

UC Santa Barbara

UC Santa Barbara Previously Published Works

Title

Spatio-temporal patterning of extensile active stresses in microtubule-based active fluids

Permalink

<https://escholarship.org/uc/item/9pg6k4f0>

Journal

PNAS Nexus, 2(5)

ISSN

2752-6542

Authors

Lemma, Linnea M

Varghese, Minu

Ross, Tyler D

et al.

Publication Date

2023-05-02

DOI

10.1093/pnasnexus/pgad130

Copyright Information

This work is made available under the terms of a Creative Commons Attribution License, available at <https://creativecommons.org/licenses/by/4.0/>

Peer reviewed

Spatio-temporal patterning of extensile active stresses in microtubule-based active fluids

Linnea M. Lemma^{a,b}, Minu Varghese^a, Tyler D. Ross^{b,c}, Matt Thomson^d, Aparna Baskaran^b and Zvonimir Dogic^{b,*}

^aDepartment of Physics, Brandeis University, 415 South St., Waltham, 02453 MA, USA

^bDepartment of Physics, University of California, Santa Barbara, 93106 CA, USA

^cDepartment of Computing and Mathematical Sciences, California Institute of Technology, 1200 E California Blvd. Pasadena, 91125 CA, USA

^dDivision of Biology and Biological Engineering, California Institute of Technology, 1200 E California Blvd., Pasadena, 91125 CA, USA

*To whom correspondence should be addressed: Email: zdogic@physics.ucsb.edu

Edited By: Petros Koumoutsakos

Abstract

Microtubule-based active fluids exhibit turbulent-like autonomous flows, which are driven by the molecular motor powered motion of filamentous constituents. Controlling active stresses in space and time is an essential prerequisite for controlling the intrinsically chaotic dynamics of extensile active fluids. We design single-headed kinesin molecular motors that exhibit optically enhanced clustering and thus enable precise and repeatable spatial and temporal control of extensile active stresses. Such motors enable rapid, reversible switching between flowing and quiescent states. In turn, spatio-temporal patterning of the active stress controls the evolution of the ubiquitous bend instability of extensile active fluids and determines its critical length dependence. Combining optically controlled clusters with conventional kinesin motors enables one-time switching from contractile to extensile active stresses. These results open a path towards real-time control of the autonomous flows generated by active fluids.

Keywords: active matter, molecular motors, fluid dynamics, optical control

Significance Statement

Being driven away from equilibrium by microscopic force-generating processes, the cellular cytoskeleton enables life-sustaining functions such as cytoplasmic streaming, cell motility, and cell division. Active fluids reconstituted from well-characterized biochemical components have the potential to replicate such lifelike phenomena in synthetic materials. However, in biological cells, mechanical functions are enabled by force generation that is under tight spatio-temporal control. In comparison, cytoskeletal active matter is fueled by microscopic activity that is generated uniformly throughout a sample. Controlling force-generating patterns is the key to building more complex materials and functions and mimicking biology. Motivated by these observations we develop and characterize optically responsive molecular motors that allow for robust and repeatable spatio-temporal patterning of active flows in microtubule-based active matter.

Introduction

The shapes of cells, tissues, and organs are determined by the patterns of the mesoscopic active stresses, which are collectively generated by molecular motors (1–6). Developing analogous synthetic force-generating materials is of fundamental interest and is essential for diverse applications (7), ranging from microfluidics and adaptive optics to soft robotics. Active matter, which is an assemblage of microscopic force-generating constituents, provides a promising experimental platform for realizing these goals (8). Bulk active materials exhibit diverse dynamical states (9–14), which can exhibit chaotic or turbulent-like flows. However, developing soft active matter systems is only the first step towards creating life-like synthetic materials; one also needs to harness their force-generating capabilities to stabilize a targeted dynamical state. In this vein, previous work demonstrated that immutable

geometrical confinement can stabilize spinning vortices or long-ranged coherent flows (15–18).

The next challenge is to develop protocols that control transitions between distinct dynamical states *in situ*. For inspiration, one can look towards biological cells, which can sense their environment and adjust force patterns accordingly (19). A first step for achieving analogous capabilities in synthetic materials is to develop active matter whose dynamics are responsive to external cues. Light patterns have been used to control motility induced phase separation and the structure and dynamics of bacteria (12, 13, 20–23). Recent advances also demonstrated optical control of cytoskeletal active matter, including the control of local contractility and aster formation, as well as influencing the motion of topological defects (24–26). Here we demonstrate robust and repeatable spatial and temporal control of active stresses in three-

Competing Interest: The authors declare no competing interest.

Received: September 11, 2022. **Revised:** February 27, 2023. **Accepted:** April 3, 2023

© The Author(s) 2023. Published by Oxford University Press on behalf of National Academy of Sciences. This is an Open Access article distributed under the terms of the Creative Commons Attribution License (<https://creativecommons.org/licenses/by/4.0/>), which permits unrestricted reuse, distribution, and reproduction in any medium, provided the original work is properly cited.

dimensional microtubule-based active fluid. To achieve precise control, we build upon opto-kinesin (24) to develop a new single-headed kinesin motor that exhibits optically induced enhanced clustering. The unique features of this system enable temporal control of the ubiquitous bend instability of active fluids, and reveal how this instability depends on the system size.

Optical control of kinesin clustering

Conventional microtubule-based active fluids are powered by clusters of kinesin-1 molecular motors (9). Motors within a single cluster bind adjacent microtubules. Depending on the microtubules' relative polarity, the motor clusters induce interfilament sliding and bundle extension (27). At high microtubule concentrations, extensile bundles form a percolating network that is continuously reconfigured by the repeating cycles of motor-driven bundles extending, buckling, fragmenting, and re-annealing (11). Such network dynamics drive the turbulent-like flows of the background fluid. Coupling energy-efficient kinesin motors with an ATP regeneration can sustain non-equilibrium dynamics for hours or even days (28).

Typically, microtubule-based active matter is powered by a 401 amino acid fragment of the *Drosophila* kinesin-1 motor (9, 11). For these motors, two fragments associate to form a dimeric kinesin motors, which we refer to as K401. These processive motors are continuously bound to a microtubule as they take consecutive steps (29, 30). K401 motors are labeled with a biotin. Adding streptavidin induces the irreversible assembly of higher order clusters containing several K401 motors, which efficiently power active matter dynamics.

Microtubule-based active matter can also be powered by a monomeric 365 amino-acid fragment of *Drosophila* kinesin-1 motor, which we refer to as K365 (28, 31). Having a shorter neck linker domain, such fragments do not dimerize. K365 motors are not processive; they detach from a microtubule after each step (32, 33). Similar to K401, K365 kinesin motors are labeled with biotin and can assemble into higher order streptavidin clusters. Notably, the K365 motor clusters can bind multiple filaments and induce their relative sliding, generating active stresses. The dynamics of an active fluid driven by clusters of K365 motors exhibit greater temporal stability of flow speeds and structural length scales, when compared to those driven by K401 motors (28). Clustering can transform non-processive motors into processive ones (34).

Multimotor clusters are essential for generating active stresses. Isolated motors move along separate filaments, but are unable to generate interfilament sliding. The biotin-streptavidin interaction used to assemble conventional clusters is an essentially irreversible non-covalent bond (35). Decreasing intra-cluster bond strength, decreased the efficiency of interfilament sliding, as was revealed by DNA-based clusters, in which the binding strength can be precisely tuned (31). Below a minimal bond strength, the clusters were unable to generate active stresses.

Such considerations suggest that controlling cluster assembly provides a route towards control of active stresses. Indeed, a recent advance fused optically responsive dimerizing domains (improved light-induced dimers, iLID) to kinesin motors to establish reversible light control of the assembly of the kinesin clusters (24, 36). In the absence of photoactivation, the binding affinity of the kinesin-iLID to its polypeptide binding partner, which is attached to another kinesin motor, is low: thus the kinesin motors are largely isolated. They consume ATP and walk along microtubules, but do not induce significant interfilament sliding [Fig. 1A and B]. When photoactivated, the iLID domain changes

conformation, exposing the binding site and increasing the affinity for motor pairs to dimerize. The newly formed motor clusters can cross-link and slide microtubules [Fig. 1A and B]. Such opto-kinesin clusters can induce photoactivated contraction of microtubule asters and generate programmable fluid flows (24).

