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# Combined Benefit of Quantitative Three-Compartment Breast Image Analysis and Mammography Radiomics in the Classification of Breast Masses in a Clinical Data Set

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Conflicts of interest are listed at the end of this article.

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**Purpose:** To investigate the combination of mammography radiomics and quantitative three-compartment breast (3CB) image analysis of dual-energy mammography to limit unnecessary benign breast biopsies.

**Materials and Methods:** For this prospective study, dual-energy craniocaudal and mediolateral oblique mammograms were obtained immediately before biopsy in 109 women (mean age, 51 years; range, 31–85 years) with Breast Imaging Reporting and Data System category 4 or 5 breast masses (35 invasive cancers, 74 benign) from 2013 through 2017. The three quantitative compartments of water, lipid, and protein thickness at each pixel were calculated from the attenuation at high and low energy by using a within-image phantom. Masses were automatically segmented and features were extracted from the low-energy mammograms and the quantitative compartment images. Tenfold cross-validations using a linear discriminant classifier with predefined feature signatures helped differentiate between malignant and benign masses by means of (a) water-lipid-protein composition images alone, (b) mammography radiomics alone, and (c) a combined image analysis of both. Positive predictive value of biopsy performed (PPV<sub>3</sub>) at maximum sensitivity was the primary performance metric, and results were compared with those for conventional diagnostic digital mammography.

**Results:** The PPV<sub>3</sub> for conventional diagnostic digital mammography in our data set was 32.1% (35 of 109; 95% confidence interval [CI]: 23.9%, 41.3%), with a sensitivity of 100%. In comparison, combined mammography radiomics plus quantitative 3CB image analysis had PPV<sub>3</sub> of 49% (34 of 70; 95% CI: 36.5%, 58.9%;  $P < .001$ ), with a sensitivity of 97% (34 of 35; 95% CI: 90.3%, 100%;  $P < .001$ ) and 35.8% (39 of 109) fewer total biopsies ( $P < .001$ ).

**Conclusion:** Quantitative three-compartment breast image analysis of breast masses combined with mammography radiomics has the potential to reduce unnecessary breast biopsies.

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Online supplemental material is available for this article.

Studies have shown that up to 60% of women screened with mammography over 10 years have at least one abnormal result, even though no breast cancer is present. Hence, reducing false-positive mammograms and false-positive biopsies could substantially lower the cost of screening (1–6). A promising approach to improve clinical decision support is radiomics. Although computer-aided detection has been part of the routine clinical assessment of screening mammograms in the United States, computer-aided diagnosis has been an area of active research for quite some time (7) but, to date, has not been approved by the U.S. Food and Drug Administration for mammography. Radiomics is an extension of computer-aided diagnosis and refers to the comprehensive quantification of tumor phenotypes by extracting a large number of quantitative

image features (8) for data mining and precision medicine. In recent years, investigators have shown success using radiomics for breast cancer, extracting a variety of clinically relevant features, merging them into signatures, and estimating the probability of malignancy of identified lesions (9–11). In addition, radiomics has been used to assess the risk of future breast cancer (12) and predict breast cancer prognosis (13,14). Observer studies have shown some improvement in radiologists' performances in diagnostic tasks when a computer aid is used (7,15,16).

There is a strong biologic basis as to why the microscopic features of a tumor produce macroscopically distinct compositions amenable to measurement. First, invasive cancer is highly angiogenic. Weind et al (17) compared the central to peripheral microvasculature of invasive

## Abbreviations

AUC = area under the receiver operating characteristic curve, CI = confidence interval, PPV<sub>3</sub> = positive predictive value of biopsy performed, 3CB = three-compartment breast

## Summary

When combined with mammography radiomics, the water-lipid-protein breast tissue composition measured with quantitative three-compartment breast image analysis may reduce unnecessary biopsies of benign breast masses and result in a higher positive predictive value of biopsy performed.

## Implications for Patient Care

- Three-compartment (water, lipid, and protein) breast imaging with noncontrast dual-energy mammography is readily implemented with existing digital mammography or tomosynthesis equipment and results in a 10% higher mean glandular dose of an average screening mammogram.
- Quantitative three-compartment breast (3CB) image analysis before breast biopsy provides predictive information about the malignant potential of breast lesions that cannot be obtained by visual interpretation of mammography alone.
- The combination of quantitative 3CB image analysis and mammography radiomics may reduce unnecessary biopsies of benign breast masses and result in a higher positive predictive value of biopsy performed in breast masses deemed suspicious by the breast radiologist.

