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Characterizing Blood–Brain Barrier Perturbations after Exposure to Human Triglyceride-Rich Lipoprotein Lipolysis Products Using MRI in a Rat Model

Kit Fai Ng,¹ Steve Anderson,² Patrice Mayo,¹ Hnin Hnin Aung,¹ Jeffrey H. Walton,³ and John C. Rutledge¹*

Purpose: Previous studies indicated hyperlipidemia may be a risk factor for Alzheimer's disease, but the contributions of postprandial triglyceride-rich lipoprotein (TGRL) are not known. In this study, changes in blood-brain barrier diffusional transport following exposure to human TGRL lipolysis products were studied using MRI in a rat model.

Methods: Male Sprague-Dawley rats (~180–250 g) received an i.v. injection of lipoprotein lipase (LpL)-hydrolyzed TGRL (n=8, plasma concentration \approx 150 mg human TGRL/dL). Controls received i.v. injection of either saline (n=6) or LpL only (n=6). The ¹H longitudinal relaxation rate R₁ = 1/T₁ was measured over 18 min using a rapid-acquired refocus-echo (RARE) sequence after each of three injections of the contrast agent Gd-DTPA. Patlak plots were generated for each pixel yielding blood-to-brain transfer coefficients, K_i, chosen for best fit to impermeable, unidirectional influx or bi-directional flux models using the F-test.

Results: Analysis from a 2-mm slice, 2-mm rostral to the bregma showed a 275% increase of mean K_i during the first 20 min after infusion of human TGRL lipolysis product that differed significantly compared with saline and LpL controls. This difference disappeared by 40 min mark.

Conclusion: These results suggest human TGRL lipolysis products can lead to a transient increase in rat BBB permeability. Magn Reson Med 76:1246–1251, 2016. © 2015 The Authors. Magnetic Resonance in Medicine published by Wiley Periodicals, Inc. on behalf of International Society for Magnetic Resonance in Medicine. This is an open access article under the terms of the Creative Commons Attribution NonCommercial License, which permits use, distribution and reproduction in any medium, provided the original work is properly cited and is not used for commercial purposes.

Key words: hyperlipidemia; triglyceride-rich lipoprotein; permeability; blood-brain barrier; Gd-DTPA

INTRODUCTION

Alzheimer's disease (AD) is a progressive neurodegenerative disease characterized by irreversible memory loss, deposition of amyloid plaques, neurofibrillary tangles, and brain atrophy (1). In 2012 alone, one in eight Americans over 65 was afflicted with AD, i.e., 5.4 million patients, or approximately 2% of the U.S. population (2). AD and cardiovascular diseases (CVD) share very similar risk factors, including hypertension, apolipoprotein-E4 genotype and type 2 diabetes (3). Furthermore, lipid profiles of AD patients are also similar to those who are at risk of CVD, and in particular high plasma triglyceride is correlated with vascular dementia and AD (4-6). Yet clinical trials aimed to lower triglyceride content using fibrate drugs have had mixed results (7,8). There is also increased recognition that blood-brain barrier (BBB) dysfunction could be a contributing factor (6,9–11). Simply put, there is still no consensus on the etiology of AD.

While numerous studies have demonstrated elevated fasting triglyceride concentration is a risk factor for AD, the contribution of postprandial hypertriglyceridemia to AD is unknown. Dietary lipids are absorbed in the intestine and secreted into the circulation as chylomicrons within 3 to 4 h after ingesting a moderate to high fat meal (12). Alternately, endogenously synthesized triglycerides are transported by very-low density lipoproteins (VLDL) that are produced in the liver. Together chylomicrons and VLDL are classified as triglyceride-rich lipoproteins (TGRL). Their compositions vary within a range of 50-90% triglyceride content and sizes vary between 25 and 1000 nm. Circulating TGRLs are hydrolyzed by endothelial-bound lipoprotein lipase (LpL) that have been found on brain microvessels (13). Hydrolyzing TGRLs releases a conglomerate of free fatty acids and phospholipids known as lipolysis products. At high physiological to pathophysiological concentrations, these lipolysis products are harmful to human aortic endothelial cells (HAEC) and pathophysiological effects include rearrangement of

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junction proteins that lead to increased endothelial permeability, inflammation and apoptosis (14). Although HAEC and cerebrovascular cells are different, it is likely they can both be injured by lipolysis products. However, it is unknown if TGRL lipolysis products cause permeability changes of the BBB, even if transiently.