Results

Steady-state dynamics of active fluids powered by opto-kinesin clusters

We first explored the ability of K401-opto clusters to control dynamics of microtubule-based extensile fluids [Fig. 1A]. In the presence of blue light, opto-clusters generated extending bundles that continuously buckled and annealed [Video 1, Supplementary Material: Materials and Methods]. Images taken 30 s apart revealed a continuously reconfiguring microtubule network [Fig. 1C, bottom]. Upon deactivation, the microtubule bundles quickly stopped extending and remained frozen in their paused configuration. Images taken 10 min apart demonstrate the lack of measurable dynamics in the absence of optical signal [Fig. 1C, top]. When exposed to continuous blue light, the photoactivated flows decayed rapidly, perhaps due to irreversible cross-linking of motors clusters. Pulsed 10 ms photoactivation every 5 s avoided this issue. Additionally, we optimized the motor concentration to achieve maximal difference between the dark and photoactivated state [Supplementary Material: Materials and Methods].

We measured the speed of the microtubule-powered flows through multiple cycles of photo-activation, using particle image velocimetry (PIV) of the fluorescent microtubule images (37) [Fig. 1D, Fig. S1, Materials and Methods]. After formation of the bundled network, the sample was alternately exposed to dark and light cycles each lasting 15 min and 1 h, respectively. When illuminated active flows increased 100-fold from ~ 20 nm/s in the dark to $\sim 2 \mu\text{m/s}$ in the light. The difference in speeds persisted over several light cycles that spanned the active network lifetime.

Quantifying the flow speeds, however, revealed subtle variations of photoactivated dynamics over time. First, within a single cycle, the maximum speed was reached within 30 s after photoactivation and then decayed to a plateau. The decay timescale increased with subsequent photo-activation cycles. Second, the plateau speed decreased with each successive photo-activation cycle. Such decay is reminiscent of aging observed in active fluids driven by the conventional K401 motor clusters (28). Finally, the background speed in the dark state increased throughout the sample lifetime [Fig. 1D inset]. The combination of increased dark flows and decreased photoactivated flows reduced the contrast between the dark and the illuminated states [Fig. S2]. These behaviors present a challenge for applications that require repeatable control of the active stress.

Motivated by the observation that K365 kinesin clusters generate more regular temporal dynamics (28), we created clusters which fused a monomeric kinesin fragment (K365) to both iLID domains [Fig. 1B, Fig. S3]. The K365 opto-clusters also powered the extensile dynamics upon photo-activation [Video 2]. After formation of the bundled network, the active fluid was exposed to repeating cycles of photo-activation. In contrast to the K401-opto motors, the K365-opto constructs exhibited a regular, reversible, and reproducible response. Photoactivated flows immediately plateaued, at $1.2 \mu\text{m/s}$, while dark state flows were ~ 7 nm/s. Subsequent photo-activation cycles generated the same speed, with no significant change over the sample lifetime. Finally, the dark state flow speeds did not increase over time, and were

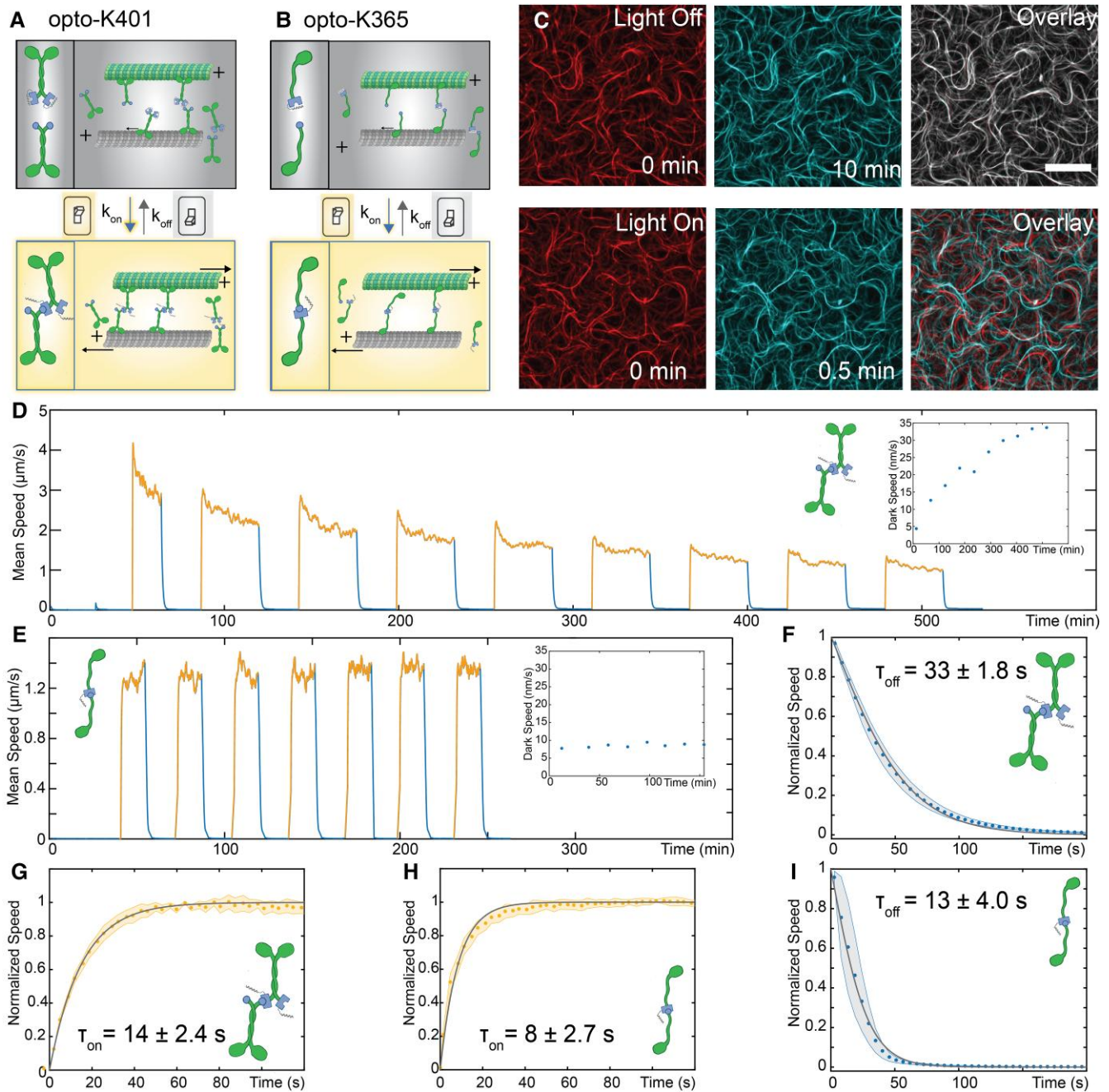


Fig. 1. Optical switching between an active extensile fluid and an inactive solid. A) The iLID optogenetic domains are fused to processive kinesin motors. When the protein is illuminated with blue light, the iLID domain changes conformation and the complementary constructs bind to each other. The clustered motors generate interfilament sliding. B) The iLID domains are fused to a K365 truncated kinesin motor. The K365 motor clusters also dimerize and induce interfilament sliding when exposed to blue light. Schematics of microtubules and kinesin motors were made using [BioRender.com](#). C) An active network of labeled microtubules powered by optogenetic kinesin clusters, K365-opto. Overlaid initial (red) and final frame (cyan) show the network dynamics (red + cyan = gray), top: In the dark, the microtubule bundles do not move. bottom: When exposed to blue light, the bundles extend and buckle generating active flows. K401-opto driven dynamics are qualitatively the same ([Video 1](#)). Scale bar, 25 μm . D) Speed of active flows generated by processive opto-kinesin clusters. Activation is cycled off (blue) and on (gold). In the on-state, the light is pulsed for 10 ms every 5 s. Inset: the average network speed in the dark state with subsequent photo-activation cycles. E) Active flow speeds with K365 opto-kinesin. Inset: dark speed over time. F) The decay of the flow speed upon turning the light off for processive motors. The shaded region is the standard deviation ($n = 9$). The line is a fit to Eq. 2. G) For processive motors, the increase in speed upon photoactivation. The line is a fit to Eq. 1. H) The increase in speed after photoactivation for K365 ($n = 7$). I) The decay in the flow speed after deactivation for K365 motors.

effectively zero when compared to enzymatically dead samples [Fig. 1E inset, Fig. S4]. Thus, K365 opto-kinesin clusters allow for robust and repeatable spatio-temporal control of active stresses.

