

RESEARCH ARTICLE SUMMARY

NEUROSCIENCE

Dynamics of cortical dendritic membrane potential and spikes in freely behaving rats

Jason J. Moore,* Pascal M. Ravassard, David Ho, Lavanya Acharya, Ashley L. Kees, Cliff Vuong, Mayank R. Mehta*

INTRODUCTION: Neurons are large, tree-like structures with extensive, branch-like dendrites spanning $>1000\ \mu\text{m}$, but a small $\sim 10\text{-}\mu\text{m}$ soma (figure). Dendrites receive inputs from other neurons, and the electrical activity of dendrites determines synaptic connectivity, neural computations, and learning. The prevailing belief has been that dendrites are passive; they merely send synaptic currents to the soma, which integrates the inputs to generate an electrical impulse, called an action potential or somatic spike, thought to be the fundamental unit of neural computation. These ideas have not been directly tested because traditional electrodes, which puncture the dendrite to measure dendritic voltages *in vitro*, do not work *in vivo* due to constant movement of the animals that kills the punctured

dendrites. Hence, the voltage dynamics of distal dendrites, constituting the vast majority of neural tissue, is unknown during natural behavior.

RATIONALE: Tetrodes are a bundle of four fine electrodes, commonly used for measuring somatic spikes from a distance, that is, extracellularly. Hence, they work well in freely behaving animals. However, tetrodes do not measure the membrane voltages of soma, let alone dendrites. Chronically implanted tetrodes also elicit a naturally occurring immune response, where glial cells encapsulate the tetrode and shield it from the extracellular medium. We tested the hypothesis that a segment of dendrite could get trapped between the tetrode tips before this glial encapsulation occurred (figure). This

would enable us to measure the dendritic membrane voltage without penetrating it in freely behaving subjects.

RESULTS: Despite low success rate, we measured the putative, distal-dendritic membrane potential in freely behaving rats for long periods, up to 4 days. These data showed frequent

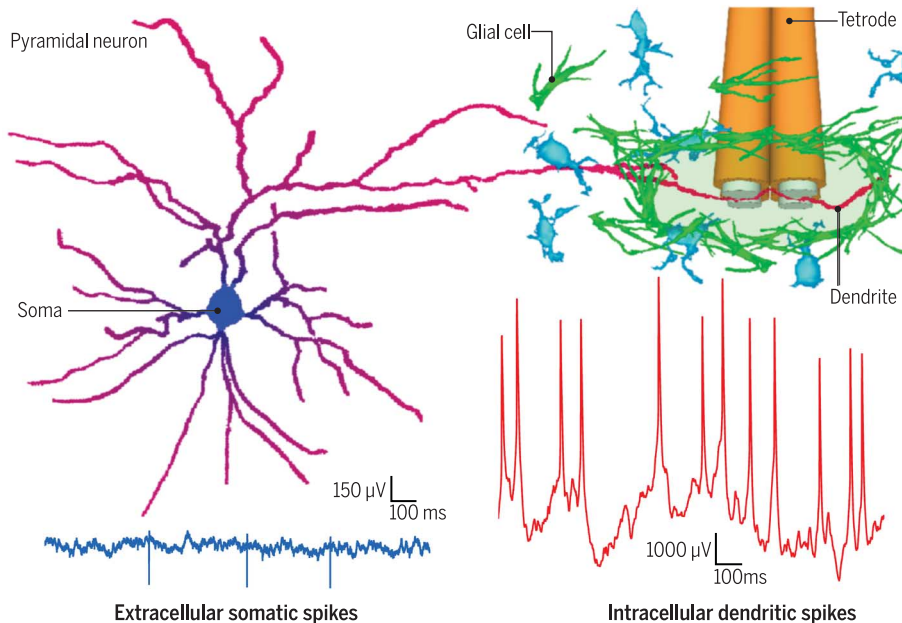
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occurrence of spikes that were quite different from somatic spikes, but they closely resembled the waveforms of spikes generated within the distal dendrites *in vitro* (figure). This finding

was further confirmed by computational modeling. The glial seal mechanism was verified using immunohistochemistry, predicted shielding of extracellular spikes during the dendritic measurements, *in vivo* impedance spectroscopy, and modeling. The identity of the general cell type from which the dendrite spikes were measured was confirmed using the analysis of short-term plasticity, suggesting that most of the dendritic measurements were from pyramidal neurons. The dendritic spike rates, however, were fivefold greater than the somatic spike rates of pyramidal neurons during slow-wave sleep and 10-fold greater during exploration. The high stability of dendritic signals suggested that these large rates are unlikely to arise due to the injury caused by the electrodes. The data also showed large subthreshold membrane voltage fluctuations. Their magnitude was always larger than that of dendritic spikes. This is the converse of comparable measurements in the soma. The dendritic spikes and subthreshold voltages contained significant information about the rat's exploratory behavior, which is comparable to somatic spikes.

CONCLUSION: The glial sheath method can be used for measuring dendritic membrane potential in freely behaving animals for long periods. The large subthreshold voltage fluctuations in dendrites, which modulate the dendritic firing rates, indicate a hybrid, analog-digital code in the dendrites. These dendritic dynamics could profoundly influence synaptic plasticity and neural computations. The dendrites generated several-fold more spikes than the soma. The large dendritic spike rates could be responsible for the seemingly weak correlations between the somatic spikes across neurons. This requires a revision of many prevailing beliefs, for example, the dendrites are largely passive *in vivo*, and the somatic spike is the fundamental unit of neural computation. ■



Glial sheath mechanism of measuring dendritic membrane potential *in vivo*. The top left shows a pyramidal neuron with soma (blue) and extensive dendrites (red). The top right shows the tetrode (gold) and glial cells (green) that trap a dendritic branch. The bottom left shows the extracellular measurements from the soma (blue), displaying few, small-amplitude, downward-going spikes. The bottom right shows membrane potential from the dendrite, displaying many, large-amplitude, upward-going spikes.

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Dynamics of cortical dendritic membrane potential and spikes in freely behaving rats

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Neural activity *in vivo* is primarily measured using extracellular somatic spikes, which provide limited information about neural computation. Hence, it is necessary to record from neuronal dendrites, which can generate dendritic action potentials (DAPs) *in vitro*, which can profoundly influence neural computation and plasticity. We measured neocortical sub- and suprathreshold dendritic membrane potential (DMP) from putative distal-most dendrites using tetrodes in freely behaving rats over multiple days with a high degree of stability and submillisecond temporal resolution. DAP firing rates were several-fold larger than somatic rates. DAP rates were also modulated by subthreshold DMP fluctuations, which were far larger than DAP amplitude, indicating hybrid, analog-digital coding in the dendrites. Parietal DAP and DMP exhibited egocentric spatial maps comparable to pyramidal neurons. These results have important implications for neural coding and plasticity.

Microelectrode techniques have enabled the long-term measurement of extracellular somatic action potentials in freely behaving subjects. However, somatic action potentials are brief (~1 ms), occur rarely (~1.5 Hz in principal neocortical neurons), and only represent the binary output of neurons, whereas the vast majority of excitatory synapses are localized on their dendritic arbors, each spanning more than 1000 μm (2). *In vitro* studies show that dendrites support local spike initiation of dendritic action potentials (DAPs) (2–16) and back-propagating action potentials (bAPs) initiated at cell somata (5–8, 12, 13, 15–22). Measurements in anesthetized, head-fixed animals (23–26) support these findings. DAPs affect synaptic integration (16, 27–33) and endow neurons with greater computational power and information capacity (14–16, 29, 30, 32–38) by turning dendritic branches into computational subunits with branch-specific plasticity (9–11, 14–16, 30–32).

Two-photon calcium imaging (21, 26, 39, 40), sharp electrode (2), or patch-clamp techniques (41) can be used to study dendrites *in vivo*. How-

ever, calcium imaging is not a direct measure of subthreshold membrane potential or dendritic sodium spikes and lacks submillisecond resolution. Sharp electrode and patch-clamp techniques damage or rupture the membrane, thus limiting the recording duration (42) and altering *in vivo* neural dynamics, including firing rates (43); they are ill suited to record from thin dendrites. In addition, these methods often require the subject to be anesthetized or immobilized, which alter neural dynamics and limit possible behavioral paradigms.

Extracellular recording techniques can also, at times, record intracellular-like signals. Sharp glass pipettes occasionally measure “quasi-intracellular” somatic recordings in anesthetized animals (44–48). These recordings can be stable for, at most, a few hours (45), and the recorded spikes have identical shapes as somatic action potentials (width, ~1 ms) (45, 47, 48). Quasi-intracellular recordings are proposed to arise from a region of high electrical resistance, electrically isolating the membrane under the microelectrode, resulting in large-amplitude, intracellular-like signals. Microelectrode arrays can achieve an “in-cell” recording configuration (49, 50) when cultured neurons engulf the recording electrodes, yielding a large seal resistance and allowing measurement of the intracellular voltage.

