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Cortical microstructural associations with CSF amyloid and pTau

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Diffusion MRI (dMRI) can be used to probe microstructural properties of brain tissue and holds great promise as a means to non-invasively map Alzheimer's disease (AD) pathology. Few studies have evaluated multi-shell dMRI models such as neurite orientation dispersion and density imaging (NODDI) and mean apparent propagator (MAP)-MRI in cortical gray matter where many of the earliest histopathological changes occur in AD. Here, we investigated the relationship between CSF pTau₁₈₁ and Aβ₁₋₄₂ burden and regional cortical NODDI and MAP-MRI indices in 46 cognitively unimpaired individuals, 18 with mild cognitive impairment, and two with dementia (mean age: 71.8 ± 6.2 years) from the Alzheimer's Disease Neuroimaging Initiative. We compared findings to more conventional cortical thickness measures. Lower CSF Aβ₁₋₄₂ and higher pTau₁₈₁ were associated with cortical dMRI measures reflecting less hindered or restricted diffusion and greater diffusivity. Cortical dMRI measures, but not cortical thickness measures, were more widely associated with Aβ₁₋₄₂ than pTau₁₈₁ and better distinguished Aβ+ from Aβ- participants than pTau+ from pTau- participants. dMRI associations mediated the relationship between CSF markers and delayed logical memory performance, commonly impaired in early AD. dMRI metrics sensitive to early AD pathogenesis and microstructural damage may be better measures of subtle neurodegeneration in comparison to standard cortical thickness and help to elucidate mechanisms underlying cognitive decline.

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INTRODUCTION

The AT(N) classification paradigm for defining Alzheimer's disease (AD) is based on biomarkers of β-amyloid deposition (A), pathologic tau (T), and neurodegeneration (N) [1]. The primary pathological characteristics of AD – abnormal amyloid (Aβ) plaque and tau neurofibrillary tangle (NFT) deposition – typically precede neurodegeneration and the onset of clinical symptoms by many years. According to the original Braak and Braak model [2, 3], Aβ is initially found within the neocortex and subsequently progresses to the allocortex and additional brain regions. By contrast, tau is first found in the locus coeruleus, trans-entorhinal and entorhinal regions, and then spreads to the hippocampus, temporal cortex, and the remaining neocortex, ultimately resulting in neuronal dysfunction, apoptosis and/or necrosis, and neurodegeneration.

Diffusion MRI (dMRI) is a non-invasive variant of standard MRI that is sensitive to subtle changes in brain cyto- and myelo-architecture. dMRI can be used to probe regional microstructural properties of brain tissue, not detectable with standard anatomical MRI, and holds great promise as a means to map AD histopathology in vivo. Most studies use single-shell diffusion tensor imaging (DTI) to evaluate white matter (WM) microstructure because of the relatively short dMRI acquisition time needed to robustly fit DTI compared to other dMRI models. However, studies have increasingly shown that DTI is also a valuable technique to study microstructural properties of gray matter (GM)

and may be valuable to study early Aβ and tau cortical deposition along the AD continuum [4]. Compared to WM, GM microarchitecture is more complex and less well organized, affecting the accuracy and complicating biological interpretations of many dMRI models including DTI. Multi-shell dMRI protocols can be used to model non-coherent neurite organization (e.g., crossing fibers) and restricted diffusion (e.g., intracellular diffusion) and may further aid in probing cortical GM microstructure.

The neurite orientation dispersion and density imaging (NODDI) [5] model is a three-compartment model that attempts to separate signal contributions from intracellular and extracellular tissue compartments in the WM. NODDI in GM is more controversial due to numerous model assumptions and parameters that were based on WM. For example, without extremely rigorous dMRI acquisitions (i.e., very high b-values and short diffusion times), NODDI cannot separate diffusion signals from the intra- and extra-cellular space when the cell membrane is unmyelinated, as in cell bodies [6]. However, certain NODDI parameters can be tuned for GM (e.g., diffusivity values) [7] to improve the precision of GM model estimates. NODDI in the GM has previously revealed cortical microstructural alterations in individuals with amyloid and tau pathology, prior to detectable changes in cortical thickness [8]. Other multi-shell dMRI models that aim to accurately recover the sources of the diffusion signal, such as mean apparent propagator (MAP)-MRI [9], impose minimal

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model assumptions. Such methods may be more sensitive to cellular and non-cellular barriers in the cortex and therefore earlier microstructural damage, but their relationship with AD CSF biomarkers has not yet been assessed.

Decreases in cerebral spinal fluid (CSF) concentrations of β -amyloid and increases in phosphorylated tau (pTau) are well-established biomarkers that can aid in AD diagnosis [10]. As A β aggregates into fibrils and is sequestered into plaques in the brain, a lower amount is able to diffuse into the CSF; conversely, an increase in intracellular pTau and tangle pathology, possibly triggered by A β aggregation in the brain, is associated with an increase in CSF pTau. Two studies have identified associations between CSF biomarkers and either single-shell DTI and 'free water' (another single-shell diffusivity measure) or multi-shell NODDI cortical measures in samples of cognitively unimpaired participants [8, 11]. As each dMRI model has known limitations, examining effects across numerous diffusion models may help to identify metrics that can be derived from clinically practical dMRI sequences to study cognitive impairment and AD.

In this study, we evaluated the effect of CSF phosphorylated tau 181 (pTau₁₈₁) and β -amyloid 1-42 (A β ₁₋₄₂) burden, as well as their ratio, on cortical NODDI and MAP-MRI microstructural measures in largely preclinical, cognitively unimpaired (69.7% CU) or mildly cognitively impaired (27.3% MCI) participants from the Alzheimer's Disease Neuroimaging Initiative (ADNI). We tuned NODDI parameters to assess both intra- and extra-cellular NODDI volume fractions in the GM and compared findings to multi-shell MAP-MRI measures. We hypothesized that while NODDI would offer greater pathological specificity, MAP-MRI would be more sensitive to overall effects. For comparison, we also examined more conventional single-shell DTI indices and cortical thickness, the most commonly used measure of GM damage beyond hippocampal volume. We then determined whether cortical MRI measures link CSF biomarkers to cognitive function. Understanding how various dMRI measures of brain microstructure relate to CSF A β and tau pathology may help to improve current AD models and provide further insight into mechanisms underlying cognitive decline.

MATERIALS AND METHODS

Participants

MRI, CSF, clinical diagnosis, demographic, and cognitive measures were downloaded from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database (<https://ida.loni.usc.edu/>). ADNI was launched in 2003, initially as a 5-year public-private partnership to assess and optimize biomarkers for clinical trials in Alzheimer's disease. In its third phase, ADNI-3 includes a multi-shell dMRI protocol in a subset of participants, making it possible to fit advanced diffusion models. Across all ADNI, a total of 70 participants were identified with both multi-shell diffusion MRI and CSF biomarker data available; CSF and multi-shell dMRI availability were the only criteria for study inclusion. Four participants were excluded after dMRI quality assurance (three CU and one dementia): one field of view was cropped and the remaining three had artifacts that were not corrected with the preprocessing pipeline described below. Data were analyzed from 66 remaining participants who ranged in age from 60 to 90 years (mean age: 71.8 \pm 6.2 years; 25 male, 41 female; Table 1); all but four participants identified as non-Hispanic White. 46 participants were cognitively unimpaired (CU), 18 were diagnosed with mild cognitive impairment (MCI), and two were diagnosed with dementia [12]. Institutional review boards at participating institutions approved all study procedures, and informed written consent was obtained from all participants.

Biomarker Assessments

Elecsys cerebrospinal fluid (CSF) immunoassay A β ₁₋₄₂ and pTau₁₈₁ estimates were downloaded from the ADNI database. Values outside the measuring range were set to the respective assay's limit and included in the analysis. Based on the thresholds proposed by Hansson et al. [13] and Blennow et al. [14], pathological CSF A β ₁₋₄₂ was defined as A β ₁₋₄₂ \leq 977 pg/ml, pathological pTau₁₈₁ was defined as pTau₁₈₁ > 24 pg/ml, and pTau₁₈₁/A β ₁₋₄₂ was defined as pTau₁₈₁/A β ₁₋₄₂ > 0.025 (Table 1).

Cognitive Assessments

Here we focused on a measure of delayed memory that is sensitive to neuropathological changes in the early stages of AD. The Wechsler Memory Scale-Revised (WMS-R) [15] delayed logical memory was used to index cognitive performance; total scores were used as the primary outcome measures.

Supplementary analyses also evaluated more general cognitive composite scores developed by the Alzheimer's Disease Sequencing Project Phenotype Harmonization Consortium (ADSP-PHC), a large-scale effort to harmonize and co-calibrate cognitive domain scores across multiple studies of cognitive aging [16]. Available ADNI3 ADSP-PHC cognitive domain scores included memory, executive function, language, and visuospatial functioning (Supplementary Table 12).

ADNI3 MRI Protocol

Subjects with multi-shell diffusion MRI underwent whole-brain MRI scanning on 3T Siemens Advanced Prisma scanners at 10 acquisition sites across North America. Anatomical 3D T1-weighted (T1w) MPRAGE sequences (256 \times 256 matrix; voxel size = 1.0 \times 1.0 \times 1.0 mm; TI = 900 ms; TR = 2300 ms; TE = 2.98 ms; flip angle = 9°), and multi-shell multiband dMRI (116 \times 116 matrix; voxel size: 2 \times 2 \times 2 mm; TR = 3400 ms; δ = 13.6 ms, Δ = 35.0 ms scan time = 7.25 min) were collected. 127 separate images were acquired for each dMRI scan: 13 b0 images, 6 b = 500 s/mm², 48 b = 1000 s/mm² and 60 b = 2000 s/mm² diffusion-weighted images (DWI). The diffusion time (t_d), the time between the first and second diffusion gradients, was 30.5 ms.

Image Processing

Cortical regions of interest (ROIs) were defined on T1w images using the Desikan Killiany atlas [17]. Raw T1w images were first denoised using ANTS non-local means [18] and further processed using the FreeSurfer version 7.1 pipeline [19]. FreeSurfer cortical segmentations were visually inspected for accuracy and manually corrected using control points.

Raw DWI were denoised using the DIPY LPCA filter [20, 21] and corrected for Gibbs ringing artifacts with MRtrix [22]. A synthetic undistorted b0 was created using Synb0-DISCO [23] and used for FSL's *topup* distortion correction [24]. Eddy correction was performed with FSL's *eddy* tool [25] including *repol* outlier replacement [26] and slice timing correction [27]. DWI then underwent B1 field inhomogeneity corrections [28].