The steady-state dynamics of extensile fluids is uniquely suited to characterize the temporal response of clusters to optical stimulus, which is related to the kinetics of the kinesin cluster assembly and disassembly. We measured the timescale for which the flows

reached their maximum speed after photo-activation. For both K401-opto and K365-opto motor clusters, the increase in speed was fitted to a bounded exponential function

$$\langle |v(t)| \rangle / v_{\max} = 1 - e^{-t/\tau_{\text{on}}}. \quad (1)$$

For K401 clusters, $\tau_{\text{on}} = 14 \pm 2.4$ s and for K365 clusters $\tau_{\text{on}} = 8 \pm 2.7$ s [Fig. 1G and H]. Similarly, we measured the time

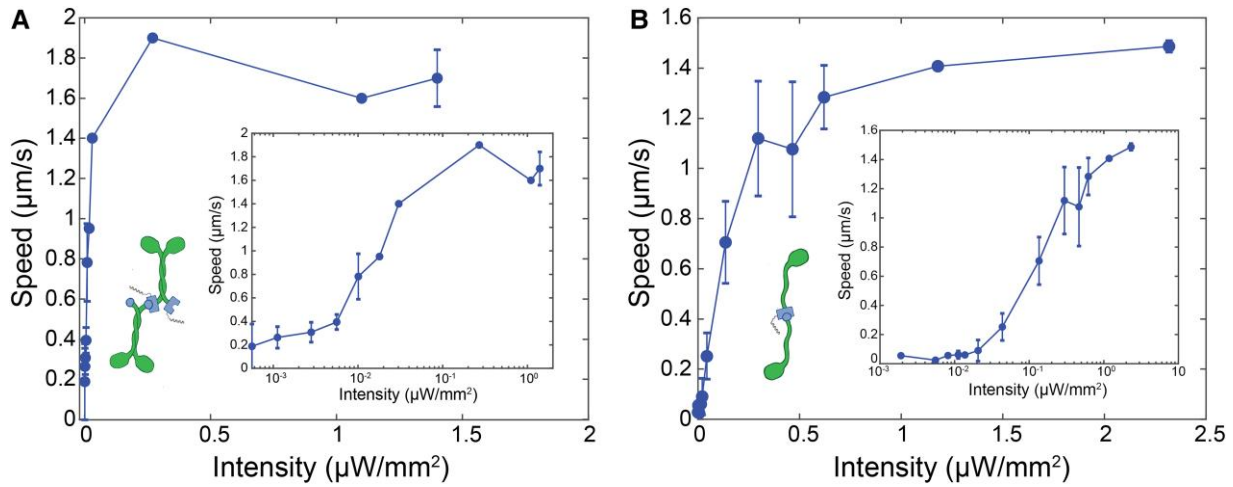


Fig. 2. Signal intensity controls speed of active flows. A) Autonomous flow speed as a function of the light intensity for processive motors ($n = 2, 2, 2, 2, 2, 1, 1, 1, 3$ Intensity = $0 \rightarrow 2 \mu\text{W}/\text{mm}^2$). B) Speed of autonomous flows measured through PIV versus the light intensity for K365 motors ($n = 3, 2, 4, 3, 1, 2, 3, 4, 2, 3, 2, 2$, Intensity = $0 \rightarrow 2.5 \mu\text{W}/\text{mm}^2$). Insets: Log-log scaling of axes. Error bars represent standard error on multiple samples' flows.

scales for the flows to cease after deactivation. We fitted the velocity decays to a logistic function:

$$\langle |v(t)| \rangle = \frac{2}{1 + e^{-t/\tau_{\text{off}}}}, \quad (2)$$

from which we extracted $\tau_{\text{off}} = 33 \pm 1.8$ s for K401 clusters and $\tau_{\text{off}} = 13 \pm 4.0$ s for K365 clusters [Fig. 1F and I]. The relative time-scales of the two motors were independent of the functional forms of Eqs. 1 and 2.

Controlling the speed of extensile flows

We next aimed to control the speed of active flows. Absorbance assays of AsLOV proteins, the native protein from which iLID was derived, indicated that the light intensity controls the fraction of dimerized domains (38). Thus, we expect that the light intensity also controls the concentration of bound motor clusters, which in turn controls the magnitude of the active stress and the flow speeds. We measured the dependence of the autonomous flow speeds on the intensity of 488 nm illuminating light at the sample plane [Fig. 2, Supplementary Material: Experimental Methods]. With increasing light intensity, the flow speed increased until $0.4 \mu\text{W}/\text{mm}^2$ for K401-opto [Fig. 2A, Fig. S5]. The K365-opto motors exhibited increasing flow speeds with increasing light intensity until saturating at $1 \mu\text{W}/\text{mm}^2$ [Fig. 2B]. Below $0.01 \mu\text{W}/\text{mm}^2$, the measured flows asymptotically approached the dark state [Fig. 2A and B inset]. The K401-opto clusters achieved a higher saturating speed, at a lower light intensity than the K365-opto clusters. Additionally, K401-opto motor clusters exhibit a speed of $\sim 0.2 \mu\text{m}/\text{s}$ as intensity approaches zero, indicating non-specific binding of motors. In contrast, the speed driven by K365-opto motor clusters approaches zero as intensity approached zero.

Controlling the extensile bend instability

To demonstrate temporal control of active stresses, we used K365 opto-clusters to probe the bend instability of shear-aligned microtubules, which is a ubiquitous feature of extensile active fluids (39–42). Once aligned due to shear flow, microtubules remained quiescent in the absence of light [Fig. 3A]. When exposed to blue light, the opto-kinesin clusters generated extensile sliding, which in turn powered the growth of the bend instability. Upon deactivation, the bend instability stopped [Fig. 3A, Video 3]. The individual

microtubule bundles within the deactivated network straightened slightly, but the material only partially relaxed towards its initial uniformly aligned state. Similar deformation dynamics occurred over multiple cycles of photo-activation, with motor clusters pushing the microtubules into an active bend, and the network partially relaxing when deactivated.

To quantify the bend instability, we measured the average in-plane filament angle (θ) away from the initial alignment, by calculating the local structure tensor from fluorescence images [Fig. 3B, Fig. S6]. In this analysis, we treat the system as quasi-2D since the bend instability was predominantly in-plane. During the photo-activation, the average angle (θ) grew as the bend instability developed. Upon deactivation, the average angle decayed, but after several minutes attained a finite-value plateau. Such dynamics are seen by overlaying the initial and final images upon photo-activation [Fig. 3C].

The decay in the average angle upon deactivation was described by:

$$\langle \theta(t) \rangle = M(t)A(t) + R(t). \quad (3)$$

Here, $M(t)$ describes the unbinding kinetics of the motor clusters, $A(t)$ describes the activity-driven angle growth and $R(t)$ describes the relaxation of the passive microtubule network. The activity drives linear growth such that $A(t) = \dot{\gamma}t$, where $\dot{\gamma} = 0.002$ rad/s is the measured angular growth rate [Fig. S7]. Upon deactivation, growth slowed due to unbinding of opto-clusters. To account for this effect, we multiply the growth rate by the rate at which the clusters fall apart. Studies of unbinding kinetics of the light activated domain revealed exponential decay, $M(t) = e^{-t/\tau}$ where $\tau = 24$ s [Fig. S8, Supplementary Material: Elastic Relaxation] (43). Modeling the microtubule network as an elastic solid, predicts $R(t) = e^{-t/r}$ where r is the elastic relaxation time. Thus:

$$\langle \theta \rangle = e^{-t/\tau} \dot{\gamma}t + Ce^{-t/r} \quad (4)$$

where τ is the characteristic unbinding time for the motors and C is a scaling fit parameter. To fit the data, we fixed $\dot{\gamma} = 0.002$ rad/s, and left the time scales τ and r as free parameters [Fig. 4B inset, Fig. S9]. Experimental fits yielded $\tau = 17 \pm 5.5$ s which is within error of the previously reported unbinding kinetics of the iLID domain (43). We also extracted, the elastic relaxation time $r = 17 \pm 9.8$ s.