How might these phenomena be leveraged to investigate dendritic activity *in vivo*? We used chronically implanted tetrodes (see methods) (51, 52), which are often flexible and have a narrow profile, to mitigate cell damage. Astrocytes and microglia can form a high impedance sheath around a tetrode and shield off the rest of the extracellular space (53–55). We hypothesized that

this process can encapsulate a dendrite alongside the tetrode such that the voltages at the tetrode tips approximate the intracellular dendritic membrane potential (DMP) without penetrating the dendrite.

We implanted nine rats with hyperdrives containing up to 22 individually adjustable tetrodes, as described previously (see methods) (51, 52). Tetrodes usually recorded standard extracellular signals, including thin (<1 ms) extracellular spikes of negative polarity with ~100- μV amplitude (Fig. 1A), presumably of somatic origin (56). However, in several instances [25 recordings made over 194 total tetrodes (13% success rate) in 21 of 847 total recording days (2% of recording sessions) across nine rats, see methods], the signal was markedly different, resembling an intracellular dendritic recording (Fig. 1B and movie S1). These signals manifested overnight, while all tetrodes were stationary. Here, the signal amplitude was orders of magnitude larger, containing broad (>5-ms base width) positive-polarity spikes with amplitudes of the order of thousands of microvolts (Fig. 1, B and C). These signals could be discerned only when the data acquisition system settings with high dynamic range were used. These measurements were obtained at a median of 18 (between 6 and 55) days after surgery and discontinuation of any psychoactive drug, ruling out any possible effects of anesthesia.

DAP versus extracellular spikes

For reasons described below, we refer to these spikes as DAP. We computed several features of the 25 DAP sources measured *in vivo* (Fig. 1D; see methods) and compared these to extracellular somatic spike measurements from 754 units across nine rats *in vivo* (Fig. 1, E to G) and to available intracellular reports of dendritic spiking (table S1) (3, 6–8, 13, 20). First, similar to in-cell and quasi-intracellular measurements (45, 46, 49, 50), DAP amplitude was always positive (850 μV ; 25 to 75% range, 570 to 2100 μV) (Fig. 1, D and E, and fig. S1), in contrast to extracellularly recorded somatic spikes simultaneously recorded from nearby tetrodes; these were of negative polarity and of much smaller amplitude (–80 μV ; 25 to 75% range, –50 to –110) (Fig. 1E and fig. S1). DAP rise time (0.57 ms; 25 to 75% range, 0.48 to 0.68 ms) was consistent across all recordings, similar to dendritic sodium spikes *in vitro*, and much larger than the rise time of the extracellular spikes (0.31 ms), but much faster than the rising phase of calcium spikes (Fig. 1, D and F, and table S1) (3, 8, 20, 39). The full-width at half maximum (half-width) of DAP (4.3 ms; 25 to 75% range, 2.7 to 6.3 ms) (Fig. 1, D and G) was much longer than the DAP rise time (fig. S2, A and B) and far greater than the half-width of extracellular (0.26 ms; Fig. 1G) or intracellular (~0.7 ms; table S1) somatic spikes; DAPs were much wider than reported “high-amplitude positive spikes” from cortex (57) and somatic spikes recorded quasi-intracellularly (44–48). However, DAP half-width was much smaller than the typical half-width of dendritic calcium spikes (table S1). DAP width was more variable both within and across recordings (fig. S2), in

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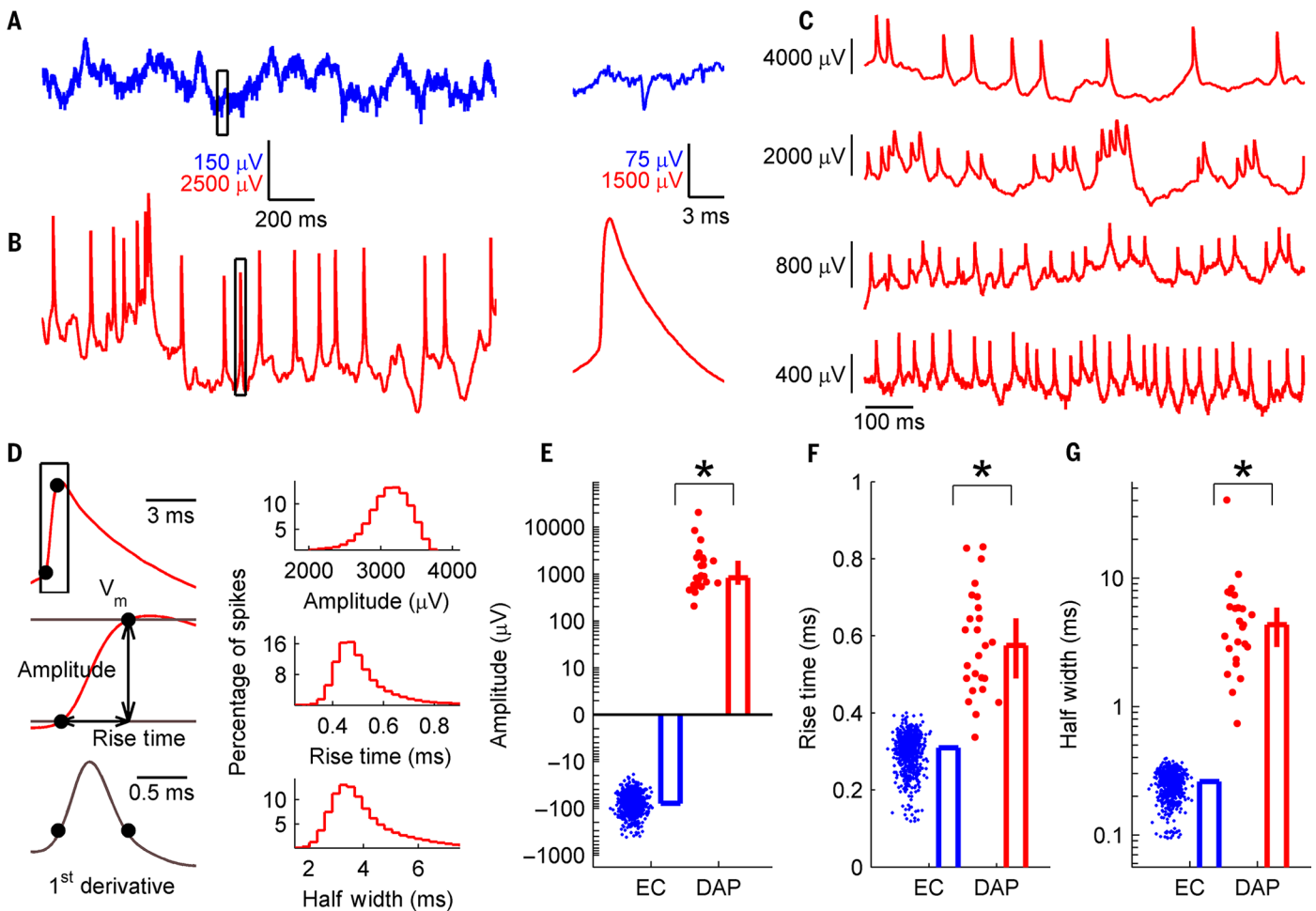


Fig. 1. Measurements of DAP in vivo. (A) Typical extracellular LFP showing $\sim 100\text{-}\mu\text{V}$ fluctuations. Somatic action potentials are visible as thin, $\sim 100\text{-}\mu\text{V}$, negative-polarity spikes (inset to right). (B) Putative DMP recording on the same tetrode presented in (A) on the following day. Fluctuations are $\sim 5000\text{-}\mu\text{V}$. DAPs are visible as broad, positive-polarity, $\sim 5000\text{-}\mu\text{V}$ spikes with a much longer falling phase than rising phase (inset to right). See also movie S1. (C) Sample membrane potential traces from four separate tetrodes, each exhibiting spontaneous dendritic spiking. (D) (Left) Quantification of DAP shape parameters (see methods). (Top right) Distribution of DAP amplitudes within a single recording session [$3120\text{-}\mu\text{V}$ (3110 to $3130\text{-}\mu\text{V}$); $n = 8187$ spikes]. (Middle right) Distribution of DAP rise times for the same recording session [0.49 ms (0.49 to 0.49 ms); $n = 8187$ spikes]. (Bottom right) Distribution of DAP half-widths for the

same recording session [3.81 ms (3.78 to 3.84 ms); $n = 8187$ spikes]. (E) Extracellular spike amplitude (EC; blue) was always negative [$-77.5\text{-}\mu\text{V}$ (-81.1 to $-73.4\text{-}\mu\text{V}$); $n = 754$ units], in comparison to DAPs (red) that were always positive [$835\text{-}\mu\text{V}$ (597 to $1900\text{-}\mu\text{V}$); $n = 25$ dendrites], and more than 10 times larger in magnitude ($P = 1.7 \times 10^{-17}$, Wilcoxon rank sum test). (F) The rise time of DAP [0.58 ms (0.49 to 0.65 ms); $n = 25$ dendrites] was significantly larger ($P = 1.7 \times 10^{-17}$, Wilcoxon rank sum test) than that of extracellular spikes [0.31 ms (0.31 to 0.31 ms); $n = 754$ units]. (G) The half-width of DAP [4.33 ms (2.92 to 5.90 ms); $n = 25$ dendrites] was also significantly larger ($P = 1.7 \times 10^{-17}$, Wilcoxon rank sum test) than that of extracellular spikes [0.26 ms (0.26 to 0.26 ms); $n = 754$ units]. Data are reported and presented as median and 95% confidence interval of the median. $*P < 0.05$.

contrast to very consistent DAP rise times across the data, and the two were significantly correlated ($r = 0.57$, $P = 0.003$) between DAP rise time and width across the recordings (fig. S2F). These differences in the variability of rise time and width across DAP are also characteristic of dendritic sodium spikes (table S1) (3, 6–8, 17, 20, 21, 26, 39).

