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Effects of oral temazepam on sleep spindles during non-rapid eye movement sleep: a high-density EEG investigation

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Abstract

Benzodiazepines are commonly used medications that alter sleep spindles during non-rapid eye movement (NREM) sleep, however the topographic changes to these functionally significant waveforms have yet to be fully elucidated. This study utilized high-density electroencephalography (hdEEG) to investigate topographic changes in sleep spindles and spindle-range activity caused by temazepam during NREM sleep in 18 healthy adults. After an accommodation night, sleep for all participants was recorded on two separate nights after taking either placebo or oral temazepam 15mg. Sleep was monitored using 256-channel hdEEG. Spectral analysis and spindle waveform detection of sleep EEG data were performed for each participant night. Global and topographic data were subsequently compared between temazepam and placebo conditions. Temazepam was associated with significant increases in spectral power from 10.33–13.83Hz. Within this frequency band, temazepam broadly increased sleep spindle duration, and

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CONTRIBUTORS

Dr. Plante designed the study, managed literature searches and analyses, and wrote the first draft of the manuscript. Mr. Goldstein and Mr. Cook performed statistical analyses, hdEEG processing and analysis, design of figures/tables, and contributed to study design and writing the manuscript. Mr. Smith, Dr. Rumble, Ms. Jelenchick, and Ms. Roth contributed to the evaluation of participants, collection of hdEEG data, and writing the article. Dr. Riedner contributed to analysis and interpretation of the data and writing the manuscript. Dr. Tononi and Dr. Benca contributed to the study design, data analysis and interpretation, and to writing the article. Dr. Peterson contributed by being the principal investigator of the parent study, contributing to the study design, participating in data analysis and interpretation, and writing the article. All authors contributed to and have approved the final manuscript.

CONFLICTS OF INTEREST

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topographically increased spindle amplitude and density in frontal and central-posterior regions, respectively. Higher frequency sleep spindles demonstrated increased spindle amplitude and a paradoxical decrease in spindle density in frontal and centroparietal regions. Further analysis demonstrated temazepam both slowed the average frequency of spindle waveforms and increased the relative proportion of spindles at peak frequencies in frontal and centroparietal regions. These findings suggest that benzodiazepines have diverse effects on sleep spindles that vary by frequency and cortical topography. Further research that explores the relationships between topographic and frequency-dependent changes in pharmacologically-induced sleep spindles and the functional effects of these waveforms is indicated.

Keywords

sleep spindle; temazepam; benzodiazepine; high density EEG

Introduction

Sleep spindles are characteristic electroencephalographic waveforms that occur during non-rapid eye movement (NREM) sleep. These waxing-waning oscillations play functionally significant roles in cortical development, sleep-dependent memory consolidation, and sleep maintenance (Fogel and Smith, 2011; Khazipov et al., 2004; Steriade, 2003). In addition, multiple investigations have demonstrated that reductions in sleep spindles may be a biomarker in schizophrenia and reflect thalamic reticular and/or thalamocortical deficits in the disorder (Ferrarelli et al., 2007; Ferrarelli et al., 2010; Genzel et al., 2015; Manoach et al., 2010; Phillips et al., 2012; Suh et al., 2013; Wamsley et al., 2012). Thus, understanding the effects pharmacologic agents have on sleep spindles is important for several spheres of research, including those related to sleep, plasticity, cognitive function, and neuropsychiatric disease.

Benzodiazepines are common psychotropic agents utilized clinically for their anxiolytic, anticonvulsant, muscle relaxant, and/or sedative-hypnotic properties, for which a sizeable prior literature details their effects on the sleep electroencephalogram (EEG) (Lancel, 1999). Multiple investigations have demonstrated that benzodiazepines increase spectral power in the spindle range (~10–16Hz) (Aeschbach et al., 1994a; Aeschbach et al., 1994b; Borbély et al., 1985; Dijk et al., 1989; Feige et al., 1999; Trachsel et al., 1990). Moreover, myriad investigations that have utilized methods to quantify sleep spindles have demonstrated that benzodiazepines increase the occurrence of these waveforms (Azumi and Shirakawa, 1982; Hirshkowitz et al., 1982; Johnson and Spinweber, 1981; Johnson et al., 1983; Monti and Altier, 1973; Suetsugi et al., 2001). This increase in sleep spindles has been hypothesized to result from positive allosteric modulation of the GABA-A receptor, which plays a key role in the generation of sleep spindles in the thalamic reticular nucleus (De Gennaro and Ferrara, 2003).

Despite several studies that have previously examined the effects of benzodiazepines on sleep spindles, prior investigations have typically utilized a limited number of EEG derivations (usually 1–2 central channels) in their analyses. This is an important limitation

of prior research because sleep spindles have a well-described topographic distribution, in which the frequency of the oscillation increases in a rostral to caudal gradient, with the occurrence of sleep spindles more prominent in midline derivations, particularly for fast (centroparietal) spindles (Andrillon et al., 2011; Peter-Derex et al., 2012; Schabus et al., 2007). Because a limited number of central channels may fail to detect pertinent alterations in sleep spindles (Ferrarelli et al., 2007), this study sought to utilize high-density EEG (hdEEG) to evaluate the topographic effects of the non-selective benzodiazepine, temazepam, on these functionally significant waveforms. Based on their previously described topography, we hypothesized that temazepam would increase slow and fast sleep spindles, most prominently in frontal and centroparietal derivations, respectively.

