 filtered but unsegmented EEG data to identify and remove eye movement and muscular
12 artifacts. ICA decomposition relied on the independent component analysis functions of
13 EEGLAB (“runica” algorithm). 64 ICA components were identified for each subject and
14 IC scalp topographies, time courses, and spectral characteristics were inspected visually
15 to identify and reject components related to blinks and eye-movements (Jung et al.,
16 1998).
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35 *Event-related potential analysis.* Data were segmented and time locked to the onset of
36 the first motor response for analysis of the ERN and the Pe components. Epochs were
37 created starting 500 ms before the onset of the error and finishing 1000 ms after it. A pre-
38 stimulus time window from -500 ms to the onset of the initial stimulus was used as a
39 baseline. First, we calculated the amplitude of the error-related negativity (ERN), an ERP
40 originating in the mPFC and associated with conflict monitoring and uncertainty (Van
41 Veen and Carter 2002; Navarro-Cebrian et al. 2013). For the ERN component, three
42 frontocentral electrode sites were selected for analysis (Fz, FCz, and Cz). As in our
43 previous research (Navarro-Cebrian et al. 2013), the average minimum amplitude
44 between -20 and 50 ms around the onset of the response was calculated to measure the
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3 activity of the ERN component. Next, we analyzed the error-related positivity (Pe) to
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5 examine whether the reaction time for the error correction (RT_{EC}) varied with the Pe
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7 latency. The Pe latency was defined as the time to the most positive point in the epoch for
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9 the average of three centro-parietal electrodes (CP1, CPz and CP2). Statistical analyses
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11 were performed in SPSS (Statistical Package for Social Sciences 15.0 for Windows).
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13 Comparisons were made using the Fisher least significant difference test (LSD) and T
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15 tests.
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22 *Time-frequency analysis.* Time-frequency calculations were computed using MATLAB
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24 scripts based on functions from the EEGLAB toolbox. Specifically, we used the
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26 “newtimef” function available for EEGLAB to calculate the event-related changes in
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28 spectral power relative to baseline (event-related spectral perturbation; ERSP). The use of
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30 the Morlet wavelet decomposition in this function allows power changes to be observed
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32 in both the time and frequency domains, in contrast with fast Fourier transform methods
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34 that only have resolution in the frequency domain. Wavelet cycles began at 3 and
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36 increased with frequency reaching half the number of cycles in the equivalent fast Fourier
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38 transform window at its highest frequency. Data were filtered to remove frequencies > 50
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40 Hz and < 0.3 Hz. We were interested in the power of the theta band as a measure of error
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42 monitoring (Luu et al. 2004; Debener et al. 2005; Trujillo and Allen 2007; Navarro-
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44 Cebrian et al. 2013). To study frontal theta band power, epochs were created starting
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46 2000 ms before the onset of the error and finishing 2000 ms after it. Values from 1000 to
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48 500 ms before the error were used as a baseline to avoid border and edges artifacts. As
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50 for the ERPs, RT_{EC} duration was used to evaluate other segments of the trial by
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3 separating epochs into two conditions (fast and slow RT_{EC}). Frequencies of 4-7 Hz were
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5 used to study the theta band in the FCz channel, as the electrode site FCz is in the most
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7 representative location for post-error monitoring activity and has been used in previous
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9 research (Cavanagh et al. 2009; Navarro-Cebrian et al. 2013) to measure post-error theta
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11 power. Time series were plotted and differences in latency and amplitude of fronto-
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13 central theta activity were calculated for the fast and slow RT_{EC} conditions by analyzing
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15 the maximum amplitude and the latency at which this maximum occurred from -500 to
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17 500 ms around the error.
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25 In addition to the fronto-central theta power analysis, we calculated whether fronto-
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27 central theta phase values were consistent over trials (inter-trial coherence, or ITC) in the
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29 FCz channel. ITC was calculated with the “std_its” function of eeglab. Phase coherence
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31 values range from 0 to 1, ‘0’ indicating random phases and ‘1’ indicating perfect phase
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33 locking to the response across trials. We compared the ITC values for fast and slow RT_{EC}
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35 in the same time window as the ERN and for the theta band (4 to 7 Hz, as above). Since
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37 the ERN has been suggested to emerge from the theta activity phase locked to the
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39 response (Luu et al. 2004), we predicted that the ITC results would agree with those
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41 obtained for the ERN. A greater ITC value at the time of the response would demonstrate
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43 more synchronization between activity within the medial prefrontal cortex and the
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45 manual response (error).
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54 Lastly, in addition to post-error behavioral changes (post-error slowing), we studied post-
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56 error neural adjustments by analyzing the inter-trial interval for differences in alpha band
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power. Here we evaluate whether alpha power varies with the degree of error salience. Epochs were created starting 2000 ms before stimulus onset and finishing 2000 ms afterward. Values from 1000 to 500 ms before the onset of the stimulus were used as a baseline. The time window from 300 to 500 ms within the inter-trial interval was used for analysis during which decisions and manual responses (corrections) no longer took place. Specifically, although participants could take longer than the 500 ms correction time window to correct themselves, no error correction was detected within the ITI after an additional 300 ms on any trial. Based on previous research into alpha suppression (Carp and Compton 2009), frequencies of 10-14 Hz were included in the analysis and one posterior midline channel location (Pz) was chosen as a representative electrode (Carp and Compton 2009; Navarro-Cebrian et al. 2013). As for the other ERP and time-frequency analyses, two groups were created and included in the analysis based upon the reaction time to the error (fast and slow RT_{EC}).