tumors and fibroadenomas and found that vasculature differed substantially among normal tissue, fibroadenomas, and different grades of invasive ductal carcinoma. Second, Cerussi et al (18) found a 20% reduction in lipid and 50% elevation in water in invasive breast cancer versus normal breast tissue and a strong positive correlation ( $R = 0.98$ ) between the macroscopic water concentration and the Scarff-Bloom-Richardson score (a histologic grading scale ranging from 3 to 9 that accounts for tubule formation, nuclear pleomorphism, and mitosis counts [19]). Third, invasive cancers have been found to have significantly lower x-ray attenuation than fibroadenomas, suggesting a distinctly different composition between cancerous and benign masses. The kinetic blood flow differences due to differential vascularization of cancerous and benign tissues have been used to improve the diagnostic accuracy of gadolinium-enhanced MRI and mammographic methods, such as contrast material-enhanced digital mammography (20,21) and contrast-enhanced breast tomosynthesis (22,23). But MRI is expensive and contrast agents are invasive and potentially toxic. Three-compartment breast (3CB) imaging is a dual-energy mammography technique that does not require a contrast agent, is easily implemented with minimal changes in workflow of digital mammography (or breast tomosynthesis) equipment, and results in only a 10% higher dose over standard mammographic views (24). Three-compartment breast imaging

yields quantitative and reproducible pixel-by-pixel estimates of water, lipid, and protein thicknesses throughout the breast (24).

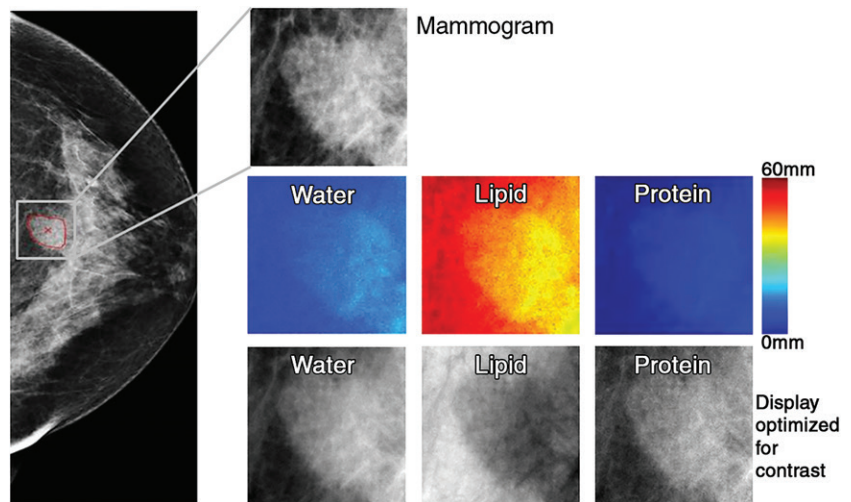
The aim of this study was to investigate the potential of mammography radiomics (lesion texture, size, shape, and morphologic characteristics), in vivo measurement of the biologic tissue composition derived from 3CB imaging with dual-energy mammography, and the two measures combined to avoid unnecessary benign biopsies. Hence, we were interested in decreasing the number of false-positive biopsy results and at the same time not missing invasive cancers that should undergo biopsy.

## Materials and Methods

This prospective diagnostic 3CB imaging clinical study was approved by the institutional review board and followed Health Insurance Portability and Accountability Act-compliant protocols. All study participants provided written informed consent.

## Study Participants

Women were recruited consecutively for participation in our study, and the inclusion criterion was presentation with Breast Imaging Reporting and Data System (BI-RADS) category 4 or 5 findings on the basis of diagnostic mammography (25). Exclusion criteria were previous biopsy in the same quadrant of the affected breast or systemic hormone therapy or chemotherapy. From 2013 through 2017, women with BI-RADS category 4 or 5 findings were identified after undergoing diagnostic mammography and approached for enrollment in our study immediately before breast biopsy at two clinical sites (University of California, San Francisco, San Francisco, Calif, and H. Lee Moffitt Cancer Center, Tampa, Fla). After providing written informed consent, study participants underwent unilateral dual-energy mammography of the affected breast with use of digital mammography equipment (Selenia; Hologic, Marlborough, Mass) to derive breast composition (24). The most common reason to decline study participation



**Figure 1:** Images in 71-year-old woman with 1.6-cm invasive ductal carcinoma (Breast Imaging Reporting and Data System category 5, with category C breast density). Low-energy mammogram and corresponding regions of interest for mammogram (top) and breast tissue composition images (bottom two rows).