Experimental Procedures

Participants

All participants and sleep EEG data utilized in this study were drawn post hoc from a larger study that examined the effects of medications on sleep restriction. The University of Wisconsin-Madison Health Sciences Institutional Review Board approved this study and subsequent analyses. Participants were healthy volunteers recruited from the greater Madison, WI area and provided written-informed consent. Inclusion criteria included age 18–35 years, right-handedness, and body mass index (BMI) 19 and 32kg/m². Baseline evaluation included the Structured Clinical Interview for DSM-IV-TR Axis I disorders (First et al., 2002), urine drug screen, and urine pregnancy test (for female participants). Exclusion criteria included current or past psychiatric disorder (based on SCID interview), current or recent major medical or neurologic illness, use of centrally acting pharmacologic agents, reported caffeine intake greater than 300mg/day, average alcohol intake greater than 3 drinks/day or 8 drinks/week, daily use of nicotine within 6 months prior to enrollment, use of illicit drugs, night/evening shift work, or travel across 3 time zones in the month preceding enrollment. Female participants were excluded if they were pregnant, planning to become pregnant during the study, nursing, or lactating. At baseline participants had to endorse a typical bedtime between 2100 and 0100 hours and a usual nightly sleep duration between 6.5 and 8.5 hours. Participants were free of clinically significant sleep-related breathing or movement disorders, verified by clinical history and screening polysomnogram, with participants excluded if they demonstrated an apnea-hypopnea index >10/hr or a periodic limb movement arousal index >10/hr. In addition, participants were excluded if they were excessively sleepy, based on either score 10 on the Epworth Sleepiness Scale (Johns, 1991) or mean sleep latency <8 minutes on baseline multiple sleep latency testing (Sullivan and Kushida, 2008)

The sleep data utilized in these analyses occurred on two separate nights of sleep (within-subjects design) that each occurred prior to a supervised sleep restriction and recovery protocol. The placebo night was drawn from the placebo-arm of a randomized study of an investigational drug; the temazepam night was drawn from an open-label extension arm of this parent study. Prior to both (placebo and temazepam) nights, all participants had spent at least two nights in the sleep laboratory during eligibility screening (which included an accommodation night with hdEEG monitoring), and at least three weeks had elapsed since

undergoing any prior sleep restriction. Sleep-wake patterns were monitored between in-laboratory testing sessions using actigraphy (Actiwatch, Mini-Mitter, Bend, OR). Participants took either oral temazepam 15mg (open-label) or placebo (single tablet, not designed to be identical to temazepam) prior to bedtime on study nights.

Sleep EEG

HdEEG signals were collected with a vertex reference and 500 Hz sampling rate, first-order high-pass (0.1Hz) filtered and band-pass (0.3–50Hz) filtered in NetStation (Electrical Geodesics, Eugene, OR). HdEEG signals were then downsampled to 128 Hz, high-pass filtered (2-way least-squares FIR, 1Hz) and re-referenced to the average scalp voltage computed in all channels in MATLAB (MathWorks, Natick, MA). Semi-automatic artifact rejection was conducted to remove channels with interrupted contact with the scalp or high-frequency artifact. Specifically, thresholds were calculated for low (1–4 Hz) and high (20–30 Hz) frequency ranges at the 99.8th and 99.5th percentile, respectively, for each channel. Spectral power in these ranges across all 6-second NREM epochs for each channel were plotted for visual inspection. In cases where epochs with substantially greater low or high frequency power did not exceed the automatic threshold, the threshold was manually lowered and all epochs exceeding the threshold were removed. Also, channels with artifact affecting a majority of the recording were removed.

Spectral analysis of NREM sleep (all N2 and N3 epochs) was performed for each channel in consecutive 6-second epochs (Welch's averaged modified periodogram with a Hamming window; frequency resolution 0.17Hz), which maintained congruence between spectral analysis and traditional sleep staging based on 30-second epochs (Goldstein et al., 2012; Plante et al., 2012). Sleep staging was performed by a registered technologist according to standard criteria (Iber et al., 2007) using Alice® Sleepware (Philips Respironics, Murrysville, PA) based on 6 EEG channels at approximate 10–20 locations (F3, F4, C3, C4, O1, and O2) re-referenced to the mastoids, sub-mental electromyogram and electrooculogram.

Spindle Detection and Characterization

Spindle detection was performed with a custom spindle detection algorithm in MATLAB with similar specifications as prior research from our laboratory (Ferrarelli et al., 2007; Ferrarelli et al., 2010; Plante et al., 2013). NREM epochs were filtered within frequency bands in the spindle range (10–16Hz), and rectified filtered signals were used as the time series for each channel. In order to increase the likelihood of identifying pertinent between group differences, our *a priori* analysis of spindle parameters (detailed below) was designed to focus on spindles detected within frequency bands in the spindle range that demonstrated significant between-condition differences using global spectral power. In addition, because pertinent topographic differences in sleep spindles could be missed solely using this approach, additional exploratory analyses examined spindles in residual frequency bands, as well as the entire spindle range (10–16Hz). Also, because prior literature has suggested functional and topographic differences between slow (~10 to ~13–14Hz) and fast (~13–14 to ~16Hz) sleep spindles (Astori et al., 2013), with variable frequency ranges used to define this dichotomous classification among investigators, spindles categorized using standard

frequency cut-offs between slow (10 to 13–14Hz) and fast (13–14 to 16Hz) spindles were also examined for comparison purposes and to clarify results.