Results

Behavioral results. Subjects completed an average of 895 trials (SD = 5.45, range = 882-900). They made an average of 148 errors (16.5% of the total number of trials, SD = 40.46, range = 91-211). The average reaction time for error correction (RT_{EC}) was 212 ms (SD = 45, range across subjects = 154-284). In keeping with previous literature, these error correction reaction times were quite rapid, suggesting that the process for movement correction begins very early in the trial (Higgins and Angel 1970; Schmidt and Gordon 1977; Fiehler et al. 2004; Christensen et al. 2008). In contrast, the average RT for the initial erroneous response in the error trials (i.e. the instigating error, or RT_E) was

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3 349 ms (SD = 41, range = 266-420), and the average RT for correct trials was 417 ms
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5 (SD = 34, range = 358-478). Consistent with other work (Gehring et al. 1993; Ratcliff
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7 and Rouder 1998; Pailing et al. 2002; Navarro-Cebrian et al. 2013), the RT_E was
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9 significantly shorter than the RT for correct responses ($t(11) = 7.58, p < 0.0001$).

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15 Based on the RT_{EC} , trials were then sorted to create 2 groups: one with trials in which
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17 RT_{EC} was equal to or less than the 25th percentile (within subjects), and one with trials in
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19 which the RT_{EC} was equal to or greater than the 75th percentile. The average RT_{EC} for the
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21 group of trials with the faster error corrections was 126 ms (SD = 43; range across
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23 subjects = 64-183 ms) and for the group of trials with the slower error corrections was 326
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25 ms (SD = 69; range across subjects = 243-467 ms). The corresponding RT_E for the group
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27 of trials with the faster error corrections was 370 ms (SD = 35; range = 326-447 ms) and
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29 for the group of trials with the slower error corrections was 322 ms (SD = 54; range =
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31 183-397 ms), both of which remained faster than for correct responses ($t(11) = 5.45; p <$
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33 0.001 and $t(11) = 7.07; p < 0.0001$, respectively) and differed significantly from each
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35 other ($t(11) = 4.1; p = 0.002$).

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43 One theory suggests that a single evidence accumulation process begins at stimulus onset
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45 (Maylor and Rabbitt 1989; Rabbitt 2002), and that the error correction response reflects
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47 not a separate error-related process, but rather the correct outcome of evidence
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49 accumulation related to the initial stimulus. Under such a theory, calculating the RT_{EC}
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51 from the time of stimulus onset (RT_{EC-SO}), rather than from the time of the initial
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53 erroneous response, might equalize average RT values for the fast and slow RT_{EC} trials.
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3 In contrast, if the RT_{EC} represents the outcome of a separate (or interacting) error-related
4 process, fast and slow RT_{EC} trials, when locked to the stimulus, should continue to give
5 rise to different RT_{EC-SO} values. To test this idea, we calculated this new stimulus-locked
6 RT_{EC-SO} value relative to the onset of the stimulus for the original fast and slow RT_{EC}
7 groups, rather than relative to the onset of the error. The RT_{EC-SO} remained significantly
8 slower for the slow RT_{EC} condition in comparison with the fast RT_{EC} condition (fast
9 $RT_{EC-SO} = 496$ ms; slow $RT_{EC-SO} = 647$ ms; $t(11) = 10.18$; $p < 0.0001$).

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12 Additionally, the combination of congruent and incongruent trials in the current
13 experiment, which was motivated by the need to collect as many trials as possible in each
14 condition, raises the possibility that fast (slow) RT_{EC} trials might consist of a
15 disproportionate number of congruent (incongruent) trials. To rule out this concern, we
16 analyzed the number of each type of trial for each condition. No significant differences
17 were found between the two conditions in the number of congruent ($t_{(11)} = 1.39$; $p = 0.19$)
18 and incongruent ($t_{(11)} = 0.29$; $p = 0.78$) trials.

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41 *ERP results.* To study whether the ERN or Pe activities were related to the RT_{EC} , we
42 compared the fast RT_{EC} and slow RT_{EC} conditions for the frontal and parietal components
43 of interest (ERN and Pe) evoked by errors – specifically, the amplitude of the ERN and
44 the latency of the Pe. We found significant differences between RT_{EC} conditions (Figure
45 2): pairwise comparisons (Fisher, LSD) showed that the fast and slow RT_{EC} conditions
46 were significantly different at the time of the ERN ($p = 0.027$) and the Pe ($p = 0.048$)
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3 signals. This finding was manifest as enhanced ERN activity and shorter Pe latency for
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5 the fast RT_{EC} condition.
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10 *Time-frequency results.* We then analyzed changes in theta power after errors. Statistical
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12 analyses demonstrated significant differences in the latency ($t(11) = 4.16$; $p = 0.002$), but
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14 not in the amplitude ($t(11) = 0.61$; $p = 0.56$ (ns)) of the theta power in FCz at the time of
15
16 the error. Figure 3a shows an earlier peak of the theta power for the fast RT_{EC} (20 ms
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18 after the error) compared to the slow RT_{EC} (100 ms after the error). We also found that
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20 compared to the slow RT_{EC} condition, the fast RT_{EC} condition showed increased inter-
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22 trial coherence (ITC) for theta activity locked to the response across trials ($t(11) = 9.93$; p
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24 = 0.002; Fig 3b).
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32 A diminished alpha power after errors, compared with correct responses, has been
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34 suggested to be indicative of higher alertness and reflective of neural adjustments (Carp
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36 and Compton 2009; Navarro-Cebrian et al. 2013). Time-frequency analyses were
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38 performed to test whether there was less post-error alpha power in those cases in which
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40 reduced frontal activity in monitoring areas led to greater uncertainty about performance
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42 and a slower reaction time to the error. Significant differences in power in the alpha band
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44 were found between the fast and slow RT_{EC} in the inter-trial interval ($t(11) = 5.21$; $p =$
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46 0.0003; Figure 4 dashed box), indicating less alpha power in the slow RT_{EC} condition.
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53 *Post-error behavioral adjustments.* Finally, we calculated the reaction times in the trials
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55 following the errors (post-error trials) to assess differences in post-error slowing (Figure
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3 4). Trials following correct responses (average RT_{n+1} of 399 ms) did not differ
4 significantly from trials following faster error corrections (average RT_{n+1} of 402 ms;
5 correct responses versus fast correction trials: $t(11) = 0.77$, $p = 0.46$). In contrast, trials
6 following slower error corrections had an average RT_{n+1} of 418 ms, which was
7 significantly longer than RTs following correct trials ($t(11) = 2.75$; $p = 0.019$) and fast
8 correction trials ($t(11) = 2.99$; $p = 0.012$). These results indicate increased post-error
9 slowing in the cases in which subjects took a longer time to respond to the error.
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20 21 22 **Discussion**