**Table 1: Description of the 109 Women with Breast Masses Imaged with the Three-Compartment Breast Protocol for Our Current Study**

Parameter	No. of Women
<b>Age</b>	
<40 y	5 (4.6)
40 to <50 y	37 (33.9)
50 to <60 y	39 (35.8)
60 to <70 y	14 (12.8)
70 to <80 y	10 (9.2)
≥80	4 (3.7)
<b>BI-RADS breast density*</b>	
A	10 (9.2)
B	49 (44.9)
C	45 (41.3)
D	4 (3.7)
<b>Menopause status</b>	
Unspecified	1 (0.9)
Premenopause	40 (36.7)
Perimenopause	2 (1.8)
Postmenopause	67 (61.5)
<b>Postmenopause HRT (n = 67)</b>	
None	58 (87)
<5 y	5 (7.4)
≥5 y	4 (6.0)
<b>BMI (kg/m<sup>2</sup>)</b>	
<18.5	3 (2.8)
18.5 to <25	29 (26.6)
25 to <30	26 (23.8)
≥30	51 (46.8)
<b>BI-RADS assessment</b>	
4	98 (89.9)
5 <sup>†</sup>	11 (10.1)
<b>Pathologic finding</b>	
Invasive cancer	35 (32.1)
Benign	74 (67.9)
<b>Mass size (mm)<sup>‡</sup></b>	
<b>Invasive cancer (n = 35)</b>	
≤5	1 (2.9)
>5 but ≤10	3 (8.6)
>10 but ≤20	18 (51)
>20 but ≤50	13 (37)
>50	0 (0)
<b>Benign (n = 74)</b>	
≤5	3 (4.1)
>5 but ≤10	34 (46)
>10 but ≤20	28 (38)
>20 but ≤50	8 (11)
>50	1 (1.4)

Note.—Numbers in parentheses are percentages. BI-RADS = Breast Imaging Reporting and Data System, BMI = body mass index, HRT = hormone replacement therapy.

\* BI-RADS breast density is as follows: A = fatty, B = scattered fibroglandular tissue, C = heterogeneously dense, D = extremely dense.

<sup>†</sup> All BI-RADS category 5 masses were invasive cancers.

<sup>‡</sup> The maximum linear size was determined from radiologist-drawn lesion outlines; radiologist-drawn outlines were not used in the radiomics and quantitative three-compartment breast methods.

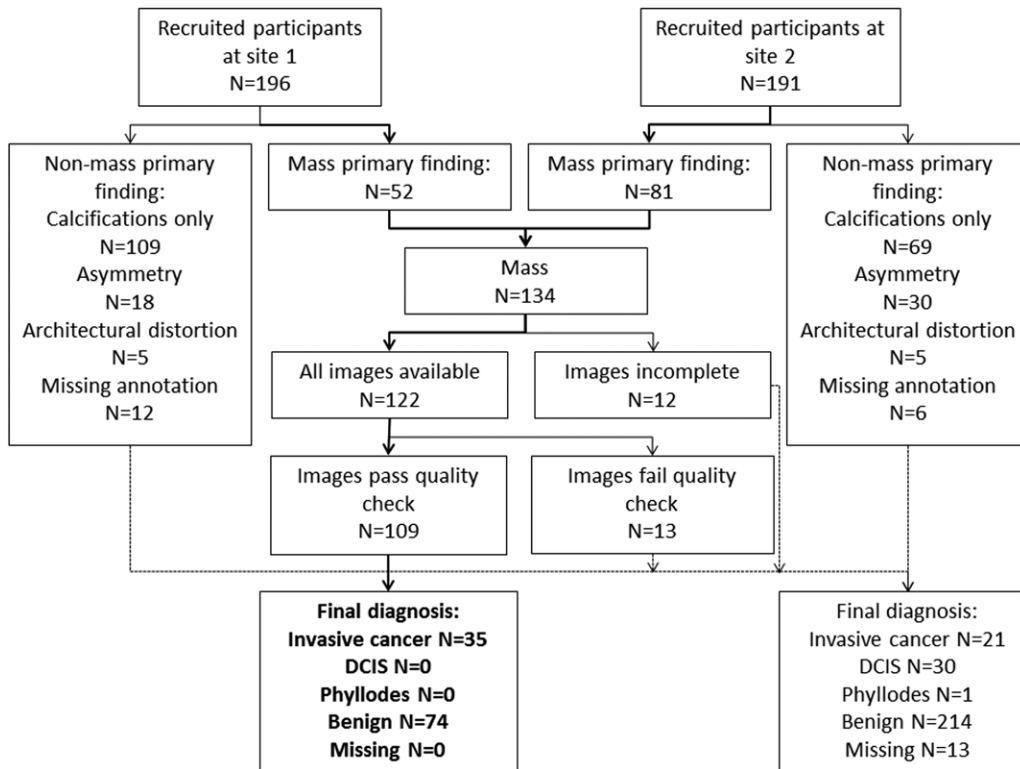
was the additional radiation exposure resulting from the need for additional views of the affected breast in addition to the previous clinical diagnostic views. However, the mammography equipment used in our prospective 3CB imaging study is approved by the U.S. Food and Drug Administration and, in future practice, 3CB imaging could replace conventional diagnostic digital mammography because low-energy mammography is performed under “standard” settings, eliminating the need for extra views.