To test this hypothesis, we used MR contrast agent (MRCA)-assisted MRI as used extensively in assessing BBB injury after stroke both clinically and experimentally (15,16). MRCA-MRI has the advantage of achieving relatively high resolution and being relatively noninvasive, allowing a subject to be monitored over time. Here in this study, MRCA-MRI was used to measure the blood-to-brain influx coefficient K_i as a measure of BBB integrity in healthy Sprague-Dawley rats after injection of saline, LpL, or prelipolyzed human TGRL (final blood concentration of 150 mg/dL TGRL, hereafter designated 150TL).

METHODS

Preparation of Human Triglyceride-Rich Lipoprotein Lipolysis Products

As approved by the UC Davis Institutional Review Board, plasma samples were collected from healthy volunteers 3.5 h after consuming a high fat meal. TGRL from these plasma samples was isolated by ultracentrifugation at 40,000 rpm at 14°C for 18 h with a density gradient solution ($\rho = 1.0063$ g/mL), followed by dialysis against a 0.9% NaCl + 0.01% ethylenediaminetetraacetic acid solution overnight. Triglyceride content was assessed using an enzymatic assay kit (Sigma, St. Louis, MO). Before animal infusion, TGRL was concentrated with Amicon 3000 MWCO centrifugal filters (Millipore, Billerica, MA) before incubation for at least 30 min with LpL added at 2 U/mL per 150 mg/dL.

Animal Preparation

Twenty Sprague-Dawley rats (Charles River Laboratories, Wilmington, MA) weighing 180–250 g were studied as approved by the Animal Use and Care Committee at the University of California, Davis. Animals were anesthetized with sodium pentobarbital (60 mg/kg body weight, i.p) and surgical plane anesthesia maintained with a quarter dose (15 mg/kg body weight, i.p) every 30 to 45 min thereafter. Body temperature was maintained by an electric heating pad during surgery and a water heating pad (Gaymar Inc., Orchard Park, NY) during MRI as described previously (17). The left femoral vein was cannulated with PE-50 polyethylene tubing for infusion of saline, LpL or 150TL, and gadopentetate dimeglumine (Magnevist; Bayer Healthcare Pharmaceuticals, Wayne, NJ).

Blood Chemistry

Blood samples from a subset of animals were drawn from the venous cannula at the conclusion of MRI data acquisition and analyzed for electrolytes, pH, P_{CO2} , P_{O2} , hemoglobin, and hematocrit using the i-STAT device (Abbott Laboratories, Abbott Park, IL).

MRI Analysis of Brain Permeability Changes

MRI data were collected using a 7 Tesla (T) Bruker Biospec MRS/MRI system (Bruker Biospin MRI, Inc., Billerica, MA). Anesthetized rats were placed supine on a custom made Plexiglas stage. The stage and rat were then placed into a 72mm radio frequency probe inside the 7T magnet centering 2 mm rostral to the bregma [slice 44 in the Scalable Brain Atlas (18)]. A previously described rapid-acquisition refocused-echo (RARE) sequence was used to create T_1 maps (19). In brief, images were captured using a 64-mm field-ofview with a matrix of 128×128 pixels with a 2-mm thickness in 1.8 min. The imaging parameters were echo time (TE) = 10.26 ms; repetition time (TR) array = 168.4, 500.2, 927.1, 1525.9, 2538, and 7500 ms; and RARE factor = 16. After a baseline T_1 map was acquired, a 0.5 mL/kg bolus of Magnevist (250 µmol/kg) was injected i.v. over approximately 4 s. The time course of contrast created by each bolus was then followed to acquire a total of $10 T_1$ maps over a period of 18 min for each of 3 Magnevist injections. The regions of interest (ROIs) were two symmetrical ROIs, one from each hemisphere, chosen to maximize the number of pixels sampled while excluding pixels in the median eminence or outside the brain in the manner described by Nagaraja et al (20). A single pixel sampling the superior sagittal sinus (SSS) was selected to follow the change in $R_1 = 1/$ T₁ for the arterial input function of each Magnevist injection as previously described (19,21). Matlab (MathWorks, Natick, MA) was used to convert T₁ maps to R₁ maps and generate Patlak plots for each pixel to calculate the blood to brain transfer rate coefficient, K_i (min⁻¹), constrained using Ftests to select the best fit between impermeable, unidirectional influx and bi-directional flux models (21,22).