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24 In order to investigate the role of evidence accumulation in error correction, we took
25 advantage of natural variation in error salience to define fast and slow error correction
26 trials and to evaluate differences in conflict monitoring, decision-making, and post-error
27 adjustments. Previous EEG studies (O'Connell et al. 2012; Kelly et al. 2013) have
28 characterized a centro-parietal electrical signal that increases with incoming evidence and
29 peaks at the time of response execution. This signal shares characteristics with the
30 classical P3b and, based on similarities between the P3b and the Pe (Ridderinkhof et al.
31 2009; Ullsperger et al. 2010), has led to proposals that the Pe indexes the accumulation of
32 evidence for the existence of an error (Steinhauser and Yeung, 2012). Consistent with
33 this notion, here we found that the amplitude of early monitoring signals was greater, and
34 the latency of the Pe was shorter, when subjects rapidly corrected themselves.
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36 Furthermore, we determined that post-error cognitive and behavioral adjustments
37 depended upon this decision-making process and, along with the latency of the Pe, varied
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3 with the RT_{EC} . Together these signals define a potential sequence of events that underlies
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5 error correction.
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10 *Error monitoring processes.* The earliest signal in this sequence of EEG events – activity
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12 of the mPFC – has long been a focus of attention in EEG studies that analyzed activity in
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14 fronto-central electrodes after errors using ERPs (ERN signal – Gehring et al 1993;
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16 Endrass et al. 2007, 2012; O’Connell et al. 2007; Shalgi et al. 2009) or time-frequency
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18 analysis, specifically in the theta band (Luu et al. 2004; Debener et al. 2005; Trujillo and
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20 Allen 2007; Cohen et al. 2008; Cavanagh et al. 2009; Cohen and Cavanagh 2011;
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22 Cavanagh et al. 2012). Here we demonstrate that the amplitude of the ERN differs
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24 between fast and slow RT_{EC} conditions, suggesting a relationship between this signal and
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26 error correction. As in a previous study (Rodriguez-Fornells et al. 2002), our data showed
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28 a larger amplitude of the ERN in fast corrections compared with slow corrections, while
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30 the latency of this EEG signal was not affected.
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39 Contrary to the results for the ERN amplitude, we did not find differences in the
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41 magnitude of the theta power. This discrepancy in our results may be explained by the
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43 fact that while the magnitude of the theta power is similar in both conditions (Figure 3
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45 A), a greater amount of the theta activity is phase-locked to the response in the fast RT_{EC}
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47 trials. This result agrees with the idea that the ERN component emerges from phase
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49 locking of theta band EEG activity (Luu and Tucker 2001). Although early viewpoints
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51 argued that ERPs result from an evoked neural response to an event (Hillyard and Picton
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53 1987), recent theories suggest that environmental events induce partial ‘phase resetting’
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3 of ongoing neural activity (Makeig et al. 2002; 2004). Such phase locking has been
4 suggested to correlate with performance (Yamagishi et al. 2008) and to be affected in
5 neurological conditions such as schizophrenia (Ford et al. 2007) and Alzheimer's disease
6 (Pijnenburg et al. 2004). Consistent with the importance of such synchronization to
7 behavior, intra-area inter-trial phase synchrony (ITC) provided a direct measure of neural
8 synchrony (Makeig et al. 2002) that identified greater phase locking of ongoing theta
9 activity in mPFC for fast versus slow RT_{EC} . Thus, for those trials in which the monitoring
10 activity of the mPFC and the motor response are more synchronized, there is improved
11 error signaling and faster error correction.
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27 Lastly in relation to the ERN results, it is important to note that, supporting previous
28 findings (Pailing et al. 2002), larger ERN amplitudes were preceded by slower RT_E ,
29 Pailing and colleagues suggested that the magnitude of ERN monitoring activity may
30 reflect individual differences in response control or impulsive behavior. Following that
31 logic, the authors showed that participants with larger mean ERN amplitudes had slower
32 RT_E , suggesting a less impulsive response strategy by those individuals. In our data, the
33 fact that larger ERN amplitudes across trials, rather than individuals, are preceded by
34 significantly slower RT_E and followed by faster RT_{EC} , further suggests that differences in
35 response control vary significantly from trial to trial within individuals.
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51 *The error-related positivity (Pe) and performance decision-making.* This initial medial
52 prefrontal signal (ERN) has been hypothesized to relate to the detection of response
53 conflict (Van Veen and Carter 2002), among other theories of medial PFC function after
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3 errors (i.e. Holroyd and Coles 2002). If true, greater response conflict should correspond
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5 with greater likelihood of an error, and evidence accumulation processes should integrate
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7 more rapidly to an error detection threshold when greater response conflict is present
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9 (Ullsperger et al. 2010). The error positivity or error-related positivity (Pe) is a parietal
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11 electrical signal evoked by errors in comparison with correct responses (Falkenstein et al.
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13 2000; Shalgi et al. 2009). Recent studies (Ridderinkhof et al. 2009; Ullsperger et al.
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15 2010) have argued that this signal is related to the motivational significance of the error
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17 in the same way that another well-known parietal ERP, the P3b, is related to the
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19 motivational significance of infrequent stimuli (e.g. oddballs). Our results show that the
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21 latency of the Pe varies with the RT_{EC} , possibly reflecting the accumulation of evidence
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23 for the error that is needed to make a correction. This theory would state that at the time
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25 of the Pe, different sources of information signaling the error contribute to integration in
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27 parietal areas until the evidence becomes strong enough to make a decision about the
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29 performance (Ullsperger et al. 2010). These results support previous data that found a
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31 modulation of the Pe amplitude when the level of the decision criterion was varied
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33 (Steinhauser and Yeung 2010; Orr and Carrasco 2011).
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44 Interestingly, this link, via the RT_{EC} , between earlier frontal and later parietal signals
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46 agrees with previous EEG studies (Philiastides and Sajda 2006; Philiastides et al. 2006)
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48 of perceptual decision-making that detected a frontal ERP component occurring
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50 approximately 220 ms after the onset of the stimulus (possibly reflecting the typical N2
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52 ERP). This component varied with the level of the perceptual difficulty and predicted the
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54 onset of a later component related to evidence accumulation (which could reflect the CPP
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3 or typical P3b ERP). Together, these findings suggest that future work might further
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5 explore interactions between earlier frontal and later parietal signals as a general
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7 mechanism in both the processing of errors (ERN and Pe) and perceptual stimuli (N2 and
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9 P3b; Wessel et al. 2012).