Mechanism of DMP measurement: Glial sheath hypothesis

We hypothesized that the DMP recordings were achieved by combining the above-mentioned in-cell (quasi-intracellular) recording (45, 46, 49, 50) and glial sheath mechanisms (53, 54). Each tetrode bundle was ~ 35 to $40\text{-}\mu\text{m}$ in diameter, with a $\sim 5\text{-}\mu\text{m}$ gap between the tips. An intact dendrite,

only a few micrometers thick (1, 8), could thus be caught in this gap, and the tetrode would record an intracellular dendritic signal once the glial sheath formed. Immunohistochemistry of cortical sections previously implanted with tetrodes (see methods) showed reactive astrocytes and microglia surrounding the tetrode location, with intact dendrites nearby (fig. S3A and movie S2). Increased resistance from the electrode tips to ground due to this encapsulation would allow recording of the intracellular membrane potential (fig. S3B). We performed impedance spectroscopy measurements on electrodes during either DMP or local field potential (LFP) recordings (fig. S3C). Fitting parameters to an electric circuit equivalent model of glial encapsulation (55, 58),

the only parameter that was significantly higher ($P = 1.8 \times 10^{-3}$) for DMP-recording electrodes, was the resistance between the electrode tip and ground, through the glial sheath (fig. S3, C and D). The estimated glial resistance was more than sixfold larger for DMP-recording electrodes compared to LFP-recording electrodes; this is precisely the condition predicted by the model that would yield glial sheath-assisted measurements of the intracellular voltage (fig. S3B).

Furthermore, we evaluated tetrode signal properties in the session before a DAP was recorded (PRE), during DAP recording (DUR), and in the session after the DAP signal was lost (POST). First, DAP amplitudes were nearly identical on all four channels of a tetrode in DUR (see methods),

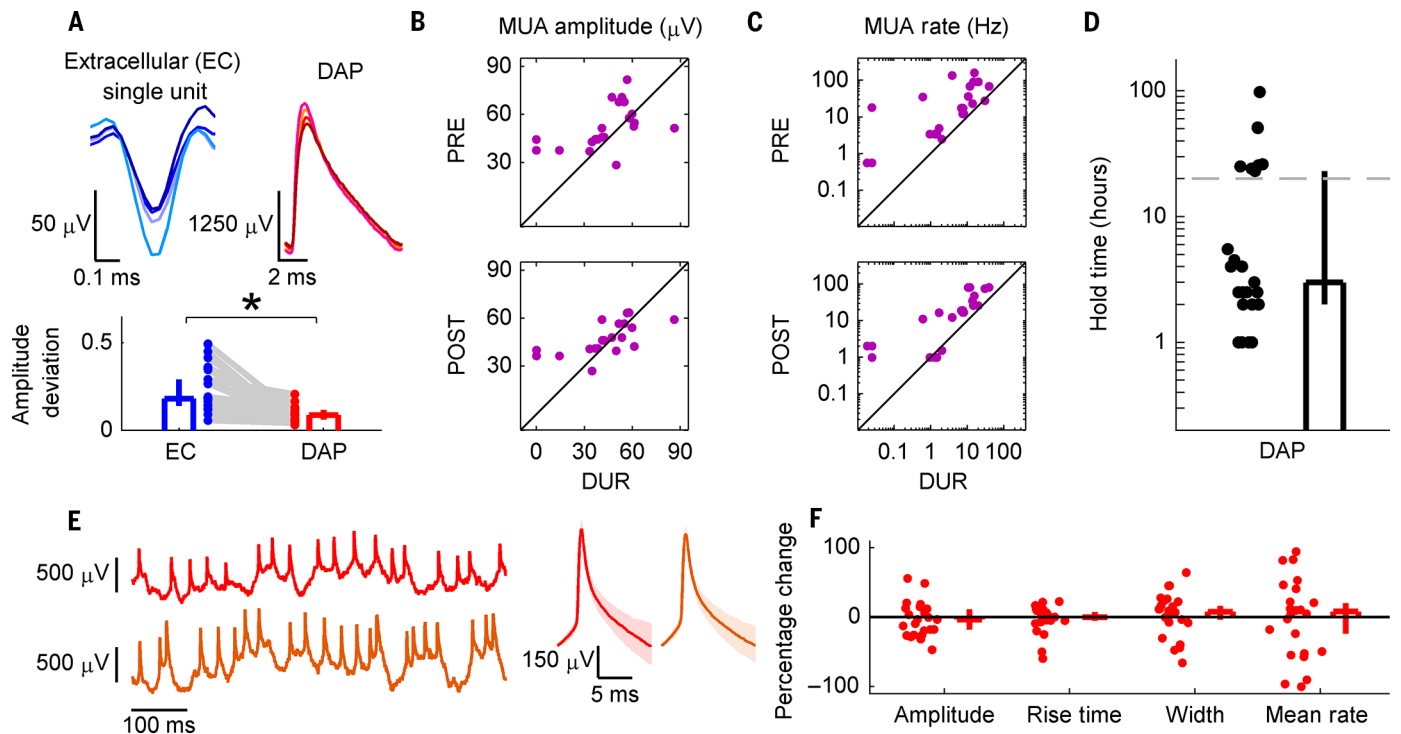


Fig. 2. DAP measurements are similar across all electrodes of a tetrode and are stable for long periods. (A) (Top) The waveform of a single extracellular spike has different amplitudes on each of the four tetrode channels (left), but the waveform of a single DAP on the same tetrode the following day has very similar amplitudes (right). (Bottom) The spike amplitude deviation across four electrodes (see methods) was significantly greater for extracellular single units recorded the day before DAPs were recorded (PRE) [0.18 (0.14 to 0.29); $n = 25$ units] compared to DAP during DMP recording (DUR) [0.09 (0.06 to 0.12); $n = 25$ DAP sources] on the same tetrode the following day ($P = 6.2 \times 10^{-6}$, Wilcoxon signed-rank test). (B) MUA amplitude during DMP recording (DUR) [41.8 μV (36.9 to 53.4 μV); $n = 25$ recordings] was significantly lower than during PRE [45.8 μV (44.3 to 54.6 μV); $n = 25$ recordings; $P = 6.6 \times 10^{-3}$, Wilcoxon rank sum test]. MUA amplitude was smaller in DUR compared to the day after DMP recording [POST; 44.1 μV (40.6 to 53.9 μV); $n = 25$ recordings], but not significantly so ($P = 6.7 \times 10^{-2}$, Wilcoxon rank sum test). (C) MUA rate was significantly lower in DUR [5.19 (1.29 to 10.7); $n = 25$ recordings] compared to both PRE [17.5 Hz (4.84 to 34.7 Hz); $n = 25$ recordings; $P = 2.1 \times 10^{-5}$, Wilcoxon rank sum test] and POST [16.5 Hz (2.01 to 25.5 Hz); $n = 25$ recordings; $P = 8.0 \times 10^{-5}$, Wilcoxon rank sum test]. (D) DAP recordings were stable

for long periods of time [3 hours (2 to 23 hours); $n = 25$ recordings], with the shortest recording lasting 1 hour and the longest lasting 97.5 hours. Durations between 5.5 and 23 hours are absent due to restrictions on total recording duration in a single day, resulting in artificial bimodality. Hence, all recording durations are likely an underestimate of actual duration for which the DAPs were held. (E) (Left) Membrane potential at the beginning of recording (top) and 90 min after (bottom) recording, showing little change in the quality of recording. (Right) Averaged DAP (median and 25th to 75th percentile) in the first part of the recording to the left ($n = 616$ DAP) compared to the averaged DAP in the later part of the recording to the right ($n = 897$ DAP). (F) Percentage change from the first 5 min of recording to the last 2 min was not significantly different from 0 for amplitude [−3.48% change (−18.0 to 11.7% change); $n = 25$ dendrites; $P = 0.55$, Wilcoxon signed-rank test], rise time [0.00% change (−5.00 to 7.69% change); $n = 25$ dendrites; $P = 0.87$, Wilcoxon signed-rank test], half-width [7.76% change (−3.64 to 16.27% change); $n = 25$ dendrites; $P = 0.35$, Wilcoxon signed-rank test], or mean firing rate [7.93% change (−23.9 to 20.5% change); $n = 25$ dendrites; $P = 0.97$, Wilcoxon signed-rank test]. Data are reported and presented as median and 95% confidence interval of the median unless otherwise noted. * $P < 0.05$.

unlike in the PRE condition where the voltages of extracellular spikes were different across the four channels (Fig. 2A). This would not occur if any single electrode of the tetrode had penetrated the dendrite, but would be expected if the dendrite and the entire tetrode tip were encapsulated during DMP recording. Second, this would result in the shielding off of the surrounding extracellular medium from the tetrode by the encapsulating glial sheath. In the DUR condition, both the amplitude and mean firing rate of detectable extracellular multiunit activity (MUA) were significantly reduced (Fig. 2, B and C; see methods) compared to PRE. In one case, one of four tetrode channels did not achieve an intracellular-like recording. MUA on only that channel was preserved, and its correlation with other channels

remained low, suggesting that the single channel was not encapsulated by the glial sheath (fig. S4). Third, there was no evidence of damage to the tetrodes that yielded DMP measurements, because all MUA properties in POST were similar to those in PRE (Fig. 2, B and C).