Participants' DWI were warped to their respective T1w image to further correct EPI-induced susceptibility artifacts and to place both modalities into the same coordinate space. First, corrected b0 images were linearly aligned to processed T1w images using a FreeSurfer derived white matter mask for FSL's *flirt* boundary-based registration (BBR) [29]. To avoid any single diffusion derived map driving the coregistration, ANTs multi-channel non-linear registration was used to warp each participant's DWI to their respective T1w [30, 31]; three equally weighted channels were used for registration: the average b0 image, DTI FA, and DTI MD [32]. The linear and non-linear registrations were concatenated and used to correct the DWI for EPI distortions in their native space with only one interpolation. Finally, the DWI underwent a multi-tissue intensity normalization using MRtrix *mtnormalize* [33].

After processing, DWI still suffered from susceptibility artifact hyperintensities particularly in the temporal lobes. DKI [34] is highly sensitive to noise artifacts and can produce implausible negative kurtosis values in affected regions [35, 36]. To automatically identify DWI regions with remaining artifacts, DKI was fitted with DIPY and a mask was created from voxels where mean kurtosis (MK) values were \leq 0 (Supplementary Fig. 1). These voxels were removed from further analysis.

Diffusion MRI Models and Scalar Indices Evaluated

Mean Apparent Propagator (MAP)-MRI. MAP-MRI was fitted to the data using Laplacian-regularization with DIPY [9, 37]. Five resulting MAP-MRI measures were evaluated: 1) mean square displacement (MSD), a measure of how far protons are able to diffuse on average during the diffusion time; 2) return-to-origin probability (RTOP), the probability that a proton will be at the same position at the first and second diffusion gradient pulse; 3) return-to-axis probability (RTAP), the probability that a proton will be along the axis of the main eigenvector of a diffusion tensor; 4) return-to-plane probability (RTPP), the probability that a proton will be on the plane perpendicular to the main eigenvector; and 5) *q*-space inverse variance (QIV), a measure of variance in the signal (see Supplementary Table 1 for further metric descriptions).

Table 1. Basic demographic and clinical characteristics of study participants.

	CSF A β or pTau Group				CSF pTau/A β Ratio Group				CSF A β and pTau Group			
	A β +	A β -	pTau+	pTau-	pTau/A β +	pTau/A β -	A β -/pTau-	A β -/pTau+	A β +/pTau-	A β +/pTau+	A β -/pTau-	A β -/pTau+
Total												
N	66	37	22	44	23	43	27	10	17	12	7	7
Age, yrs (SD)	71.8 (6.2)	70.8 (6.7)	72.4 (7.2)	71.5 (5.8)	74.5 (6.2)	70.3 (5.8)	71.1 (6.4)	70.2 (7.8)	72.2 (4.6)	74.2 (6.4)	7	7
Sex, N Male	25	11	10	15	11	14	8	3	7	7	7	7
APOE4^a, N carriers	27	10	11	16	15	12	10	0	2	15	2	2
	N = 63	N = 36	N = 20	N = 43	N = 21	N = 42	N = 26	N = 10	N = 17	N = 10	N = 17	N = 10
Education, yrs (SD)	16.2 (2.6)	16.4 (2.4)	15.2 (2.7)	16.7 (2.4)	15.8 (3.0)	16.4 (2.4)	16.7 (2.4)	15.4 (2.4)	16.7 (2.6)	15.1 (2.9)	16.7 (2.6)	15.1 (2.9)
MMSE (SD)	28.2 (2.4)	27.4 (3.0)	27.6 (3.2)	28.4 (1.9)	27.0 (3.2)	28.8 (1.6)	28.5 (1.8)	29.3 (0.9)	28.2 (2.0)	26.3 (3.8)	28.2 (2.0)	26.3 (3.8)
Delayed Logical Memory (SD)	11.6 (5.7)	10.1 (6.7)	9.8 (6.3)	12.5 (5.1)	8.7 (6.7)	13.1 (4.4)	12.9 (4.1)	12.5 (6.5)	11.8 (6.5)	7.6 (6.5)	11.8 (6.5)	7.6 (6.5)
Clinical Dx, N												
CU	46	17	13	33	11	35	22	7	11	6	7	6
MCI	18	10	7	11	10	8	5	3	6	4	3	4
Dementia	2	0	2	0	2	0	0	0	0	2	0	2
CSF, pg/mL (SD)												
Aβ₁₋₄₂	1104.8 (482.7)	629.4 (211.6)	1013.4 (491.9)	1150.5 (477.0)	594.5 (235.4)	1377.7 (355.6)	1476.5 (253.7)	1479.8 (241.1)	632.6 (206.7)	624.8 (227.7)	1479.8 (241.1)	632.6 (206.7)
pTau₁₈₁	22.4 (9.9)	24.4 (12.4)	32.7 (10.1)	17.2 (3.9)	29.2 (12.3)	18.7 (5.8)	17.5 (3.5)	29.5 (6.9)	16.7 (4.6)	35.4 (11.8)	16.7 (4.6)	35.4 (11.8)
pTau₁₈₁/Aβ₁₋₄₂	0.027 (0.022)	0.044 (0.023)	0.043 (0.025)	0.019 (0.015)	0.052 (0.019)	0.014 (0.004)	0.012 (0.002)	0.021 (0.008)	0.031 (0.018)	0.061 (0.019)	0.031 (0.018)	0.061 (0.019)

There was a significant relationship between continuous CSF biomarker values and clinical diagnosis (A β : $F = 3.8$, $p = 0.03$; pTau: $F = 4.4$, $p = 0.02$; A β /pTau: $F = 9.8$, $p = 0.0002$), but not sex (A β : $F = 3.8$, $p = 0.03$; pTau: $F = 4.4$, $p = 0.02$; A β /pTau: $F = 9.8$, $p = 0.0002$). Age was significantly correlated with CSF pTau ($r = 0.39$, $p = 0.001$) and pTau/A β ($r = 0.30$, $p = 0.01$), but not A β ($r = -0.17$, $p = 0.18$), while MMSE was correlated with A β ($r = 0.34$; $p = 0.006$) and pTau/A β ($r = -0.46$, $p = 0.0001$), but not pTau ($r = -0.17$, $p = 0.18$). Education was only correlated with pTau ($r = -0.26$, $p = 0.04$), not A β ($r = -0.17$, $p = 0.18$) or pTau/A β ($r = -0.18$, $p = 0.15$). There was no significant relationship between dichotomized CSF A β and pTau subgroup (i.e., A β -/pTau-, A β -/pTau+, A β +/pTau-, A β +/pTau+) and clinical diagnosis ($\chi^2 = 11.6$, $p = 0.07$), sex ($\chi^2 = 3.3$, $p = 0.35$), or age ($F = 0.96$, $p = 0.42$). However, we found group differences in MMSE ($F = 3.97$, $p = 0.01$).

^a Subset of participants (N) for whom APOE data were available is noted

Neurite Orientation Dispersion and Density Imaging (NODDI). NODDI was fitted with DMIPY [5, 38] using a multi-tissue approach (MT-NODDI) [39, 40]. The original NODDI formulation assumes one tissue response (S_0) across the whole brain. This assumption introduces a systematic bias in estimating tissue compartment volume fractions as different brain tissue types (WM, GM, CSF) have different T2 relaxation times; MT-NODDI incorporates estimates of tissue-specific S_0 for each of the three NODDI compartments [39, 40]. To improve NODDI volume fraction estimates in the cortical GM, the intracellular and the extracellular compartments (ICVF and ECVF) were adjusted by the GM's S_0 , while the isotropic free-water or CSF compartment (ISOVF) was adjusted by the CSF's S_0 . Parallel diffusivity (d_{\parallel}) varies across brain tissue, and Guerrero et al. [7] have shown that the default d_{\parallel} value assumed by NODDI, $1.7 \mu\text{m}^2/\text{ms}$, is too high for the GM. Here, to find the optimal d_{\parallel} value, MT-NODDI was fit with d_{\parallel} values ranging from $0.5\text{--}1.6 \mu\text{m}^2/\text{ms}$ in increments of 0.1 . We then compared the average mean squared error (MSE) between the measured and predicted DWI signals within FreeSurfer derived medial cortical ribbon voxels (as described in the section below) of CU participants to identify the d_{\parallel} with lowest error. Two-sided paired t-tests revealed the MSE found with $d_{\parallel} = 0.8 \mu\text{m}^2/\text{ms}$ was significantly lower than all other d_{\parallel} values evaluated (Supplementary Fig. 2). Our analyses, therefore, used $d_{\parallel} = 0.8 \mu\text{m}^2/\text{ms}$ to model NODDI in the GM.

Diffusion Tensor Imaging (DTI). For comparison with commonly available single-shell measures, we estimated mean diffusivity (MD) using the DTI model. Compared to DTI fractional anisotropy (FA), MD has been shown to be both more sensitive to clinical symptoms and age-associated neurodegeneration, and more appropriate for evaluating brain regions with less coherent organization than WM, such as cortical GM [4, 41–43]. DTI was fitted with FSL's *dtifit* with weighted least squares using only the subset of b_0 and $b = 1000 \text{ s/mm}^2$ volumes.

Cortical Gray Matter Measures. DWI to T1w transformations were applied to 10 dMRI scalar maps to bring them into T1w coordinate space for analysis. To mitigate partial volume effects in FreeSurfer cortical segmentations, a surface was created at the halfway point between the pial and white matter surface, or the FS medial cortical ribbon. Voxels corresponding to noise in dMRI images, identified with a DKI MK value ≤ 0 , were removed from the medial cortical ribbon. For each of the 10 diffusion MRI measures, a robust mean was calculated across the remaining FS medial cortical ribbon voxels within 34 ROIs using an iterative *M*-estimator from the 'WRS2' package in R [44, 45]. To further diminish any partial volume effects and any misregistration between diffusion and structural images, 1) voxels with an ISOVF > 0.5 and 2) voxels with ICVF values in the 1st and 99th percentiles across all participants were excluded from the mean (i.e., voxels in the ribbon that had extreme ICVF values for the sample; Supplementary Fig. 1). We also analyzed an AD signature meta-ROI (AD-metaROI) of cortical regions that are sensitive to early AD consisting of the bilateral inferior parietal, middle temporal, inferior temporal, pre-cuneus, fusiform, and entorhinal regions [46]. In total, we evaluated 35 ROIs – 34 individual ROIs and one AD-metaROI.

Statistical Analyses

Regional Cortical MRI Measure Associations. Mixed effect linear regressions were used to identify associations between cortical ROI dMRI measures and $A\beta_{1-42}$, pTau₁₈₁, pTau₁₈₁/ $A\beta_{1-42}$ CSF biomarkers. The data collection site was used as the random-effects grouping variable, and fixed-effects covariates included age, sex, and years of education. A statistical mixed-effects model harmonization approach was used to account for site effects in lieu of an ROI-level harmonization approach like ComBat [47], as previous comparisons across even more comprehensive sets of the heterogeneous single- and multi-shell ADNI3 dMRI acquisition protocols and sites have shown that ComBat did not improve or change results found with random-effect linear regressions [42, 48]. Regression analyses were conducted with the 'nlme' package in R (version 3.2.3). Effect sizes, after accounting for all covariates, were estimated as standardized β coefficients. The false discovery rate procedure (FDR) [49] was used to correct for multiple comparisons across 1050 tests (35 ROIs * 10 dMRI measures * 3 CSF biomarkers; $q = 0.05$). We used the same model to compare CSF associations with regional FreeSurfer cortical thickness measures (CTh). CTh results were corrected for multiple comparisons using FDR across 105 tests (35 ROIs * 3 CSF biomarkers). CSF biomarkers were modeled as continuous variables for our primary analyses. For comparison, associations with \log_{10} -transformed pTau₁₈₁ were assessed in supplementary analyses.