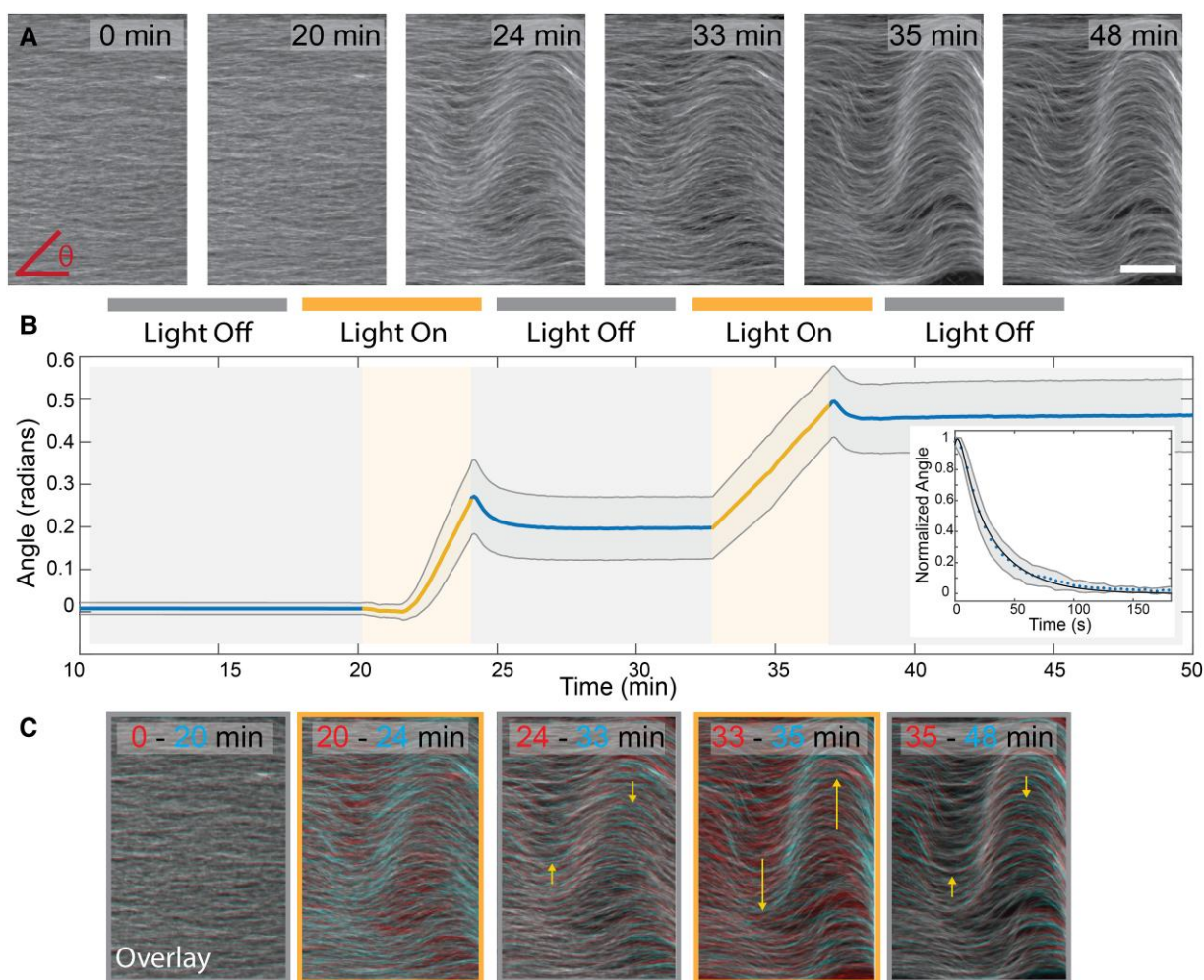


Fig. 3. Controlling the bend instability. A) Time series of a flow aligned opto-kinesin microtubule network exposed to alternating dark and light conditions. Scale bar, 200 μm . B) The time-evolution of the average in-plane angle of deformation for two photo-activation cycles. Inset: The average in-plane angle as a function of time elapsed after deactivation. The shaded region is standard deviation ($n = 5$). C) Overlays of time points in (a) with early time in red shows relative microtubule movement across each light cycle. Yellow arrows direct the eye forward in time.

Spatial patterning of active stresses

Theory predicts that the bend instability only develops when the sample size is larger than a critical length scale, which in turn is determined by the ratio of the sample elasticity to the activity (39, 44). Opto-kinesin clusters enable application of spatially patterned stress, which can elucidate how the interplay between geometry and activity controls the onset of the bend instability.

Shear flow associated with chamber loading induced initial alignment of microtubule bundles. When uniformly illuminated, such samples exhibited the previously described bend instability [Fig. 3] (42). We used a laser scanning confocal microscope to photoactivate square regions ranging in size from $50 \times 50 \mu\text{m}^2$ to $500 \times 500 \mu\text{m}^2$. At a single photoactivation intensity, the $500 \times 500 \mu\text{m}^2$ region exhibited the bend instability, while the smaller regions remained quiescent, demonstrating a size-dependent instability [Fig. 4A to C, Video 4].

To quantify the size-dependent instability, we systematically changed the photoactivation intensity within a single region. We placed an opaque mask above the sample with a $400 \times 400 \mu\text{m}^2$ square opening. Exposing such samples to light photoactivated the exposed area, while leaving the rest of the sample inactive. With sequentially increasing light intensity, we observed three

regimes [Video 5]. At very low intensities, the microtubules inside the activated region remained stationary [Fig. 4D]. Beyond a threshold intensity, the microtubules started sliding past each other along the alignment direction, but there was no deformation in the perpendicular direction [Fig. 4E]. Finally, at high intensities, the microtubules buckled in the direction perpendicular to alignment [Fig. 4F]. We refer to these as the quiescent, sliding, and buckling regimes.

To quantify these observations, we measured the microtubule displacement field after the region was photoactivated for a defined time [Fig. S10]. The direction of the initial alignment was the x-axis, while y-axis was the perpendicular direction in the image plane. In-plane deformations dominated the instability at these confinements, as long as the microtubules were initially well aligned. Thus, for the purposes of this analysis, we neglected the out of plane component. We calculated the build up of strain over time by averaging γ_{xx} and γ_{yy} over the photoactivated area [Fig. 4G to H]. In the quiescent regime γ_{xx} remained zero, indicating lack of any measurable motor-driven dynamics. Interestingly, γ_{yy} decreased over time [Fig. 4H]. This can be attributed to the depletion-induced contraction (45). Indeed, never photoactivated flow-aligned samples exhibited slight contractions, pulling