Details of the spindle detection algorithm have been described elsewhere (Ferrarelli et al., 2007). Briefly, a spindle was detected when the mean signal amplitude exceeded an upper threshold (6 times the mean amplitude). The peak amplitude for each spindle was the local maximum above the upper threshold. The beginning and end of a spindle occurred when the amplitude of the time series fell below a lower threshold (2 times the mean amplitude), occurring 0.25 seconds from the peak. We examined the following spindle parameters: density (number of spindles divided by artifact-free NREM sleep time), maximal amplitude, duration, and integrated spindle activity (ISA; integrated absolute amplitude values of each spindle divided by artifact-free NREM sleep time) (Ferrarelli et al., 2010).

Statistics

Sleep staging variables, as well as spectral power and spindle morphology data were compared between conditions (placebo vs. temazepam) using paired t-tests. To increase the signal-to-noise ratio, all hdEEG analyses were restricted to channels falling within a plotting radius of 0.57 specified in the topoplot function of the EEGLAB plug-in for MATLAB (Delorme and Makeig, 2004), resulting in 173 channels overlaying the scalp. For analyses, global spectral power was defined as the average of these 173 channels. Topographic comparisons of spectral and spindle data were performed using channel-by-channel paired t-tests. Statistical non-parametric mapping (SnPM) with suprathreshold cluster testing was utilized to correct for multiple comparisons of topographic data using a t-value threshold corresponding to $\alpha=0.05$ for the uncorrected comparisons (Nichols and Holmes, 2002), with missing data for a given channel interpolated using the average of surrounding channels in order to maintain maximal degrees of freedom without altering the mean signal of the group. All statistical analyses were performed using MATLAB.

Results

Sleep staging, spectral activity and spindle morphology

Participants (11 female; 7 male) were aged 23.5 ± 3.6 years (range 18–29). Sleep staging demonstrated no significant differences between placebo (PLC) and temazepam (TMZ) nights on standard variables (Table 1). Sixteen of the 18 participants had intact actigraphy for analysis (two had device failure) that confirmed similar bedtimes (mean 00:03 hours for PLC and 00:08 hours for TMZ) and sleep duration (7.68 hours for PLC and 7.48 hours for TMZ, $p=0.25$) prior to polysomnography. There were no significant between condition differences in percent of retained N2/N3 epochs (PLC: $94.3\pm 2.6\%$ vs. TMZ: $93.2\pm 5.8\%$; $p=0.40$) or retained channels (PLC: $96.0\pm 4.7\%$ vs. TMZ: $96.0\pm 4.8\%$; $p=0.97$) after artifact rejection.

Analyses of global (average of 173 channels) spectral power in the spindle range demonstrated TMZ was associated with significant increases from 10.33–13.83Hz (Figure 1). Topographic analyses of spectral activity within this frequency band demonstrated

increases that were most prominent in frontal and parieto-occipital channels in midline and bilateral derivations in TMZ relative to PLC (Figure 2).

Using global spindle detection data within 10.33–13.83Hz, spindle duration and amplitude were significantly increased for TMZ relative to PLC, without significant changes in density or ISA (Table 2). Topographic analysis demonstrated the scalp distribution of density of these slower sleep spindles was more prominent in bilateral frontocentral areas for both PLC and TMZ conditions, consistent with prior literature (Figure 2) (Andrillon et al., 2011; Peter-Derex et al., 2012; Schabus et al., 2007). However, topographic increases in spindle density were observed in central-posterior derivations (e.g. outside of frontocentral regions) for TMZ relative to PLC (Figure 2). In addition, spindle amplitude significantly increased in frontocentral regions (Figure 2). Topographic analysis also demonstrated spindle duration increased in the vast majority of channels, except for a few centrolateral derivations (Figure 2). There were no significant topographic changes for ISA observed. Similar global and topographic patterns were observed for spindles detected with frequencies 10–14Hz and 10–13Hz (data not shown).

Spindle detection within a residual fast spindle range (13.83–16Hz) demonstrated significant increases in global spindle amplitude and decreases in spindle density, without significant differences in duration or ISA (Table 2). Topographic analysis of spectral power in this band demonstrated no significant differences between conditions (Figure 3). Topographic data demonstrated these faster spindles were more common in central midline derivations for both conditions, consistent with prior literature (Figure 3) (Andrillon et al., 2011; Peter-Derex et al., 2012; Schabus et al., 2007). Notably, topographic analysis also demonstrated a decrease in spindle density and a concurrent increase in spindle amplitude in frontal and central midline derivations in TMZ relative to PLC (Figure 3). Additionally, a minor right posterolateral increase in spindle duration was observed with TMZ, without topographic changes for ISA (Figure 3). Similar global and topographic patterns were observed for spindles detected between 14–16Hz and 13–16Hz (data not shown).

For comparison purposes, data using the full spindle range (10–16Hz) were additionally analyzed. Global data demonstrated a similar pattern to slower (i.e. 10.33–13.83Hz) spindles with significant increases in spindle duration and amplitude in TMZ relative to PLC, without significant differences in density or ISA (Table 2). Topographically, as observed in both slower and faster (i.e. 13.83–16Hz) spindles, amplitude was increased by TMZ in frontocentral regions (Figure 4). In addition, TMZ broadly increased spindle duration in frontal, central, and lateroposterior areas, with no significant topographic differences in spindle density or ISA between conditions.