Secondarily, participants were classified into $A\beta_{1-42}$ and pTau₁₈₁ CSF biomarker groups ('+' or '-'), dichotomized using established pathological thresholds of $A\beta_{1-42} \leq 977 \text{ pg/ml}$ and pTau_{181} > 24 \text{ pg/ml} [13, 14]. Differences in summary AD-metaROI cortical measures between dichotomized $A\beta_{1-42}$ and pTau₁₈₁ groups were tested with an analysis of covariance (ANCOVA) using the same statistical model from our primary analyses. Pairwise tests were subsequently performed to directly compare CSF biomarker groups; dMRI comparisons were FDR corrected for 60 pairwise tests and CTh for 6 tests. We also tested the interactive effects of $A\beta_{1-42}$ and pTau₁₈₁ groups (i.e., '+' or '-') on AD-metaROI cortical measures. Using the same mixed effect model from our primary analyses, we tested associations between each cortical MRI measure and either $A\beta$ -by-pTau group (i.e., continuous $A\beta_{1-42}$ by dichotomized pTau₁₈₁) or pTau-by- $A\beta$ group (i.e., continuous pTau₁₈₁ by dichotomized $A\beta_{1-42}$) interactions. FDR was again used to correct for 20 dMRI or two CTh tests.}

In supplementary analyses, we used the same mixed effect model from our primary analyses to evaluate cortical ROI MRI measure associations with clinical diagnosis; we compared cortical measures between cognitively unimpaired (CU; $N = 46$) and cognitively impaired (CI: MCI or dementia; $N = 20$) participants. Effect sizes for group differences, after accounting for all covariates, were estimated as *d*-values. FDR was used to correct for 350 dMRI tests (35 ROIs * 10 dMRI measures) or 35 CTh tests.

Exploratory Classification of CSF Biomarker Groups by Cortical Measures. As an exploratory analysis, we used mixed effect logistic regressions to determine whether dMRI and CTh AD-metaROI measures could accurately classify participants into $A\beta_{1-42}$, pTau₁₈₁, pTau₁₈₁/ $A\beta_{1-42}$ groups ('+' or '-') dichotomized using established cut-point thresholds [13, 14]. In addition to AD-metaROI measures, site was included in the model as a grouping variable for random-effects regression. To assess performance, the area under the receiver operating characteristics curve (AUC) was calculated using the 'pROC' package in R. FDR was used to correct for 30 dMRI or three cortical thickness tests.

In supplementary analyses, we evaluated classification AUCs of residualized AD-metaROI MRI after adjusting for age, sex, and education. The data were also split into five 80% and 20% train-test subsets and the AUC across the five folds was averaged to assess performance.

Cortical Mediators between CSF Biomarkers and Delayed Memory. We first identified the relationship between CSF $A\beta_{1-42}$, pTau₁₈₁, and pTau₁₈₁/ $A\beta_{1-42}$ load and cognitive performance by computing linear regressions with CSF biomarkers as the independent variable and delayed logical memory performance (WMS-R logical memory) as the dependent variable, after adjusting for fixed-effects (age, sex, education) and random-effects (site) covariates. In supplementary analyses, ADSP-PHC cognitive composite scores were also evaluated. These included scores for memory, executive function (available for $N = 64$ of 66 participants), language ($N = 65$), and visuospatial functioning ($N = 29$).

To better understand the underlying microstructural process by which pathological markers influence cognition, we then completed mediation analyses using the 'mediation' package in R to determine whether AD-metaROI cortical MRI measures (both structural and diffusion) would explain the observed relationships between CSF biomarkers and cognitive measures; we used the same covariate structure (Supplementary Fig. 3). Per convention, mediation analyses were performed only for AD-metaROI cortical measures that were significantly associated with CSF biomarkers in the primary analyses.

RESULTS

Participant demographics

Basic demographic and clinical characteristics of study participants are reported in Table 1. There was a significant relationship between continuous CSF biomarker values and clinical diagnosis ($A\beta$: $F = 3.8$ $p = 0.03$; pTau: $F = 4.4$ $p = 0.02$; $A\beta$ /pTau: $F = 9.8$ $p = 0.0002$), but no relationship between dichotomized CSF $A\beta$ and pTau subgroup (i.e., $A\beta$ -/pTau-, $A\beta$ -/pTau+, $A\beta$ +/pTau-, $A\beta$ +/pTau+) and clinical diagnosis ($\chi^2 = 11.6$, $p = 0.07$). In addition, clinical characteristics of study participants within each diagnostic group (CU or CI) are reported in Supplementary Table 2, along with regional differences in cortical MRI metrics between groups in Supplementary Table 6 and Supplementary Fig. 9.

Correlations between cortical AD-metaROI MRI measures

Pearson's correlations between cortical AD-metaROI MRI measures revealed that many dMRI measures were highly correlated across participants (Supplementary Fig. 4). The strongest correlations (Pearson's $r > |0.9|$) were found between MAP-MRI MSD, QIV, and DTI MD ($r = 0.92$ – 0.99), and between MAP-MRI RTAP, RTOP, and RTPP ($r = 0.97$ – 0.99); MAP-MRI RTAP, RTOP, and RTPP were negatively correlated with MAP-MRI MSD and DTI MD ($r = -0.9$ to -0.97). NODDI ISOVF was also highly correlated with MAP-MRI MSD and DTI MD ($r = 0.94$), and negatively correlated with MAP-MRI RTPP ($r = -0.94$). These dMRI measures remained correlated in the subset of CU and A β^- participants, however CTh was notably less correlated with dMRI measures in this subset (Supplementary Fig. 4).

Primary CSF biomarker associations with regional cortical MRI measures

For each CSF and MRI measure, the number of cortical ROIs in which a significant association was detected after multiple comparisons correction (dMRI $p \leq 0.012$; CTh $p \leq 0.0056$) and the direction of associations are reported in Supplementary Table 3.

At least one ROI was associated with A β_{1-42} across nine out of the 10 dMRI measures evaluated; only ECVF measures were not associated. The largest and most widespread negative associations were detected with QIV (16 ROIs) and ISOVF (15 ROIs) in largely the same temporal and frontal ROIs; MD also showed associations in a similar subset of ROIs (13 ROIs; Fig. 1). The largest effects were detected with QIV in the *pars opercularis*, *pars triangularis* and insular cortex ($\beta = -0.39$), followed by the parahippocampal and entorhinal cortex ($\beta = -0.38$). ICVF was significant in 14 regions but, in addition to frontal and temporal regions, included more parietal cortex associations (largest $\beta = 0.34$ in supramarginal gyrus). The fewest associations were detected with ODI, RTAP, and RTOP; however, one of the largest overall effects was detected with ODI in the supramarginal gyrus ($\beta = -0.38$).

Fewer dMRI measures were associated with pTau₁₈₁ than with A β_{1-42} , but overall effect sizes were larger (Fig. 2). The largest and most widespread negative associations were detected with ECVF (7 ROIs), followed by positive associations with ISOVF (6 ROIs) and QIV (5 ROIs) in largely frontal and parietal regions. No other dMRI measures were associated with pTau₁₈₁. The greatest overall effects were detected in the paracentral gyrus (ECVF $\beta = -0.47$; ISOVF $\beta = 0.40$). Similar associations were found when testing log₁₀-transformed pTau₁₈₁ (Supplementary Results 2.4).

More widespread associations were detected with pTau₁₈₁/A β_{1-42} across all 10 dMRI measures compared to A β_{1-42} or pTau₁₈₁ alone (Fig. 3). The most widespread positive associations were detected with ISOVF (29 ROIs) and MD (24 ROIs). The largest dMRI effects were detected with QIV in the entorhinal cortex ($\beta = 0.51$), parahippocampal gyrus, and *pars orbitalis* ($\beta = 0.49$). As with A β_{1-42} , the fewest associations were detected with RTAP, RTOP, ECVF, and ODI.

Significant associations between CTh and both A β_{1-42} and pTau₁₈₁/A β_{1-42} were more localized compared to the widespread associations detected with cortical dMRI measures; comparable numbers of dMRI and CTh associations were detected with pTau₁₈₁ (7 ROIs) but not log₁₀-transformed pTau₁₈₁ (3 ROIs; Supplementary Results 2.4). CTh was only associated with A β_{1-42} in the entorhinal cortex ($\beta = 0.33$). Across all MRI measures evaluated, however, the largest pTau₁₈₁ and pTau₁₈₁/A β_{1-42} associations were detected with CTh in the superior parietal ($\beta = -0.49$) and entorhinal ($\beta = -0.59$) cortex, respectively.

In sensitivity analyses, associations between CSF and cortical MRI measures that were significant in the entire cohort were tested in individuals without dementia (i.e., 64 of 66 participants). 98.5% of significant associations remained significant (Supplementary Results 2.5).

Secondary AD-metaROI MRI measure comparisons between CSF biomarker groups

Across all cortical AD-metaROI measures, ANCOVA revealed significant group differences between four dichotomized (+/-) A β_{1-42} and pTau₁₈₁ groups (dMRI $p \leq 0.041$; CTh $p \leq 0.0002$; Fig. 4A, B). In pairwise comparisons, all dMRI measures other than RTOP, RTAP, and ECVF were nominally different between A β^- /pTau- and A β^+ /pTau+ individuals ($p < 0.05$). ISOVF, ICVF, and QIV were nominally different between those A β^- /pTau+ and A β^+ /pTau+; QIV was also different between A β^- /pTau- and A β^+ /pTau- individuals. Only CTh differences between A β^+ /pTau+ and the other three groups remained significant after multiple comparisons correction. Overall, there was no detectable difference between pTau- and pTau+; only CTh within A β^+ individuals was significantly different between pTau- and pTau+.

While underpowered for statistical comparisons (N as low as 2 to 6 participants per group), further breakdown of biomarker groups by clinical diagnosis suggests that dMRI effects may be driven by A β^+ participants with MCI or dementia, regardless of pTau status (Supplementary Figs. 10–11).