DAP properties remained stable for long periods of time (Fig. 2, D to F). Our recordings typically lasted several hours, and DAP from the same tetrode could be recorded for up to 4 consecutive days (Fig. 2D; see methods). From the beginning to the end of the recording span of any single DMP, there was no systematic change in DAP amplitude, rise time, width, or mean firing rate (Fig. 2, E and F). These observations indicate that the tetrode did not damage the dendrite during these measurements (42, 43, 59, 60).

Cellular identity of DAP

Although the rise times and widths of the spikes described above are consistent with dendritically generated sodium spikes, that is, DAP, they are also consistent with somatically generated spikes (bAP) (6–8, 12, 13, 15–22). Hence, we compared the firing properties of DAP to those of extracellular somatic spikes recorded simultaneously on nearby tetrodes (see methods). We first examined data from slow-wave sleep (SWS) to minimize the influence of behavioral parameters (Fig. 3; see methods). DAP mean firing rates were high (7.1 Hz), more than fourfold greater than the mean firing rates of extracellular units (1.6 Hz) (Fig. 3, A and B). The high DAP firing rates were not due to multiple DAP sources being pooled together, because all DAP had interspike interval

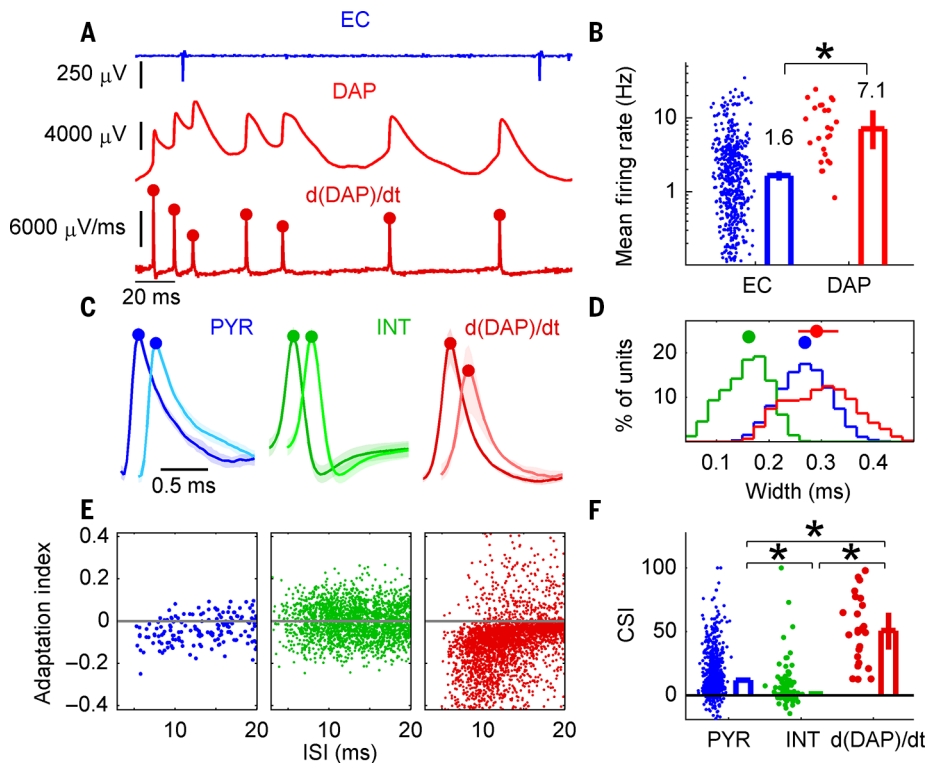


Fig. 3. DAPs are likely to be from pyramidal neurons but have much greater firing rates and stronger short-term plasticity. (A) (Top) Sample LFP showing a single extracellular unit firing at a relatively low rate. (Middle) Sample putative membrane potential showing a DAP firing at a higher rate. (Bottom) First temporal derivative of the membrane potential trace. Red dots indicate the peak value of identified DAP. Note activity-dependent attenuation. (B) In SWS, the mean spontaneous firing rate of extracellularly recorded units [1.65 Hz (1.41 to 1.91 Hz); $n = 754$ units] was more than fourfold smaller ($P = 4.1 \times 10^{-8}$, Wilcoxon rank sum test) than the firing rate of DAP [7.07 Hz (3.76 to 12.6 Hz); $n = 25$ dendrites]. Notice the near-complete absence of low (<1 Hz) DAP firing rate. (C) Demonstration of extracellular waveforms. The median and 25th to 75th percentile of sample pyramidal neuron (PYR; blue, $n = 140$ spike pairs), interneuron (INT; green, $n = 6987$ spike pairs), and $d(\text{DAP})/dt$ (red; 130 spike pairs) waveforms are plotted for the first spike (darker color) and the second spike in burst pairs (lighter color). PYR and DAP are broad, and the second spike has a smaller amplitude. This is not the case for INT. (D) Extracellular spike widths of PYR [0.27 ms (0.26 to 0.27 ms); $n = 657$ units] and DAP [0.29 ms (0.25 to 0.33 ms); $n = 25$ dendrites] were significantly greater than the extracellular spike width of INT [0.16 ms (0.15 to 0.17 ms); $n = 97$ units; PYR versus INT, $P = 1.2 \times 10^{-52}$; DAP versus INT, $P = 5.1 \times 10^{-14}$, Wilcoxon rank sum test for both]. DAPs were also significantly wider than PYR ($P = 1.5 \times 10^{-2}$, Wilcoxon rank sum test). (E) Adaptation index (see methods) plotted against ISI for a sample pyramidal neuron, interneuron, and DAP. For PYR and DAP, but not INT, the adaptation index is largely negative for ISI less than 20 ms. For clarity, every fifth spike pair is plotted for INT and DAP. (F) PYR CSI [12.0 (10.3 to 13.5); $n = 657$ units] was significantly greater ($P = 1.0 \times 10^{-11}$, Wilcoxon rank sum test) than that of INT [1.02 (0.25 to 2.99); $n = 97$ units], but smaller ($P = 2.9 \times 10^{-10}$, Wilcoxon rank sum test) than that of DAP [50.8 (36.0 to 65.0); $n = 25$ dendrites]. DAP CSI was significantly greater ($P = 4.7 \times 10^{-12}$, Wilcoxon rank sum test) than that of INT. Data are reported and presented as median and 95% confidence interval of the median unless otherwise noted. $*P < 0.05$.

(ISI) and amplitude distributions inconsistent with multiple independent sources (fig. S5; see methods). The high rates were also unlikely to be due to damage or otherwise altered activity of dendrites because of the longevity of recording (Fig. 2D) and the absence of any systematic changes in DAP kinetics or rate (Fig. 2, E and F) over long periods of time.

Could the high DAP rates be a result of preferentially recording from high-rate interneurons (61)? Interneurons have narrow spikes that exhibit very little spike amplitude attenuation within high-frequency bursts, characterized by very low

complex spike index (CSI) (see methods) (51, 61–64). In contrast, pyramidal neurons have wide spikes that exhibit consistent amplitude attenuation. These distinctions between cell types are present in dendrites as well (8, 16, 18, 19, 65, 66). Thus, DAP should have wide spikes and a high CSI if recorded from pyramidal neurons.

We separated the extracellular units into putative pyramidal neurons and interneurons using standard methods (fig. S6A) (61) and compared their widths and CSI to the first temporal derivative of DAP, as an approximation of the extracellular waveform (56, 67). Our data set contained

far more pyramidal neurons (87%) than interneurons (13%). As expected, pyramidal neurons had significantly lower firing rates and larger widths and CSI than the interneurons (Fig. 3, C to F, and fig. S6B) (61, 62, 68). The estimated extracellular widths of DAP were slightly larger than pyramidal neurons but about twice as large as interneurons (Fig. 3D). The DAP CSI was slightly greater than that of pyramidal neurons but 50-fold greater than that of interneurons (Fig. 3, E and F). The distributions of both of these DAP measures were unimodal and most similar to pyramidal neurons, indicating that our DAPs were measured from the dendrites of pyramidal neurons.