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15 More broadly, these data agree with other EEG work supportive of a centro-parietal
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17 evidence accumulation mechanism. Recent EEG studies (O'Connell et al. 2012; Kelly et
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19 al. 2013), for example, have characterized a brain electrical signal that shares properties
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21 described by models of this process in primates and humans (Ratcliff and McKoon 2008).
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23 Interestingly, this signal, called the centro-parietal positivity (CPP), shares characteristics
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25 with the P3b signal (O'Connell et al. 2012). Although early studies touched on decision-
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27 making in relation to the P3b (Smith et al. 1970), the most influential theory, the context-
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29 updating model (Donchin 1981), states that the P3b is related to a memory update
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31 process. According to this theory, the brain constantly generates hypotheses about the
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33 environment, with the P3b signal generated every time that the environment changes and
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35 the context representation needs to be updated. However, newer studies (Nieuwenhuis et
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37 al. 2001; O'Connell et al. 2012; Kelly et al. 2013) suggest a re-evaluation of previous P3b
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39 results to consider this slow EEG potential as a dynamically evolving component rather
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41 than the culmination of a unitary event (Kelly et al. 2013).
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51 *Post-error adjustments: alpha power and post-error slowing.* Once conflict is detected
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53 and evidence for an error has reached threshold, not only must a correction be made, but
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55 behavioral modifications must also be implemented to avoid the occurrence of further
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3 errors in the future. In EEG studies, suppression of the inter-trial interval (ITI) alpha
4 power, for example, is used to measure an increase in cortical arousal (Carp and Compton
5 2009; Compton et al. 2011, 2013, 2014; van Driel et al. 2012) that may be interpreted as
6 cognitive adjustments occurring after an error is made (Navarro-Cebrian et al. 2013). An
7 increase in alpha power, mainly in posterior areas, often occurs when subjects finish a
8 trial and wait for the next one to start. This alpha in the ITI is considered a sign of task
9 disengagement, and its increase is suppressed when one's behavior deviates from a goal.
10 In other words, greater alpha suppression after errors suggests higher alertness. In the
11 present study, those trials accompanied by longer RT_{EC} were associated with less alpha
12 power, suggestive of higher alertness following these more uncertain errors. Such
13 findings are consistent with the reduced confidence associated with trials in which
14 evidence accumulates more slowly (Kiani and Shadlen 2009).
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34 In accordance with these results, subjects also slowed down after more uncertain errors
35 (i.e. errors that took longer to correct). Post-error slowing is often defined as longer RTs
36 in trials following errors in comparison to correct responses (Rabbitt 1966). In our study,
37 the fact that RT_{EC} values covaried with activity of mPFC and parietal cortex, as well as
38 the degree of post-error slowing, suggests that signaling in the frontal and parietal
39 cortices may influence these later processes. Interestingly, not all studies have found the
40 same relationship between the ERN and the degree of post-error slowing. In contrast
41 with our finding of an inverse relationship (i.e. faster RT_{EC} is associated with both a
42 greater ERN and lesser post-error slowing), Gehring and colleagues found a greater ERN
43 to be followed by greater post-error slowing (Gehring et al. 1993). One possibility for
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3 this discrepancy relates to the nature of the ERN itself. As shown previously, ERN
4 amplitude is increased by perceptually difficult stimuli (Philiastides et al. 2006), possibly
5 reflecting uncertainty at the stimulus phase (Navarro-Cebrian et al. 2013); in contrast,
6 internal fluctuations in monitoring areas at the time of the response may result in a
7 smaller ERN. As a result, including trials following errors related to stimulus uncertainty
8 rather than motor failures might predispose to finding a direct relationship. A second
9 possibility is that the nature of the relationship between ERN amplitude and post-error
10 slowing may be driven by a more proximate signal – i.e. the latency of the Pe. A third
11 possibility has to do with our task design: because the ITI was relatively brief (550ms),
12 slower error correction may simply have impacted subjects' abilities to attend to the next
13 stimulus. We note that even the slowest of error correction responses had been
14 completed by 300ms into the ITI, and that subsequent alpha power also distinguished
15 these trials. Nonetheless, future work to explicitly vary the duration of the ITI would be
16 helpful.