Statistical Analysis

Unless otherwise stated, data are reported as mean \pm SEM. Analysis of variance for repeated measures was used to test for differences between treatments using the criterion of P < 0.05. When differences between treatments were found, the Student-Newman-Keuls (SNK) posthoc test for multiple comparisons was used to determine which and when treatments were different.

RESULTS

Physiological Data

Venous blood samples from a subset of rats (n = 9) were analyzed and summarized in Table 1. Mean $P_{\rm CO_2}$ was 57.51 ± 5.23 mmHg and there were no significant differences between treatment groups. Mean $P_{\rm O_2}$ was 39.29 ± 3.66 mmHg. Because physiological venous $P_{\rm O_2}$ is near 40 mmHg and $P_{\rm CO_2}$ is between 40 and 50 mmHg, the rats were slightly hypoxic and hypercapnic.

K_i Was Significantly Increased in Rats Treated with TGRL Lipolysis Products

 K_i was calculated on a pixel-by-pixel basis and then averaged over two ROIs selected symmetrically about the midline from each hemisphere away from the median eminence and ventricles. Representative images of K_i for an animal injected with 150TL are shown in Figure 1. 1248

Table 1	
Physiologic	Data+

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Na (mmol/L) K (mmol/L)	$\begin{array}{c} 140.78 \pm 1.33 \\ 4.71 \pm 0.29 \end{array}$
TCO ₂ (mmol/L)	33.00 ± 1.66
Ca (mmol/L)	1.30 ± 0.05
Hematocrit (%PCV)	37.44 ± 0.60
Hemoglobin (g/DL)	12.74 ± 0.21
рН	7.35 ± 0.02
PCO ₂ (mmHg)	57.51 ± 5.23
PO ₂ (mmHg)	39.29 ± 3.66
HCO ₃ ⁻ (mmol/L)	31.14 ± 1.50

^aVenous blood samples from a subset of animals were analyzed using i-STAT (N = 9).

(Data were collected from rats lying supine but the images were inverted for illustration purposes.) Representative ROIs are highlighted by green border and the SSS used for the arterial input function is indicated by the white arrow. Mean K_i for each treatment group was plotted against time (Fig. 2) demonstrating K_i for 150TL increased 275% from baseline control. Analysis of variance (ANOVA) for repeated measures showed mean K_i for 150TL was significantly greater than LPL and saline when results for all three time points were included. The SNK posthoc analysis showed K_i for 150TL was significantly greater than for LpL alone for the 0- to 20-min interval but SNK showed no significant difference between treatments for the 20- to 40-min interval. Standard t-tests for the 0- to 20-min interval comparing 150TL with saline and LpL infusions gave P = 0.024 and 0.035, respectively. Finally, in an effort to quantify the number of leaky sites, for each animal we counted the number of pixels with K_i 2 SDs greater than the mean of its own control K_i. Consistent with findings described above, ANOVA for repeated measures showed there was an increased number of high K_i pixels in the 150TL group compared with both LpL alone as well as for saline. Standard ANOVA followed by SNK analysis showed the

significant difference between treatments occurred for the 0- to 20-min interval (Fig. 3). Although SNK analysis did not show significant differences between individual treatments at any particular time, standard t-tests comparing 150TL with saline and LpL infusions had *P*-values of 0.052 and 0.026, respectively for the 0- to 20-min interval and 0.081 and 0.043, respectively, for the 20- to 40-min interval.

DISCUSSION

The neurovascular unit remains a central focus of AD research. It is composed of such components as endothelial cells, basement membrane, astrocytes, pericytes, and neurons. The endothelial cells normally maintain a barrier to segregate blood-borne substances from the brain extracellular fluid, i.e., the BBB, while regulating the entry of endocrine factors, immune cells and cytokines, and the secretion of cytokines (23,24). BBB permeability can be increased by perturbations such as hypoxia, ischemia/reperfusion, inflammation, and brain tumors and assessing these changes is important for understanding the etiology of cerebrovascular diseases (25,26).