DAP mean rate was significantly greater (more than fivefold) than that of pyramidal neurons ($P = 1.3 \times 10^{-9}$) (fig. S6B), as was the peak firing rate (DAP, 93.5 Hz; pyramidal, 67.6 Hz; $P = 1.0 \times 10^{-2}$; fig. S6C, only ~40%). The differential pattern of the mean and peak rates might be explained by the differences in short-term plasticity (62), which is greater in the pyramidal neuron dendrites compared to soma (18, 19). This is manifested in activity-dependent adaptation of DAP amplitude, rise time, and width, similar to those in pyramidal neuron dendrites in vitro (fig. S6, D and E) (18, 19).

To determine whether these are bAP or DAP and the locus of their measurement, we compared our experimental results with the simulations of a multicompartiment model of cortical layer 5 pyramidal neuron (fig. S7) (69–73). The rise time and widths of our data had a significant overlap with those of simulated DAP generated in the distal-most dendrites and measured locally (fig. S7, B and D). In contrast, these measured parameters had only a partial overlap with the bAP (fig. S7, C and D). These results suggest that for the case of layer 5 pyramidal neurons, most of our measured DAPs are locally generated and measured in the distal-most dendrites. Similar results may hold for other pyramidal neuron types and dendrites. This hypothesis is further supported by the observation that DAP rates are several-fold greater than somatic rates (Fig. 3B and fig. S6B).

Further analysis of DAP properties did not show evidence of two different populations. The DAP rates were similar at all depths (from 330 to 1240 μm ; $P = 0.24$; fig. S8A) and were greater than somatic rates at all depths (fig. S8B). Other properties of DAP sources were uncorrelated with DAP rate as well, including amplitude ($P = 0.19$), rise time ($P = 0.14$), half-width ($P = 0.49$), and CSI ($P = 0.57$) (fig. S8C), suggesting no clear demarcation between high- and low-rate DAP. The disparately large rates of DAP compared to somatic spikes suggest that only a fraction of DAPs elicit somatic spiking, indicating a significant decoupling of dendrites and somata (2, 5, 6, 8, 19, 31, 32).

Subthreshold dendritic potential dynamics during SWS

Subthreshold fluctuations accompanying DAP during SWS had characteristics suggesting that they represent the DMP (Fig. 4A; see methods). The subthreshold fluctuations were of the order

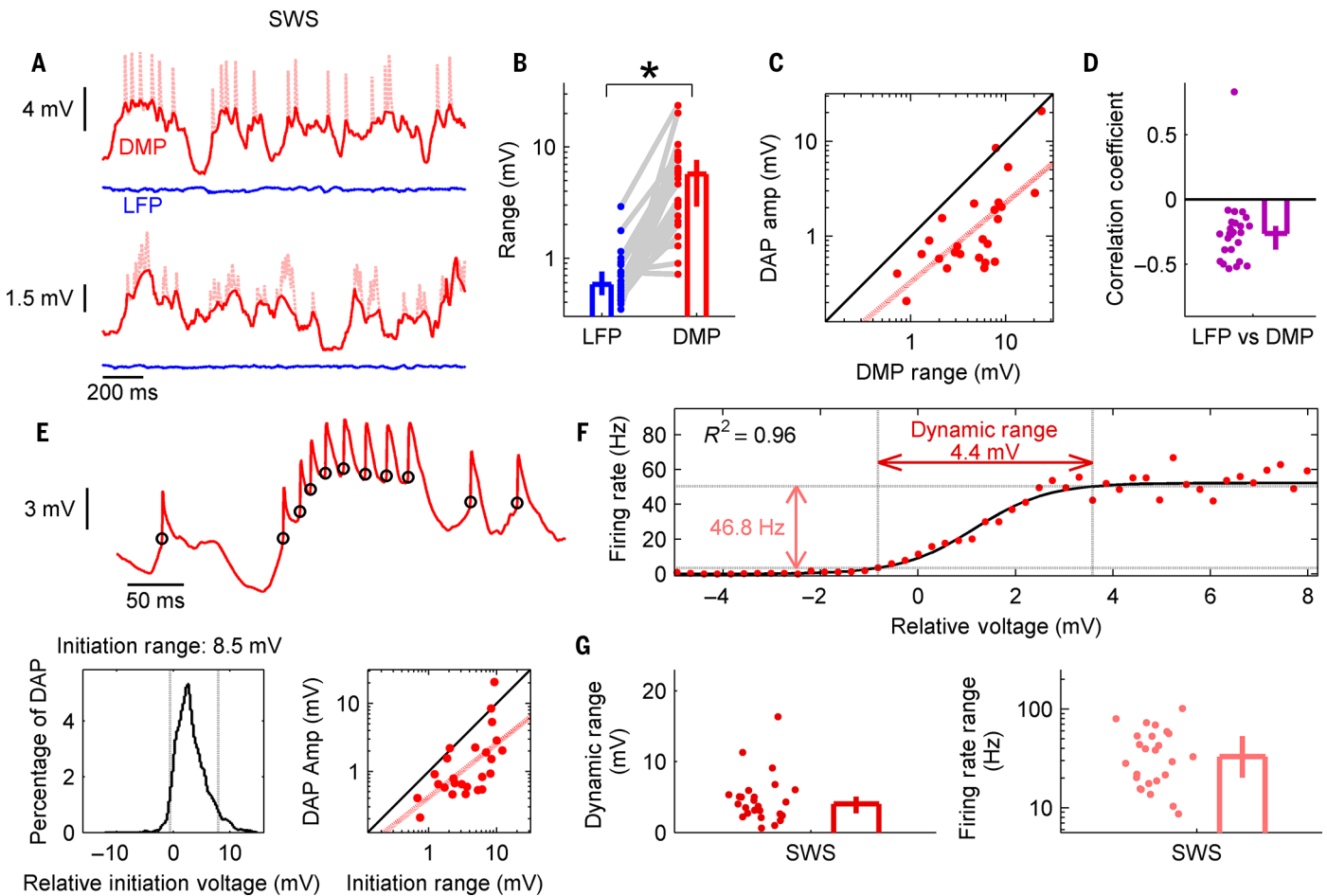


Fig. 4. Large subthreshold membrane potential fluctuations modulate DAP rates during SWS. (A) (Top) Sample DMP (red) trace during SWS, showing prominent oscillations of the same order of magnitude as DAP. DAPs are shown in light red to highlight the spike-clipped subthreshold membrane potential. Below on the same scale is the LFP (blue) recorded simultaneously on a nearby tetrode. (Bottom) Same as above but from a different pair of tetrodes in a different recording session. (B) The range of the LFP [0.58 mV (0.47 to 0.76 mV); $n = 25$ LFP] was nearly an order of magnitude (9.9-fold) smaller than the subthreshold DMP accompanying DAP [5.72 mV (2.92 to 7.69 mV); $n = 25$ dendrites]. $*P = 1.6 \times 10^{-8}$, Wilcoxon signed-rank test. (C) In SWS, the range of subthreshold DMP was nearly always larger ($P = 1.4 \times 10^{-5}$, Wilcoxon signed-rank test) than the corresponding DAP amplitude [0.84 mV (0.60 to 1.90 mV); $n = 25$ dendrites] and positively correlated [$r = 0.71$ (0.44 to 0.86); $P = 6.9 \times 10^{-5}$, two-sided t test]. (D) In all but one case, LFP and simultaneously recorded DMP during SWS were negatively correlated [$r = -0.26$ (-0.38 to -0.20)]. See also movie S1.

(E) (Top) Sample DMP trace segment showing a dynamic threshold for DAP initiation, with the initiation points marked by black circles. (Bottom left) Histogram of initiation voltages for the entire recording session from which the above was taken; the 5 to 95% range of initiation voltages spans 8.5 mV. (Bottom right) DAP initiation range [3.67 (2.24 to 6.99); $n = 25$ dendrites] was larger ($P = 5.1 \times 10^{-5}$, Wilcoxon signed-rank test) than the corresponding DAP amplitude and positively correlated [$r = 0.63$ (0.31 to 0.82); $P = 7.4 \times 10^{-4}$, two-sided t test]. (F) Sample DAP firing rate as a function of relative voltage, which was well approximated (fig. S9G) by a sigmoidal logistic function (black line). Firing rates here vary by 46.8 Hz over a dynamic range of 4.4 mV. (G) (Left) The population of DAP had a large dynamic range of initiation voltages [4.03 mV (2.74 to 5.07 mV); $n = 25$ dendrites], as defined in (F). (Right) The firing rate range of the DAP population was similarly wide [33.1 Hz (20.3 to 53.1 Hz); $n = 25$ dendrites]. Data are reported and presented as median and 95% confidence interval of the median.

of thousands of microvolts, reaching up to 20 mV (Fig. 4, A and B), far exceeding the range of the LFP on nearby tetrodes (Fig. 4B). The range of the subthreshold fluctuation was positively correlated with the DAP amplitude on the same recording (Fig. 4C). Nearby LFP range was not correlated with DAP amplitude (fig. S9A). These results could arise because of the quality of glial-sealed encapsulation (figs. S3 and S4). The subthreshold range was always greater (6.8-fold) than the corresponding DAP amplitude (Fig. 4C), a membrane property primarily observed in vitro

in dendrites that are electrotonically distant from the soma (3, 5–8, 20, 23–25). In all but one case, the DMP signal in SWS was significantly negatively correlated with the LFP signal on a nearby tetrode (Fig. 4D, fig. S9B, and movie S1), similar to somatic membrane results (74).