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39 *Timing diagram for adaptive decision-making.* Taken together, our data link together
40 several findings from previous studies (Pailing et al. 2002; Rodriguez-Fornells et al.
41 2002; Steinhauser and Yeung 2010; Ullsperger et al. 2010; Wessel et al. 2011; Murphy et
42 al. 2012; Steinhauser and Yeung 2012) under a potential evidence accumulation
43 framework, and provide a hypothetical timing diagram for adaptive decision-making after
44 errors (Figure 5). Specifically, more cognitive control at the time of the selection of the
45 response (slower RT_E ; Pailing et al. 2002) may lead to a more accurate comparison
46 between the representation of the correct response and the efference copy of the
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3 (incorrect) motor commands. As a consequence, a greater mismatch and a larger ERN
4 will be observed in those trials (Pailing et al. 2002). Therefore, stronger error signaling in
5 these responses will lead to more rapid accumulation of evidence for the erroneous
6 response and a faster RT_{EC} .
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15 It is important to note that the RT_{EC} may occur quickly (average for fast RT_{EC} condition:
16 126 ms) following the initial erroneous response. These fast corrections, replicating
17 previous studies (e.g. Rodriguez-Fornells et al. 2002), may represent accumulation of
18 evidence for the error if they occur after the comparison of an efference copy of the
19 erroneous motor commands with the correct commands (Figure 5; Higgins and Angel
20 1970; Coles et al. 2001; Rodriguez-Fornells et al. 2002; Christensen et al. 2008).
21 Moreover, if this comparison between representations of correct and error responses is
22 triggered by the arrival of the efference copy (Coles et al. 2001), it may occur even before
23 the actual motor response (error) takes place. This last possibility may help us to
24 understand both the early latency of the ERN observed in this and previous studies (i.e.
25 Wiersema et al. 2007; Maier and Steinhauser 2013; Navarro-Cebrian et al. 2013) and the
26 fast error-correcting responses (RT_{EC}).
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46 An alternative account would argue that the processes necessary for conscious error-
47 signaling responses and subsequent corrections require more than 150 ms (Rabbitt 2002)
48 and that this type of fast correction may instead represent “delayed correct responses”
49 that are completed after impulsive errors (Maylor and Rabbitt 1989; Rabbitt 2002).
50 Following this idea, our rapid RT_{EC} values may be due to the continuation of the
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3 accumulation of the stimulus information without the explicit detection of the initial
4 error; they would therefore not reflect accumulation of evidence for having made an
5 error, and the Pe in the present example would simply be the continuation of the P3b in
6 relation to the processing of the stimulus. This account would be supported by the fact
7 that our task reflects error corrections rather than error signaling (Ullsperger and von
8 Cramon 2006). Our data suggest, however, that this possibility may not explain the early
9 latency found for the ERN, which in our and other work (i.e. Wiersema et al. 2007; Maier
10 and Steinhauser 2013; Navarro-Cebrian et al. 2013) can precede the motor response. An
11 additional complication for this account may come from the results of the RT_{EC} relative to
12 the onset of the stimulus (RT_{EC-SO}). We continue to observe significant differences
13 between the slow and fast RT_{EC-SO} conditions when those reaction times are calculated
14 relative to the onset of the stimulus. One might expect no differences between those two
15 RT_{EC-SO} values if evidence accumulation is related to the processing of the stimulus alone
16 (i.e. irrespective of the erroneous response) in both cases.
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39 Similarly, the argument might be made that fast and slow errors represent qualitatively
40 distinct cognitive processes – specifically, that unlike long values, fast RT_{EC} values
41 reflect a motor plan that has previously been initiated and that is ultimately implemented
42 without awareness of the error. In our previous work using this paradigm (Navarro-
43 Cebrian et al. 2013), we demonstrated that correct and unaware errors are characterized
44 by small ERN amplitudes that differ significantly from the large ERN amplitudes
45 accompanying aware errors. If rapid RT_{EC} values reflected a lack of error awareness, we
46 would expect that ERN amplitudes would be significantly smaller for fast RT_{EC} trials
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3 than for slow RT_{EC} trials. However, we find the opposite result, arguing that error
4 awareness cannot explain the difference between these trial types in this data set.
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10 *Conclusions.* The current data demonstrate how variation in error salience, as indexed by
11 the RT_{EC} , implicates areas previously associated with evidence accumulation in both the
12 evaluation of decisions and the implementation of compensations when those decisions
13 deviate from goals. Importantly, the study of error-related EEG signals within a
14 decision-making context allows us to describe a potential timing diagram for adaptive
15 decision-making when errors are made. Moreover, mechanisms of error correction,
16 beyond the initial detection of an error, may be relevant to therapies that address
17 behavioral change in patient populations. Future work might therefore investigate how
18 this sequence of events differs when the ability to monitor and then alter behavior is
19 impaired.
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37 **Figure Legends:**