Effect of CSF biomarker interactions on AD-metaROI measures

There were no significant associations between CSF A β_{1-42} -by-pTau₁₈₁ group (i.e., continuous A β_{1-42} by dichotomized pTau₁₈₁) interactions and dMRI AD-metaROI measures. However, a significant A β_{1-42} -by-pTau₁₈₁ group interaction was found on CTh ($\beta = 0.64$; $p = 0.0051$) whereby lower CSF A β_{1-42} was associated with lower CTh only in those individuals who were pTau+ (Supplementary Fig. 12). No significant CSF pTau₁₈₁-by-A β_{1-42} group (i.e., continuous pTau₁₈₁ by dichotomized A β_{1-42}) interactions were detected for any AD-metaROI MRI measure (Supplementary Fig. 13).

Exploratory classification of CSF biomarker groups by cortical MRI measures

As reported in Fig. 4B and Supplementary Table 7, except for ECVF, dMRI AD-metaROI measures better distinguished A β^+ from A β^- participants than CTh did (dMRI AUC = 0.74–0.82; CTh AUC = 0.73); QIV performed best (AUC = 0.82) while MD, ICVF, RTPP, and MSD performed within 0.05 of QIV (AUC = 0.77–0.79). In contrast, only CTh significantly classified pTau₁₈₁ positivity (AUC = 0.67). While all MRI measures were significant, pTau₁₈₁/A β_{1-42} positivity was also best classified by QIV (AUC = 0.92) with comparable performance (i.e., within 0.05) by ICVF, ISOVF and MD (AUC = 0.87–0.88). Similar classification trends were found 1) in the subset of participants without dementia, 2) when AD-metaROI MRI measures were first residualized (i.e., adjusted for age, sex, and education), and 3) with five-fold cross-validation using 80/20 training/test splits (Supplementary Results 2.9).

Cortical MRI mediators between CSF biomarker and delayed memory

Lower CSF A β_{1-42} was associated with poorer delayed memory performance ($p = 0.01$; $\beta = 0.30$), as hypothesized. In previous analyses, A β_{1-42} was significantly associated with QIV, ICVF, and ODI AD-metaROI measures (Fig. 1). The effect of A β_{1-42} on memory was fully mediated by ICVF (33% of the total effect) and QIV (41%; Table 2).

Greater pTau₁₈₁/A β_{1-42} was also associated with poorer delayed memory performance ($p = 5.9 \times 10^{-5}$; $\beta = -0.50$). CSF pTau₁₈₁/A β_{1-42} was significantly associated with CTh and all AD-metaROI measures except ODI and ECVF (Fig. 3). Each of the seven dMRI AD-metaROI measures was found to partially mediate the effect of pTau₁₈₁/A β_{1-42} on delayed memory (~17–28% of the total effect). CTh did not have a mediating effect (Table 2).

We did not find significant associations between CSF pTau₁₈₁ ($p = 0.22$) or log₁₀-transformed pTau₁₈₁ ($p = 0.08$) and delayed memory.

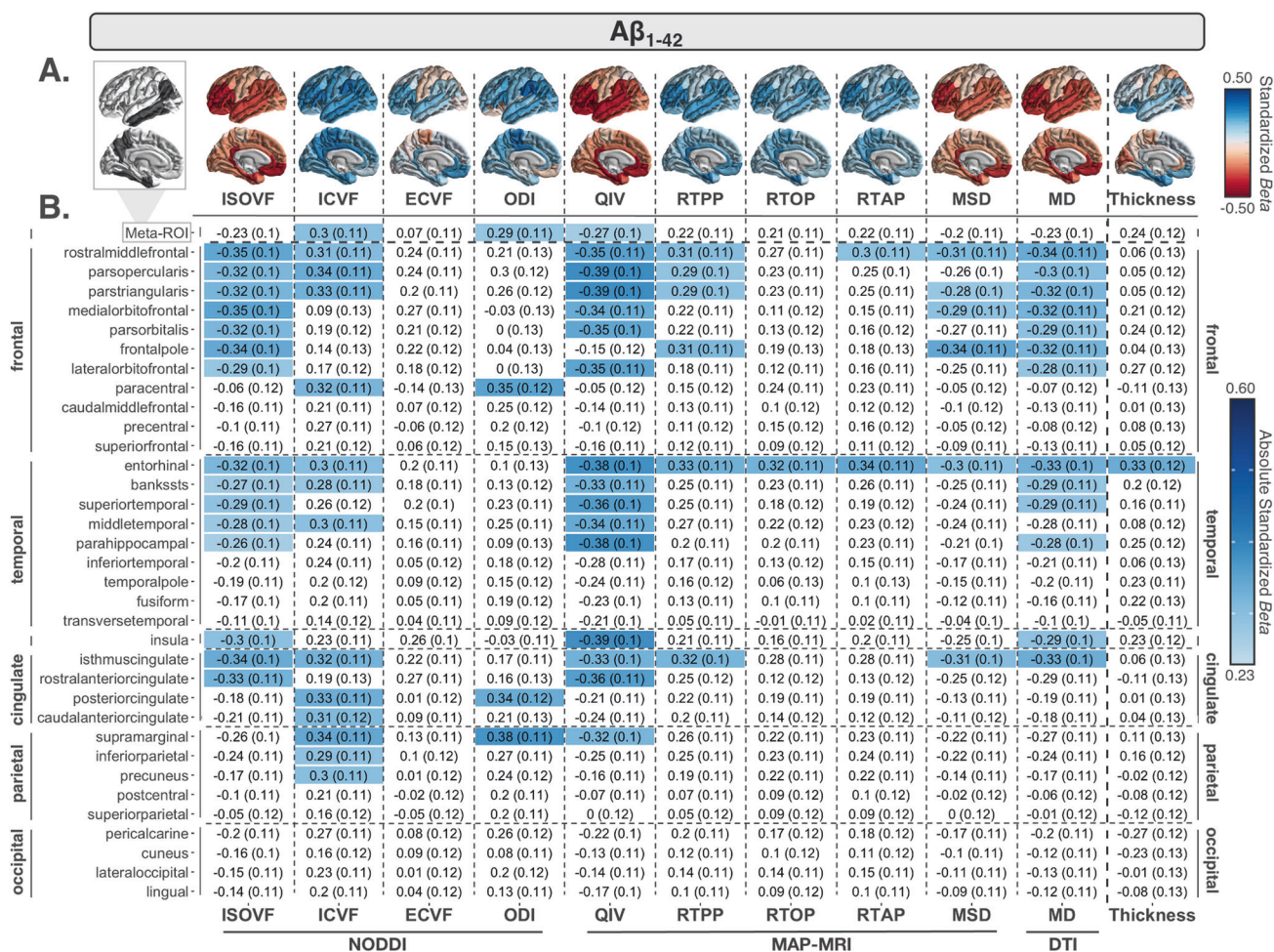


Fig. 1 CSF $A\beta_{1-42}$ associations with cortical MRI measures. **A** Regional effect sizes ($Beta$ -values) for associations between CSF $A\beta_{1-42}$ and each cortical measure across participants. For reference, the ROIs comprising the AD-metaROI are highlighted in gray (top left). **B** $Beta$ -values and standard errors for significant associations (dMRI $p \leq 0.012$; CTh $p \leq 0.0056$) are shaded according to the absolute value of their effect size.

Mediation results from sensitivity analyses excluding two individuals with dementia revealed similar results to those in the whole sample (Supplementary Table 11). Supplementary mediation analyses of harmonized composite cognitive domains from the ADSP-PHC can be found in Supplementary Results 2.11. Briefly, effects of $A\beta_{1-42}$ ($p = 0.03$; $\beta = 0.23$), \log_{10} -transformed $p\text{Tau}_{181}$ ($p = 0.03$; $\beta = -0.27$), and $p\text{Tau}_{181}/A\beta_{1-42}$ ($p = 0.0015$; $\beta = -0.37$) on composite memory scores were fully mediated only by QIV (41.7% of the total effect), CTh (64.1%), and ISOVF (36.9%) respectively (Supplementary Table 13). No MRI mediation effects were detected with executive function or language, and no CSF metrics were associated with visuospatial scores.

DISCUSSION

In this study, we investigated the relationship between regional microstructural dMRI measures in cortical gray matter and CSF $A\beta$ and $p\text{Tau}$ in a population of largely cognitively unimpaired and MCI individuals from the third phase of the Alzheimer's Disease Neuroimaging Initiative. We found that lower CSF $A\beta$ and higher CSF $p\text{Tau}$ were associated with cortical DTI, NODDI, and MAP-MRI dMRI measures reflecting less hindered or restricted diffusion (i.e., lower RTAP, RTOP, RTPP, ICVF) and greater diffusivity (i.e., higher MD, MSD, QIV, ECVF, ISOVF). Cortical dMRI measures were more widely associated with $A\beta$ than $p\text{Tau}$ and better distinguished $A\beta+$ from $A\beta-$ participants. In contrast, cortical thickness was more tightly linked with $p\text{Tau}$. dMRI associations mediated the

relationship between CSF markers and performance on delayed logical memory tasks, which is vulnerable to AD pathogenesis.

CSF $A\beta$ associations with cortical MRI measures

Cortical dMRI measures were widely associated with CSF $A\beta$ concentrations, particularly in AD vulnerable regions such as the entorhinal, isthmus cingulate, and frontal cortex. These extensive associations are consistent with patterns of both amyloid PET tracer uptake [50–52] and post-mortem amyloid deposits found throughout the neocortex [53] in early to intermediate disease stages.

Across all dMRI measures, QIV from MAP-MRI showed the most robust associations with CSF $A\beta$ and it best distinguished $A\beta+$ from $A\beta-$ participants. QIV is a general measure of the variance of the diffusion signal, which has been shown to be highly sensitive to the presence of biological barriers in regions with lower restriction and greater isotropic volume fractions values, such as in the cortical ribbon [37]; conversely, RTOP and RTAP (also derived from MAP-MRI) may only be sensitive in regions with extremely high restriction such as the WM. MAP-MRI is fitted to the overall diffusion signal (i.e. from both intra- and extra-cellular compartments) and imposes few assumptions, potentially offering greater sensitivity to amyloid load than multi-compartment models such as NODDI.