We next quantified the relationship between the instantaneous subthreshold DMP magnitude and DAP rate (see methods) (75). The range of subthreshold DMP at which DAP initiated was 4.4-fold larger than the magnitude of the corresponding DAP and positively correlated with DAP

amplitude (Fig. 4E). The large DAP initiation range (Fig. 4E) is similar to that reported for dendrites in vitro (3, 5–8, 20, 25), further supportive of the dendritic origin of our measurements.

Subthreshold DMP strongly modulated DAP rates. During SWS, DAP rate had a slowly increasing, sigmoidal dependence on subthreshold DMP (Fig. 4F), with the rate increasing over a large dynamic voltage range (see methods), which often exceeded the magnitude of DAP themselves (Fig. 4, F and G, and fig. S9C). The firing rate was modulated from nearly 0 Hz at low values of the

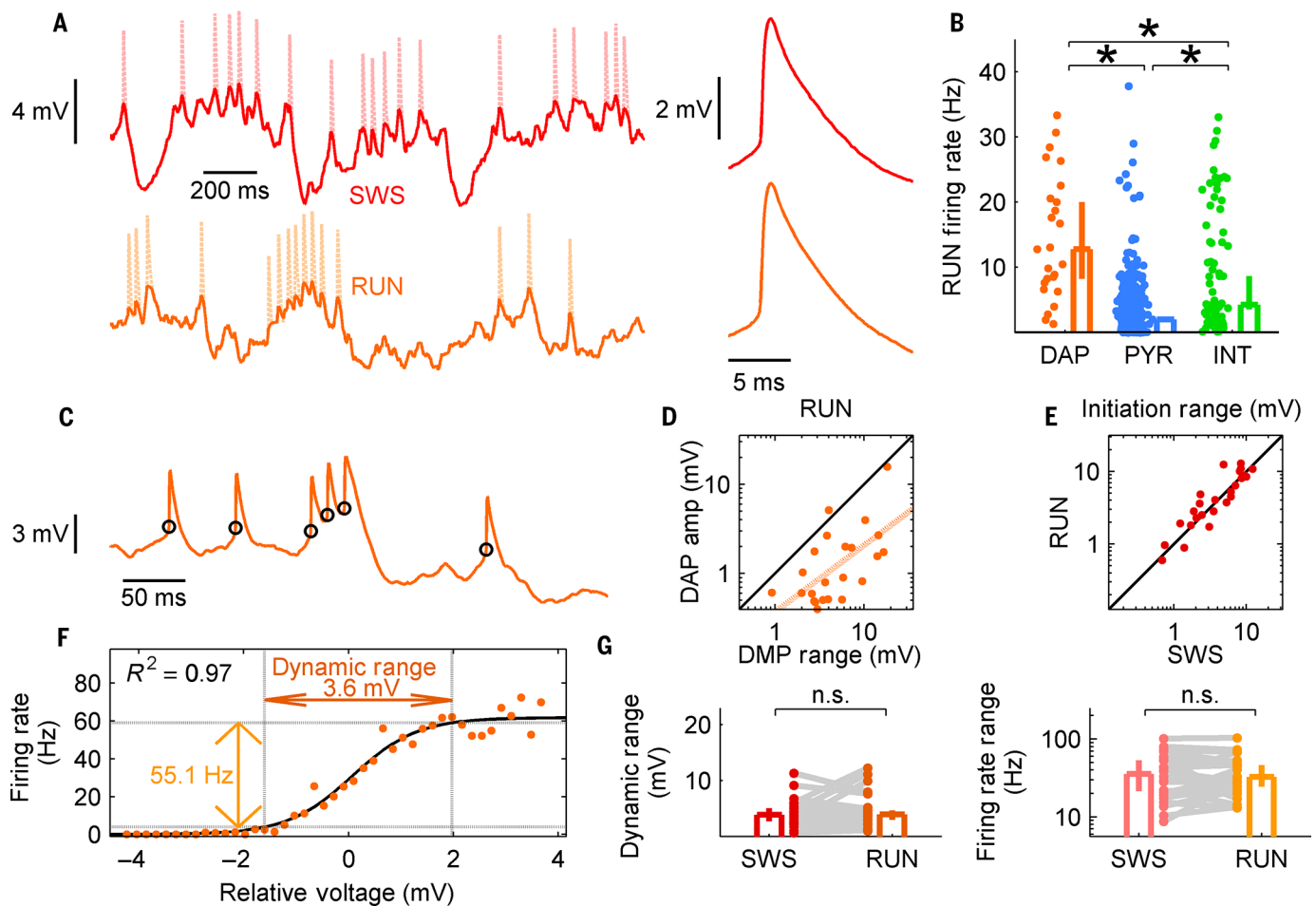


Fig. 5. Large subthreshold membrane potential fluctuations modulate DAP rates during RUN. (A) Sample membrane potentials during SWS (red; left) and locomotion (RUN; orange; right) show similar dynamics and amplitude of both DMP and DAP (middle). (B) DAP mean firing rate during RUN [12.8 Hz (8.29 to 20.0 Hz); $n = 25$ dendrites] was significantly greater than that of pyramidal neurons [1.99 Hz (1.63 to 2.37 Hz); $n = 657$ units; $P = 1.8 \times 10^{-5}$, Wilcoxon rank sum test] and interneurons [4.25 Hz (3.57 to 8.65 Hz); $n = 97$ units; $P = 8.3 \times 10^{-3}$, Wilcoxon rank sum test]. (C) Sample DMP trace during RUN shows a dynamic initiation range similar to that observed in SWS (Fig. 4E). (D) DMP range during RUN [3.82 mV (2.76 to 6.17 mV); $n = 25$ dendrites] was significantly larger ($P = 1.6 \times 10^{-5}$, Wilcoxon signed-rank test) than the corresponding DAP amplitude [0.82 mV (0.52 to 1.78 mV); $n = 25$ dendrites] and significantly correlated [$r = 0.68$ (0.39 to 0.85); $P = 2.0 \times 10^{-4}$, two-sided t test]. (E) DAP initiation ranges in SWS [3.67 mV (2.24 to

6.99 mV); $n = 25$ dendrites] and RUN [4.07 mV (2.51 to 8.14 mV); $n = 25$ dendrites] were positively correlated [$r = 0.91$ (0.80 to 0.96); $P = 3.4 \times 10^{-10}$, two-sided t test] and not significantly different ($P = 0.46$, Wilcoxon signed-rank test). (F) Sample V - R curve during RUN, which was well described (fig. S11) by a sigmoidal logistic function. (G) Twenty-four of 25 dendrites had sufficient data to characterize V - R curves in RUN. (Left) The dynamic voltage range during RUN [3.90 mV (2.98 to 4.67 mV); $n = 24$ dendrites] was not significantly different ($P = 0.73$, Wilcoxon signed-rank test) from the dynamic range in SWS [3.87 mV (2.74 to 5.03 mV); $n = 24$ dendrites]. (Right) The firing rate range in RUN [32.5 Hz (24.6 to 46.5 Hz); $n = 24$ dendrites] was not significantly different ($P = 0.86$, Wilcoxon signed-rank test) from the range during SWS [35.6 Hz (21.6 to 53.1 Hz); $n = 24$ dendrites]. Data are reported and presented as median and 95% confidence interval of the median. * $P < 0.05$; n.s., not significant.

membrane voltage up to above 100 Hz at the highest membrane voltages (Fig. 4, F and G, and fig. S9C). Because short-term ion channel dynamics could influence spike initiation properties (75), the above calculations were also done for only those DAPs that were separated from all others by at least 50 ms (termed solitary DAP), with only minor differences (fig. S9, D to H).

Dendritic sub- and suprathreshold membrane potential in freely moving rats

The stability of our recordings allowed us to compare dendritic activity and its subthreshold modulation between SWS and during spontane-

ous, free locomotion (RUN) (Fig. 5A; see methods). DAP mean rate during RUN (12.8 Hz) was nearly twice as large compared to the mean rate during SWS (6.87 Hz; Fig. 5B) and significantly greater than that of pyramidal neurons (1.99 Hz) or interneurons (4.25 Hz). There was no significant difference in the firing rates between slow and fast runs in DAP. DAP amplitude was slightly smaller during RUN compared to SWS (fig. S6, D and E), and rise time and width were slightly longer, though the difference in width was not statistically significant (Fig. 5, A and B).