38 Fig. 1. **Paradigm.** After a fixation cross, flanker faces (congruent or incongruent with the
39 target) were shown alone for 80 ms and then together with the target for 30 ms more.
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41 Participants were instructed to indicate with a button press whether the target was upright
42 or upside down. They were asked to correct themselves as fast as possible if an error was
43 made. An inter-trial interval of 550 ms was presented before the next trial started.
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53 Fig 2. **ERP responses.** The response-locked average in frontal electrodes (Fz, FCz, Cz) is
54 shown in the upper figure and response-locked average in parietal electrodes (CP1, CPz,
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3 CP2) is shown in the lower figure. Fast RT_{EC} (error correction) is shown in blue and slow
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5 RT_{EC} is shown in red. Panels show a greater ERN amplitude (Figure 2A) and a shorter Pe
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7 latency (Figure 2B) for the fast RT_{EC} condition.
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12 **Fig 3. Event-related changes in theta power.** A. Event-related changes in theta power
13 in the FCz channel. A decreased latency of the theta amplitude for the fast RT_{EC} condition
14 (fast error correction, in blue) can be seen in comparison with the slow RT_{EC} condition
15 (red). B. A greater inter-trial phase coherence (ITC) can be seen in the theta band for the
16 fast RT_{EC} condition (left) compared to the slow RT_{EC} condition (right) at the time of error
17 onset.
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29 **Fig 4. Post-error adjustments.** A. The reaction time (RT_{n+1}) for trials following correct
30 responses, trials following fast RT_{EC} errors (fast correction), and trials following slow
31 RT_{EC} errors (slow correction), respectively. The plot indicates a greater post-error
32 slowing (RT in the trial following the error) after trials with a slow RT_{EC} error. B. Less
33 alpha power can be seen in the inter-trial interval (dashed rectangle) in the slow RT_{EC}
34 condition (right) compared to the fast RT_{EC} condition (left).
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46 **Fig 5. Timing diagram for adaptive decision-making.** This diagram represents the
47 different cognitive processes (boxes), behavioral signatures (ellipses), and EEG signals
48 that derive from error processing, error correction and post-error adjustments. We
49 hypothesize that after the incorrect motor commands are selected, an efference copy of
50 these commands is generated and compared with the predicted correct response
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3 representation. An ERN signal will be elicited when a mismatch is produced, and a
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5 greater ERN will lead to more rapid corrections (Rodriguez-Fornells 2002). In addition,
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7 the ERN signal will correlate with the speed with which evidence for an error
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9 accumulates (Ullsperger et al. 2010) so that a greater ERN signal will lead to a faster
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11 evidence accumulation process, as reflected in the latency of the Pe signal (Murphy et al.
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13 2012). Lastly, these differences in cognitive control and decision-making after the initial
14
15 error will influence post-error cognitive and behavioral adjustments. When participants
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17 more easily identify their errors (more cognitive control) and correct them quickly, they
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19 are better able to disengage during the ITI (more alpha power), and these errors will have
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21 a reduced influence on the next trial (reduced post-error slowing).
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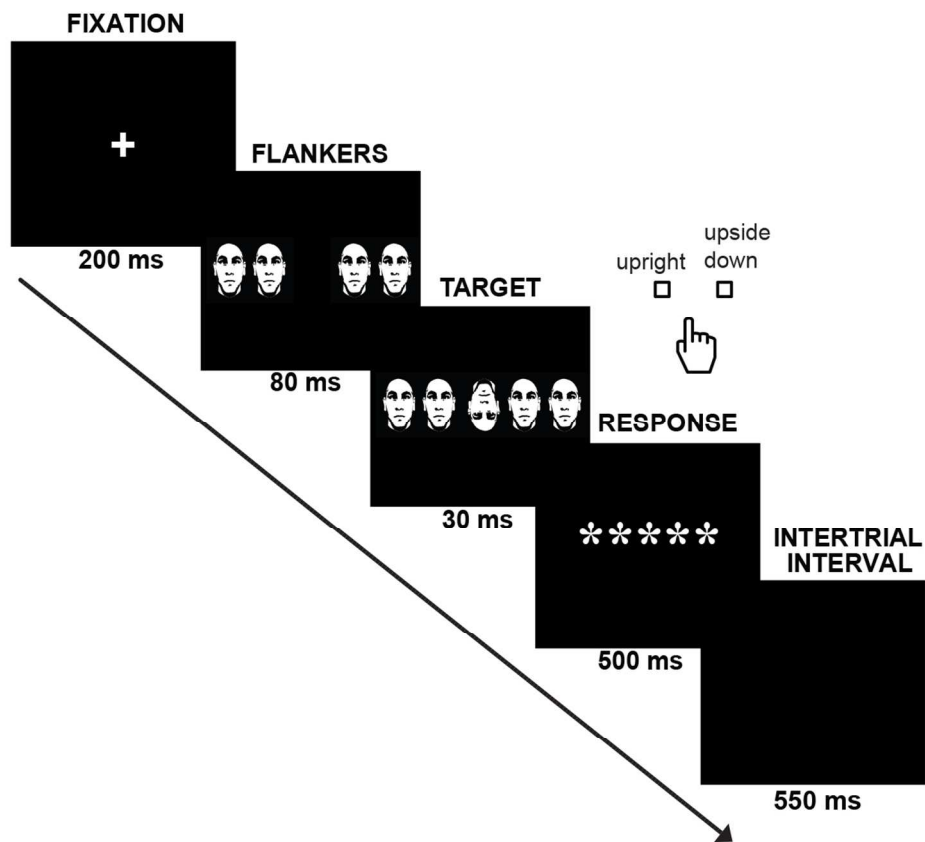