AD is one such disease in which BBB integrity seems to play an important role. In the AD mouse model Tg2576 BBB integrity was compromised as early as 4 months in some areas of the cerebral cortex (27). In humans, disturbances in the cerebral-spinal fluid albumin index (a measure of BBB integrity) are positively correlated with AD progression (28). Damage to the BBB in the hippocampus is also correlated with AD in the early stage (29). In an analogous system, loss of endothelial integrity in the systemic circulation is also correlated with atherosclerosis (30). In addition, risk factors for CVD also coincide with AD. These shared risk factors include hypertension, high LDL cholesterol, low HDL cholesterol, diabetes, and high triglycerides (3,5,31). However, evidence also exists for no overlap of these risk factors (4) and clinical trials lowering high plasma triglyceride with fibrate drugs have yielded mixed results (7,8).

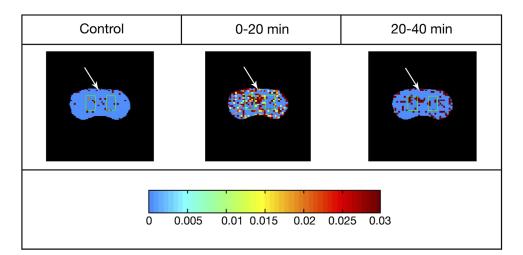


FIG. 1. Representative images of rat brain treated with 150TL at different time points. The color bar below the images shows changes in blood-brain barrier transfer coefficient K_i varying from 0 to 0.03 min⁻¹. Pixels with $K_i > 0.03$ min⁻¹ are assigned the same color as $K_i = 0.03$ min⁻¹. For each map, representative ROIs in each hemisphere are highlighted by green border and the white arrow points to the SSS. Rats were lying supine during data collection and images were inverted for illustration purposes. Please see text for further detail.

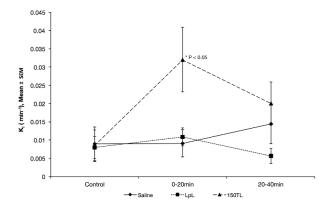


FIG. 2. Mean blood to brain transfer rate coefficients K_i are plotted against time. ROIs are selected from brain hemispheres and combined to calculate a mean for each animal. Then mean K_i for all animals in each treatment is plotted at three different time points representing the time for data acquisition (control, 0–20 min and 20–40 min). ANOVA for repeated measures showed a significant difference (P < 0.05) in K_i between animals infused with 150TL (n=8) and those infused with either saline (n=6) or with LpL alone (n=6). Posthoc analysis showed in particular that a difference between 150TL and LpL alone occurred at the 0–20 min time point (*P < 0.05).

Some of these mixed results could be due to the difference between triglyceride and triglyceride lipolysis products. Vascular lipoprotein lipase hydrolyzes TGRLs and releases neutral and oxidized free fatty acids. We previously demonstrated that these lipolysis products of TGRLs caused extensive rearrangement of junctional proteins such as ZO-1 and occludins in HAEC (14) and increased reactive oxygen species production (32). In contrast, un-hydrolyzed TGRL did not induce similar effects, suggesting that it is the released contents from TGRL hydrolysis and not the plasma concentration of triglyceride that is deleterious to the vasculature. There-

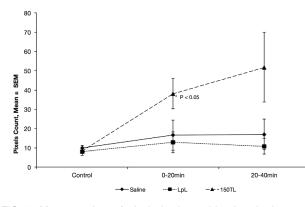


FIG. 3. Mean number of pixels having a blood to brain transfer coefficient K_i more than 2 SDs greater than the same animal's control plotted against each time point. Using the criteria outlined by Nagaraja et al (20), pixels are considered to be very leaky if the K_i is more than 2SDs greater than control. ANOVA for repeated measures shows animals infused with 150TL have more leaky pixels by this criterion compared with those infused with saline or LpL alone (P < 0.05). Standard ANOVA for multiple comparisons showed the effect of treatment was significant for the 0–20 min interval (*P < 0.05).

fore, prelipolyzed triglyceride was used to study the acute effect on the BBB in this study.