Subthreshold DMP measures were also comparable in SWS and RUN. First, the magnitude of subthreshold DMP was equally large in the two

conditions (Fig. 5A and fig. S10). This is in contrast to the LFP, where fluctuations are severely diminished during locomotion compared to the large fluctuations present in SWS (fig. S10) (76, 77). The subthreshold DMP magnitude during locomotion was 4.7-fold larger than the corresponding DAP amplitude, and the two were highly correlated (Fig. 5, C and D), as in SWS. Second, DAP had a large initiation range in RUN (Fig. 5, C and E) that was fivefold larger than the corresponding DAP amplitude, as in SWS (fig. S11A). DAP rate during RUN was also modulated by subthreshold DMP in a sigmoidal fashion (Fig. 5, F and G, and fig. S11B) over a wide dynamic voltage range and spanned a large range of firing

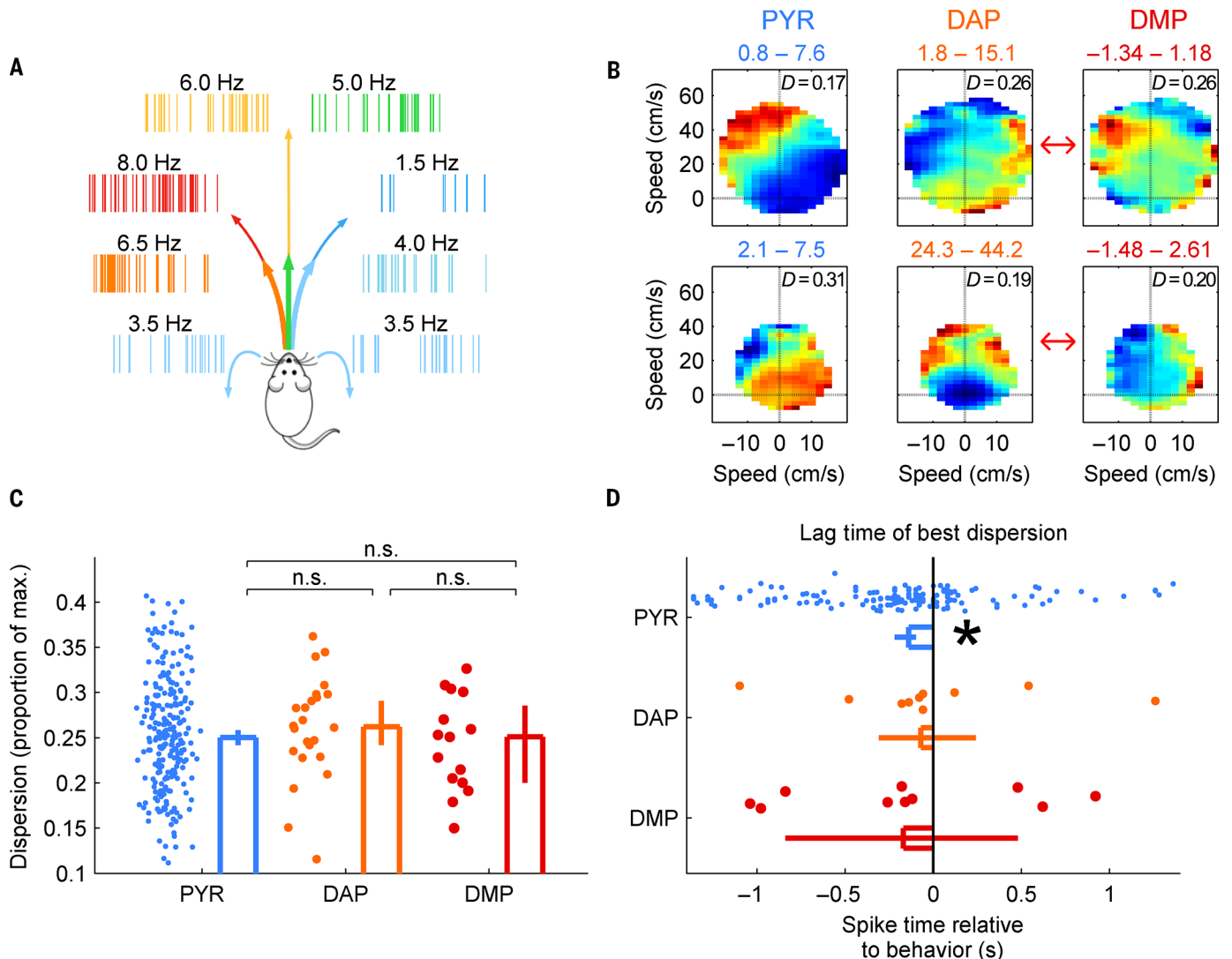


Fig. 6. DAP and DMP exhibit egocentric tuning comparable to somatic spikes. (A) Schematic of egocentric map computation. In this example, the neuron fires maximally (8 Hz, red) during a left-hand turn at high velocity and minimally (1.5 Hz, blue) during a right-hand turn at high velocity. (B) Two-sample pyramidal (PYR, left), DAP (middle), and DMP (right) egocentric maps. The minimum and maximum firing rates (mean voltages for DMP) for each map are displayed in the title, and the normalized dispersion D (see methods and fig. S10, A and B) is displayed in the upper-right corner. Red arrows indicate DAP and DMP from the same recording sessions. (C) The normalized dispersion (see methods) of PYR [0.25 (0.24 to 0.26); $n = 245$ maps] was not significantly smaller than that of DAP [0.26 (0.24 to 0.29); $n = 24$ maps; $P = 0.4$, Wilcoxon rank sum test] and DMP [0.25 (0.20 to 0.30); $n = 15$ maps; $P =$

0.57, Wilcoxon rank sum test]. DAP and DMP dispersions were not significantly different from each other ($P = 0.33$, Wilcoxon rank sum test). (D) The time lag corresponding to the optimal tuning for PYR with significant tuning [-140 ms (-220 to -100 ms); $n = 146$ maps with significant tuning] was significantly different from 0 ($P = 9.4 \times 10^{-7}$, Wilcoxon signed-rank test). The same measure for DAP [-70 ms (-310 to 240 ms); $n = 10$ maps with significant tuning] was not different from 0 ($P = 0.61$, Wilcoxon signed-rank test). DMP lag [-170 ms (-840 to 480 ms); $n = 10$ maps with significant tuning] was also not significantly different from 0 ($P = 0.43$; Wilcoxon signed-rank test) and not significantly different from either PYR ($P = 0.94$, Wilcoxon rank sum test) or DAP ($P = 0.5$, Wilcoxon rank sum test). Data are reported and presented as median and 95% confidence interval of the median. * $P < 0.05$; n.s., not significant.

rates, both of which were as large as in SWS (Fig. 5, F and G). These results were similar when performed on solitary DAP during locomotion (fig. S11, C to H).

Modulation of DAP, DMP, and soma by behavior

Do DAP and DMP contain information about instantaneous behavior? Previous studies have shown that somatic spike rates in the posterior parietal cortex (PPC) are modulated by specific

types of movements, including forward running, left turns, and right turns (Fig. 6A) (78, 79), and have an anticipatory component to their response (Fig. 6B and fig. S12A; see methods) (78). We computed the normalized dispersion, or spread, and depth of modulation of egocentric response maps for parietal DAP rate, subthreshold DMP voltage, and somatic spike rate (Fig. 6B and fig. S12A; see methods) during free locomotion in a rest box and a random foraging task (fig. S12B; see methods). The anticipatory component was

quantified by finding the time lag corresponding to the best tuning (fig. S12C; see methods).

There were similar properties of egocentric tuning in pyramidal somata (PYR), DAP, and DMP (Fig. 6C). Normalized dispersion for PYR (0.25) was slightly but not significantly better than that for DAP (0.26; $P = 0.40$, Wilcoxon rank sum test) and DMP (0.25; $P = 0.5714 \times 10^{-2}$, Wilcoxon rank sum test), which were also not significantly different from each other ($P = 0.33$, Wilcoxon rank sum test). The depth of modulation

of egocentric maps was comparable between all three groups (fig. S12D), with a similar percentage having a depth of modulation significantly above chance [PYR, 146 of 245, 60% (53 to 66%); DAP, 10 of 24, 42% (22 to 63%); DMP, 10 of 15, 67% (38 to 88%)]. Coherence showed a different pattern, with DMP having the highest coherence (fig. S12E), but this is likely an artifact because coherence is computed on unsmoothed rate maps, and the continuous DMP signal has more data than spiking point processes. Similar to dispersion, both short-term (fig. S12F) and long-term (fig. S12G) stability for PYR was larger than that for DAP and DMP, but the differences were not statistically significant.

The time lag corresponding to the optimal depth of modulation for pyramidal neurons with significant tuning was significantly negative (-140 ms, $P = 9.4 \times 10^{-7}$) (Fig. 6D) (78), indicating a preference to code for future movements. In some instances, somatic spikes were best tuned for behavior several seconds in the future or past (fig. S12H). The optimal lag time for significantly tuned DAP (-70 ms) and DMP (-170 ms) was not significantly different from 0 (DAP, $P = 0.50$; DMP, $P = 0.43$).

Hence, pyramidal neuron somata and dendrites both code for egocentric movement, but with differences that illustrate potential computational principles within a neuron. Pyramidal somatic responses are less dispersed than DAP and DMP responses, although equivalent percentages of PYR, DAP, and DMP are significantly tuned. The optimal coding occurs at negative time lags, or prospectively, for pyramidal somatic spikes but not for DAP or DMP.