Figure 1
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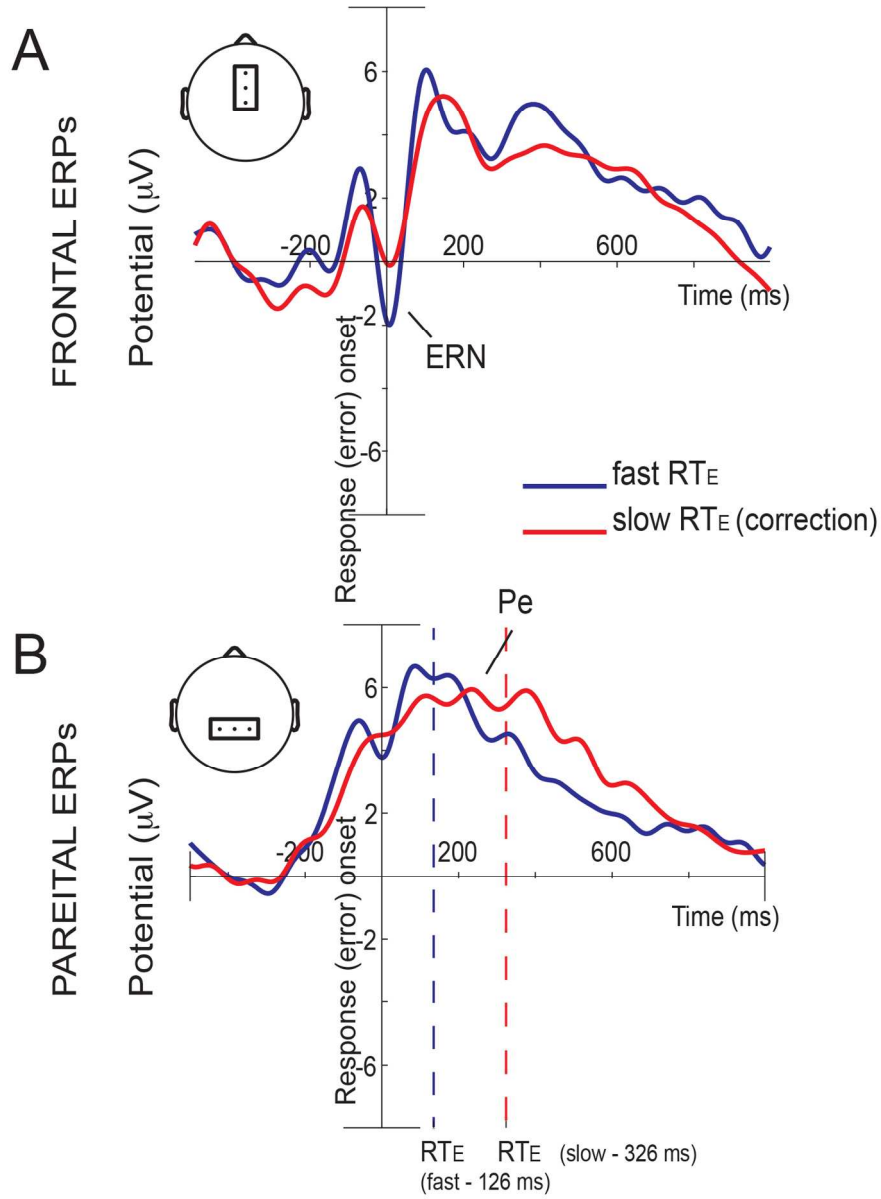


Figure 2
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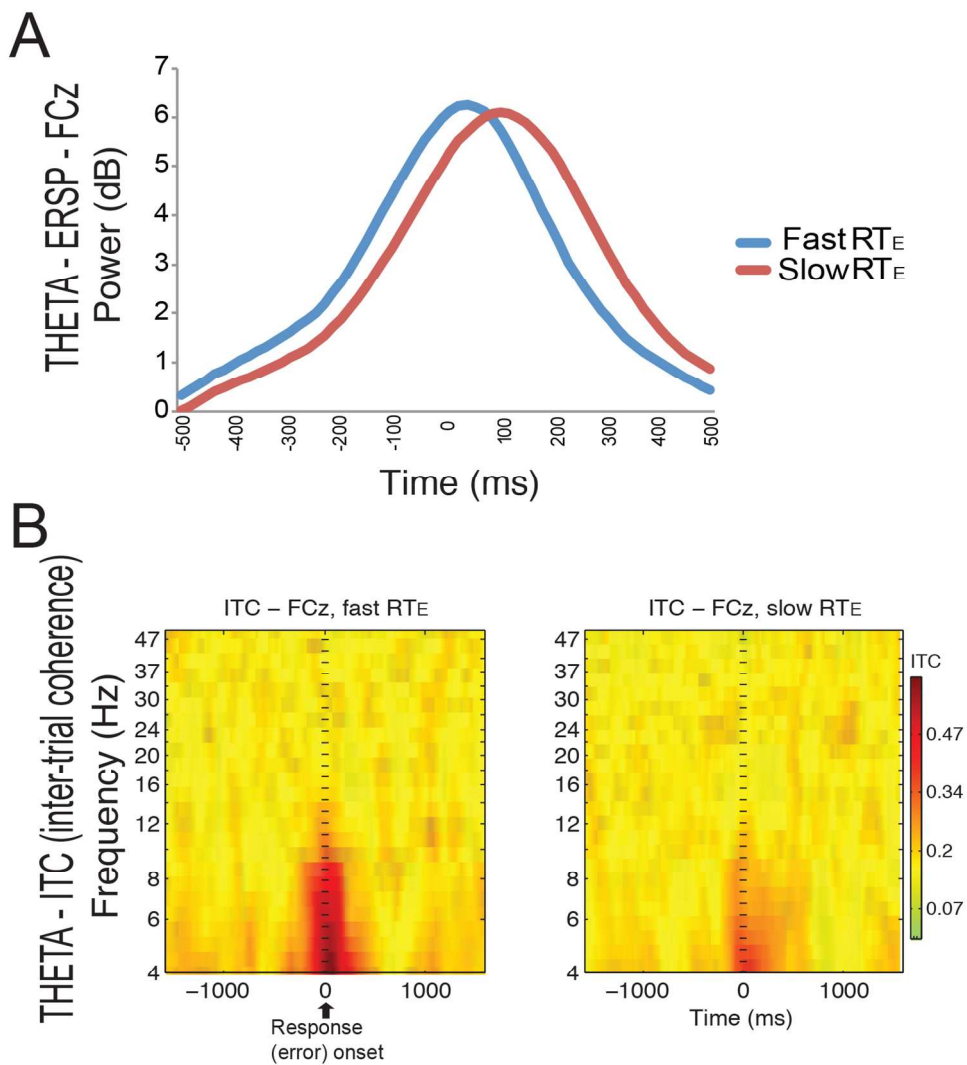