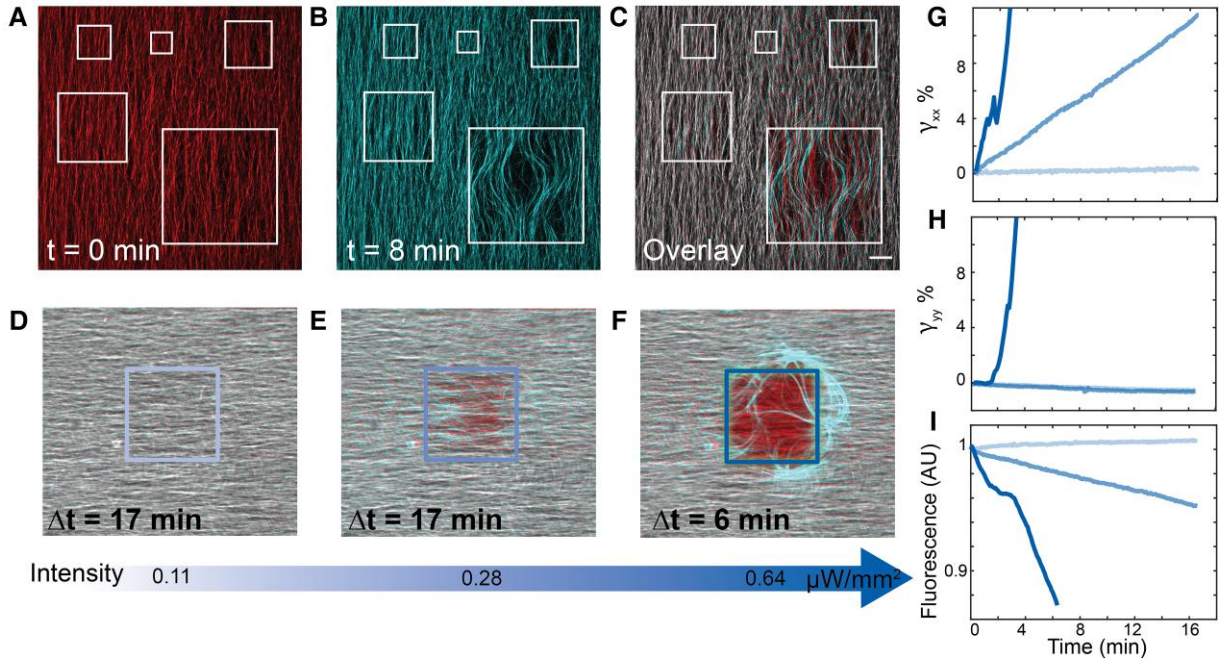


Fig. 4. Instability of confined active fluid. A) White squares indicate activation regions from $50 \mu\text{m}^2$ to $500 \mu\text{m}^2$ of aligned microtubules. B) Microtubule network after 8 min of constant photoactivation within the confined regions. C) The overlay of the initial and final images. D–F) The dynamics of the quiescent, sliding and buckling regime is illustrated by overlaying of initial (red) and final (cyan) state of a flow aligned network. $400 \times 400 \mu\text{m}$ square region was activated. Gray indicates no movement of filaments (red + cyan = gray). G) γ_{xx} within the activated region over time for each activation intensity. H) γ_{yy} within the activated region over time for the three regimes. I) The average fluorescence intensity inside the activated region over time for the three regimes.

toward the chamber center [Fig. S11]. In the sliding regime, γ_{xx} increased linearly with time, indicating a constant extension rate. Concurrently, γ_{yy} decreased to the same extent as the quiescent regime, indicating lack of motor-driven transverse dynamics. In the buckling regime, γ_{xx} grew quickly, increasing by more than 100% in 5 min. Simultaneously, γ_{yy} became positive and grew rapidly, indicating filament motion perpendicular to the direction of extension.

We estimated the material flux through the boundary of the photoactivated region, by measuring the change in the average fluorescent intensity of labeled microtubules within the exposed region [Fig. 4I]. Similar to the strain analysis results, the fluorescent intensity in the quiescent regime showed a slight increase of material over time due to the depletion-induced contraction. In the sliding regime, the intensity decreased linearly as microtubules extended out of the photoactivated region along the x -axis. In the buckling regime, the intensity decreased rapidly as the bend instability pushed the microtubules out of the photo-activation region. When expelled in the background, microtubules became stationary and did not return to the exposed region. Thus, with continued illumination, the photo activated region eventually became devoid of microtubules [Video 6].

The combination of the width W and the height H of the microfluidic channel determines the length scale of the bend instability (42). We illuminated aligned samples with rectangular patterns, with length L along the alignment direction and width W perpendicular to the alignment [Fig. 5A]. We systematically increased the light intensity to find the threshold activity required for the bend instability. The signature of bending is the growth of γ_{yy} . We defined a threshold intensity for the bend instability to be when the strain γ_{yy} exceeded 0.5% over a 17 min activation [Fig. 5B, Fig. S12]. The intensity of light required to generate buckling in this time depended on the size of the illuminated region. For

example, the intensity required to generate buckling of $L \sim 100 \mu\text{m}$ region was three times larger than for $L \sim 500 \mu\text{m}$ squares [Fig. 5C].

The threshold intensity for buckling exhibits a $1/L^2 + C$ dependence on confinement length scale, where C is a fixed constant [Fig. 5C, Fig. S13]. The hydrodynamic theory predicts that the instability is controlled by a dimensionless activity parameter $\alpha_{\text{eff}} = (\alpha(S_0 + \zeta))/(2\eta D_R \kappa)$, where, S_0 is the magnitude of initial order, ζ is the flow alignment parameter, D_R is the rotational diffusion, κ is the elastic constant, η is the viscosity of the active fluid [Supplementary Material: Hydrodynamic Model]. The instability occurs when α_{eff} is equal to a geometrical constraint such that:

$$\alpha_{\text{eff}} = \begin{cases} \pi^2 L^2 \left(\frac{1}{L^2} + \frac{1}{W^2} + \frac{1}{H^2} \right)^2, & \frac{1}{L^2} > \frac{1}{H^2} + \frac{1}{W^2} \\ 4\pi^2 \left(\frac{1}{W^2} + \frac{1}{H^2} \right), & \frac{1}{L^2} < \frac{1}{H^2} + \frac{1}{W^2} \end{cases} \quad (5)$$

Here, L , W , and H are the dimensions of the activated region [Fig. 5A].

If we assume that the active stress is linearly proportional to the intensity of the optical signal, $I = a\alpha_{\text{eff}}$, where a is a fit parameter, the hydrodynamic model captures the $1/L^2 + C$ scaling of the experimental data [Fig. 5C]. The theory further predicts that if the confinement perpendicular to the direction of alignment is held constant $W = 400 \mu\text{m}$ while the length L of the illuminated region varies, the threshold intensity will saturate when $1/L^2 = 1/W^2 + 1/H^2$ to an effective activity $4\pi^2(1/W^2 + 1/H^2)$. Theoretical predictions agree with the experiments, where $a = 1.17 \pm 0.1 \text{ nW}^{-1}$ and $a = 0.93 \pm 0.06 \text{ nW}^{-1}$ for the respective fits [Eq. 5, Fig. 5C and D].

Switching active stress from contracting to extensile

So far, we demonstrated quantitative control of the extensile active stresses in space and time. In comparison, biological cells