Additional Exploratory Analyses

Since the effects of TMZ on sleep spindles varied depending on the frequency range in which detected spindles were evaluated, the effects of TMZ on the distribution of detected spindles across the broad spindle frequency range were analyzed. The average frequency for detected spindles at each channel was compared between conditions (Figure 5). In addition, the distribution of detected spindles was apportioned into adjacent 0.25Hz bins, and the peak frequency and relative magnitude (% of total detected spindles) of the peak of the

distribution were compared between TMZ and PLC (Figure 5). TMZ reduced the average and peak frequencies of detected spindles, most prominently in frontal derivations, while increasing the peak magnitude of the distribution in frontal and midline channels. For visualization purposes, these effects are displayed in twelve midline derivations in Supplemental Figure 1, illustrating the leftward shift (i.e. reduction) of the frequency distribution of detected spindles and an increased percentage of spindles at the peak frequency in TMZ relative to PLC. Thus the decreased density of fast sleep spindles observed occurred in the context of generalized slowing of all detected spindles, that was most pronounced in frontocentral derivations.

Also, because the maximal amplitude of a sleep spindle is a function of waxing and waning amplitudes, which are hypothesized to result from different mechanisms (Urakami et al., 2012), we examined whether TMZ differentially affected the latency to the maximal amplitude for detected spindles. We found no significant topographic differences between conditions for latency to the maximal amplitude (both absolute and normalized to spindle duration), nor the waxing or waning slope of the oscillation (derived from spindle onset to maximal amplitude and maximal amplitude to termination, respectively) (Supplemental Figure 2).

Although we chose to examine sleep spindles in all N2/N3 sleep to minimize the chance that differences in sleep architecture/staging or intra-individual differences in drug metabolism during the course of the night might influence results, we additionally explored differences in sleep spindles between PLC and TMZ in separate sleep cycles [i.e. separate NREM episodes using previously defined criteria (Kurth et al., 2010)]. Similar topographic findings were observed for spindle amplitude and duration for both slow and fast spindles for the first three NREM episodes. Spindle density also showed similar topographic patterns for slow and fast spindles, except the increased density of slow spindles due to TMZ expanded to include frontocentral channels in the first NREM sleep cycle (data not shown).

To examine whether BMI might have affected findings given a fixed dose of temazepam within a heterogeneous participant group (mean BMI 23.6, range 19.3–31.8kg/m²), we explored correlations between BMI and change in spindle density, amplitude, and duration. We found no significant correlations between BMI and these parameters for either slow or fast spindles using global measures. Additionally, we performed exploratory correlations between global slow wave activity (EEG power 1–4.5Hz for all epochs of N2/N3 sleep) and spindle parameters (density, duration, and amplitude) for fast and slow spindles, finding no significant correlations among these variables for either PLC or TMZ conditions.

Discussion

Consistent with prior investigations, our findings demonstrate that the oral administration of the non-selective benzodiazepine temazepam results in alterations in spectral activity in the spindle range, as well as spindle density and morphology during non-rapid eye movement sleep. In regards to global spectral power, our results are consistent with several prior reports demonstrating that the increase in spindle range activity during NREM sleep associated with benzodiazepines is typically below ~14Hz (Aeschbach et al., 1994a;

Aeschbach et al., 1994b; Borbély et al., 1985; Dijk et al., 1989; Trachsel et al., 1990). Our study and the use of high-density EEG to evaluate sleep spindles additionally further extends the previous literature in several ways. First, we found that the density, amplitude, and duration of slower (~10–14Hz) sleep spindles were differentially increased by temazepam, with varying cortical topographies for these measures. Second, temazepam resulted in an unexpected topographic decrease in spindle density of faster (~14–16Hz) sleep spindles, despite a concurrent increase in amplitude. Third, the differential effects of temazepam on slow and fast spindles observed in this study were mediated, at least in part, by a shift in the distribution of spindles to lower frequencies, without an overall net change in spindle density from 10–16Hz.

Although this study is not designed to evaluate the cellular and molecular mechanisms through which temazepam alters sleep spindle morphology, it is most likely that the drug enacts its effects through agonism of the GABA-A receptor at thalamic reticular neurons. The spindle rhythm is generated by rhythmic interactions between inhibitory neurons of the reticular nucleus and excitatory thalamocortical neurons (Urakami et al., 2012). Recent work has suggested that the duration of a sleep spindle is dependent on the inhibitory activity of reticular neurons, such that termination of the oscillation occurs once inhibitory input decreases below a minimal value required for evoking rebound bursts in thalamocortical cells (Barthó et al., 2014). Similarly, the degree and/or duration of inhibitory post-synaptic potentials imposed by reticular neurons on thalamocortical cells is the primary determinant of intra-spindle frequency (Urakami et al., 2012). Of note, the duration of slow spindles in both placebo and temazepam conditions in this investigation was greater than that of fast spindles, a finding that has also been observed in other investigations most prominently in frontal electrodes (Ujma et al., 2015). Therefore the changes in spindle duration and frequency caused by temazepam observed in this study would most likely result from potentiation of the GABA-A receptor in thalamic reticular neurons, and although speculative, suggests that potentiation of the GABA-A receptor may have more substantial effects on the duration of slow relative to fast spindles.