Figure 3
138x150mm (300 x 300 DPI)

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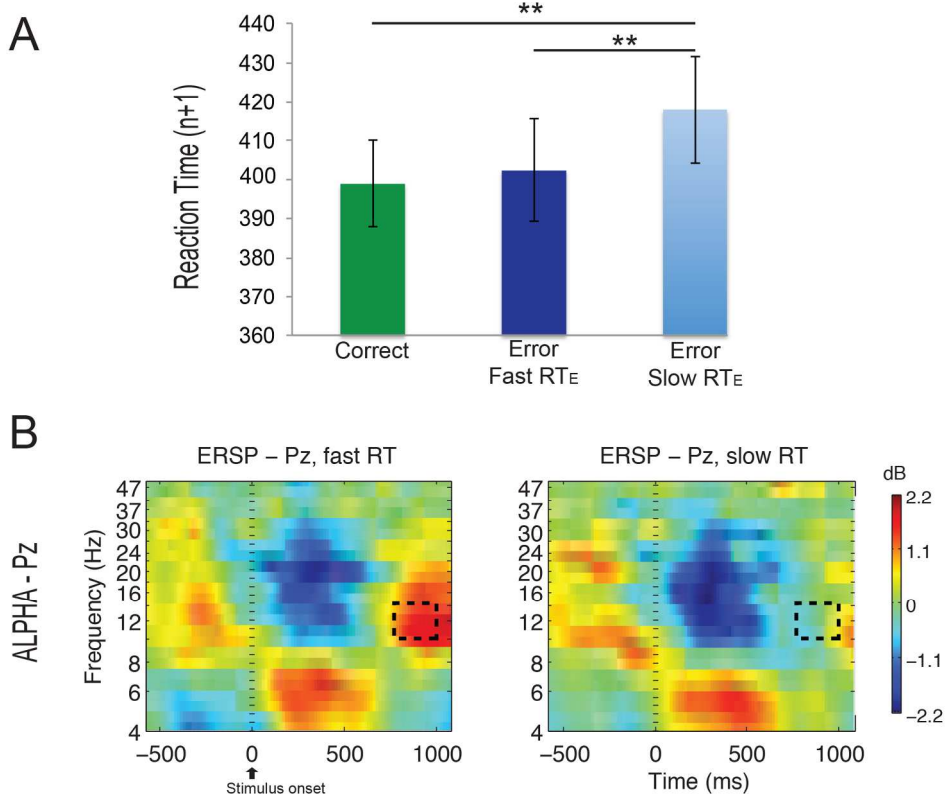


Figure 4
186x149mm (300 x 300 DPI)

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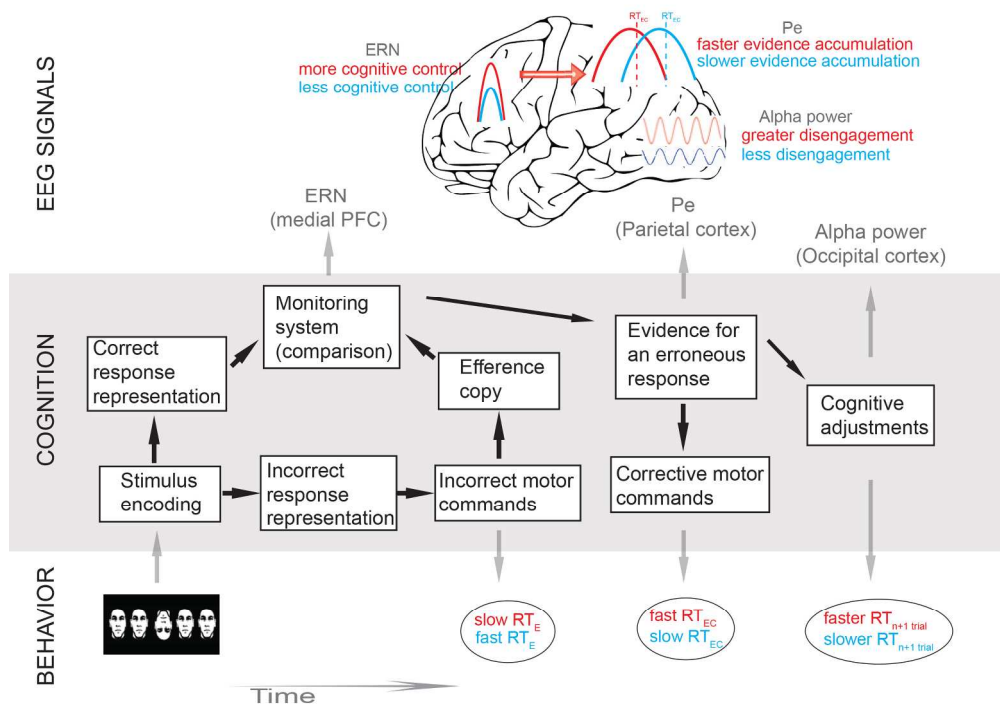


Figure 5
211x153mm (300 x 300 DPI)

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