In contrast, NODDI parses the signal into intra- and extra-cellular spaces and resulting ICVF, ECVF, and ISOVF measures may be sensitive to different aspects of AD histopathology. Measures

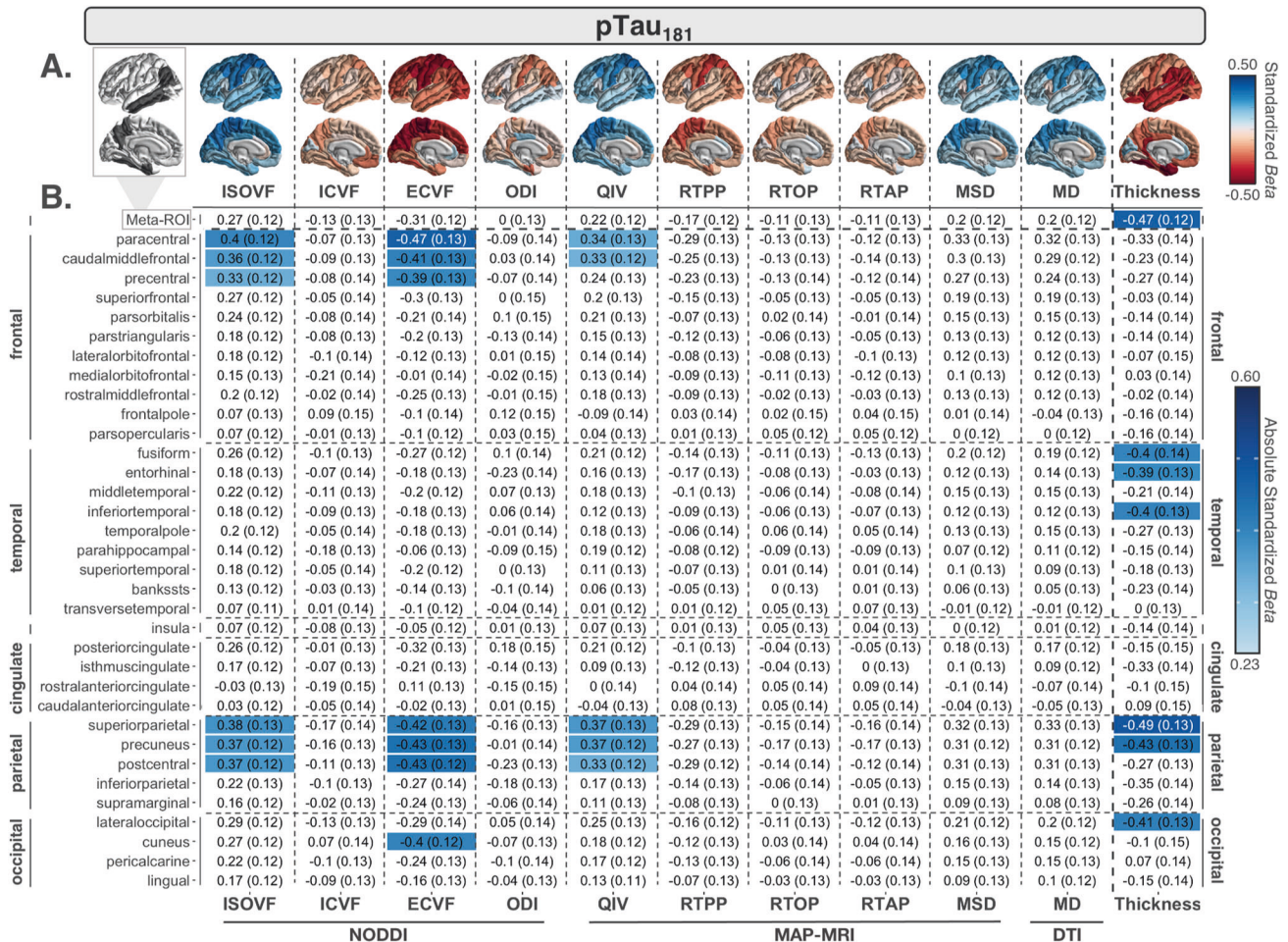


Fig. 2 CSF pTau₁₈₁ associations with cortical MRI measures. **A** Regional effect sizes (*Beta*-values) for associations between CSF pTau₁₈₁ and each cortical measure across participants. For reference, the ROIs comprising the AD-metaROI are highlighted in gray (top left). **B** *Beta*-values and standard errors for significant associations (dMRI $p \leq 0.012$; CTh $p \leq 0.0056$) are shaded according to the absolute value of their effect size.

reflecting lower diffusion restriction (i.e., lower ICVF) may reflect loss of cortical neurites, while lower ODI (also derived from NODDI) may be associated with lower complexity in dendritic arborization. Greater ISOVF or free-water volume could be a function of both neurodegeneration and greater inflammation-associated edema [54–56]. Inflammation plays a substantial role in AD pathogenesis [57]. Persistent immune response in the brain is not only associated with neurodegeneration but exacerbates A β and tau pathology and may even link initial A β pathology to subsequent NFT development [58].

ICVF and ISOVF also showed spatially distinct patterns of associations with amyloid; while ICVF associations were strongest in fronto-temporal regions, ISOVF associations also included parietal regions. Among regions that were selectively associated with each measure, the largest effect size differences between ICVF and ISOVF amyloid associations were found in either the earliest or latest myelinating regions of the neocortex: ISOVF showed larger effects in medial orbitofrontal cortex (late/lightly myelinated), while ICVF showed larger effects in paracentral cortex (early/heavily myelinated; Supplementary Fig. 17). These measures may capture the proposed inverse relationship between the pattern of pathology progression and myelination during development [59, 60]. Selective associations between ISOVF and amyloid in late myelinating regions that are vulnerable to early pathogenesis could reflect more advanced degeneration in these regions. However, it is also possible that compared to ICVF, ISOVF is a better suited metric for regions that simply lack sufficient

myelin. NODDI may fail to properly estimate measures of restriction in unmyelinated tissue [61].

Although amyloid plaques are formed in the extracellular space, we found no associations between CSF A β and ECVF. This may be partially due to the dMRI acquisition parameters used in ADNI, where the diffusion time is $t_d = 30.5$ ms and the maximum b -value is $b = 2000$ s/mm². When dMRI sequences do not have sufficiently short diffusion times ($t_d \leq 20$ ms) and high b -values ($b > 3000$ s/mm²), the NODDI model is unable to differentiate the extracellular space from permeable cell bodies due to water exchange between these compartments [6]; the ECVF measurement therefore loses the specificity touted by biophysical models. Sequences with such advanced parameters can be used to fit models such as soma and neurite density imaging (SANDI) [62], which can also estimate cell body size and density. These sequences can currently only be acquired on one of the few existing ultra-high gradient strength Connectome scanners [62, 63], and are not currently feasible for large-scale multisite clinical studies of neurodegenerative disorders.

Our results, however, support the use of measures derived from common single-shell sequences, such as DTI MD, for associations with CSF amyloid. We found both MD regional associations and classification performance were comparable to multi-shell ISOVF. While multi-shell ISOVF and single shell MD gave similar patterns of results, ISOVF and other multi-shell metrics like QIV and ICVF often showed larger effect sizes or spatially distinct patterns of CSF associations (including supplementary comparisons between

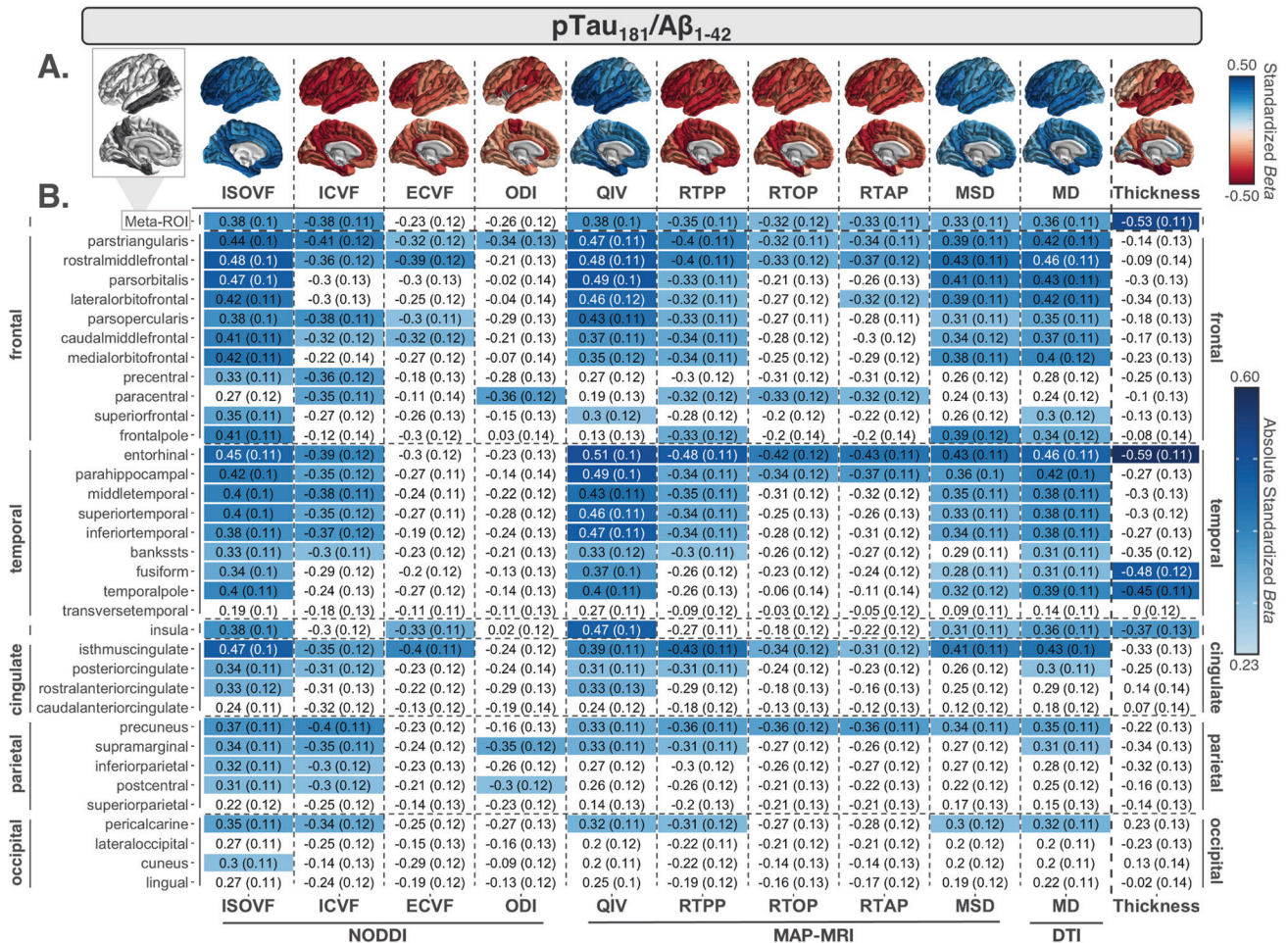


Fig. 3 CSF pTau₁₈₁/Aβ₁₋₄₂ associations with cortical MRI measures. **A** Regional effect sizes (Beta-values) for associations between CSF pTau₁₈₁/Aβ₁₋₄₂ and each cortical measure across participants. Effect sizes are shown regardless of P-value. For reference, the ROIs comprising the AD-metaROI are highlighted in gray (top left). **B** Beta-values and standard errors for significant associations (dMRI $p \leq 0.012$; CTH $p \leq 0.0056$) are shaded according to the absolute value of their effect size.