The probable mechanism through which temazepam increased spindle amplitude in our study is less clear. The maximal amplitude of the spindle oscillation is a function of waxing and waning amplitudes, the former correlated to the amplitude of neuronal excitatory post-synaptic potentials and the latter likely resulting from cortical feedback to the thalamus as well as deterioration of synchronization of thalamocortical neurons, with resultant asynchrony of reticular neurons (Urakami et al., 2012). Since temazepam should increase cortical *inhibitory* post-synaptic potentials, increases in spindle amplitude via effects on the waning rather than waxing amplitude seem more likely. However, because there were no observable differences between placebo and temazepam conditions in our study for either latency to maximal amplitude or the waxing/waning slopes of the oscillation, our data do not point to differential effects of temazepam on the waxing versus waning portions of sleep spindles (i.e. the symmetry of the waveform), and thus mechanisms through which temazepam increases spindle amplitude are highly speculative. However, regardless of the mechanism through which temazepam increases spindle amplitude, the results of this study are consistent with the findings of prior investigations (Hirshkowitz et al., 1982).

Our results are further consistent with prior research that has demonstrated that slow (~10 to ~13–14Hz) and fast (~13–14 to ~16Hz) spindles have different cortical topographies, with slow spindles more prominent in frontal regions, and fast spindles more pronounced in centroparietal areas (Andrillon et al., 2011; Peter-Derex et al., 2012; Schabus et al., 2007). It has been suggested that slow and fast spindles have varying functional roles, particularly in the context of sleep-dependent memory consolidation (Astori et al., 2013). It is noteworthy that our results suggest temazepam decreases the density of fast sleep spindles, as prior studies that have not utilized hdEEG have reported increases in sleep spindles associated with benzodiazepine administration. In this context, our results may elucidate the paradox that benzodiazepines have been associated with increases in sleep spindles using limited EEG montages, but decrements in some forms of sleep-related memory consolidation.

The motor sequence task (MST) is a widely used paradigm to investigate the effects of sleep and EEG waveforms on motor memory (Albouy et al., 2013; Barakat et al., 2011; Nishida and Walker, 2007; Wamsley et al., 2013; Wamsley et al., 2012). Improvement on the MST has been positively associated with spindle density, particularly with fast spindles in centroparietal regions (Barakat et al., 2011; Nishida and Walker, 2007). Notably, the non-selective benzodiazepine triazolam paradoxically worsens overnight performance on the MST, despite reports that this medication increases the density of sleep spindles (Johnson and Spinweber, 1981; Morgan et al., 2010). Our results suggest that impairment on the MST caused by benzodiazepines may be due to topographic decreases in fast sleep spindles, that may not have been previously observed in other studies due to either inadequate topographic resolution of sleep EEG and/or failure to distinguish between slow and fast spindles. However, it is certainly also plausible that other factors such as slowed response time or functionally different properties of pharmacologically-induced sleep spindles compared to those produced endogenously, may account for the paradoxical worsening on the MST associated with benzodiazepines.

To extend our results utilizing temazepam to other non-selective benzodiazepines, and thus assume that the alterations in sleep spindles observed in this study are a class effect, must be done with caution. Although benzodiazepines have a shared mechanism of action, they have a diversity of pharmacokinetic profiles that could theoretically result in variable effects on sleep spindles. Moreover, the results of this study cannot be extended to other GABAergic sedative hypnotics, such as non-benzodiazepine benzodiazepine receptor agonists (BZRAs). Both zolpidem and eszopiclone have been shown to increase spindle density without changes in frequency, amplitude, or duration of spindles (Mednick et al., 2013; Wamsley et al., 2013). Notably, the reticular nucleus is devoid of GABA-A α_1 -receptors, and synaptic inhibition is mediated by α_3 -receptors; while α_1 -receptors mediate inhibition in thalamocortical relay neurons (Huntsman et al., 1999; Jia et al., 2005; Pirker et al., 2000). Correspondingly, in vitro studies have demonstrated that zolpidem exerts larger effects on thalamocortical neurons, while eszopiclone has larger effects on reticular neurons (Jia et al., 2009). Because these GABAergic agents have also demonstrated divergent effects on the MST (Mednick et al., 2013; Morgan et al., 2010; Wamsley et al., 2013), future research that examines the relationship between GABA-A subtype receptor affinity, sleep spindle density/morphology, and pharmacological enhancement of sleep-dependent memory consolidation, may yield further insights into the relationships between these factors.

There are limitations of this study that merit discussion. First, this was a fixed-dose study, and thus observed differences between temazepam and placebo conditions may have differed if a higher dose were utilized, particularly since dose-response effects of benzodiazepines on sleep spindle incidence have been previously reported (Hirshkowitz et al., 1982). Second, the temazepam night was part of an open-label extension, and thus our unblinded design may have affected results. However, prior studies utilizing temazepam have demonstrated that even in double-blind protocols, study participants are usually able to discern whether they are on active drug or placebo (Morin et al., 1995), which reduces the likelihood that our results would have differed using a blinded protocol. Third, there may have been an order effect as TMZ nights occurred after PLC nights. However, the risks of order effects are minimized by the relative stability of spindle activity from night to night (Curcio et al., 2004; Le Bon et al., 2001). Fourth, caffeine intake was based on self-report and not verified by objective assay, which may have affected results since caffeine can increase power in the sigma range (Drapeau et al., 2006; Landolt et al., 2004). Fifth, our spindle detection algorithm was selected due to its previous application in hdEEG studies (Ferrarelli et al., 2007; Ferrarelli et al., 2010; Plante et al., 2013) and to maximize precision over recall (Warby et al., 2014), to minimize the likelihood that false positive detections would lead to spurious results. However, our results may have differed had we utilized a different spindle detection algorithm, particularly one that utilizes intra-individual thresholds for slow and fast spindles, such as proposed by Bódizs and colleagues (Bódizs et al., 2009). Finally, the phase of the menstrual cycle at the time of hdEEG recordings was not ascertained for female participants, which may have affected results, as spindle range activity has been reported to increase in the luteal relative to the follicular phase (Baker et al., 2007; Baker et al., 2012). Because prior research has also demonstrated a sex and menstrual phase effect on sleep-related memory consolidation and sleep spindle activity after learning (Genzel et al., 2012), future research that examines the effects of exogenous benzodiazepines on sleep EEG across the menstrual cycle, and their interactive effects on learning, may prove a fruitful avenue of investigation.