Our study here shows that after normal rats were fed regular chow, infusing human lipolysis products to obtain a blood level of 150 mg/dL TGRL transiently increased the blood-to-brain transfer coefficient (K_i) for Gd-DTPA (Fig. 2). That is, the time course of our experiment suggests K_i increased within 20 min after injecting 150TL and then fell toward baseline within 40 min afterward. This rise-and-fall trend, however, does not appear to be true for the mean number of pixels having K_i more than 2 SDs above control (Fig. 3). While the change is not statistically significant using the Student-Newman-Keuls test, the difference in the trends could be due to variability of the pixels sampled with the MRI. While the majority of pixels made low to moderately leaky by the 150TL infusion were no longer significantly different from those treated with saline or LpL after 40 min, t-test analysis suggests a trend showing the mean number of very leaky pixels (i.e., >2 SD greater than baseline) is greater 40 min after 150TL treatment than after LpL infusion. One interpretation of this result is that lower permeability sites recover while more leaky sites do not recover within the same time interval. This, however, remains speculative and requires further study.

Furthermore, the infusion of human TGRL lipolysis products is physiologically relevant despite the acute nature of the infusion. Even though blood TGRL in humans rises steadily from initial fat assimilation in the intestine to peak at 3 h after ingesting a particular meal (12), allometric considerations suggest this is accelerated in rats. In addition, it is well documented that LpL can be found within brain microvessels as well as brain and nervous system (13,33). Therefore incubating TGRL with lipoprotein lipase (LPL) before injection would likely accelerate the observed effects of TGRL lipolysis products. As a corollary, injecting TGRL without LpL incubation would likely just delay the onset of the permeability changes. Further studies will be required to test this assertion as well.

While our current study does not tell us the mechanism of the observed blood-to-brain transfer coefficient changes, it would likely involve the transforming growth factor-B/SMAD pathway as suggested by previous observations in HAEC with similar treatments (unpublished results). Nonetheless certain artifacts could be ruled out. First, the Patlak model for the blood-to-brain transfer rate coefficient K_i (as the product of capillary permeability and surface area per tissue volume) could depend on the flow rate, as Ewing et al estimated a perfusion rate less than 50 times K_i could create a flow-limited situation (21). The reason being that changes in blood flow could be associated with changes in surface area and/or measured permeability if contrast agent delivery is flow limited. Using an MRI sequence to generate perfusion weighted images from our samples, more than 90% of our dataset had a cerebral blood flow above this limit (data not shown).

Furthermore, to the extent that K_i measurements are flow-limited, this will underestimate K_i . Therefore the increases we measured in the 150TL group are a conservative estimate and any possible flow-limitation will not invalidate the conclusion that 150TL infusion increases the K_i. Second, even though the experimental animals were slightly hypoxic and hypercapnic, likely due to the use of Nembutal that is known to suppress ventilation without procedural intervention, studies have shown that only after 3 h of acute and severe hypercapnia ($PA_{CO_2} > 65$ mmHg), but not after continuous hypercapnia, was BBB function disturbed in rabbits (34). Mean P_{CO_2} in the experimental animals is well below this level of hypercapnia (Table 1) and no correlation between venous P_{CO_2} and K_i could be found (data not shown). Therefore, the observed changes in blood-tobrain transfer coefficient are not likely due to blood flow changes in the brain or hypoxia or hypercapnia.

While pinpointing the exact lipolysis product that caused the observed changes is beyond the scope of this study, there can be possible candidates. Apart from transporting lipid, TGRL can also transport amyloid-beta (A β). Chylomicrons, a class of TGRL produced in the intestine to facilitate triglyceride transport from dietary lipid, are carriers for A β (35,36). Elevated triglyceride also preceded $A\beta$ deposition in two AD mouse models (37). Takechi et al hypothesized the increased Aβchylomicron load that occurs during chronic high fat feeding might lead to more intestinally produced AB deposition in the brain (38). It is possible that TGRL lipolysis released this $A\beta$ fraction that injured the BBB and led to the study observations. Further studies will be needed to distinguish the effects, if any, between TGRL lipolysis products and AB in our model.

In conclusion, we have demonstrated in this study that RARE-MRI measurement of changes in T_1 following contrast agent infusion is a useful technique to monitor the changes of blood-brain barrier function in vivo following TGRL lipolysis product infusion and that under the conditions of this study, TGRL lipolysis products transiently increase the blood-to-brain transfer coefficient for Gd-DTPA. To our knowledge this is the first use of this technique to examine this phenomenon in vivo. This result provides important insight into the effects of lipids on BBB permeability and this technique could be a valuable tool for testing the efficacy of lipid-modulating drugs in maintaining BBB function.

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