### Computational Methods

Radiomic analysis was performed by using the low-energy mammograms (equivalent to mammograms acquired with conventional clinical settings) obtained in the “for processing” mode (craniocaudal and mediolateral oblique diagnostic images of 0.07-mm resolution). The corresponding quantitative breast tissue composition images, that is, the 3CB thickness maps of water, lipid, and protein, were derived from the dual-energy mammograms from the attenuation at both high and low energy in combination with an in-image phantom of known modeled compartment thickness combinations (0.14-mm resolution) (Fig 1; Appendix E1 [online]). The high-energy mammograms were used only to derive the 3CB thickness maps and were not otherwise analyzed.

Only in-house–developed software was used. The classification task of interest was the differentiation between malignant and benign breast masses. The mammography radiomics method required the approximate lesion center of the mass on a mammogram as determined from the lesion outline drawn by an expert radiologist. Each lesion was then automatically segmented (26), and lesion image features were extracted from the mammograms by using the computer segmentations (Appendix E2 [online]). For quantitative 3CB image analysis, features were extracted from the corresponding water, lipid, and protein composition images, again by using the computer segmentations (Appendix E1 [online]).

In our analyses, we used predefined lesion signatures, that is, predefined feature combinations, directly obtained from prior work on different data sets for both mammography radiomics (27) and quantitative 3CB (27,28). For mammography radiomics, a five-feature signature was used: the lesion size, average gray value, contrast, and two features describing a combination of mass shape and margin, which was derived in previous work from 432 biopsy-proven mass lesions imaged with a Senographe 2000D system (GE Medical Systems, Milwaukee, Wis) (27). For quantitative 3CB, a four-feature signature was derived from feature selection within pilot study data (no overlap with the current data set) of 45 breast lesions (including 27 masses, five of which were cancerous) (28,29). Because 3CB thickness maps are quantitative, “simple” quantitative 3CB features, such as mean and median of the water-lipid-protein compartment thicknesses within each mass and its surrounding parenchyma, were extracted (Appendix E1 [online]). Features selected from the pilot study data and used herein were the median water thickness within a mass, the median water thickness within the surrounding parenchyma, the ratio of the median water thicknesses of a mass and the surrounding parenchyma, and the skewness of the lipid thickness



**Figure 2:** Flowchart of study participant enrollment. DCIS = ductal carcinoma in situ; site 1 = University of California, San Francisco, San Francisco, Calif; site 2 = H. Lee Moffitt Cancer Center, Tampa, Fla.

**Table 2: Subtype and Hormone Receptor Status of Invasive Cancers**

Parameter	No. of Cancers (n = 35)
<b>Subtype</b>	
Ductal	28 (80)
Ductal with lobular features	1 (2.8)
Lobular	4 (11)
Carcinoma with neuroendocrine features	1 (2.8)
Unspecified	1 (2.8)
<b>Hormone receptor status</b>	
Estrogen and/or progesterone positive and HER-2 negative	19 (54)
HER-2 enriched	4 (11)
HER-2 equivocal	6 (17)
Triple negative	4 (11)
Unavailable	2 (5.7)

Note.—Numbers in parentheses are percentages. HER-2 = human epidermal growth factor receptor 2.

within a mass (quantifying the asymmetry of the lipid thickness distribution). For the combined mammography radiomics plus quantitative 3CB analysis, the radiomics and quantitative 3CB signatures were combined into a predefined nine-feature signature (five features from mammography radiomics and four from quantitative 3CB) (Appendix E3 [online]). Given the modest size of the data set, we (a) performed 10-fold cross-validation for classifier training and testing, (b) used a “simple” but robust

classifier (linear discriminant analysis), and (c) used predefined mass feature signatures as explained earlier, that is, no feature selection was performed. In the 10-fold cross-validations, within each fold, 90% of the data (extracted tumor features) served as training and 10% as testing. In each of the 10 training or testing folds, the classifier was trained by using the training data, which were then applied to the left-out test fold. Partitioning of the data set for cross-validation was performed “by lesion”: All images (craniocaudal, mediolateral oblique, and corresponding water, lipid, and protein thickness images when applicable) pertaining to a given lesion were either