CU and CI participants). This suggests multi-shell measures may still offer sensitivity and specificity beyond DTI MD. We note that higher MD and ISOVF measures may be particularly confounded by exacerbated partial volume effects in the presence of cortical atrophy; however, we mitigated these effects by excluding voxels with ISOVF > 0.5 from all mean cortical dMRI measures [64]. In fact, AD-metaROI MD and ISOVF were more tightly correlated with ICVF than cortical thickness, suggesting they capture microstructural phenomena beyond the partial voluming that can be attributable to atrophy.

In contrast to dMRI measures, cortical thickness was only associated with amyloid in the entorhinal cortex. Aβ biomarker abnormalities are thought to precede tau and neurodegeneration in many proposed models of the AD pathological cascade. T1w macrostructural measures, such as cortical thickness, are the most frequently used biomarkers of neurodegeneration, however our results support evidence that changes in microstructural dMRI measures can precede those detectable with T1w MRI and may be more suitable for detecting early cortical Aβ pathology.

CSF pTau associations with cortical MRI measures

Compared to amyloid, dMRI measures showed fewer regional associations with CSF pTau, albeit larger effect sizes. These effects were restricted to frontal and parietal regions implicated in later Braak stages, Braak 5-6. This aligns with our exploratory

comparisons between CSF biomarker groups which show that pTau effects appear to be driven only by Aβ+ individuals (N = 12), particularly those with MCI or dementia (N = 6; Supplementary Figs. 10-11), suggesting a later disease stage. These preliminary comparisons are highly limited by the number of individuals in each group, which could also explain the limited number of regional pTau associations detected in our study.

Counterintuitively, given the evidence showing intracellular pTau accumulation that results in cell body NFTs, the most robust dMRI effects detected were lower ECVF. Although the specific mechanisms are unknown, accumulation and aggregation of pTau in the intracellular space (i.e., cell body), in conjunction with extracellular pathology (e.g., amyloid plaques, inflammatory cytokines, ghost tangles) may together create enough barriers to hinder diffusion captured by ECVF. Since cell death occurs heterogeneously in the cortex, the lack of ICVF associations could be driven by opposing effects of intracellular pTau aggregation in some cells increasing restriction (i.e., increased ICVF) and the death of other cells decreasing restriction (i.e., decreasing ICVF). The observed association between higher ISOVF with greater pTau in late Braak regions could be the result of a greater degree of neuronal loss in later stages. As one of the first studies examining these effects, the mechanisms driving our findings are still unknown; however, increases in both cortical ICVF and ISOVF have been previously reported in studies of human tauopathy mouse models (rTg4510) [65].

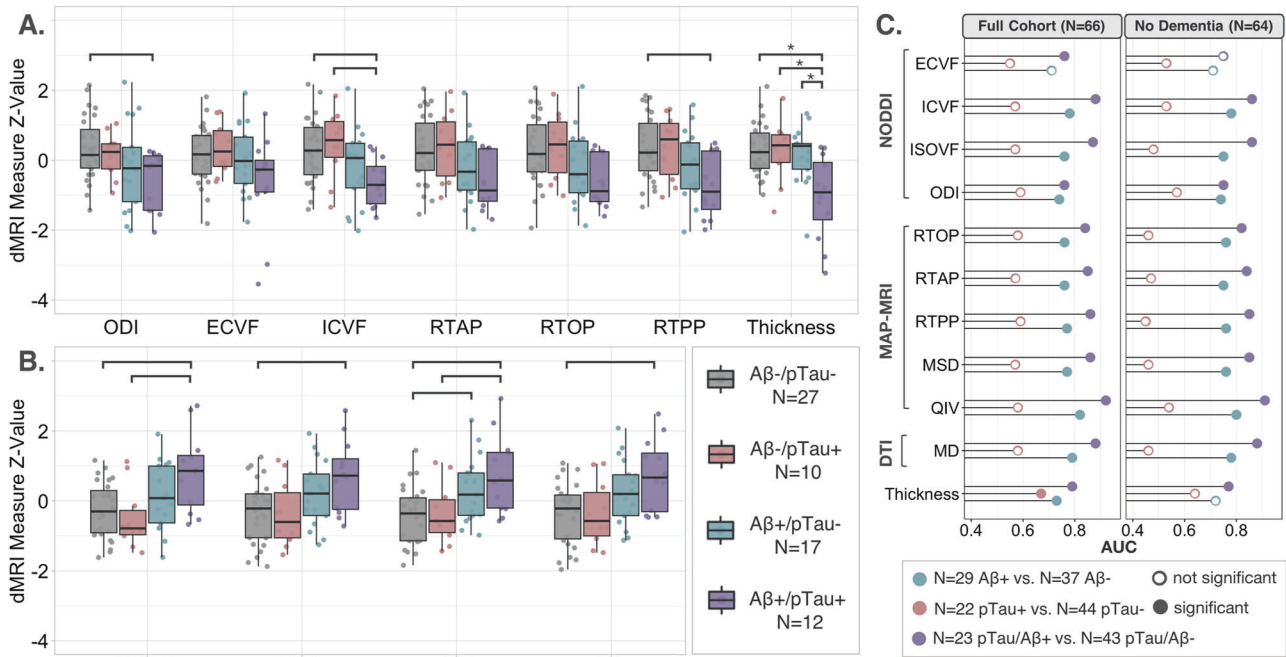


Fig. 4 CSF biomarker cut-point group differences. Scaled cortical AD-metaROI measures grouped by CSF biomarker cut-points show (A) lower MT-NODDI ODI, ECVF, ICVF, MAP-MRI RTAP, RTOP, RTPP, and FreeSurfer CTh and (B) higher MT-NODDI ISOVF, MAP-MRI MSD, QIV, and DTI MD in $A\beta^+$ compared to $A\beta^-$ individuals. The greatest differences are visible between those $A\beta^-/p\text{Tau}^-$ and those $A\beta^+/p\text{Tau}^+$; within $A\beta^-$ individuals, no major differences are seen between $p\text{Tau}^-$ and $p\text{Tau}^+$ individuals. Nominal group differences ($p < 0.05$) are denoted with brackets; only CTh $A\beta^+/p\text{Tau}^+$ differences were significant after multiple comparisons correction, as denoted with asterisks. C For each cortical AD-metaROI measure, the area under the curve (AUC) for each dichotomized CSF group classification is reported. Significant associations after multiple comparisons correction are indicated by filled circles (Full cohort: dMRI $p \leq 0.021$, CTh $p \leq 0.016$; No Dementia: dMRI $p \leq 0.029$, CTh $p \leq 0.0036$).

Higher $p\text{Tau}$ was most strongly associated with lower cortical thickness in the superior parietal cortex and metaROI. Early *Braak 1-4* temporal and metaROI $p\text{Tau}$ associations were only detected with cortical thickness, perhaps suggesting more advanced atrophy in regions with earlier involvement. Medial temporal tau increases with age and does not necessarily indicate AD pathology [66]. In contrast, significant $p\text{Tau}$ associations in the latest *Braak 6* regions, including postcentral, paracentral, cuneus, and precentral cortex, were only detected with microstructural dMRI measures, which may capture earlier stages of degeneration. Larger studies will allow for event-based modeling to estimate the sequence in which these cortical biomarkers become abnormal [67]. This approach can be used to help build an understanding of the dynamics of not only typical disease progression, but also to identify distinct spatiotemporal trajectories of tau subtypes [68].

CSF $p\text{Tau}/A\beta$ associations with cortical MRI measures

As expected, we found the largest overall associations between cortical MRI measures and CSF $p\text{Tau}/A\beta$. Cortical measures also better classified dichotomized CSF ratios than individual $A\beta$ or $p\text{Tau}$ measures. While most of the associations between imaging and CSF ratios aligned with results when examining $A\beta$ and $p\text{Tau}$ separately, MAP-MRI measure associations were more widespread than those observed using the measures individually, consistent with studies showing better diagnostic accuracy of CSF biomarkers when analyzed together [69, 70].

Cortical MRI mediators between CSF biomarker and delayed memory

While both CSF $A\beta$ and $p\text{Tau}/A\beta$ were associated with delayed memory, $p\text{Tau}/A\beta$ had larger effects. This supports the large body of literature showing that amyloid burden does not correlate well with clinical severity and that both amyloid and tau are necessary

for cognitive decline [71, 72]. We found that dMRI measures mediated a larger proportion of $A\beta$ effects (up to 41%) than $p\text{Tau}/A\beta$ (up to 28%), in line with the limited direct relationship between amyloid and cognitive outcomes compared to tau. Amyloid may drive downstream cognitive impairment through microstructural damage. Interestingly, only dMRI measures mediated the relationship between $p\text{Tau}/A\beta$ and memory while cortical thickness did not. Given that the sample was largely cognitively unimpaired, this aligns with our findings that dMRI measures are more sensitive to earlier pathological changes such as amyloid deposition.

There is a large body of literature showing that $p\text{Tau}$ is more tightly linked with neurodegeneration and clinical severity than $A\beta$, however we did not find significant associations between CSF $p\text{Tau}$ and WMS-R delayed logical memory. This may be due in part to the limited number of participants in our study, particularly those with high $p\text{Tau}$ concentrations. As shown in Supplementary Fig. 18 two CU individuals (one $A\beta^+$ and one $A\beta^-$) with high delayed memory scores and high $p\text{Tau}$ were sufficient to drive the association (or lack thereof). Supplementary analyses of more general ADSP-PHC composite memory scores, however, did reveal a significant relationship with $p\text{Tau}$; in agreement with published findings, cortical thickness mediated a large proportion of this effect (64%).

Comparison to other studies

Several AD dMRI studies of preclinical, asymptomatic individuals have suggested a non-monotonic or biphasic relationship between AD pathology and dMRI measures of brain microstructure [4], including two studies specifically evaluating associations between CSF amyloid and tau biomarkers and either 1) single-shell free-water and DTI MD [11], or 2) multi-shell NODDI ICVF and ODI cortical measures [8]. An early transient stage of increased diffusion restriction or lower diffusivity followed by a later phase of lower restriction and increased diffusivity has been identified in

Table 2. Cortical AD-metaROI MRI mediators between CSF markers and delayed logical memory.