In conclusion, we have demonstrated temazepam results in global and topographic changes in spectral power and spindle density/morphology during the sleep EEG. These findings suggest that benzodiazepines have myriad effects on spectral activity and sleep spindles that vary depending on cortical topography and frequency of the waveform. Further studies that explore the relationship between topographic and morphological changes in sleep spindles induced by benzodiazepines and other related compounds, and their effects on sleep-dependent memory consolidation, development, and neuropsychiatric disorders, are indicated to clarify the functional significance of these findings.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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Sanofi had no further role in the design of this study, collection of data, analysis and interpretation of data, or writing of the manuscript. Sanofi was provided courtesy review of the manuscript prior to submission, but did not play a role in the decision to submit the report for publication.

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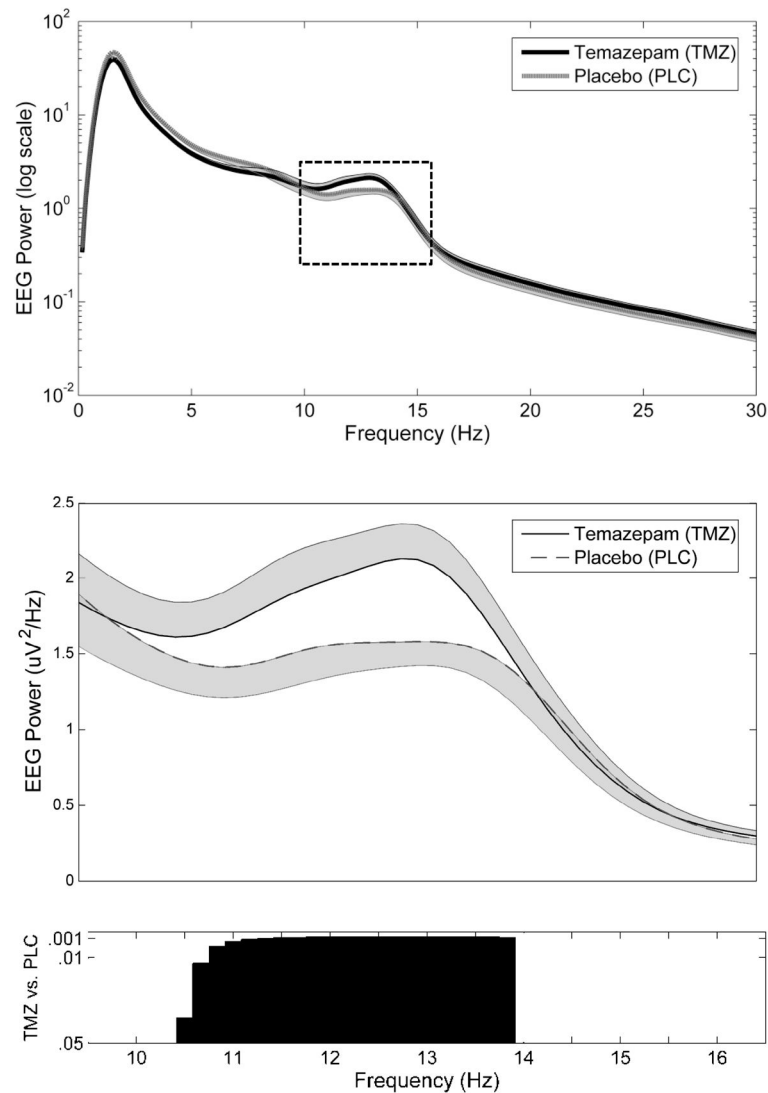


Figure 1. Differences in global spectral power in the spindle range between TMZ and PLC nights during NREM sleep. Global (average 173 channels overlying the scalp) EEG spectral power \pm SEM for TMZ and PLC plotted for each 0.17Hz frequency bin from 1–30Hz (top panel) and 10–16Hz (middle panel). Corresponding p-values for comparison between TMZ vs. PLC from 10–16Hz (lower panel). Significant differences in global power were observed between conditions for bins 10.33–13.83Hz.