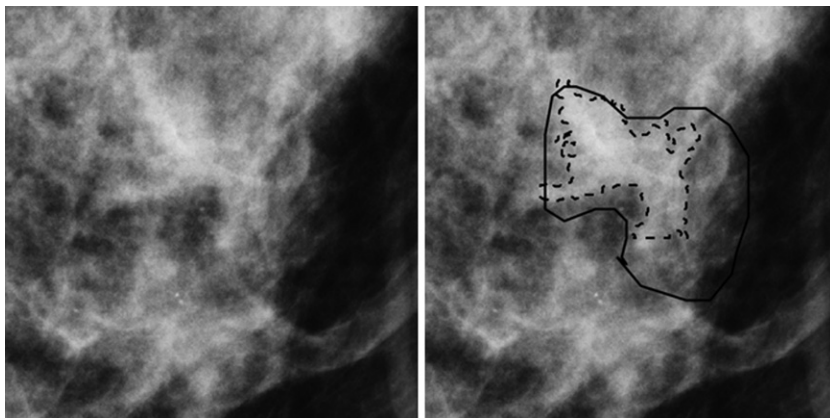
all part of a training fold or all part of a testing fold to avoid training the classifier on some images of a given lesion and then testing it on different images of that same lesion.

Note that 10-fold cross-validation does not result in a single model (classifier weights), even when predefined feature signatures are used, but rather results in 10 models (one for each training fold). If models obtained from the different training folds are similar, one can derive a “final” model from these 10 models (Appendix E3 [online]) and the cross-validation is expected to give a realistic impression of the classification performance of the final model in an independent test setting (if larger data sets were available).

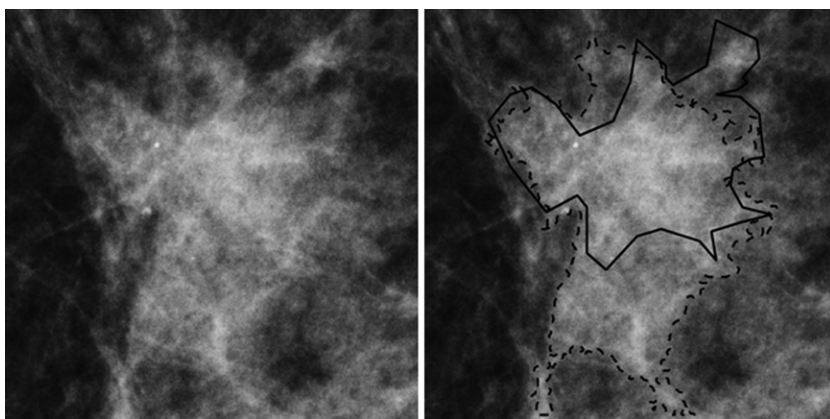
Performance was evaluated “by lesion,” and estimated image-based probabilities of malignancy for images (craniocaudal, mediolateral oblique views for mammography radiomics and corresponding water, lipid, and protein images for quantitative 3CB) of the same lesion were averaged.

**Statistical Analysis**

Classification performance was assessed for the radiologists’ diagnoses based on conventional diagnostic digital mammography as part of the regular clinical assessment and for all three proposed approaches: quantitative 3CB analysis alone, mammography radiomics alone, and combined radiomics plus quantitative 3CB analysis. The primary performance metric was positive predictive value of biopsy performed (PPV<sub>3</sub>) at maximum sensitivity. To attain maximum sensitivity, the “optimal” threshold for the decision variable (estimated probability of malignancy) was determined within the classifier



**Figure 3:** Region of interest from digital mammography depicts invasive cancer misclassified with mammography radiomics. Images in 50-year-old woman with invasive cancer (Breast Imaging Reporting and Data System category 4, with category C breast density) without (left) and with (right) radiologist and computer delineations (solid and dashed lines, respectively).



**Figure 4:** Region of interest from digital mammography depicts invasive cancer misclassified with quantitative three-compartment breast (3CB) analysis and combined mammography radiomics plus quantitative 3CB analysis. Images in 53-year-old woman with invasive cancer (Breast Imaging Reporting and Data System category 4, with category C breast density) without (left) and with (right) radiologist and computer delineations (solid and dashed lines, respectively).

training and testing cross-validation. For each training fold, the threshold value for the estimated probability of malignancy resulting in 100% sensitivity for that training fold was determined and subsequently applied to the corresponding “unseen” test fold. Note that this does not guarantee 100% sensitivity for the test folds. The corresponding  $PPV_3$  was then calculated per the BI-RADS manual (25) along with the adjunct performance metrics of obtained sensitivity, specificity, and negative predictive value.