CSF	MRI Model	Cortical Mediator	Direct Effect		Mediation Effect		%
			β	P	β	P	
$A\beta$ $p = 0.01$ $\beta = 0.30$	MT-NODDI	ICVF	0.21	0.078	0.10	0.014**	32.7
		ODI	0.28	0.026**	0.02	0.592	6.4
	MAP-MRI	QIV	0.17	0.14	0.12	0.008**	41.2
$p\text{Tau}/A\beta$ $p = 5.9 \times 10^{-5}$ $\beta = -0.50$	MT-NODDI	ICVF	-0.40	<2 × 10^{-16**}	-0.10	0.036**	19.8
		ISOVF	-0.36	0.004**	-0.14	0.008**	27.6
	MAP-MRI	MSD	-0.38	<2 × 10^{-16**}	-0.12	0.012**	22.1
		QIV	-0.34	0.006**	-0.13	0.01**	27.2
		RTAP	-0.40	<2 × 10^{-16**}	-0.10	0.014**	20.2
		RTOP	-0.42	<2 × 10^{-16**}	-0.09	0.026**	17.4
	DTI	MD	-0.36	0.004**	-0.12	0.01**	25.8
		FreeSurfer	CTh	-0.37	0.006**	-0.11	0.12

Only AD-metaROI measures associated with $A\beta_{1-42}$ or $p\text{Tau}_{181}/A\beta_{1-42}$ in primary analyses were evaluated; we corrected for multiple comparisons across 12 mediation tests. The *direct effect* reflects the effect of CSF on delayed memory. The *mediation effect* reflects the effect of CSF on memory that goes through the cortical MRI mediator. Effect sizes (β), uncorrected p -values, and the percent of the total CSF effect on memory (direct + indirect) that was mediated are reported.

** $p < \text{FDR Threshold for 12 tests; Direct } p \leq 0.026; \text{ Mediation } p \leq 0.036$

dMRI studies of both GM [73] and WM [74, 75]. These studies propose that lower diffusivity associations with greater amyloid burden, measured with CSF or PET, in the earliest stages could be attributable to factors such as cellular hypertrophy or inflammatory microglia infiltration and proliferation increasing the number of diffusion barriers. Subsequent associations showing higher diffusivity with greater amyloid load may be driven by cellular loss and neurodegeneration. Our findings in a mix of largely CU and MCI participants are in line with the second part of this trajectory. Future work evaluating a larger sample of CU participants is needed to isolate earlier signatures. As CSF changes may occur before changes in the brain are detectable with PET, using both data types would further allow for the examination of the earliest diffusion trajectories in CSF+/PET- participants.

Limitations and future directions

There are several limitations to this study. First, the small number of ADNI participants with multi-shell dMRI and CSF data limited our ability to parse specific neuroimaging patterns within each diagnostic and biomarker group. Second, ADNI is a predominantly non-Hispanic White cohort and there is a need to establish the generalizability of our findings to diverse communities. Third, the ADNI3 dMRI acquisition does not support the standard NODDI modeling assumptions in the GM, therefore, additional studies are also needed across heterogeneous dMRI acquisitions (i.e., higher b -values/shorter diffusion times) to replicate these findings. Our results may be considered preliminary until replicated in additional larger, independent cohorts. Fourth, while our mediation models were based on theoretical models of causality, we cannot infer a causal relationship given the cross-sectional dataset. Future work will investigate this relationship using a longitudinal design. Finally, our "AD signature" metaROI was based on cortical thickness associations with Braak neurofibrillary tangle stage at autopsy [46], potentially biasing our classification and mediation analyses. There may be a need to define meta-ROIs based on associations between dMRI measures and amyloid.

CONCLUSIONS

Understanding the relationship between various dMRI measures of brain microstructure and amyloid and tau pathology may

improve upon current AD models and provide further insight into mechanisms underlying cognitive decline. Diffusion MRI metrics, calculated across multiple models, may better track amyloid progression through non-invasive means compared to cortical thickness, the most commonly used measure of cortical damage.

DATA AVAILABILITY

Data used in this study, including MRI, CSF, clinical diagnosis, demographic, and cognitive measures, are available through the Alzheimer's Disease Neuroimaging Initiative (ADNI) database (<https://ida.loni.usc.edu/>).

REFERENCES

- Jack CR Jr., Bennett DA, Blennow K, Carrillo MC, Dunn B, Haeberlein SB, et al. NIA-AA research framework: toward a biological definition of Alzheimer's disease. *Alzheimers Dement.* 2018;14:535–62.
- Braak H, Braak E. Neuropathological staging of Alzheimer-related changes. *Acta Neuropathol.* 1991;82:239–59.
- Braak H, Braak E. Evolution of neuronal changes in the course of Alzheimer's disease. *J Neural Transm Suppl.* 1998;53:127–40.
- Weston PS, Simpson IJ, Ryan NS, Ourselin S, Fox NC. Diffusion imaging changes in grey matter in Alzheimer's disease: a potential marker of early neurodegeneration. *Alzheimers Res Ther.* 2015;7:47.
- Zhang H, Schneider T, Wheeler-Kingshott CA, Alexander DC. NODDI: practical in vivo neurite orientation dispersion and density imaging of the human brain. *Neuroimage.* 2012;61:1000–16.
- Jelescu IO, Budde MD. Design and Validation of Diffusion MRI Models of White Matter. *Front Phys.* 2017;5:61.
- Guerrero JM, Adluru N, Bendlin BB, Goldsmith HH, Schaefer SM, Davidson RJ, et al. Optimizing the intrinsic parallel diffusivity in NODDI: An extensive empirical evaluation. *PLoS One.* 2019;14:e0217118.
- Vogt NM, Hunt JFV, Adluru N, Ma Y, Van Hulle CA, Ili DCD, et al. Interaction of amyloid and tau on cortical microstructure in cognitively unimpaired adults. *Alzheimers Dement.* 2022;18:65–76.
- Ozarslan E, Koay CG, Shepherd TM, Komlos ME, Irfanoglu MO, Pierpaoli C, et al. Mean apparent propagator (MAP) MRI: a novel diffusion imaging method for mapping tissue microstructure. *Neuroimage.* 2013;78:16–32.
- Olsson B, Lautner R, Andreasson U, Ohrfelt A, Portelius E, Bjerke M, et al. CSF and blood biomarkers for the diagnosis of Alzheimer's disease: a systematic review and meta-analysis. *Lancet Neurol.* 2016;15:673–84.
- Montal V, Vilaplana E, Alcolea D, Pegueroles J, Pasternak O, Gonzalez-Ortiz S, et al. Cortical microstructural changes along the Alzheimer's disease continuum. *Alzheimers Dement.* 2018;14:340–51.