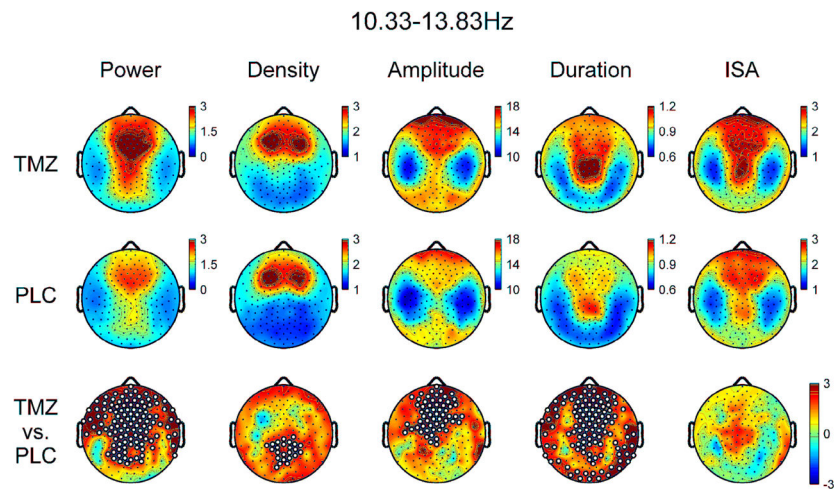


Figure 2. Topographic EEG power and slow spindle parameters for TMZ and PLC nights from 10.33–13.83Hz. Bottom row denotes t-values for channel-by-channel paired t-tests between TMZ and PLC. White dots denote significant channels after statistical non-parametric mapping with suprathreshold cluster test.

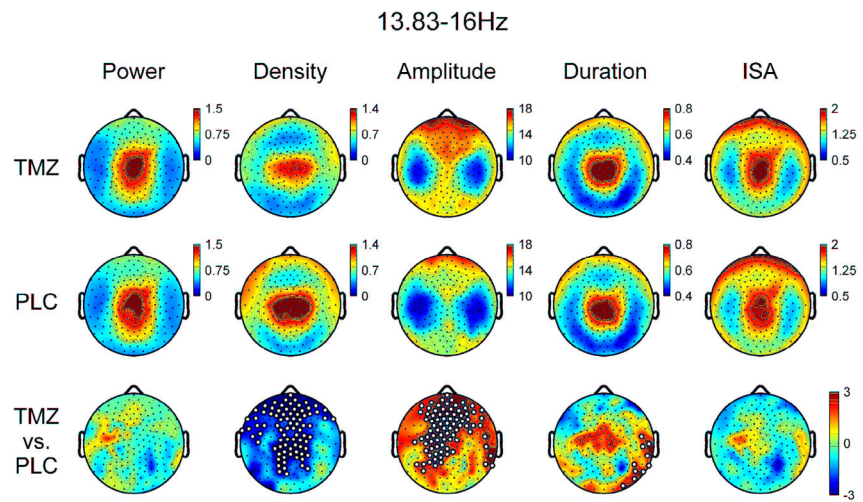


Figure 3. Topographic EEG power and fast spindle parameters for TMZ and PLC nights from 13.83–16Hz. Bottom row denotes t-values for channel-by-channel paired t-tests between TMZ and PLC. White dots denote significant channels after statistical non-parametric mapping with suprathreshold cluster test.

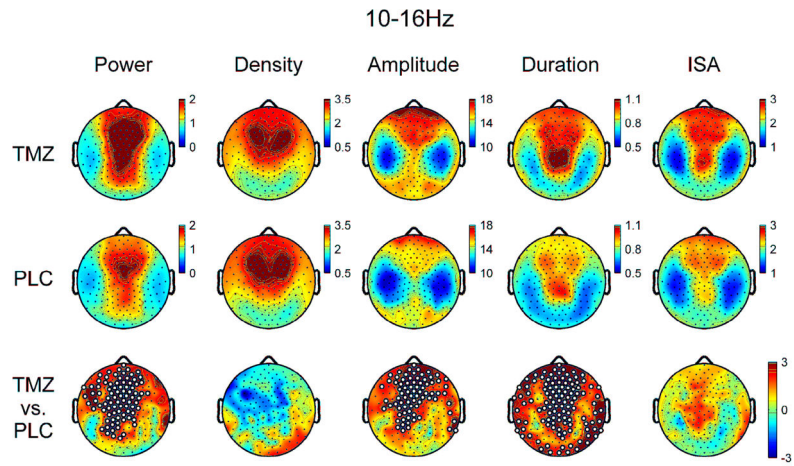


Figure 4. Topographic EEG power and spindle parameters for TMZ and PLC nights for all detected spindles 10–16Hz. Bottom row denotes t-values for channel-by-channel paired t-tests between TMZ and PLC. White dots denote significant channels after statistical non-parametric mapping with suprathreshold cluster test.