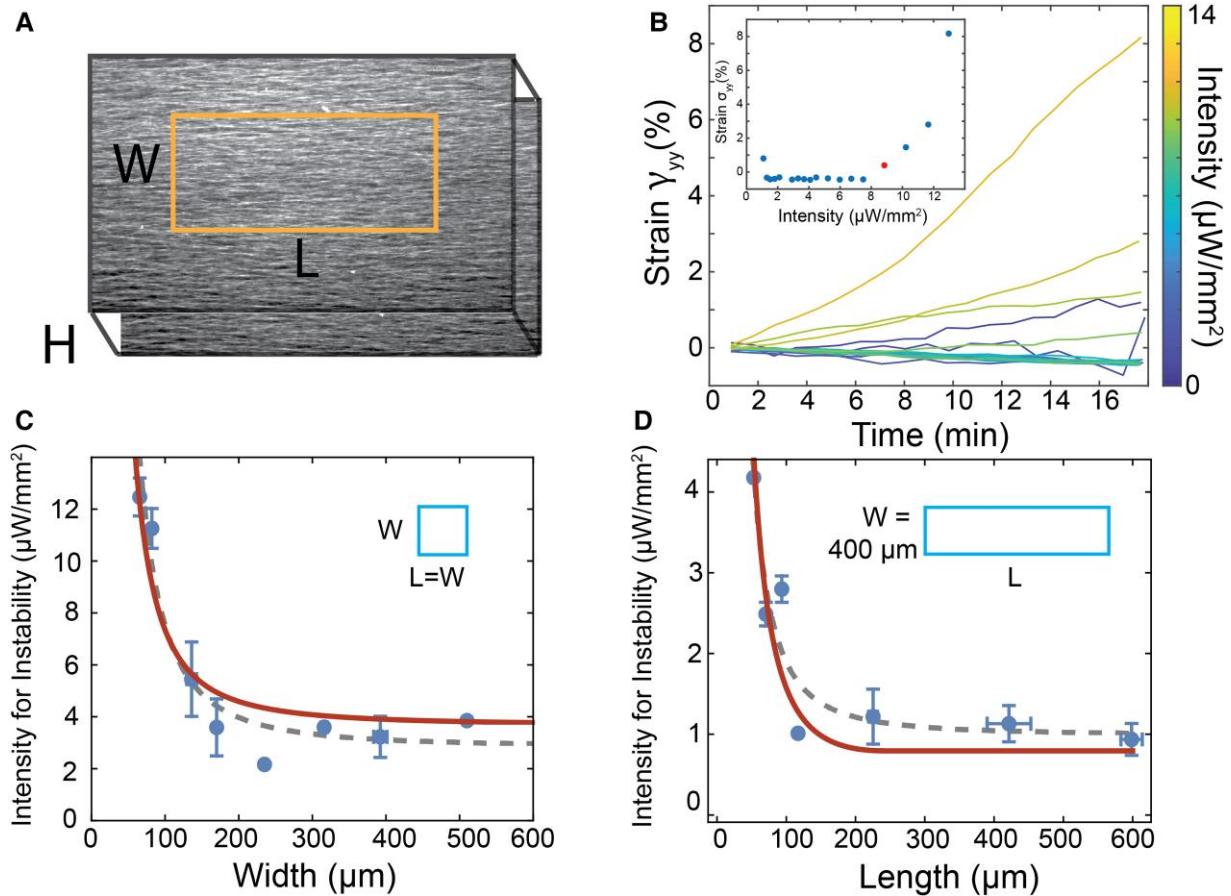


Fig. 5. Length scale of the bend instability. A) A rectangular region (length L and width W) of flow-aligned microtubules is activated. The system confinement is three-dimensional, with the height H defined as the height of the chamber. B) γ_{yy} plotted over time with increasing intensity (color). Inset: the strain after 17 min of photoactivation versus intensity. The bend instability is defined at the lowest intensity for which γ_{yy} increases by more than 0.5% over 17 min, indicated by the red dot. C) The threshold intensity for instability plotted versus the $L = W$ of a square activated region in a chamber $H = 100 \mu\text{m}$. Gray dashed line is fit to generic scaling of $1/L^2 + C$. The solid red line is fit to theory Eq. 5 with $a = 1.17 \pm 0.1 \text{ nW}^{-1}$. Error bars indicate standard error on multiple activated areas ($n = 2, 2, 4, 3, 1, 2, 3, 1$ from $W = 50 \rightarrow 500 \mu\text{m}$). D) The threshold intensity for instability for $W = 400 \mu\text{m}$ plotted versus the length L of the activated region in a chamber $H = 300 \mu\text{m}$. Error bars indicate standard error on multiple activated areas ($n = 1, 2, 2, 1, 3, 2, 3$ from $L = 50 \rightarrow 600 \mu\text{m}$). Gray dashed line is fit to generic scaling of $1/L^2 + C$. Solid red line is fit to theory Eq. 5 with $a = 0.93 \pm 0.06 \text{ nW}^{-1}$.

are able to control not only the magnitude but also the sign of the active stress to perform complex functions. Although both contraction and extension have been observed in a wide variety of cytoskeletal active matter systems (46–48), an on-demand switch between these two regimes has yet to be realized. Motivated by such reasoning, we explored the dynamics of a multi-motor material composed of K365 opto-kinesin clusters and full length kinesin-14. The latter is a minus-end directed molecular dimer motor with a passive microtubule-binding domain, a long neck linker, and a motor domain that steps processively at $\sim 20 \text{ nm/s}$, more than an order of magnitude slower than kinesin-1 [Fig. 6A] (49, 50). Thus, kinesin-14 can simultaneously passively bind one microtubule and advance towards the minus end of another microtubule, inducing their relative microtubule sliding (51). Kinesin-14 powers interfilament sliding in aligned microtubule networks that is independent of the local filament polarity (52).

In the presence of a depletion agent, kinesin-14 alone contracted a microtubule network [Supplementary Material: Materials and Methods]. The active contraction led to the formation of a single macroscopic bundle aligned with the chamber walls, which continued contracting isotropically for tens of hours, pulling from the edges of the chamber along and perpendicular to the direction of alignment. [Fig. 6B, Video 7]. Next, we combined

the kinesin-14 contracting network with K365 opto-kinesin [Fig. 6C]. When left in the dark, the material still formed a contracting network, as it would without the opto-kinesin [Fig. 6D]. However, upon illumination, the opto-kinesin clusters generated their own active stresses [Fig. 6E, Video 8]. The system exhibited extension and buckling in the photoactivated region which suggested extensile active stresses. The extensile behavior was localized to the activated region, thus the system simultaneously exhibited spatially distinct regions of extensile and contractile active stress [Fig. 6F]. On-demand transition from contractile to extensile stresses opens the door for new fundamental studies related to the sign of active stress, as well as engineering applications. However, the transition was not reversible, highlighting that the microscopic mechanism requires further study.

Discussion

We developed and characterized optically responsive kinesin clusters of non-processive K365 motors, showing that they are optimized for controlling extensile active stresses. These motors add to a growing toolbox of optical control of active dynamics (22, 24, 25). The K365-opto clusters induced up to a 200-fold increase in the speed of autonomous flows between a dark and a fully

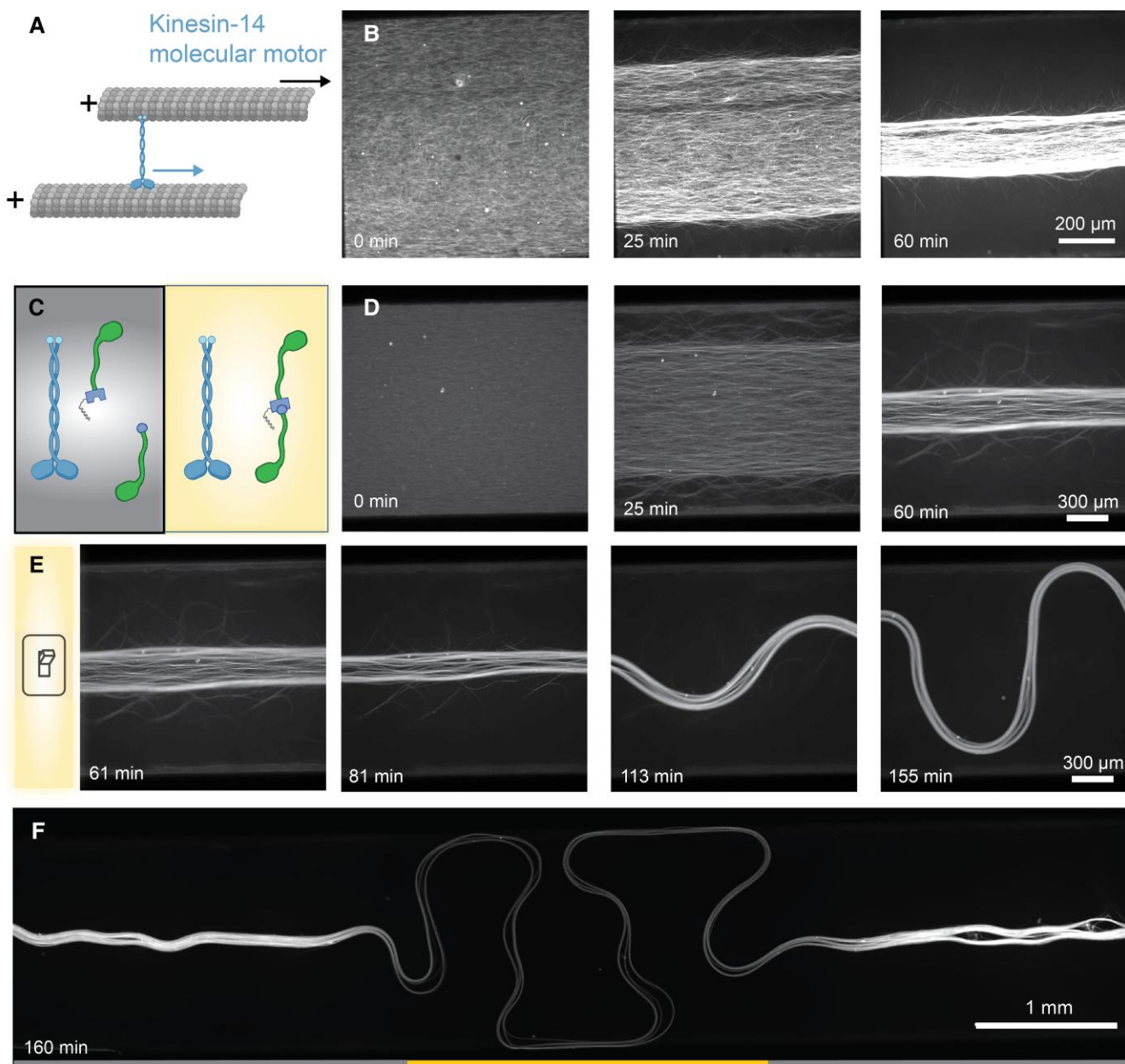


Fig. 6. Optogenetic switch from contractile to extensile active stress. A) Kinesin-14 motor has a passive microtubule binding domain and a motor domain that steps toward the microtubule minus end (blue arrow). The kinesin drives interfilament sliding (black arrow). B) A time series of the kinesin-14-driven microtubule contractile dynamics of an aligned microtubule gel. C) Microtubule-based active matter powered by kinesin-14 and K365 opto-kinesin clusters. In the dark state, kinesin-14 dominates system dynamics, generating contraction. In the illuminated state, opto-kinesin clusters generate competing extensile stresses. D) A two motor-network with deactivated opto-kinesin clusters contracts. E) The contracting network is locally photoactivated with $10 \mu\text{W}/\text{mm}^2$ at 61 min, and the opto-kinesin induce extension. A time series shows the transition to extensile, buckling behavior. F) Entire sample after photo-activation at $t = 156$ min. The yellow region has been illuminated. Outside this region, opto-kinesin remain deactivated.