12. Petersen RC, Aisen PS, Beckett LA, Donohue MC, Gamst AC, Harvey DJ, et al. Alzheimer's Disease Neuroimaging Initiative (ADNI): clinical characterization. *Neurology*. 2010;74:201–9.
13. Hansson O, Seibyl J, Stomrud E, Zetterberg H, Trojanowski JQ, Bittner T, et al. CSF biomarkers of Alzheimer's disease concord with amyloid- β PET and predict clinical progression: A study of fully automated immunoassays in BioFINDER and ADNI cohorts. *Alzheimer's Dement*. 2018;14:1470–81.
14. Blennow K, Shaw LM, Stomrud E, Mattsson N, Toledo JB, Buck K, et al. Predicting clinical decline and conversion to Alzheimer's disease or dementia using novel Elecsys Abeta(1–42), pTau and tTau CSF immunoassays. *Sci Rep*. 2019;9:19024.
15. Wechsler D. *WMS-R: Wechsler Memory Scale-Revised* : Manual: Psychological Corporation; 1987.
16. Mukherjee S, Choi SE, Lee ML, Scollard P, Trittschuh EH, Mez J, et al. Cognitive domain harmonization and cocibration in studies of older adults. *Neuropsychology*. 2023;37:409–23.
17. Desikan RS, Segonne F, Fischl B, Quinn BT, Dickerson BC, Blacker D, et al. An automated labeling system for subdividing the human cerebral cortex on MRI scans into gyral based regions of interest. *Neuroimage*. 2006;31:968–80.
18. Manjon JV, Coupe P, Marti-Bonmati L, Collins DL, Robles M. Adaptive non-local means denoising of MR images with spatially varying noise levels. *J Magn Reson Imaging*. 2010;31:192–203.
19. Fischl B. *FreeSurfer*. *Neuroimage*. 2012;62:774–81.
20. Manjón JV, Coupé P, Concha L, Buades A, Collins DL, Robles M. Diffusion weighted image denoising using overcomplete local PCA. *PLoS One*. 2013;8:e73021.
21. Garyfallidis E, Brett M, Amirbekian B, Rokem A, van der Walt S, Descoteaux M, et al. Dipy, a library for the analysis of diffusion MRI data. *Front Neuroinform*. 2014;8:8.
22. Kellner E, Dhital B, Kiselev VG, Reiser M. Gibbs-ringing artifact removal based on local subvoxel-shifts. *Magn Reson Med*. 2016;76:1574–81.
23. Schilling KG, Blaber J, Huo Y, Newton A, Hansen C, Nath V, et al. Synthesized b0 for diffusion distortion correction (Symb0-DisCo). *Magn Reson Imaging*. 2019;64:62–70.
24. Andersson JL, Skare S, Ashburner J. How to correct susceptibility distortions in spin-echo echo-planar images: application to diffusion tensor imaging. *Neuroimage*. 2003;20:870–88.
25. Andersson JLR, Sotiropoulos SN. An integrated approach to correction for off-resonance effects and subject movement in diffusion MR imaging. *Neuroimage*. 2016;125:1063–78.
26. Andersson JLR, Graham MS, Zsoldos E, Sotiropoulos SN. Incorporating outlier detection and replacement into a non-parametric framework for movement and distortion correction of diffusion MR images. *Neuroimage*. 2016;141:556–72.
27. Andersson JLR, Graham MS, Drobnjak I, Zhang H, Filippini N, Bastiani M. Towards a comprehensive framework for movement and distortion correction of diffusion MR images: Within volume movement. *Neuroimage*. 2017;152:450–66.
28. Tustison NJ, Avants BB, Cook PA, Zheng Y, Egan A, Yushkevich PA, et al. N4ITK: improved N3 bias correction. *IEEE Trans Med Imaging*. 2010;29:1310–20.
29. Greve DN, Fischl B. Accurate and robust brain image alignment using boundary-based registration. *Neuroimage*. 2009;48:63–72.
30. Avants BB, Epstein CL, Grossman M, Gee JC. Symmetric diffeomorphic image registration with cross-correlation: evaluating automated labeling of elderly and neurodegenerative brain. *Med Image Anal*. 2008;12:26–41.
31. Avants BB, Tustison NJ, Song C, Cook PA, Klein A, Gee JC. A reproducible evaluation of ANTs similarity metric performance in brain image registration. *Neuroimage*. 2011;54:2033–44.
32. Basser PJ, Mattiello J, LeBihan D. MR diffusion tensor spectroscopy and imaging. *Biophys J*. 1994;66:259–67.
33. Raffelt D, Dhillon T, Tournier J-D, Tabbara R, Smith R, Pierre E, et al. Bias Field Correction and Intensity Normalisation for Quantitative Analysis of Apparent Fibre Density 2017.
34. Jensen JH, Helpert JA, Ramani A, Lu H, Kaczynski K. Diffusional kurtosis imaging: the quantification of non-gaussian water diffusion by means of magnetic resonance imaging. *Magn Reson Med*. 2005;53:1432–40.
35. Henriques RN, editor *Advanced Methods for Diffusion MRI Data Analysis and their Application to the Healthy Ageing Brain* 2018.
36. Hutchinson EB, Avram AV, Irfanoglu MO, Koay CG, Barnett AS, Komlos ME, et al. Analysis of the effects of noise, DWI sampling, and value of assumed parameters in diffusion MRI models. *Magn Reson Med*. 2017;78:1767–80.
37. Fick RHJ, Wassermann D, Caruyer E, Deriche R. MAPL: Tissue microstructure estimation using Laplacian-regularized MAP-MRI and its application to HCP data. *Neuroimage*. 2016;134:365–85.
38. Fick RHJ, Wassermann D, Deriche R. The Dmipy Toolbox: Diffusion MRI Multi-Compartment Modeling and Microstructure Recovery Made Easy. *Front Neuroinform*. 2019;13:64.
39. Frigo M, Fick RHJ, Zucchelli M, Deslauriers-Gauthier S, Deriche R. Multi-Tissue Multi-Compartment Models of Diffusion MRI. *bioRxiv*. 2021.2021.01.29.428843. <https://www.biorxiv.org/content/10.1101/2021.01.29.428843v1.full>.
40. Jeurissen B, Tournier JD, Dhollander T, Connelly A, Sijbers J. Multi-tissue constrained spherical deconvolution for improved analysis of multi-shell diffusion MRI data. *Neuroimage*. 2014;103:411–26.
41. Salminen LE, Conturo TE, Laidlaw DH, Cabeen RP, Akbudak E, Lane EM, et al. Regional age differences in gray matter diffusivity among healthy older adults. *Brain Imaging Behav*. 2016;10:203–11.
42. Zavaliangos-Petropulu A, Nir TM, Thomopoulos SI, Reid RI, Bernstein MA, Borowski B, et al. Diffusion MRI Indices and Their Relation to Cognitive Impairment in Brain Aging: The Updated Multi-protocol Approach in ADNI3. *Front Neuroinform*. 2019;13:2.
43. Vogt NM, Hunt JF, Adluru N, Dean DC, Johnson SC, Asthana S, et al. Cortical Microstructural Alterations in Mild Cognitive Impairment and Alzheimer's Disease Dementia. *Cereb cortex (N. Y., NY : 1991)*. 2020;30:2948–60.
44. Wilcox R. Chapter 3 - Estimating Measures of Location and Scale. In: Wilcox R, editor. *Introduction to Robust Estimation and Hypothesis Testing (Third Edition)*. Boston: Academic Press; 2012. p. 43-101.
45. Mair P, Wilcox R. Robust statistical methods in R using the WRS2 package. *Behav Res Methods*. 2020;52:464–88.
46. Schwarz CG, Gunter JL, Wiste HJ, Przybelski SA, Weigand SD, Ward CP, et al. A large-scale comparison of cortical thickness and volume methods for measuring Alzheimer's disease severity. *Neuroimage Clin*. 2016;11:802–12.
47. Fortin JP, Parker D, Tunc B, Watanabe T, Elliott MA, Ruparel K, et al. Harmonization of multi-site diffusion tensor imaging data. *Neuroimage*. 2017;161:149–70.
48. Thomopoulos SI, Nir TM, Villalon-Reina JE, Zavaliangos-Petropulu A, Maiti P, Zheng H, et al. editors. Diffusion MRI metrics and their relation to dementia severity: effects of harmonization approaches. *Symposium on Medical Information Processing and Analysis*; 2021 p. 14. <https://www.spiedigitallibrary.org/conference-proceedings-of-spie/12088/2606337/Diffusion-MRI-metrics-and-their-relation-to-dementia-severity/10.1117/12.2606337.short?SSO=1>.
49. Benjamini Y, Hochberg Y. Controlling the false discovery rate: a practical and powerful approach to multiple testing. *J R Stat Soc Series B Stat Methodol* 1995; 289–300.
50. Grothe MJ, Barthel H, Sepulcre J, Dyrba M, Sabri O, Teipel SJ, et al. In vivo staging of regional amyloid deposition. *Neurology*. 2017;89:2031–8.
51. Mattsson N, Palmqvist S, Stomrud E, Vogel J, Hansson O. Staging beta-Amyloid Pathology With Amyloid Positron Emission Tomography. *JAMA Neurol*. 2019;76:1319–29.
52. Meyer PF, McSweeney M, Gonneaud J, Villeneuve S. AD molecular: PET amyloid imaging across the Alzheimer's disease spectrum: From disease mechanisms to prevention. *Prog Mol Biol Transl Sci*. 2019;165:63–106.
53. Thal DR, Rub U, Orantes M, Braak H. Phases of A beta-deposition in the human brain and its relevance for the development of AD. *Neurology*. 2002;58:1791–800.
54. Di Biase MA, Zalesky A, Cetin-Karayumak S, Rath Y, Lv J, Boerigter D, et al. Large-Scale Evidence for an Association Between Peripheral Inflammation and White Matter Free Water in Schizophrenia and Healthy Individuals. *Schizophrenia Bull*. 2020;47:542–51.
55. Febo M, Perez PD, Ceballos-Diaz C, Colon-Perez LM, Zeng H, Ofori E, et al. Diffusion magnetic resonance imaging-derived free water detects neurodegenerative pattern induced by interferon-gamma. *Brain Struct Funct*. 2020;225:427–39.
56. Oestreich LKL, O'Sullivan MJ. Transdiagnostic In Vivo Magnetic Resonance Imaging Markers of Neuroinflammation. *Biol Psychiatry Cogn Neurosci Neuroimaging*. 2022;7:638–58.
57. Heneka MT, Carson MJ, El Khoury J, Landreth GE, Brosseron F, Feinstein DL, et al. Neuroinflammation in Alzheimer's disease. *Lancet Neurol*. 2015;14:388–405.
58. Kinney JW, Bemiller SM, Murtishaw AS, Leisgang AM, Salazar AM, Lamb BT. Inflammation as a central mechanism in Alzheimer's disease. *Alzheimers Dement (N. Y.)*. 2018;4:575–90.
59. Bartzokis G, Lu PH, Mintz J. Human brain myelination and amyloid beta deposition in Alzheimer's disease. *Alzheimers Dement*. 2007;3:122–5.
60. Braak H, Braak E. Development of Alzheimer-related neurofibrillary changes in the neocortex inversely recapitulates cortical myelogenesis. *Acta Neuropathol*. 1996;92:197–201.
61. Jelescu IO, de Skowronski A, Geffroy F, Palombo M, Novikov DS. Neurite Exchange Imaging (NEXI): A minimal model of diffusion in gray matter with inter-compartment water exchange. *Neuroimage*. 2022;256:119277.
62. Palombo M, Ianus A, Guerreri M, Nunes D, Alexander DC, Shemesh N, et al. SANDI: A compartment-based model for non-invasive apparent soma and neurite imaging by diffusion MRI. *Neuroimage*. 2020;215:116835.
63. Jones DK, Alexander DC, Bowtell R, Cercignani M, Dell'Acqua F, McHugh DJ, et al. Microstructural imaging of the human brain with a 'super-scanner': 10 key advantages of ultra-strong gradients for diffusion MRI. *Neuroimage*. 2018;182:8–38.
64. Henf J, Grothe MJ, Brueggen K, Teipel S, Dyrba M. Mean diffusivity in cortical gray matter in Alzheimer's disease: The importance of partial volume correction. *Neuroimage Clin*. 2018;17:579–86.

65. Colgan N, Siow B, O'Callaghan JM, Harrison IF, Wells JA, Holmes HE, et al. Application of neurite orientation dispersion and density imaging (NODDI) to a tau pathology model of Alzheimer's disease. *Neuroimage*. 2016;125:739–44.
66. Vemuri P, Lowe VJ, Knopman DS, Senjem ML, Kemp BJ, Schwarz CG, et al. Tau-PET uptake: Regional variation in average SUVR and impact of amyloid deposition. *Alzheimers Dement (Amst)*. 2017;6:21–30.
67. Venkatraghavan V, Bron EE, Niessen WJ, Klein S, Alzheimer's Disease Neuroimaging I. Disease progression timeline estimation for Alzheimer's disease using discriminative event based modeling. *Neuroimage*. 2019;186:518–32.
68. Vogel JW, Young AL, Oxtoby NP, Smith R, Ossenkoppele R, Strandberg OT, et al. Four distinct trajectories of tau deposition identified in Alzheimer's disease. *Nat Med*. 2021;27:871–81.
69. Palmqvist S, Zetterberg H, Mattsson N, Johansson P, Alzheimer's Disease Neuroimaging I, Minthon L, et al. Detailed comparison of amyloid PET and CSF biomarkers for identifying early Alzheimer disease. *Neurology*. 2015;85:1240–9.
70. Dubois B, Feldman HH, Jacova C, Hampel H, Molinuevo JL, Blennow K, et al. Advancing research diagnostic criteria for Alzheimer's disease: the IWG-2 criteria. *Lancet Neurol*. 2014;13:614–29.
71. Desikan RS, McEvoy LK, Thompson WK, Holland D, Brewer JB, Aisen PS, et al. Amyloid-beta-associated clinical decline occurs only in the presence of elevated P-tau. *Arch Neurol*. 2012;69:709–13.
72. Desikan RS, McEvoy LK, Thompson WK, Holland D, Roddey JC, Blennow K, et al. Amyloid-beta associated volume loss occurs only in the presence of phospho-tau. *Ann Neurol*. 2011;70:657–61.
73. Fortea J, Sala-Llonch R, Bartsch-Faz D, Bosch B, Llado A, Bargallo N, et al. Increased cortical thickness and caudate volume precede atrophy in PSEN1 mutation carriers. *J Alzheimers Dis*. 2010;22:909–22.
74. Dong JW, Jelescu IO, Ades-Aron B, Novikov DS, Friedman K, Babb JS, et al. Diffusion MRI biomarkers of white matter microstructure vary nonmonotonically with increasing cerebral amyloid deposition. *Neurobiol Aging*. 2020;89:118–28.
75. Racine AM, Adluru N, Alexander AL, Christian BT, Okonkwo OC, Oh J, et al. Associations between white matter microstructure and amyloid burden in pre-clinical Alzheimer's disease: A multimodal imaging investigation. *NeuroImage Clin*. 2014;4:604–14.

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AUTHOR CONTRIBUTIONS

TMN, JVR, and NJ conceived and designed the analysis. TMN, EH, HZ, NJ, and SIT curated, processed, and analyzed the data. PMT and NJ acquired funding and supervised. CRJ and MWW were involved in project administration and provided study resources. TMN and LES wrote the first draft of the manuscript. All authors critically reviewed and edited the manuscript and approved the final content of the manuscript.

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COMPETING INTERESTS

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