Receiver operating characteristic analysis was used to assess overall classification performance for the task of differentiating between breast cancers and benign breast masses, and receiver operating characteristic curves, as well as areas under the receiver operating characteristic curves (AUCs), were estimated by using the proper binormal model (30) (available at metz-roc.uchicago.edu). Note that receiver operating characteristic analysis could not be performed for conventional diagnostic digital mammography because probabilities of malignancy were not routinely provided in the clinical work-up.

All statistical analyses were performed in Matlab (version R2018a; MathWorks, Natick, Mass). Bootstrapping (1000 bootstrap samples) was used to calculate 95% confidence intervals (CIs) of the performance metrics. The statistical significance of differences in performance was determined from the bootstrap samples through 95% CIs and the associated  $P$  values for these differences. The  $PPV_3$  of conventional diagnostic digital mammography and our analyses were compared in ascending order (three comparisons). AUCs were compared in a similar fashion (two comparisons).  $P$  values were corrected for multiple comparisons by using the Holm-Bonferroni method (31). A corrected  $P < .05$  was considered to indicate a statistically significant difference in performance.

## Results

### Study Participants

At the time of this analysis, 387 women with BI-RADS category 4 or 5 findings had enrolled in our 3CB imaging study. Only women with masses were included because the radiomics method used was developed for segmentation and classification of breast masses (27). A total of 122 women had a mass as the primary finding, and a total of 109 of these women (mean age, 51 years; age range, 31–85 years) had mammograms, 3CB images, radiologist delineations, and pathologic “truth” from biopsy (Table 1, Fig 2). In 11 women, microcalcifications were present as a secondary finding (six malignant and five benign findings), and these were included in our analysis. All malignant masses were invasive cancer (Table 2).

### Performance Evaluation and Statistical Analysis

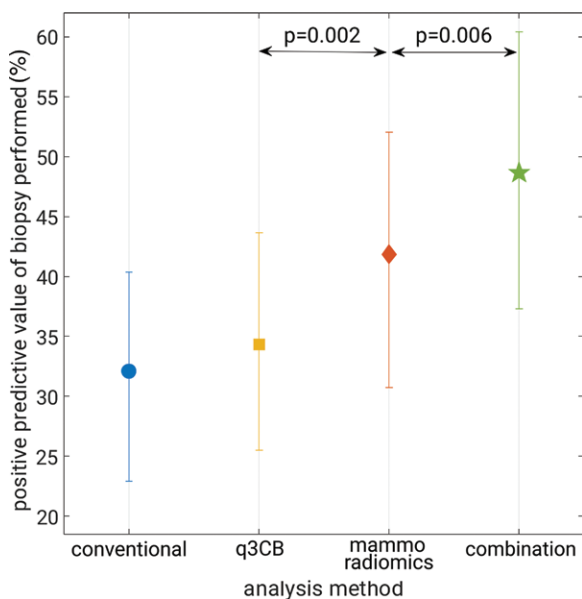
The derived classification models were stable, and quantitative 3CB analysis and mammography radiomics demonstrated an additive benefit in the estimation of the probabilities of malignancy (Appendix E4 [online]). The quantitative 3CB analysis demonstrated a higher  $PPV_3$ , that is, it suggested nine fewer unnecessary benign biopsies (nine of 74) than conventional diagnostic digital mammography ( $P < .001$ ) but also erroneously eliminated biopsy of one cancer (one of 35) ( $P < .001$ ) (Table 2; Figs 3, 4).

Both mammography radiomics and the combined approach avoided more benign biopsies (28 of 74 [ $P < .001$ ] and 38 of 74 [ $P < .001$ ] fewer benign biopsies than conventional diagnostic digital mammography, respectively), but also on average misclassified one cancer (one of 35) ( $P < .001$ ) (Figs 3, 4). One invasive cancer was misclassified with mammography radiomics.

**Table 3: Performance Metrics Corresponding to the Maximum Attained Sensitivity**

Technique	PPV <sub>3</sub> (%)	Sensitivity (%)	Specificity (%)	NPV (%)
Conventional diagnostic digital mammography	32.1 (35/109) [23.9, 41.3]	100	0	0
q3CB	34 (34/99) [25.0, 43.1]	97 (34/35) [90.3, 100]	12 (9/74) [4.2, 18.7]	90 (9/10) [62.0, 100]
Mammography radiomics	41 (34/82) [31.7, 53.0]	97 (34/35) [90.0, 100]	35 (26/74) [25, 46.7]	96 (26/27) [86.0,100]
Combined mammography radiomics plus q3CB	49 (34/70) [36.5, 58.9]	97 (34/35) [90.3, 100]	51 (38/74) [39.9, 60.1]	97 (38/39) [91.1,100]

Note.—Data are from 109 masses, 35 of which were invasive breast cancers. Numbers in parentheses are raw data, and numbers in brackets are 95% confidence intervals. NPV = negative predictive value, PPV<sub>3</sub> = positive predictive value of biopsy performed, q3CB = quantitative three-compartment breast image analysis.