illuminated state. Importantly, gels powered with K365-opto clusters displayed greater temporal regularity when compared to K401-opto clusters, a finding that parallels the analogous observation of conventional streptavidin-bound clusters (28). In comparison, the K401 opto-motors drove extensile active fluids for longer times and exhibited faster flows. These results have wide implications both within the field of active matter, and beyond.

Kinesin clusters can both generate active stresses and passively cross-link microtubule bundles (53–55). With decreasing ATP concentration, the motors' primary role switches from generating active stresses to cross-linking filaments (53). Consequently, ATP controls a transition between a quiescent elastic solid and a spontaneously

flowing active fluid. Opto-kinesin clusters provide a dynamical switch between an active fluid and a quiescent elastic network. In the dark state, the K365 opto-kinesin have a reduced tendency to dimerize. Thus, one might expect the microtubule network in the dark state to remain fluid-like. However, we found that upon deactivation, the network froze, and the bundles retained their structure. Upon re-activation, the flows were well correlated with the flow field measured just before deactivation [Fig. S14]. This behavior demonstrates, that even in the absence of motor clusters, a microtubule network is an elastic solid that is held together by PEG-induced depletion.

The properties of opto-kinesin provide insight into the bend instability, which is a ubiquitous feature of extensile fluids

(39, 41, 42, 40). In conventional systems, a uniformly aligned state is unstable to spontaneously growing bend deformation that increase in time, eventually generating turbulent-like dynamics. Opto-kinesin clusters enable one to pause the bend generation. Once deactivated, the deformed network only partially relaxed, wherein the microtubule bundles locally straightened as if released from tension. In comparison, a deformed conventional liquid crystal, relaxes to a uniformly aligned state. The partial relaxation again demonstrates that microtubule-based fluids have complex viscoelastic and plastic properties, that remain unexplored.

Changing the photoactivation intensity of spatially illuminated shear-aligned sample, revealed a size-dependent lower critical illumination intensity, below which the bend instability was not observed. This is in agreement with theory, which predicts a suppression of the bend instability for active nematics that are confined below a critical length scale (39, 44). In comparison, the size-dependent suppression of the instability was not experimentally observed for shear aligned microtubule fluids confined in microfluidic channels (42). The notable difference between the two systems is the nature of the boundaries. Microfluidic channels aligned the filaments, but compressible isotropic active fluids could easily separate from the wall, leaving behind regions devoid of active material. In comparison, partially illuminated aligned gels remained physically connected to the background elastic network. When a confined region was activated below the instability threshold for long times, the region did eventually buckle [Video 9]. However, in this regime microtubules slid against each other, leading to net outflux of the material, suggesting that the material properties of the network changed, before the onset of the instability.

Light intensity controls the speed of the active flows. Two observations suggest a complex relationship between measured flow speeds and activity that warrants further studies. The active fluids exhibited a hysteresis in speeds [Fig. S15 A]. Increasing photoactivation intensity from low intensities increased the speed of the fluid flows. However, after saturating the system and returning to low intensities, the fluid speed was five times higher than the original photoactivation at the same intensity. In between photoactivation events, the dark speed remained constant and near zero, indicating that the motors returned to their low affinity dark state and exhibited no irreversible binding. There was a noticeable change in the gel structure between the early and late low-light activation [Fig. S15 B]. These data suggest that the network properties, rather than the motors contribute to the hysteresis. Furthermore, we also observed that the intensity for the speed saturation of the bulk fluid flow was lower than the intensities which induced sliding and buckling in the confined system. We attribute this to the hydrodynamic constraints of the system in which the activity (or intensity) required for saturation is inversely proportional to the confinement.

Our results have implications beyond the field of active matter. In one direction, control of extensile active stresses provide a foundation for experimentally steering turbulent dynamics towards a targeted dynamical state (56). These foundations also extend to attempts to control droplet motility in active liquid-liquid phase separation systems (57). In a different direction, in the absence of ATP, kinesin motors can bind to the microtubules, acting as photo-inducible cross-linkers that can be patterned in space and time to control the structure and mechanical properties of elastic fibrous networks (58).

Acknowledgments

We acknowledge useful discussions with Seth Fraden. We thank Claire E. Walczak and Stephanie C. Ems-McClung for the gift of

kinesin-14 protein. We thank Bezia Lemma for help with kinesin-14 experiments.

Supplementary material

Supplementary material is available at PNAS Nexus online.

Funding

This work was primary supported by the Department of Energy (DOE) DE-SC0022291. Biochemical portion of this work was supported by the Brandeis Center for Bioinspired Soft Materials, an NSF MRSEC (DMR-2011846). We also acknowledge the use of a MRSEC optical and biosynthesis facility supported by NSF-MRSEC-2011846, the use of the NRI-MCDB Microscopy Facility at UCSB supported by NSF-MRI grant 1625770.

Authors' contribution

L.M.L. and Z.D. conceived the experiments; L.M.L. and T.D.R. conducted experiments; M.V. and A.B. created the hydrodynamic model; L.M.L. and M.V. performed data analysis; M.T., A.B. and Z.D supervised the project; all authors wrote and reviewed the manuscript.

Preprints

A preprint of this article is published at <https://arxiv.org/abs/2209.06277>.

Data availability

Data is available from <https://doi.org/10.5061/dryad.83bk3j9vh>.

References

- 1 Saadaoui M, Rocancourt D, Roussel J, Corson F, Gros J. 2020. A tensile ring drives tissue flows to shape the gastrulating amniote embryo. *Science*. 367:453–458.
- 2 Martin AC, Gelbart M, Fernandez-Gonzalez R, Kaschube M, Wieschaus EF. 2010. Integration of contractile forces during tissue invagination. *J Cell Biol*. 188:735–749.
- 3 Behrmdt M, et al. 2012. Forces driving epithelial spreading in zebrafish gastrulation. *Science*. 338:257–260.
- 4 Eournay R, et al. 2015. Interplay of cell dynamics and epithelial tension during morphogenesis of the drosophila pupal wing. *eLife*. 4:e07090.
- 5 Mitchell NP, et al. 2022. Visceral organ morphogenesis via calcium-patterned muscle constrictions. *eLife*. 11:e77355.
- 6 Nerurkar NL, Lee C, Mahadevan L, Tabin CJ. 2019. Molecular control of macroscopic forces drives formation of the vertebrate hindgut. *Nature*. 565:480–484.
- 7 Needleman D, Dogic Z. 2017. Active matter at the interface between materials science and cell biology. *Nat Rev Mater*. 2:17048.
- 8 Marchetti MC, et al. 2013. Hydrodynamics of soft active matter. *Rev Mod Phys*. 85:1143–1189.
- 9 Nédélec FJ, Surrey T, Maggs AC, Leibler S. 1997. Self-organization of microtubules and motors. *Nature*. 389:305–308.
- 10 Schaller V, Weber C, Semmrich C, Frey E, Bausch AR. 2010. Polar patterns of driven filaments. *Nature*. 467:73–77.
- 11 Sanchez T, Chen DTN, DeCamp SJ, Heymann M, Dogic Z. 2012. Spontaneous motion in hierarchically assembled active matter. *Nature*. 491:431–434.