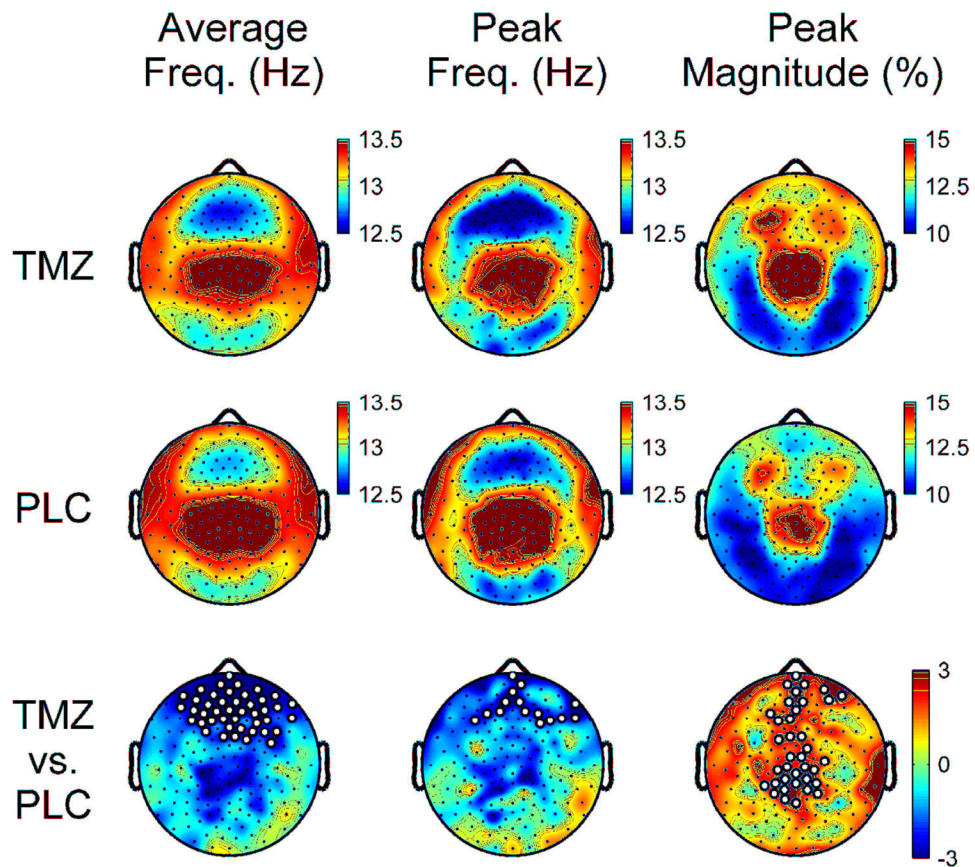


Figure 5. Topography of spindle frequency and peak magnitude of the distribution of detected spindles for TMZ and PLC nights. Average frequency analyzed as a continuous variable and represents the mean spindle frequency for all detected spindles at each channel. Peak frequency derived by apportioning detected spindles at each channel into adjacent 0.25Hz bins from 10–16Hz and determining the bin of maximal proportion of oscillations relative to the total number of detected spindles at each channel (peak magnitude). Bottom row denotes t-values for channel-by-channel paired t-tests between TMZ and PLC. White dots denote significant channels after statistical non-parametric mapping with suprathreshold cluster test.

Table 1

Sleep staging data.

	PLC	TMZ	p-value
TST (min)	424.7 (47.4)	436.6 (41.1)	0.32
WASO (min)	35.8 (32.1)	35.4 (43.7)	0.97
SE (%)	90.1 (8.5)	91.1 (9.1)	0.54
SOL (min)	12.2 (14.3)	7.4 (6.8)	0.16
N1 (min)	51.7 (34.6)	36.3 (25.0)	0.15
N1 (%)	12.6 (9.3)	8.3 (5.6)	0.10
N2 (min)	260.7 (50.0)	280.5 (52.6)	0.19
N2 (%)	61.2 (8.0)	64.3 (10.1)	0.29
N3 (min)	44.5 (30.5)	51.4 (25.5)	0.46
N3 (%)	10.2 (6.7)	11.8 (5.8)	0.44
REM (min)	68.0 (32.2)	68.4 (33.8)	0.95
REM (%)	16.0 (7.6)	15.6 (7.5)	0.82
REM Latency (min)	144.5 (92.3)	141.8 (92.4)	0.93

PLC, placebo; TMZ, temazepam; TST, total sleep time; WASO, wake after sleep onset; SE, sleep efficiency (TST/time in bed); SOL, sleep onset latency; N1/2/3, NREM stage 1/2/3 (minutes and % of TST); REM, stage REM (minutes and % of TST); REML, REM latency (time from sleep onset to first REM sleep epoch).

Values are displayed as mean (standard deviation).

* p -value derived using 2-tailed, paired t-tests.

Table 2

Global spindle characteristics.

	PLC	TMZ	p-value
Spindle Frequency: 10.33–13.83Hz			
Density (count/min)	2.01 (0.68)	2.13 (0.68)	0.17
Amplitude (μ V)	14.13 (3.80)	15.10 (3.67)	0.01
Duration (sec)	0.89 (0.13)	0.98 (0.19)	0.0008
ISA (μ V ² /min)	2.22 (0.78)	2.37 (0.91)	0.37
Spindle Frequency: 13.83–16Hz			
Density (count/min)	0.84 (0.49)	0.67 (0.40)	0.01
Amplitude (μ V)	13.59 (3.62)	14.64 (3.49)	0.002
Duration (sec)	0.61 (0.10)	0.59 (0.11)	0.11
ISA (μ V ² /min)	1.46 (0.55)	1.45 (0.47)	0.88
Spindle Frequency: 10–16Hz			
Density (count/min)	2.80 (0.58)	2.85 (0.63)	0.36
Amplitude (μ V)	13.99 (3.76)	14.99 (3.67)	0.006
Duration (sec)	0.82 (0.13)	0.91 (0.19)	0.0007
ISA (μ V ² /min)	2.07 (0.76)	2.22 (0.91)	0.33

Global values derived from the average of 173 channels overlying the scalp. PLC, placebo; TMZ, temazepam. Values are displayed as mean (standard deviation).

* *p*-value derived using 2-tailed, paired t-tests uncorrected for multiple comparisons.

Significant between condition values marked in bold.