**Figure 5:** Graph shows positive predictive value of biopsy performed at maximum attained sensitivity. Error bars represent 95% confidence intervals. *combination* = combined quantitative three-compartment breast (q3CB) analysis and mammography radiomics analysis, *conventional* = conventional diagnostic digital mammography, *mammo* = mammography.

A different cancer was misclassified with quantitative 3CB analysis and the combined analysis (Figs 3, 4). These misclassified cancers were both BI-RADS category 4. Overall, the combined approach suggested 35.8% (39 of 109) fewer total biopsies than did conventional diagnostic digital mammography, at the cost of a 2.9% (one of 35) reduction in sensitivity ( $P < .001$ ). The improvements in PPV<sub>3</sub> for mammography radiomics versus quantitative 3CB analysis (34 of 82 vs 34 of 99, respectively;  $P = .002$ ) and the combined approach versus mammography radiomics (34 of 70 vs 34 of 82;  $P = .006$ ) were statistically significant (Table 3, Fig 5).

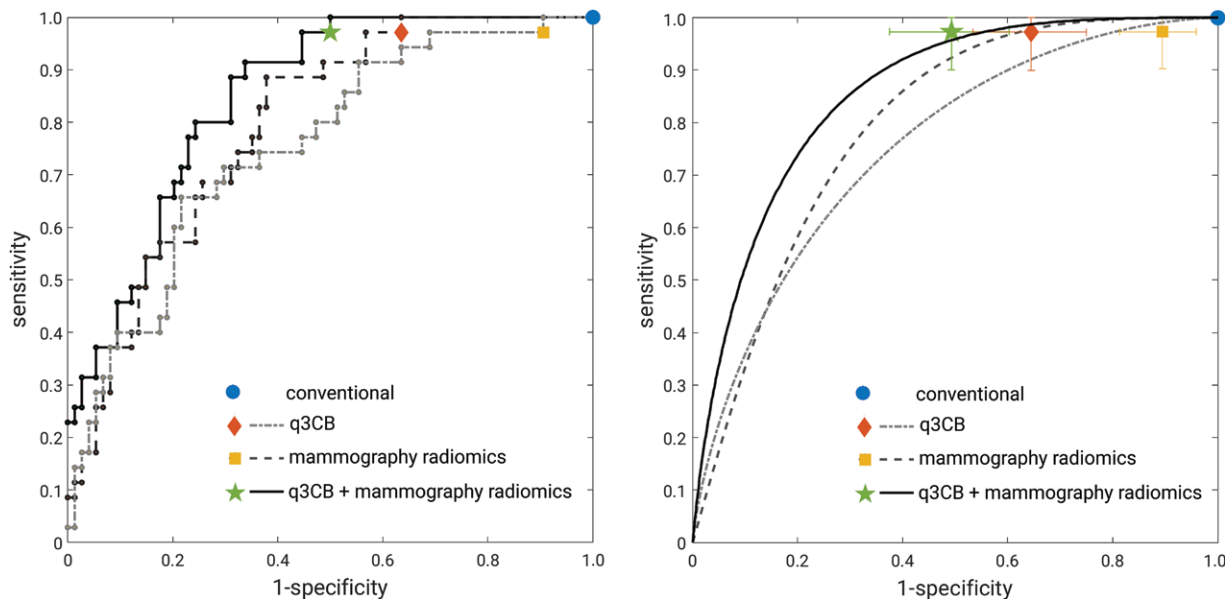
At receiver operating characteristic evaluation, the AUCs for the task of differentiating between malignant and benign masses were 0.76 (95% CI: 0.66, 0.85), 0.80 (95% CI: 0.72, 0.88), and 0.86 (95% CI: 0.78, 0.92), for quantitative 3CB analysis, mammography radiomics, and the combined approach, respectively (Fig 6). Although the improvement in AUC

for mammography radiomics relative to quantitative 3CB failed to reach statistical significance ( $P = .55$ ), the combined analysis outperformed mammography radiomics at a statistically significant level ( $P = .04$ ).