Conclusions

We directly recorded the membrane potential and sodium spikes of putative neocortical distal dendrites in freely behaving rats without the confounding effects of recent anesthesia or restraint typically used with *in vivo* patch-clamp or optical imaging procedures. These measurements were done at submillisecond temporal resolution and were stable for at least 1 hour and up to 4 days. DAP kinetics were similar to those seen *in vitro* and in anesthetized animals (3, 5–8, 20, 23–25). These recordings revealed a number of interesting properties of dendritic activity. First, DAP occurred at very high rates *in vivo*, far greater than somatic rates. Second, DAPs were accompanied by large subthreshold DMP fluctuations, the magnitudes of which were always larger than the DAP amplitude. Third, this was present not only during SWS but also during free locomotion. Fourth, DAP rates varied by an order of magnitude as a function of the subthreshold DMP in a graded fashion during both SWS and movement, suggesting a large dynamic range. Fifth, unlike previous reports (26, 39), our measurements from PPC showed substantial differences between DAP, DMP, and somatic spikes in both quality and temporal dynamics.

Discussion

DAPs have long been hypothesized to endow neurons with greater computational power by turning

dendritic branches into computational subunits with branch-specific plasticity (14–16, 29–37). Dendrites support initiation and propagation of action potentials *in vitro* via voltage-gated sodium, potassium, and calcium channels (3, 5–8, 16, 20, 27–32). It has been unclear whether the conditions for generating DAP exist *in vivo* during natural behavior. Patch-clamp recordings in head-fixed mice suggest that proximal dendrites in visual cortex support spikes, though most of them were bAP and some were DAP (26). In contrast, our recordings are putatively from electrotonically distal-most dendrites, which generate dendritic spikes locally, and where somatically generated bAPs are mostly absent (2, 5, 6, 8, 19). These recordings were stable for hours or days at a time during free locomotion, with no evident damage to the dendrite.

We hypothesize that our tetrodes are in a “glial-assisted” configuration similar to *in-cell* or quasi-intracellular recordings (45, 46, 49, 50). In this model, the requisite high-seal resistance comes from glial encapsulation (53, 54) trapping a segment of a thin dendrite between the four electrode tips and the glial cells, forming a stable configuration, providing high-quality, positive-polarity, sub- and suprathreshold signals. Our immunohistochemical labeling and *in vivo* impedance spectroscopy measurements support this model, and the negative correlation between the subthreshold DMP and LFP is consistent with the whole-cell results from the soma (74). The encapsulation process might be facilitated by the fine-scale geometry of our gold-plated tetrode tips. However, the tetrodes have to be positioned close enough to a neuron to trap the dendrite without puncturing it. Our current success rate of dendritic recordings is quite low but comparable to the success rate of somatic whole-cell recordings during natural behavior (60, 80, 81).

Several signal properties, including dendritic spike rise time and width, firing rate, and short-term plasticity, are consistent with the hypothesis that our measurements are from the electrotonically distal-most dendrites of pyramidal neurons, and the dendritic spikes are generated locally in the dendrites, not back-propagated from the soma. The high DAP rates are unlikely to come from damage to the neuron due to stable DAP properties over hours. Spike properties, such as width and complex spiking, indicate that our data are from the pyramidal neurons but not from inhibitory interneurons. This may be because less than 20% of neurons are interneurons and their dendritic arbor is far smaller than that of pyramidal neurons, thus reducing the chances of encountering interneurons. The dendritic spike properties were unimodal, with low variability and no refractory violations, indicating a single dendritic source. Although many dendrites could be potentially trapped between the tetrode tips, very few would remain intact, reducing the success rate and the chance of recording multiple sources. This is consistent with recording two orders of magnitude less (than expected) extracellular cells using tetrodes (56).

Because these rates greatly exceed those of pyramidal units in the same brain region, a large

amount of activity and information processing in a neuron may be occurring in the dendrites without being read out in the postsynaptic soma, consistent with *in vitro* studies showing decoupling of somatic and dendritic compartments (2, 5, 6, 8, 11, 19, 31, 32). The results of DAP computations could travel to the rest of the network via second messengers and presynaptic mechanisms. The semi-independence of distal dendrites suggests that *N*-methyl-D-aspartate-dependent plasticity, which crucially depends on depolarization, could be induced in only a specific dendritic branch, allowing for more input-specific plasticity and clustering of synapses with similar information (11, 14, 33–37) and greatly expanding the computational capacity of a single neuron.

DAP firing rates are modulated in a graded fashion by the subthreshold DMP. This endows the dendrites with an analog code, defined by the depolarization level of the dendrite, reminiscent of the sigmoidal response profile of the hidden layer of artificial neural networks (34, 35). The digital coding, carried out by DAP, coexists with the subthreshold modulation, indicating a hybrid, analog-digital code in the dendrites. This large subthreshold modulation range (average, ~ 5 mV; maximum, ~ 20 mV) is consistent with but greater than recent results from the somata of hippocampal CA1 neurons (59, 60, 81), entorhinal stellate cells (82), and barrel cortex neurons (83). The true subthreshold voltage range in our case is likely even greater, because the magnitude of signals obtained through our measurement technique would be smaller than the true range and influenced by the quality of the glial seal. Our modeling results suggest that DAPs are measured at a distance from the site of initiation. Hence, local subthreshold fluctuations and variable propagation efficacy could result in variation in DAP peak voltage.

Somatic spikes in PPC are modulated by movement in an egocentric reference frame (79) in an anticipatory fashion during free behavior (78). DAP and DMP also exhibit egocentric modulation, but are more disperse and do not show significant anticipatory behavior. Our findings suggest a computational framework in which individual cortical neurons take information about the current state of the world, present in the dendrites, and form an anticipatory, predictive response at the soma, a computation similar to that performed by a Kalman filter (84) or hidden Markov model (85). Unlike network models of sequence learning, each individual neuron may behave like a feed-forward circuit that performs predictive coding based on nonpredictive inputs arriving from many dendritic branches (36, 86, 87). The intermediate integration step performed by the dendrites is likely a crucial one in neurons with extensive dendritic trees to allow inputs at distal tufts to be integrated in the somatic response (5).

These results demonstrate that dendrites generate far more spikes than the soma. This has important implications in many fields. The total energy consumption in neural tissue, measured in functional magnetic resonance imaging studies, could be dominated by the dendritic spikes

(88). Correlations between neuronal somatic spikes may be weak (89) due to the larger number of dendritic spikes, with only a fraction generating somatic spikes, possibly owing to inhibitory synapses interrupting propagation. Thus, the abundance of digital dendritic spikes and large analog subthreshold fluctuations in vivo could profoundly alter synaptic plasticity, altering the nature of neural coding and memory. This hybrid, analog-digital code in a dendrite, generated by a local cluster of excitatory synapses (36), may be the fundamental building block of neural information processing.

Methods summary

Data were obtained from nine adult male Long-Evans rats. The animals were food- and water-restricted. They received sugar water or solid cereal rewards during spatial exploration tasks, while their spatial position was monitored using an overhead camera. Rats were implanted with independently adjustable NiChrome tetrodes targeting prefrontal cortex and/or posterior parietal cortex. All methods were analogous to procedures described previously (51, 52) and in accordance with NIH approved protocols. Neural signals were recorded continuously using the Neuralynx data acquisition system and screened for intracellular-like signatures (e.g., broad, large-amplitude spikes of reverse polarity compared with extracellular units). Putative DAP were identified as positive peaks in the intracellular-like signal that exceeded noise threshold (fig. S1). Movement in an egocentric reference frame was computed frame by frame by calculating the difference in position and heading direction between the start and end of a moving time window (78). In vivo impedance spectroscopy was done during extracellular recording and DAP recording separately and fitted with a biophysical model to estimate the putative glial seal parameters. Upon the completion of experiments, brains were extracted and immunohistochemistry performed (fig. S3).

Compartmental modeling (fig. S7) was performed in NEURON version 7.2 (70) using a modification of a previously published model of a layer V pyramidal neuron (69). Tests of significance between unpaired data or paired data were conducted using the Wilcoxon rank-sum test or Wilcoxon signed-rank test, respectively. Unless otherwise stated, all values are reported as median and 95% confidence interval of the median, estimated using resampling statistics. All analyses were done offline using custom-written codes in MATLAB. Details of experimental methods, analyses, and modeling can be found in the supplementary materials (51, 52).

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SUPPLEMENTARY MATERIALS

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Dynamics of cortical dendritic membrane potential and spikes in freely behaving rats

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Dendrites are more active than expected

Dendrites occupy more than 90% of neuronal tissue. However, it has not been possible to measure distal dendritic membrane potential and spiking in vivo over a long period of time. Moore *et al.* developed a technique to record the subthreshold membrane potential and spikes from neocortical distal dendrites in freely behaving animals. These recordings were very stable, providing data from a single dendrite for up to 4 days. Unexpectedly, distal dendrites generated action potentials whose firing rate was nearly five times greater than at the cell body.

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