- 12 Palacci J, Sacanna S, Steinberg AP, Pine DJ, Chaikin PM. 2013. Living crystals of light-activated colloidal surfers. *Science*. 339: 936–940.
- 13 Dell'Arciprete D, et al. 2018. A growing bacterial colony in two dimensions as an active nematic. *Nat Commun*. 9:4190.
- 14 Soni V, et al. 2019. The odd free surface flows of a colloidal chiral fluid. *Nat Phys*. 15:1188–1194.
- 15 Wu KT, et al. 2017. Transition from turbulent to coherent flows in confined three-dimensional active fluids. *Science*. 355:eaal1979.
- 16 Guillamat P, Ignés-Mullol J, Sagués F. 2016. Control of active liquid crystals with a magnetic field. *Proc Natl Acad Sci USA*. 113: 5498–5502.
- 17 Wioland H, Woodhouse FG, Dunkel J, Kessler JO, Goldstein RE. 2013. Confinement stabilizes a bacterial suspension into a spiral vortex. *Phys Rev Lett*. 110:268102.
- 18 Nishiguchi D, Aranson IS, Snezhko A, Sokolov A. 2018. Engineering bacterial vortex lattice via direct laser lithography. *Nat Commun*. 9:1–8.
- 19 Discher DE, Janmey P, Wang YL. 2005. Tissue cells feel and respond to the stiffness of their substrate. *Science*. 310:1139–1143.
- 20 Vizsnyiczai G, et al. 2017. Light controlled 3D micromotors powered by bacteria. *Nat Commun*. 8:15974.
- 21 Frangipane G, et al. 2018. Dynamic density shaping of photokinetic *E. coli*. *eLife*. 7:36608.
- 22 Arlt J, Martinez VA, Dawson A, Pilizota T, Poon WCK. 2018. Painting with light-powered bacteria. *Nat Commun*. 9:768.
- 23 Aubret A, Youssef M, Sacanna S, Palacci J. 2018. Targeted assembly and synchronization of self-spinning microgears. *Nat Phys*. 14:1114–1118.
- 24 Ross TD, et al. 2019. Controlling organization and forces in active matter through optically defined boundaries. *Nature*. 572: 224–229.
- 25 Zhang R, et al. 2021. Spatiotemporal control of liquid crystal structure and dynamics through activity patterning. *Nat Mater*. 20:875–882.
- 26 Qu Z, et al. 2021. Persistent fluid flows defined by active matter boundaries. *Commun Phys*. 4:198.
- 27 Lemma LM, et al. 2021. Multiscale microtubule dynamics in active nematics. *Phys Rev Lett*. 127:148001.
- 28 Chandrakar P, et al. 2022. Engineering stability, longevity, and miscibility of microtubule-based active fluids. *Soft Matter*. 18: 1825–1835.
- 29 Thorn KS, Ubersax JA, Vale RD. 2000. Engineering the processive run length of the kinesin motor. *J Cell Biol*. 151:1093–1100.
- 30 Yildiz A, Tomishige M, Vale RD, Selvin PR. 2004. Kinesin walks hand-over-hand. *Science*. 303:676–678.
- 31 Tayar AM, Hagan MF, Dogic Z. 2021. Active liquid crystals powered by force-sensing DNA-motor clusters. *Proc Natl Acad Sci USA*. 118:e2102873118.
- 32 Berliner E, Young EC, Anderson K, Mahtani HK, Gelles J. 1995. Failure of a single-headed kinesin to track parallel to microtubule protofilaments. *Nature*. 373:718–721.
- 33 Hancock WO, Howard J. 1998. Processivity of the motor protein kinesin requires two heads. *J Cell Biol*. 140:1395–1405.
- 34 Furuta K, et al. 2013. Measuring collective transport by defined numbers of processive and nonprocessive kinesin motors. *Proc Natl Acad Sci USA*. 110:501–506.
- 35 Sedlak SM, Schendel LC, Gaub HE, Bernardi RC. 2020. Streptavidin/biotin: tethering geometry defines unbinding mechanics. *Sci Adv*. 6:5999.
- 36 Guntas G, et al. 2015. Engineering an improved light-induced dimer (iLID) for controlling the localization and activity of signaling proteins. *Proc Natl Acad Sci USA*. 112:112–117.
- 37 Thielicke W, Stamhuis E. 2014. PIVlab—towards user-friendly, affordable and accurate digital particle image velocimetry in matlab. *J Open Res Softw*. 2:e30.
- 38 Salomon M, Christie JM, Knieb E, Lempert U, Briggs WR. 2000. Photochemical and mutational analysis of the *fmn*-binding domains of the plant blue light receptor, phototropin. *Biochemistry*. 39:9401–9410.
- 39 Simha RA, Ramaswamy S. 2002. Hydrodynamic fluctuations and instabilities in ordered suspensions of self-propelled particles. *Phys Rev Lett*. 89:058101.
- 40 Sokolov A, Mozaffari A, Zhang R, de Pablo JJ, Snezhko A. 2019. Emergence of radial tree of bend stripes in active nematics. *Phys Rev X*. 9:031014.
- 41 Martínez-Prat B, Ignés-Mullol J, Casademunt J, Sagués F. 2019. Selection mechanism at the onset of active turbulence. *Nat Phys*. 15:362–366.
- 42 Chandrakar P, et al. 2020. Confinement controls the bend instability of three-dimensional active liquid crystals. *Phys Rev Lett*. 125:257801.
- 43 Hallett RA, Zimmerman SP, Yumerefendi H, Bear JE, Kuhlman B. 2016. Correlating in vitro and in vivo activities of light-inducible dimers: a cellular optogenetics guide. *ACS Synth Biol*. 5:53–64.
- 44 Gao T, Blackwell R, Glaser MA, Betterton MD, Shelley MJ. 2015. Multiscale polar theory of microtubule and motor-protein assemblies. *Phys Rev Lett*. 114:048101.
- 45 Braun M, Lansky Z, Hilitski F, Dogic Z, Diez S. 2016. Entropic forces drive contraction of cytoskeletal networks. *BioEssays*. 38: 474–481.
- 46 Foster PJ, Furthauer S, Shelley MJ, Needleman DJ. 2015. Active contraction of microtubule networks. *eLife*. 4:e10837.
- 47 Kumar N, Zhang R, de Pablo JJ, Gardel ML. 2018. Tunable structure and dynamics of active liquid crystals. *Sci Adv*. 4:eaat7779.
- 48 Mizuno D, Tardin C, Schmidt CF, MacKintosh FC. 2007. Nonequilibrium mechanics of active cytoskeletal networks. *Science*. 315:370–373.
- 49 Hentrich C, Surrey T. 2010. Microtubule organization by the antagonistic mitotic motors kinesin-5 and kinesin-14. *J Cell Biol*. 189:465–480.
- 50 Walczak CE, Verma S, Mitchison TJ. 1997. XCTK2: a kinesin-related protein that promotes mitotic spindle assembly in *xenopus laevis* egg extracts. *J Cell Biol*. 136:859–870.
- 51 Cai S, Weaver LN, Ems-McClung SC, Walczak CE. 2009. Kinesin-14 family proteins HSET/XCTK2 control spindle length by cross-linking and sliding microtubules. *Mol Biol Cell*. 20: 1348–1359.
- 52 Fürthauer S, et al. 2019. Self-straining of actively crosslinked microtubule networks. *Nat Phys*. 15:1295–1300.
- 53 Gagnon DA, et al. 2020. Shear-induced gelation of self-yielding active networks. *Phys Rev Lett*. 125:178003.
- 54 Sarfati G, Maitra A, Voituriez R, Galas JC, Estevez-Torres A. 2022. Crosslinking and depletion determine spatial instabilities in cytoskeletal active matter. *Soft Matter*. 18:3793–3800.
- 55 Najma B, et al. 2022. Competing instabilities reveal how to rationally design and control active crosslinked gels. *Nat Commun*. 13: 6465.
- 56 Norton MM, Grover P, Hagan MF, Fraden S. 2020. Optimal control of active nematics. *Phys Rev Lett*. 125:178005.
- 57 Adkins R, et al. 2022. Dynamics of active liquid interfaces. *Science*. 377:768–772.
- 58 Broedersz CP, MacKintosh FC. 2014. Modeling semiflexible polymer networks. *Rev Mod Phys*. 86:995–1036.