### Discussion

In the classification for malignancy of mammographic BI-RADS category 4 and 5 breast masses, we obtained, with use of in-house–developed mammography radiomics and quantitative 3CB methods, a PPV<sub>3</sub> of 49% (34 of 70) and an AUC of 0.86 (95% CI: 0.78, 0.92) for the combined mammography radiomics plus quantitative 3CB analysis. Our study demonstrated synergy between mammography radiomics and quantitative 3CB analyses, with  $P$  values corrected for multiple comparisons of less than .05 when comparing the PPV<sub>3</sub> for the combined approach to that for mammography radiomics and to conventional diagnostic digital mammography. This suggests that the water-lipid-protein breast tissue composition measured with 3CB imaging yielded biomarkers that cannot be gleaned from traditional mammographic techniques. One should note that both mammography radiomics and quantitative 3CB analysis can be performed in real time.

Because 3CB imaging to date has been used only in the diagnostic rather than screening setting, all breast masses included in our study were BI-RADS category 4 or 5 findings, that is, they all underwent biopsy. Both mammography radiomics and combined radiomics plus quantitative 3CB analyses would have resulted in substantially higher PPV<sub>3</sub> values than the actual value for this data set, albeit at the cost of, on average, missing one of the 35 cancers. This loss in sensitivity resulted from the determination of the threshold value for the estimated probability of malignancy within each training fold of the classifier training and testing protocol (and applying the threshold obtained for a given training fold to the corresponding unseen test fold). In contrast, a posteriori selection of a single threshold value for the entire set would have given the illusion of operating at no loss in sensitivity (100% sensitivity) but would have been incorrect because then one would effectively have used the pathologic truth for the entire data set twice: first to determine the optimal threshold resulting in 100% sensitivity and then to calculate PPV<sub>3</sub> at that threshold. The sensitivity of the combined approach of 97% (95% CI: 90.3%, 100%) at a specificity of 51% (95% CI: 39.9%,



**Figure 6:** Receiver operating characteristic analysis. Left, “raw staircase” receiver operating characteristic curves with operating points (no error bars for clarity) and, right, receiver operating characteristic curves fitted with the proper binormal model (30) with operating points. Error bars represent 95% confidence intervals. *q3CB* = quantitative three-compartment breast analysis.

60.1%) in our diagnostic study was comparable to the 98% sensitivity observed in a breast cancer radiomics study (11) and does not seem unreasonable compared with results reported in a large retrospective reading study in which 26 radiologists assessing screening mammograms obtained a sensitivity of 89% (95% CI: 86%, 92%) at 51% specificity in the detection and diagnosis of mammographic breast masses in 7000 cases with 1137 cancers (32).

Our study had some limitations. First, we used in-house-developed methods both for 3CB image acquisition and mammography radiomics. Even though these methods have been described in previous publications (24,26–28), this may hamper reproduction of our results. Second, our data set size is modest despite being accumulated over 4 years of active participant recruitment. Moreover, even though this study served as a validation of predetermined mass feature signatures, the data set was not used as a true independent test set. The latter was not possible given that the mammography radiomics signature was defined by using mammograms obtained with different equipment (27), hence requiring recalibration of the classifier because mammography radiomics generally depends on the imaging equipment and protocols used during acquisition. Moreover, even though 3CB imaging yields quantitative and reproducible breast composition maps, the pilot study data set for the quantitative 3CB analysis was too small to serve as a training set (28). Conversely, we conducted our analyses taking utmost care to minimize the risk of overfitting. The performances obtained by using predefined mass feature signatures were similar to those observed in the published pilot study (28) in which leave-one-case-out analyses yielded AUCs of 0.72 (standard error, 0.07) for quantitative 3CB analysis, 0.81 (standard error, 0.07) for mammography radiomics, and 0.86 (standard error, 0.04) for a merged approach. Note that while our current quantitative 3CB mass signature did not contain any features pertaining to protein

content, these features may be important for classification of other lesion types or for classification of cancer subtypes.

Future work will expand the analysis to include all suspicious lesions being considered for biopsy rather than only the subset of mammographic masses and will include a multireader, multicase radiologist reading study focusing on whether mammography radiomics and quantitative 3CB analysis have potential to reduce unnecessary benign biopsies and improve specificity. It should be noted that while quantitative 3CB analysis on its own did not perform as well as mammography radiomics, 3CB imaging provides both mammograms and 3CB composition maps. Because 3CB imaging can be performed with conventional mammography or breast tomosynthesis equipment with minimal changes in workflow and minor modifications, and with only a 10% higher dose (24), the potential exists for wide application of 3CB imaging in diagnostic breast imaging and perhaps also in screening. Our study showed that more investigation into the application of 3CB imaging is warranted, and we have initiated a research study incorporating 3CB imaging into breast tomosynthesis.

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